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OPEN Cardiac magnetic resonance patterns of left ventricular remodeling in patients with severe aortic stenosis referred to surgical aortic valve replacement

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Left ventricular (LV) hypertrophy is a common finding in patients with severe aortic stenosis (AS). Cardiac magnetic resonance (CMR) is the gold-standard technique to evaluate LV remodeling. Our aim was to assess the prevalence and describe the patterns of LV adaptation in AS patients before and after surgical aortic valve replacement (AVR). Prospective study of 130 consecutive patients (71y [IQR 68–77y], 48% men) with severe AS, referred for surgical AVR. Patterns of LV remodeling were assessed by CMR. Besides normal LV ventricular structure, four other patterns were considered: concentric remodeling, concentric hypertrophy, eccentric hypertrophy, and adverse remodeling. At baseline CMR study: mean LV indexed mass: 81.8 ± 26.7 g/m²; mean end-diastolic LV indexed volume: 85.7 ± 23.1 mL/ m² and median geometric remodeling ratio: 0.96 g/mL [IQR 0.82–1.08 g/mL]. LV hypertrophy occurred in 49% of subjects (concentric 44%; eccentric 5%). Both normal LV structure and concentric remodeling had a prevalence of 25% among the cohort; one patient had an adverse remodeling pattern. Asymmetric LV wall thickening was present in 55% of the patients, with predominant septal involvement. AVR was performed in 119 patients. At 3-6 months after AVR, LV remodeling changed to: normal ventricular geometry in 60%, concentric remodeling in 27%, concentric hypertrophy in 10%, eccentric hypertrophy in 3% and adverse remodeling (one patient). Indexes of AS severity, LV systolic and diastolic function and NT-proBNP were significantly different among the distinct patterns of remodeling. Several distinct patterns of LV remodelling beyond concentric hypertrophy occur in patients with classical severe AS. Asymmetric hypertrophy is a common finding and LV response after AVR is diverse.

Keywords Aortic stenosis, Cardiac magnetic resonance, Left ventricular hypertrophy and remodeling

Abbreviations

ACE	Angiotensin-converting enzyme
ARBs	Angiotensin receptor blockers
AS	Aortic stenosis
AV	Aortic valve
AVA	Aortic valve area
AVmean	Mean aortic transvalvular pressure gradient
AVR	Aortic valve replacement

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CMR	Cardiac magnetic resonance
ECG	Electrocardiography
EOA	Effective orifice area
GLS	Global longitudinal strain
hsTn-T	Cardiac troponin T
Htc	Hematocrit
LGE	Late gadolinium enhancement
LV	Left ventricle
LVEDVi	Left ventricular end-diastolic volume index
LVEF	Left ventricular ejection fraction
LVH	Left ventricular hypertrophy
LVMi	Left ventricular mass index
MRAs	Mineralocorticoid receptor antagonists
M/V	Geometric remodeling ratio (CMR)
NT-ProBNP	N-terminal pro b-type natriuretic peptide
NYHA	New York Heart Association
RWT	Relative wall thickness
TTE	Transthoracic echocardiogram

Aortic valve stenosis (AS) is the most common primary valvular heart disease, with an increasing prevalence with advancing age, being an important cause of morbidity and mortality in middle aged and elderly adults¹.

Progressive valve narrowing leads to chronic pressure increase and hemodynamic load, being the main determinant for left ventricular (LV) adaptation and remodeling². However, LV response to chronic pressure overload depends also on a multitude of factors, such as age, gender, neurohormonal activation, and several comorbidities, including hypertension and reduced vascular compliance, diabetes, and chronic kidney disease^{2,3}. Both structural and functional LV changes in this setting take part in the pathophysiology of the disease. Indeed, *"looking to the ventricle, beyond the valve*", provides information toward the staging of valvular disease, with independent prognostic value for its natural history, predicting outcomes after aortic valve replacement (AVR)^{4,5}.

LV remodeling is believed to begin as a compensatory mechanism to maintain wall stress. Although classically described as increased LV mass, i.e., hypertrophy, this is not always the case for LV remodeling in the context of AS⁶⁻⁸. The correlation between LV hypertrophy and the severity of valve stenosis seems to be weak and old echocardiographic studies have showed that some 10 to 20% of patients with severe AS do not have LV hypertrophy and over 10% of them have inappropriately high LV mass⁶⁻⁸. Moreover, it has been demonstrated that patients with inappropriate concentric remodelling or excessive LV mass, with the same degree of AV narrowing, are more prone to adverse cardiovascular events, both before and after AVR⁶⁻⁸.

Cardiac magnetic resonance (CMR) imaging is the gold standard technique for the assessment of LV volumes, mass, and ejection fraction^{9,10}. However, most imaging studies addressing LV remodeling and adaptation in AS were performed with echocardiography, an imaging modality with inherent limitations regarding LV mass calculation and geometric assumptions. Besides that, there is paucity of information in what concerns reverse remodeling after AVR.

The aim of this study is to describe the patterns of LV adaptation and their differences both before and after surgical AVR in patients with severe AS, as assessed by CMR.

Methods

Study population, clinical data, and study design

Patients with isolated severe symptomatic AS (aortic valve area—AVA < 1.0 cm²) electively referred for surgical AVR at our tertiary single-centre, between 2019 and 2022, were prospectively included in the study. This is part of a research protocol involving both pre- and post-operative LV structural and functional assessment by multimodality imaging. Study approval was granted by the ethical committee of Nova Medical School University (number 61/2018/CEFCM) conforming to the principles of the Helsinki declaration. All participants gave written informed consent before inclusion.

Patients with previous diagnosis of sub/supra valvular aortic stenosis, concomitant severe non-aortic valve dysfunction and associated moderate to severe aortic regurgitation were excluded. Those with any of the following conditions were also excluded: previous cardiac surgery, active endocarditis, previous history of myocardial infarction, myocarditis, ischemic and non-ischemic cardiomyopathy including amyloidosis and other infiltrative diseases, non-cardiac inflammatory disease, active infection, under immunosuppressive and chronic anti-inflammatory therapy, under chemotherapy and with previous chest radiotherapy.

Clinical parameters (demographics, major cardiovascular risk factors, symptomatic status including the presence of angina, syncope, and New York Heart Association [NYHA] class, current medication) were collected at the time of inclusion, which was followed, at the same day, by both twelve-lead electrocardiography (ECG) and transthoracic echocardiography (TTE). Cardiac magnetic resonance (CMR) ensued at the same day or at no more than 2 weeks after patient inclusion, and a blood sample was collected at the day of this examination for the specific evaluation of hematocrit (Htc), renal function (creatinine, urea), high sensitivity cardiac troponin T (hsTnT) and N-terminal pro b-type natriuretic peptide (NT-ProBNP). Both TTE and CMR studies were planned to be performed within 6 months before AVR.

If clinically justified for coronary artery disease exclusion, patients performed a coronary angiography before intervention, and coronary revascularization was added to AVR when indicated. Surgical myectomy was concomitantly performed if planned before intervention because of asymmetric septal hypertrophy or at surgeon's

discretion. As per institutional protocol all patients underwent pre-discharge TTE following surgery, whose data were not included in the analysis.

To assess LV morphological and functional changes after surgery, all patients had a detailed TTE and CMR study between the 3rd and 6th month after surgery, as there is evidence that the majority (>80%) of volumetric and geometric LV changes have already occurred at this time point¹¹. These studies included the same parameters as that from pre-intervention.

Standard echocardiographic study-evaluation for aortic stenosis

All patients underwent a comprehensive TTE by experienced cardiologists before AVR, using commercially available ultrasound systems (Vivid E95; GE Healthcare, Chicago, IL, USA) with a 4D probe (3.5-MHz 2D phased array transducer), in accordance with current guidelines^{12,13}. Imaging analysis and measurements were performed on image data stored in the image vault and re-examined using EchoPAC version 202 for PC (GE Healthcare, Milwaukee, WI, USA). As proposed^{12,14} and for the quantification of AS, LV outflow tract diameter was measured on parasternal long-axis view and pulsed-wave and continuous-wave Doppler were used to record velocities across the LV outflow tract and aortic valve (AV), respectively. LV stroke volume index was calculated as LV outflow tract velocity time integral (obtained at 5-chamber apical view) x LV outflow area/body surface area. Multiple TTE windows, including apical, subcostal, right parasternal and suprasternal, were assessed to obtain the highest well defined AV velocity signal, which was used to obtain the peak AV velocity and mean AV gradient, estimated using the Bernoulli equation. AV area was calculated with the continuity equation.

In patients with low gradient AS, measurements of aortic valve area were checked for correctness. Both aortic valve calcium and low dose dobutamine were used according to LVEF and flow status, in accordance with the guidelines.

All reported bidimensional and Doppler derived measurements were averaged over 3, or at least 5 cardiac cycles for patients in atrial fibrillation. Additional echocardiographic evaluation, beyond aortic valve assessment, was performed in all patients as a comprehensive TTE, in accordance with current guidelines^{13,15}.

TTE study at the 3–6th month after AVR included all the above-mentioned parameters in addition to specific prosthetic assessment, as recommended¹⁶. This involved peak velocity and mean transprosthetic gradient, acceleration time at the contour of the jet velocity, Doppler velocity index and the effective orifice area (EOA) when in the presence of above-normal prosthetic gradients. Moderate and severe patient-prosthesis mismatch was defined as indexed EOA below 0.85cm²/m² and 0.65cm²/m², respectively.

Cardiac magnetic resonance

CMR study was performed at a 1.5 Tesla scanner (*Magnetom Avanto; Siemens Medical Solutions, Erlangen, Germany*), using the protocol described by *Kramer CM*. et al.¹⁷. Post-processing and quantification were performed using a dedicated software (*Circle Cardiovascular Imaging, CVI version 5.12, Calgary, Canada*). LV volume, mass and ejection fraction were measured using standard volumetric techniques after endocardial and epicardial delineations in all end-diastolic and end-systolic phase short-axis images. Native and postcontrast T1 mapping was performed using a *Modified Look-Locker Inversion* recovery (MOLLI) sequence in expiratory apnea, into three segments of the LV short-axis (base, mid and apex) before and 15 to 20 min after contrast injection, for extracellular volume (ECV) quantification, defined as ECV = $(1-Htc) \times [\Delta R1 \text{ myocardium}]/[\Delta R1 \text{ blood}]^{18}$, with the estimated hematocrit (Htc) from the collected blood sample at the same day. The LV short-axis stack of LGE was first assessed visually for the presence of LGE, followed by its quantification, when present, also after endocardial and epicardial delineations. LGE was defined as areas of signal intensity \geq 5 standard deviations from normal myocardium and was expressed as total mass and the percentage of total LV myocardial mass. Those with subendocardial LGE were excluded from the analyses.

LV mass and volumes were indexed to body surface area (calculated using the *Mosteller* formula). Left ventricular dilatation and hypertrophy were defined as a higher-than-normal left ventricular indexed end-diastolic volume (LVEDVi) and mass (LVMi), respectively, according to age and gender¹⁹. Geometric remodelling was calculated by dividing the LV mass by the left ventricular end-diastolic volume, being used as an indicator of LVMi normalized to chamber size²⁰.

All patients, including those in atrial fibrillation, had controlled heart rates (between 50 and 90 beats per minute). All CMR results were read by two experienced readers (JA and AF) with Level 3 CMR accreditation by the European Society of Cardiovascular Imaging, blinded to both clinical and echocardiographic data.

Patterns of LV hypertrophy and remodelling—definitions

The adaptation of the LV to chronic pressure overload and AS has been previously defined by the combined assessment of LV mass, cavity dimensions/volumes and wall thickness^{21,22}.

As previously proposed by Dweck et al.⁹, five patterns of LV adaptation were defined in our cohort, as assessed by both pre and post-operative CMR and according to the LVMi, LVEDVi and M/V ratio (Supplementary table 1): normal LV ventricular structure, concentric remodeling concentric hypertrophy, eccentric hypertrophy, and adverse remodeling. Asymmetric LV hypertrophy was also considered, regardless of the other five patterns, and defined as a regional wall thickening \geq 13 mm (from the short-axis views of the LV in end diastole, with exclusion of LV trabeculations) that was also > 1.5-fold greater than the thickness of the opposing myocardial segments, on at-least two adjacent short-axis slices.

Statistical analysis

Categorical values are presented as absolute numbers (and percentage). Continuous variables as mean ± standard deviation (normal distribution) or as median and interquartile range (IQR; non-parametric). Kolmogorov–Smirnov test was used to test normality of the variables.

Independent and paired sample T-Test, Mann–Whitney U, Wilcoxon, One-way ANOVA and Pearson's Chisquared (x^2) tests were applied for comparison where appropriate. Statistical significance was set at P-value < 0.05 (two-sided). Correlation between normally distributed data was performed using Pearson's correlation to provide r^2 values. To assess correlations between NT-proBNP and late gadolinium enhancement (LGE) mass with LVMi, Spearman correlation coefficients were used. All analyses were performed using Statistical Package for the Social Sciences Statistics v27.0 (IBM Corporation, Armonk, NY, USA).

Ethics approval

This study was approved by the local ethics committee and the ethical committee of Nova Medical School University (number 61/2018/CEFCM), fulfilling the principles of the Helsinki declaration.

Consent to participate

All patients gave written informed consent before pre-operative imaging studies.

Results

Study population and clinical data

Overall, we prospectively studied 130 consecutive patients with severe symptomatic AS and complete pre-operative CMR study, with an age of 71 years [IQR 68–77y], 62 (48%) men. A mean period of 3.9 ± 2.5 months elapsed between imaging studies and valve surgery. Demographic, clinical and laboratory related data are summarized in Table 1. Regarding cardiovascular risk factors and comorbidities, at pre-operative study: 89% (n = 116) had a previous diagnosis of hypertension; 26% (n = 34) patients were diabetic, and 32% of patients (n = 42) had chronic kidney disease defined by a glomerular filtration rate below 60 mL/min/1.73m² (all of them with creatinine clearance above 25 ml/min; no patient under dialysis). All patients with hypertension were under therapy with at least one anti-hypertensive agent (predominantly with ACE inhibitors/ARBs: 65%; followed by diuretics: 36%; beta-blockers 29%; and 2% with MRAs). The specific assessment of appropriate blood pressure control before surgery, such as ambulatory measurements, was not performed.

Preoperative imaging evaluation (Table 2)

Mean aortic valve area was 0.7 ± 0.2 cm² and 96% of patients had high gradient (>40 mmHg) AS (mean transvalvular pressure gradient of 61 ± 18 mmHg). Five patients had a mean transvalvular gradient between 35 and 40 mmHg. Normal flow condition (stroke volume index above 35 mL/m²) occurred in 85% (n = 110) of patients. Mean LVEF by TTE was $58 \pm 9\%$ and mean global longitudinal strain was $-14.7 \pm 3.8\%$. Only 7 patients (5%) had preoperative LVEF below 40% (85% with LVEF >50%; 10% with LVEF between 40 and 50%). Overall, the great majority of patients (n = 107; 82%) had classical normal flow, high gradient severe AS. Low-flow low-gradient

Total study population: n = 130	
Clinical characteristics	
Age, years	71 (68–77)
Male	62 (47.7%)
BSA m ²	1.80 ± 0.19
Hypertension	108 (83%)
Diabetes mellitus	34 (26.1%)
Dyslipidemia	78 (60%)
Chronic Kidney disease	42 (32.3%)
NYHA functional class	
Ι	7 (5.4%)
II	99 (76.2%)
III	24 (18.5%)
Anginal symptoms	35 (26.9%)
Syncope	30 (23.1%)
Laboratory results	
Creatinine, mg/dL	0.91 (0.77-1.11)
Estimated glomerular filtration rate, mL/min	70.1 (55.5-86.9)
NT-proBNP, pg/mL	568 (219-1479)
Troponin, ng/L	13 (9–20)

Table 1. Baseline clinical, laboratory and surgical data of the study cohort. Values are median (interquartile range), mean ± standard deviation. *BSA* body surface area, *NYHA* New York Heart Association.

Total study population: n = 130			
Echocardiography			
Aortic valve area, cm ²	0.7 ± 0.2		
Maximum aortic gradient, mmHg	98.6±27.2		
Mean aortic gradient, mmHg	61.1±17.6		
Stroke volume index, mL/m ²	47.5 ± 10.9		
Relative wall thickness	0.51 ± 0.13		
Septal thickness, mm	16±2.7		
LV mass, g	287.8±98.3		
LV indexed mass, g/m ²	158.3 ± 53.2		
LVEDV, mL	86.9±33.9		
LVEDV indexed, mL/m ²	48.1 ± 17.1		
LVESV, mL	41.7±21.9		
LVESV indexed, mL/m ²	22.9±11.1		
LV ejection fraction, %	57.9±9.3		
Global longitudinal strain, %	-14.7 ± 3.8		
Cardiac magnetic resonance (CMR)			
LV mass, g	147.9±52.7		
LV indexed mass, g/m ²	81.8 ± 26.7		
LVEDV, mL	155.1 ± 47.4		
LVEDV indexed, mL/m ²	85.7±23.0		
LVESV, mL	65.3±33.6		
LVESV indexed, mL/m ²	36.1±17.4		
Geometric remodeling, g/mL	0.96 (0.82-1.08)		
LV ejection fraction, %	59.7±10.1		
Global native T1, ms	1053 (1023–1071)		
Global ECV, %	24 (21–27)		

Table 2. Baseline imaging data: TTE and CMR. Values are median (interquartile range), mean ± standard deviation. *ECV* extracellular volume, *LV* left ventricle, *LVEDV* left ventricle end diastolic volume, *LVESV* left ventricle end systolic volume.

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a ortic stenosis, defined as: mean transaortic gradient < 40 mm Hg, valve area < 1.0 cm² and SVi < 35 mL/m², was present in 2 patients.

Mean LV indexed mass before surgery at the TTE was 158.1 ± 53.2 g/m², with a mean relative wall thickness (RWT) of 0.5 ± 0.13 .

At preoperative CMR study, mean LVEF was $60 \pm 10\%$, mean indexed LV mass [LVMi]: 81.8 ± 26.7 g/m²; indexed mean end-diastolic LV volume [LVEDVi]: 85.7 ± 23.1 mL/m² and median geometric remodeling ratio [M/V]: 0.96 g/mL [IQR 0.82–1.08 g/mL]. Non-ischemic late gadolinium enhancement (LGE), excluding patients with exclusive junctional LGE, was observed in 70 patients (54%), all with a non-ischemic combined mid-wall and junctional enhancement pattern, except one patient who presented a non-transmural subendocardial LGE (previously unknown ischemic scar).

Patterns of left ventricular adaptation before surgery

Concentric hypertrophy and remodeling were the predominant patterns of LV adaptation (representing 69% of the patients). Notably, 25% of the patients had normal LV geometry before surgery (Fig. 1) and LV wall asymmetry was present in 71 (55%) patients, most often affecting the basal anterior and mid inferior septum. None of these patients had significant pre-operative intra-ventricular gradients. All patients with reduced LVEF except one had normal LV volumes (only one patient matching the definition of adverse remodeling).

Meaningful differences were observed regarding AS severity, echocardiographic parameters of LV function (LVEF and GLS) and loading (E/E', Left atrial indexed volume, NT-ProBNP values) when comparing patients with distinct patterns of LV adaptation (Table 3). LVEF (as assessed by CMR) was also distinct between different patterns of LV remodelling. At tissue characterization, patients with concentric hypertrophy had higher absolute masses of LGE.

No difference was observed regarding the prevalence of hypertension, creatinine clearance and use of different anti-hypertensive classes of drugs.

When assessing those with asymmetric LV wall thickening, these patients had higher transvalvular gradients and NT-proBNP levels. At CMR, this group was characterized by lower LVEF, higher LVMi and absolute LGE mass (Supplemental Table 2). Prevalence of asymmetric hypertrophy was significantly higher in patients with concentric hypertrophy pattern (Table 3; Supplemental Table 2). There were no significant differences among distinct patterns of remodeling and LV asymmetric hypertrophy regarding native T1 myocardium values and



Figure 1. Patterns of left ventricle remodeling at baseline/preoperative assessment—left ventricular structure alongside CMR short-axis images.

ECV. From the multiparametric pre-operative CMR study involving both mapping derived indexes and LGE, there was no suspicion of amyloid infiltration at the individual patient level.

No significant correlation was found between LVMi and aortic valve narrowing. However, LV mass was significantly related to both NT-proBNP levels and LGE mass (Fig. 2).

Evolution of LV remodeling after AVR

AVR was already performed in 119 patients (92%) and 89% (116 patients) completed the post-operative study with TTE and CMR at the 3rd to 6th month post-AVR. Comparative analysis between pre- and postoperative imaging data at both TTE and CMR studies revealed significant reductions of LV mass and volumes after surgery, with significant improvement of LV systolic function indexes (Table 4).

There was no severe prosthesis dysfunction at echocardiographic follow-up. Two patients with above labeled prosthetic gradients were identified with moderate patient-prosthesis mismatch. Four of 116 patients (3%) had mild paravalvular regurgitation. None of the patients presented intraventricular or left ventricular outflow tract gradients at TTE follow-up after AVR. The majority of patients (94%) had a bioprosthetic implantation and subaortic septal myectomy was added to the procedure, as reported by the surgical team, in 60% (n = 71) of the cases. At surgical report there was no reference to the extension of myectomy, namely in what concerned the dimension of the excised sample of the interventricular septum.

Contrary to pre-operative predominant pattern of LV remodeling, 60% of the patients had a normal LV geometry after AVR, and this came from the adaptative change of patients with both concentric remodeling and concentric hypertrophy (Fig. 3). However, there was a similar percentage of patients with concentric remodeling after surgery when compared to preoperative data. This was the result of a reduction of LV mass in some patients with pre-operative concentric hypertrophy and notably from a change of pattern in some patients with normal LV geometry before surgery. After surgery, asymmetric wall thickening persisted in 40 patients (35% of patients with completed imaging evaluations), with a shift from basal to mid septum wall segments (Fig. 4).

We found no significant differences in the percentage of patients submitted to concomitant myectomy across distinct patterns of remodeling. However, this procedure was more frequently performed in patients with asymmetric hypertrophy (48% vs. 63%, p = 0.091).

Discussion

This study describes the different morphological patterns of remodeling and LV hypertrophy in a cohort of patients with predominant normal flow, high gradient, preserved EF, severe AS. Our main findings were that: (1) LV response to chronic pressure overload differed widely between patients; (2) the severity of AS, functional repercussion and LV loading conditions were independently associated with the pattern of LV adaptation before surgery; (3) asymmetric wall thickening was highly prevalent (4) short-term follow up after surgical AVR revealed that LV response was dynamic after surgery, with diverse patterns of remodeling as well.

To our knowledge this is one of the few CMR studies specifically addressing LV remodeling and adaptation in patients with severe symptomatic AS both before and after surgical AVR. Previous works with CMR had smaller samples, included patients with moderate AS and did not provide longitudinal data following intervention.

As previously reported from echocardiographic studies and consistent in pathophysiological terms^{8,23}, LV hypertrophy was prevalent, albeit far from being the sole pattern of LV adaptation. The significant proportion of patients with asymmetric hypertrophy may explain the relative proportion of distinct LV patterns in our study, more like that described by Dweck et al.⁹. LV mass estimation from TTE derives from linear M-mode

	Normal ventricle	Concentric remodeling	Concentric hypertrophy	Eccentric hypertrophy	Adverse remodeling	p value*
Number of patients	33	33	57	6	1	-
Male sex, %	35	53	51	17	100	0.144
Age, years	72±9	73±7	70±8	73.8±7.6	67	0.591
Hypertension, n (%)	28 (85)	26 (79)	47 (82)	6 (100)	1 (100)	0.521
ACE inhibitors/ARBs, n (%)	24 (73)	17 (52)	38 (67)	5 (83)	0	0.176
Diuretics, n (%)	15 (46)	8 (24)	21 (37)	3 (50)	0	0.337
Beta-blockers, n (%)	13 (39)	12 (36)	10 (18)	3 (50)	0	0.058
MRAs, n (%)	1 (3)	0	2 (4)	0	0	0.826
Diabetes mellitus, n (%)	5 (15)	10 (30)	17 (30)	2 (33)	0	0.527
Dyslipidemia, n (%)	18 (55)	23 (70)	32 (56)	5 (83)	0	0.301
Creatinine Clearance, ml/min	73.5±22.7	66.6±21	74.7±23.8	63.6±26	97.8	0.307
NT-pro BNP, pg/mL	417.5 (181.2-1188.3)	219.1 (131-426.1)	954 (475-2686)	1709 (1201.3-3019.3)	7493	< 0.001
Echocardiography	t	·	1			
Indexed Aortic Valve Area, cm ²	0.40 ± 0.2	0.43 ± 0.07	0.38±0.10	0.43 ± 0.67	0.44	0.080
Mean Aortic gradient, mmHg	54.0±15.3	51.9±8.8	71.1±17.6	55.9±13.3	50.1	0.001
Stroke volume index, mL/m ²	44.8±8.7	45.9±9.0	49.5±12.8	51.1 ± 10.7	48.6	0.284
Relative wall thickness	0.48±0.13	0.54 ± 0.14	0.53 ± 0.12	0.40 ± 0.15	0.31	0.012
LV indexed mass, g/m ²	138.7±44.3	128.9±22.6	183.3±58.1	186.9±54.1	177.0	< 0.001
Indexed LVEDV, mL/m ²	40.5±16.9	34.1±11.7	53.3±19.0	67.0±7.1	89.4	< 0.001
LV ejection fraction, %	60.6 ± 6.4	59.7±9.3	56.4±9.8	53.7±7	35	0.012
GLS, %	-17.3 ± 3.3	-15.8 ± 3.6	-12.9 ± 3.4	-14.6±4	-11.6	< 0.001
E/A ratio	0.77 (0.61–1.14)	0.74 (0.56 - 0.78)	0.71 (0.56-0.89)	1.6 (0.72–1.7)	0.66	0.363
E/e²	11.1 (8.9–17.1)	12.0 (9.7–17)	14.5 (12-20.5)	26.5 (13.5-32.5)	13.6	0.013
LAVi (ml/m2)	39.2 (35-49.5)	36.4 (27,5 - 42.9)	44.3 (36.3-57.5)	58.2 (48.5-72.3)	42.1	< 0.001
PASP (mmHg)	38 (28.8-49.0)	37 (31–37)	34 (29–50)	48 (39–59)	45	0.522
TAPSE, mm	22.1±3.3	22.5±3.9	21.5±3.9	21.2±4.6	29	0.262
STDI, cm/s	11.2±6.7	8.2±7.3	11.3±5.6	8.7±7.4	14	0.194
Cardiac magnetic resonanc	e					
Ejection fraction, %	61.3±8.2	63.9±9.2	56.8±10.7	57.9±7.4	41	0.003
LV mass index, g/m ²	59.8±10.6	66.7±10.2	103.1±24.7	81.9±15.9	89.9	< 0.001
Indexed LVEDV, mL/m ²	80.5±15.4	66.7±11.2	96.6±23.4	106.9±12.1	139.7	< 0.001
Geometric remodeling, g/mL	0.75 (0.68–0.82)	0.98 (0.92–1.09)	1.03(0.95-1.17)	0.75 (0.70-0.82)	0.64	< 0.001
Asymmetric hypertrophy, n (%)	11 (33)	15 (50)	42 (74)	3 (50)	0	< 0.001
LGE, g	0 (0-5.55)	3.63 (0-6.65)	6.2 (1.67–13.3)	0.27 (0-5.64)	2.70	0.013
LGE, % of mass	0 (0-4.55)	3.35 (10-6.53)	4.5 (1.04-8.05)	0.25 (0-4.10)	1.60	0.041
Global native T1, ms	1056 (1013–1074)	1041 (1018–1062)	1056 (1036–1074)	1063 (1039–1078)	1070	0.210
Global ECV, %	25 (21-28)	24 (21-26)	23 (19–27)	21 (20-23)	28	0.238

Table 3. Comparative analyses between different patterns of LV structure in patients with severe symptomatic AS before AVR. Values are median (interquartile range), mean \pm standard deviation. *LV* left ventricle, *LVEDV* left ventricle end diastolic volume, *LAVI* left atrium volume index, *PASP* pulmonary artery systolic pressure, *TAPSE* tricuspid annulus plane systolic excursion, *STDI* right ventricular systolic velocity at tissue Doppler imaging, *ECV* extracellular volume, *LGE* late gadolinium enhancement. **p* value provided from comparisons between 5 remodeling LV patterns according to one-way ANOVA; Bold *p*-values are statistically significant; Patients with exclusive junctional LGE were excluded from the analyses of LGE; LGE quantification was performed in 70 patients.

measurements, which are greatly influenced by LV cavity dimension and also basal septal thickness. Basal septal thickness did not represent global LV wall thickening in a great proportion of patients as we report LV asymmetric thickening in more than half of them. This probably explains TTE mass overestimation. Distinct LV volumes by both techniques are also probably explained by differences in both TTE and CMR in what concerns spatial resolution and techniques for volume estimation: *Simpson's* rule by TTE, with endocardial interface definition, probably affected by concentric remodeling and hypertrophy, *versus* each slice contour definition at short-axis



	Before AVR n=130	After AVR n=116	<i>p</i> value		
Echocardiography					
Maximum aortic gradient, mmHg	98.6±27.2	23.1±8.7	< 0.001		
Mean aortic gradient, mmHg	61.1±17.6	12.7±5.2	< 0.001		
DVI	0.20 ± 0.05	0.49 ± 0.10	< 0.001		
Relative wall thickness	0.51±0.13	0.46 ± 0.14	0.001		
LV indexed mass, g/m ²	158.3±53.2	128.9 ± 44.2	< 0.001		
LVEDV, mL	86.9±33.9	85.5±32.7	0.607		
LV ejection fraction, %	57.9±9.3	59.7±7.9	0.095		
Global Longitudinal strain, %	-14.7 ± 3.8	-16.2 ± 3.2	< 0.001		
Cardiac magnetic resonance					
LV indexed mass, g/m ²	81.8±26.7	62.7±15.1	< 0.001		
LVEDV, mL	155.1±47.4	141±44.2	< 0.001		
Geometric remodeling, g/mL	0.96 (0.82-1.08)	0.84 (0.71-0.93)	< 0.001		
LV ejection fraction, %	59.7±10.1	58 ± 8.8	0.034		

Table 4. Comparative analyses between imaging data: TTE and CMR in patients with severe symptomatic AS before and at the 3rd to 6th month post-surgical AVR. Values are median (interquartile range), mean ± standard deviation. *LV* left ventricle, *LVEDV* left ventricle end diastolic volume. Bold *P* values are statistically significant. Comparative sensitivity analysis was performed only for patients who complete post-operative study with TTE and CMR at the 3rd to 6th month post-AVR.



Figure 3. *Sankey* diagram of cardiac magnetic resonance patterns (pre- and post-surgical aortic valve replacement) of left ventricular hypertrophy in aortic stenosis patients.

segmentation by CMR. Contrary to ancillary echocardiographic studies relying on M-mode measurements and extrapolations, the estimation of LV mass and geometry by CMR more accurately reflects LV structural and geometrical changes. In the same scope, there is a proportion of patients with preoperative normal LV geometry and mass, and a predominant proportion of patients returning to this morphological pattern after AVR, which follows the expected physiological response after the treatment of a pressure overload. Nevertheless, some patients still maintain either concentric remodeling and hypertrophy after surgery or evolve from a normal LV geometry through concentric patterns. This was not certainly due to the procedure, as there were only two patients with moderate patient-prosthesis mismatch. As previously proposed^{24,25}, this could be related to several factors, beyond valve disease, such as hypertension, neuro-endocrine environment, and their mutual interaction, precluding post-operative reverse remodelling. Additionally, the presence of replacement fibrosis, which was more prevalent in our patients with concentric hypertrophy and may represent an advanced stage of LV disease in this setting, might be a predictor of the impairment of reverse remodeling after AVR. Finally, genetic factors controlling extracellular matrix remodeling and protein/collagen deposition/turnover in the myocardium, may stem considerable differences on the phenotypic expression of the LV in this context^{26,27}. Overall, we should stress out that at the first glance our cohort of patients is predominantly composed of a homogeneous group of patients: with the same phenotype of high gradient, normal flow, preserved EF severe AS. However, considerable heterogeneity exists as far as LV adaptation is concerned, and this falls in line with recent concepts emerging



Figure 4. Distribution of hypertrophied LV segments in patients with asymmetric pattern of LV remodeling before (left) and after (right) AVR (based on 17-segment model of the LV).

from observational studies⁹. Classically, the idea of progressive transition through LV phenotypes in patients with severe AS, from normal geometry to concentric remodeling, hypertrophy, eccentric hypertrophy, and adverse remodeling prevailed, and this would have implications towards the condition of flow and gradients⁶. Instead, it is becoming apparent that both initiation and inhibition of hypertrophy involve multiple distinct signalling pathways from the beginning of pressure overload, i.e., less than severe AS, supporting the multifactorial genesis of LV remodeling². Indeed, the lack of relation between aortic valve orifice area and LV mass in our cohort supports this concept. Moreover, we found significant differences among distinct patterns of remodeling regarding LV function and loading. These findings are mirrored by the positive relation between LV mass and BNP values, and supposed to be related to the association between increased LV mass and LGE (both structural and tissue remodeling), as we previously demonstrated following additional correlation data from the same cohort²⁸. Here we specifically excluded patients with exclusive junctional LGE, as there is also evidence that this pattern is highly prevalent, unspecific and unrelated to adverse prognosis^{28,29}.

We also observed an asymmetric pattern of LV hypertrophy, as defined by CMR, in more than half of the patients. This is more than reported by Dweck et al.⁹ and higher above previously reported prevalence from surgical teams³⁰, even considering that the definition was derived from pre-operative TTE in preceding studies, and not from CMR assessment. Asymmetric wall thickening was identified across distinct patterns of remodeling and was associated with higher transvalvular gradients, BNP levels and worse indexes of LV function. At CMR, this group was characterized by higher LVMi and absolute LGE mass. As previously proposed³¹ it would be tempting to interpret this as a genotypic predisposition, related to hypertrophic cardiomyopathy, to asymmetric rather than concentric remodeling in a pressure overload condition. However, this was observed in a high proportion of patients, well-above the estimated prevalence of any genetic cardiomyopathy, lacking additional morphologic and functional characteristics features. Besides, the presence of a pressure overload condition such as AS, seems counterintuitive regarding the concept of hypertrophic cardiomyopathy. Our belief is that genetics is far from being the sole main driver of such a common geometric pattern. Furthermore, we might also speculate that regional distribution of endocavitary pressure on basal LV segments, following Laplace's law, could eventually explain asymmetric wall thickening in some particular segments in some of the patients. Additional studies focused on the possible interaction between genetics, clinical factors, haemodynamic conditions and original cavitary geometry before valve disease development, converging for asymmetric wall thickening, are needed. Ultimately, its clinical meaning and predictors are important to define as this could impact the decision of when to associate myectomy to surgical AVR.

Limitations

Our study had some limitations. As it was conducted at a single tertiary centre with a moderate sample size, the size of the different pattern's groups of LV remodeling is necessarily small, thus limiting the extrapolation of the results. Patients referred for transcatheter procedures were not included, this possibly excluding a significant proportion of patients with either eccentric or adverse patterns of remodelling.

Likewise, we were not able to collect accurate data specifically addressing the length of time from the diagnosis of severe AS, beginning of symptoms or clinical indication for aortic valve replacement. These would have been important when trying to understand the remodeling process. Similarly, we did not appropriately assess the impact of long-standing factors which might have also influenced LV adaptative response, such as both pre- and post-operative blood pressure and diabetes control. In the same way, we were not able to evaluate if surgical myectomy was independently related to the particular type of post-operative remodeling. As the design of our research protocol also included endomyocardial septal biopsies during AVR, we believe that this could explain the high prevalence of surgical myectomy reported by the surgical team. Unfortunately, we have no data addressing its extension, and this could have been important as to assess its impact on postoperative remodeling. However, we have recently published data on the same cohort showing that post-operative changes in LV mass and volumes were independent from surgical septal myectomy³².

From pre-operative CMR we did not have the suspicion of cardiac amyloidosis, but we could not definitely confirm this in the whole cohort as we did not perform additional targeted investigation³². Likewise, we were not able to exclude possible concomitant diagnosis of hypertrophic cardiomyopathy, eventually explaining the high prevalence of asymmetric LV hypertrophy.

Finally, this was mainly a descriptive imaging study, and our aim was not to find predictors for a specific type of remodeling. Unfortunately, we are also not yet able to provide prognostic data for distinct patterns of LV adaptation in the long-term follow-up after AVR.

Conclusion

In this prospective cohort of patients with predominant classical severe symptomatic AS we have demonstrated that concentric hypertrophy was not the sole pattern of LV remodeling. Indeed, diverse patterns of adaptation exist, and asymmetric hypertrophy is a common finding, with distinct features in what concerns LV function and loading. LV re-adaptative remodeling following surgical AVR is also diverse and occurs in the short-term.

Data availability

All data generated or analysed during this study are included in this published article [and its supplementary information files].

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Author contributions

The first draft of the manuscript was written by R.R.S. and J.A.; S.M. incorporated feedback in subsequent drafts and revisions; P.L., L.O., P.F., A.F., R.R., M.J.A., M.S.U., J.P.N., V.G. and N.C. contributed to revisions and reviewed the final draft; R.R.S. composed the figures and submitted the final version of this article, on behalf of all the authors.

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