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## **OPEN** Tannic acid-mediated synthesis of flower-like mesoporous $MnO_2$ nanostructures as $T_1-T_2$ dual-modal MRI contrast agents and dual-enzyme mimetic agents

Farzaneh Sorouri<sup>1,2,6</sup>, Elham Gholibegloo<sup>1,6</sup>, Tohid Mortezazadeh<sup>3</sup>, Sahar Kiani<sup>2</sup>, Alireza Foroumadi<sup>4</sup>, Loghman Firoozpour<sup>4</sup> & Mehdi Khoobi<sup>1,5</sup>

This study introduces a simple method for preparing a new generation of MnO<sub>2</sub> nanomaterials (MNMs) using tannic acid as a template. Two shapes of MnO<sub>2</sub> NMs, flower-like M1-MnO<sub>2</sub> and near-spherical M2-MnO<sub>2</sub>, were prepared and compared as dual-active nanozymes and contrast agents in magnetic resonance imaging (MRI). Various parameters, including the crystallinity, morphology, magnetic saturation (M<sub>s</sub>), surface functionality, surface area, and porosity of the MNMs were investigated. Flower-like M1-MnO<sub>2</sub> NMs were biocompatible and exhibited pH-sensitive oxidase and peroxidase mimetic activity, more potent than near-spherical M2-MnO<sub>2</sub>. Furthermore, the signal intensity and r<sub>1</sub> relaxivity strongly depended on the crystallinity, morphology, pore size, and specific surface area of the synthesized MNMs. Our findings suggest that flower-like M1-MnO<sub>2</sub> NM with acceptable dualenzyme mimetic (oxidase-like and peroxidase-like) and T<sub>1</sub> MRI contrast activities could be employed as a promising theranostic system for future purposes.

Diagnostic science, as an interdisciplinary field, has long been known to understand the components, processes, dynamics, and treatment of a disease at the biochemical and molecular levels<sup>1-3</sup>. Magnetic resonance imaging (MRI) has emerged as a non-invasive molecular imaging method for the early detection, diagnosis, and visualization of diseases. Unlike X-ray computed tomography (CT) and positron emission tomography (PET), MRI does not utilize ionizing radiation<sup>4,5</sup>. However, contrast agents (CAs)-free MRI is a double-edged approach for indicating soft tissues. The long relaxation time of water protons (H<sup>+</sup>) results in images with poor contrast and low sensitivity. Therefore, CAs can be used to differentiate the normal and abnormal tissues, leading to more accurate diagnosis of pathologies<sup>6</sup>. Paramagnetic and superparamagnetic metals are mainly utilized as CAs in MRI, generating high-resolution information regardin spatial and temporal characters of typical and malignant cellular processes. Most of the currently used  $T_1$ - or  $T_2$ -MRI CAs are based on gadolinium (Gd), manganese (Mn), and magnetite nanoparticles (Fe<sub>3</sub>O<sub>4</sub> NPs)<sup>7-10</sup>. To date, Gd has been the predominant lanthanide used as a  $T_1$ -positive CA. Owing to the seven unpaired electrons,  $Gd^{+3}$  possesses a high net magnetic moment. However, due to the potential toxicity and short blood circulation times, Food and Drug Administration (FDA) has limited clinical applications of Gd-based CAs. Nephrogenic systemic fibrosis in patients with severe renal failure is also another important drawback of the Gd-based CAs<sup>7,11</sup>. A few iron-based nanoparticles (NPs) have been approved by FDA as  $T_2$ -negative CAs. Despite some interesting features of  $Fe_3O_4$  NPs such as low toxicity and high stability, application of these NPs is restricted due to their intrinsic dark signals and magnetization artifacts which lead to the bleeding defects and thus misdiagnosis<sup>9</sup>. To overcome these drawbacks, Mn-based CAs have

<sup>1</sup>Department of Radiopharmacy, Faculty of Pharmacy, Tehran University of Medical Sciences, Tehran, Iran. <sup>2</sup>Department of Brain and Cognitive Sciences, Cell Science Research Center, Royan Institute for Stem Cell Biology and Technology, ACECR, Tehran, Iran. <sup>3</sup>Department of Medical Physics, School of Medicine, Tabriz University of Medical Sciences, Tabriz, Iran. <sup>4</sup>Department of Medicinal Chemistry, Faculty of Pharmacy, Tehran University of Medical Sciences, Tehran, Iran. <sup>5</sup>Biomaterials Group, Pharmaceutical Sciences Research Center, The Institute of Pharmaceutical Sciences (TIPS), Tehran University of Medical Sciences, Tehran 1417614411, Iran. <sup>6</sup>These authors contributed equally: Farzaneh Sorouri and Elham Gholibegloo. <sup>Sem</sup>email: m-khoobi@tums.ac.ir; mehdi.khoobi@gmail.com

gained considerable attention because of their biocompatibility and positive contrast enhancement. Mn, as a non-lanthanide metal resembling  $Ca^{2+}$ , is a natural cellular constituent. It often operates as a regulatory cofactor for enzymes and receptors. Furthermore, it possesses inherent characteristics such as high spin number, lengthy electronic relaxation time, and unstable water exchange. Mn+2 ions, with five unpaired electrons, could shorten the  $T_1$  of water protons, enhancing the  $T_1$  signal intensity<sup>12-15</sup>. In addition, Mn has a small  $T_2$  effect, reducing the signal intensity and producing dark images. It has critical roles in mitochondrial function and it could be accumulated in mitochondria-rich cells such as hepatocytes. Therefore, it could be applied as a proper CA for imaging of mitochondria-rich organs, including liver, pancreas, and kidney<sup>8,16</sup>. Mn-based CAs could be mainly divided into two categories, including Mn<sup>2+</sup>-bearing complexes and manganese oxide NPs. Manganese in its ionic form (Mn<sup>+2</sup>) has a short plasma half-life, leading to poor stability. A high level of this ion can result in the neurodegenerative abnormalities and can damage the brain. Therefore, using a Mn<sup>+2</sup> complex as an imaging CA is not entirely without any issues. Different manganese oxides, at different oxidation states, including MnO<sub>3</sub>, MnO<sub>3</sub>,  $Mn_3O_4$ , and  $MnO_3$ , have been reported so far. Although MnO NPs have a good T<sub>1</sub> effect in MRI, their long-term retention in the reticuloendothelial system could be toxic. Moreover,  $Mn_3O_4$  NPs with a mixed valence of +2 and + 3, exhibit no effective T<sub>1</sub> relaxation, due to the fewer unpaired electrons and shorter electron spin relaxation time compared to the divalent Mn ions. While, MnO<sub>2</sub> NPs could react with GSH in the tumor environment and Mn<sup>4+</sup>could be reduced to Mn<sup>2+</sup>, enhancing T<sub>1</sub> MRI. Therefore, among different manganese oxides, MnO<sub>2</sub> nanostructures could be considered as promising CAs for improved imaging and therapeutic applications.

Using natural enzymes as catalysts in biological systems have inherent disadvantages such as high cost, easy denaturation and inactivation, which limit their usage. To overcome these limitations, synthetic enzymes, by mimicking the function of natural enzymes, have been considered as promising alternatives. In particular, nanozymes can mimic the activity of the enzymes while maintaining the unique physical and chemical properties of nanomaterials<sup>17</sup>. Moreover, nanozymes can serve as CAs in tumor imaging and medical diagnosis<sup>18</sup>. Recently,  $MnO_2$  nanostructures have attracted much attention as nanozyme candidates. It has been reported that  $MnO_2$  has single oxidase-like or peroxidase-like activities. They have attracted attention of the researchers due to the lattice oxygen defects in their structure, plenty of natural reserves, low cost, non-toxicity, good biological safety, and biocompatibility<sup>19,20</sup>. Liu et al.<sup>17</sup> found that  $MnO_2$  NPs show peroxidase- and oxidase-like activities. Under the Fenton reaction with  $H_2O_2$ ,  $MnO_2$  NPs produce the most harmful reactive oxygen species (ROS), which could be used against cancerous cells<sup>21–23</sup>. These findings have encouraged many researchers to employ  $MnO_2$  NPs as safe therapeutic agents in cancer theranostics.

Tannic acid (TA) is an organic polyphenolic compound with interesting characteristics such as low cost, non-toxicity, environmentally friendly nature, and excellent metal reduction and metal chelation properties<sup>24-26</sup>. It was used as a porogen to prepare mesoporous silica<sup>27</sup> and porous  $Fe_3O_4$  NPs<sup>25,28</sup>. In the light of the above findings, in this work, we first aimed to find a new method to reach hierarchical mesoporous Mn-based NMs; and then we aimed to investigate the impact of morphology, surface area and porosity of two different Mn-based NMs on the MR contrast enhancement as well as nanozyme activity. The interesting features of TA as a natural template inspired us to develop a simple method for synthesizing novel hierarchical flower-like mesoporous MnO<sub>2</sub> nanomaterials (MNMs). The flower-like MNMs (M1-MnO<sub>2</sub>) and spherical MnO<sub>2</sub> (M2-MnO<sub>2</sub>) were synthesized and compared in term of the crystallinity, size, morphology, surface area, porosity, and magnetic properties. The nanozyme activity (peroxidase- and oxidase-like activities), cytocompatibility, and cellular uptake of the MNMs were also evaluated. Furthermore, the  $r_1$  relaxivity and intensity of  $T_1$ -weighted images were investigated to study the effect of different parameters on the maximum contrast enhancement. To the best of our knowledge, this is the first work to report a simple and environmentally friendly method for the preparation of novel mesoporous  $MnO_2$  NMs with flower-like morphology using TA as a template. Although there are some studies on the synthesis of  $MnO_2$  as a contrast agent, to the best of our knowledge, no study has been reported so far in which the efficacy of flower-like mesoporous and spherical  $MnO_2$  nanostructures was compared in both MRI contrast enhancement and nanozyme activity. We hope our findings can open a new way to develop novel Mn-based theranostic system for future studies.

#### **Experimental sections**

**Materials.** Chemical reagents including potassium permanganate (KMnO<sub>4</sub>, 97.5%), Manganese(II) nitrate tetrahydrate (Mn(NO<sub>3</sub>)<sub>2</sub>·4H<sub>2</sub>O, >97%), sodium hydroxide (NaOH, 99.9%), 3,3',5,5'-tetramethylbenzidine (TMB), and hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>, 30%) were obtained from Sigma–Aldrich Company. Tannic acid (TA) and 3-(4,5-dimethylthiazolyl-2)-2, 5-diphenyltetrazolium bromide (MTT) were supplied by Merck (Germany). MCF-7 (human epithelial breast cancer) and MCF-10A (non-malignant breast epithelial) cell lines were provided by the National Cell Bank of Iran (NCBI), affiliated with the Pasteur Institute. Dulbecco's modified Eagle medium (DMEM), RPMI 1640 medium, and phosphate-buffered saline (PBS) were purchased from Gibco BRL (Cergy Pontoise, France).

**Synthesis of the MnO<sub>2</sub> NMs through two different methods.** To synthesize M1-MnO<sub>2</sub> NMs, 1 gr of TA, as a template, was dissolved in 10 mL of deionized (DI) water and stirred for 5 min. Then,  $Mn(NO_3)_2$ ·4H<sub>2</sub>O (1.73 gr, 7.8 mmol) and KMnO<sub>4</sub> (0.73 gr, 4.6 mmol) were dissolved in 10 mL of DI water, separately. In the next step,  $Mn(NO_3)_2$ ·4H<sub>2</sub>O and KMnO<sub>4</sub> solutions were slowly added to the TA solution, simultaneously, via two separate dropping funnels within two hours and the mixture was heated in an oil bath to 80 °C with vigorous stirring. After adding both solutions, the reaction mixture was stirred for another four hours. The precipitate was separated using centrifugation. To remove free reactants, the precipitate was washed three times with DI water, and then dried in an oven overnight at 140 °C. The dried solid was then calcined at 500 °C for 3 h to obtain M1-MnO<sub>2</sub> NMs.

For the synthesis of semispherical M2-MnO<sub>2</sub> NMs, KMnO<sub>4</sub> (0.7 g, 4.4 mmol) was dispersed in 10 mL of DI water and the mixture was stirred for 5 min to give a dark purple solution. Then, NaOH (0.8 gr, 20 mmol) was added to the KMnO<sub>4</sub> solution, and stirring was continued for 24 h, until the solution turned brown. The obtained NMs were precipitated by centrifugation, washed three times with DI water, and dried in a vacuum desiccator at room temperature. The product was finally calcined at 500 °C for 3 h.

**Characterization of the synthesized MNMs.** UV–visible absorption spectra were acquired using a UV–visible spectrometer (Thermo Scientific, USA) in the wavelength range of 200–700 nm by using a 10 mm cuvette. Fourier transform infrared (FT-IR) spectra were obtained by FT-IR Magna 550, Nicolet using the KBr plates between 400 and 4000 cm<sup>-1</sup>. The X-ray diffraction (XRD) patterns were recorded on a Rigaku Ultima IV diffractometer, using Cu Ka radiation ( $\lambda$ =0.1542 nm), operated at 40 kV and 40 mA. The crystallite size was calculated by the Debye-Scherer equation (Eq. 1), where D is the particle size,  $\lambda$  is the X-ray wavelength, K is the Scherer's constant (K=0.94),  $\beta$  is full width at half maximum (FWHM), and  $\theta$  is the angle of diffraction.

$$D = \frac{K\lambda}{\beta \cos \theta} \tag{1}$$

The X-ray photoelectron spectroscopy (XPS) was measured on an X-ray photoelectron spectrometer using Al K $\alpha$  X-ray radiation source. The morphology of the MNMs was determined by field emission scanning electron microscope (FESEM, Tescan/Mira, Czech Republic). The energy dispersive X-ray spectroscopy (EDX, Shimadzu, Japan) was used to determine the elemental composition of the synthesized MNMs. The hydrodynamic diameter of MNMs was obtained from dynamic light scattering (DLS) measurements by a Zetasizer ZEN3600 (Malvern Instruments). The surface areas of the MNMs were analyzed using the Brunauer Emmett Teller (BET) method. The pore volume and pore size distribution were also determined using the Barrett–Joyner–Halenda (BJH) method. To measure the magnetic properties of the samples, a vibrating sample magnetometer (VSM, MDKB model) was used against an applied field of  $\pm$  20 kOe.

Peroxidase- and oxidase-like activities of the MNMs. The peroxidase-like activity of the MNMs was investigated by the catalytic oxidation of TMB in the existence of  $H_2O_2$ . Briefly, certain amounts of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs were separately suspended in phosphate-citrate buffer (0.15 M) to obtain different concentrations of the samples (1, 5, 10, 25, 50, 100  $\mu$ g/mL). 200  $\mu$ L of the each sample was added to each well of a 96-well plate along with 2  $\mu$ L of TMB solution (1.25 mM, ethanol solution) and 4  $\mu$ L of H<sub>2</sub>O<sub>2</sub>. Then, the plate was vibrated in the dark to provide a homogeneous mixture, and the UV-visible spectrum (500-800 nm) of the samples was recorded using a microplate reader. For each sample, we varied one of the parameters while keeping the other parameters constant to investigate the effect of pH, temperature, and sample concentration on the catalytic oxidation reaction of TMB. Absorbance at 652 nm was measured after the reaction for 10 min using UV-visible spectroscopy. The relative activity (%) was used as the index to optimize the experimental conditions, which was calculated through dividing the current absorbance by the maximum absorbance at 652 nm related to the specific experimental conditions. Subsequently, the TMB substrate was used to evaluate the oxidase-like activity of the MNMs in the absence of  $H_2O_2$ . The experiment was performed using 200  $\mu$ L of the samples suspended in phosphate-citrate buffer and 2  $\mu$ l of TMB. After incubation for 10 min, the UVvisible absorption spectroscopy (500-800 nm) was recorded for each sample. The effect of pH, temperature, and different concentrations of the samples was also investigated as described in peroxidase-like activity.

**Cell cytotoxicity and apoptosis assay.** The cytotoxicity of MNMs against MCF-7 and MCF-10A cell lines, was assessed using MTT method according to the standard protocol<sup>29</sup>. The cells were seeded in 96-well cell culture plates and incubated in DMEM and RPMI 1640 medium at 37 °C (cell density of  $4 \times 10^3$ ) with 5% CO<sub>2</sub> for 24 h. The cells were then exposed to a sample solution of the MNMs prepared at various concentrations of 0 (untreated), 10, 25, 50, and 100 µg mL<sup>-1</sup>. The treated cells were then incubated for an additional 24 and 48 h. After removing the medium solution and washing the cells 3 times with PBS, 200 µL of MTT solution (5 mg mL<sup>-1</sup>) was added to each well and the wells were then incubated for 4 h. The MTT solution was then replaced with DMSO (200 µL/well) in the dark. The plate was placed on a shaker for 15 min. Survival of the treated cells in each well was measured using the optical density (OD) at 570 nm in wells of an ELISA plate reader (Stat Fax 2100, USA) and normalized to the untreated control cells. The assay was evaluated with three replicates (n = 3).

Flow cytometry was also performed to define the cell death mechanism for treated and untreated MCF-7 cells. MCF-7 cells were incubated in a 6-well plate  $(3 \times 10^5 \text{ cells per well})$  with the MNMs (50 µg/mL) for 24 h. Untreated MCF-7 cells were considered as the control. Collected cells were stained with fluorescein isothiocyanate (FITC)-annexin V and propidium iodide (PI) apoptosis detection kit (Hoffman-La Roch Ltd, Basel, Switzerland). After 15 min, the ratio of apoptotic cells was determined by a flow cytometer (Partec CyFlow<sup>\*</sup>).

**Cellular uptake assay.** Cell internalization of MNMs was examined with a fluorescence microscope (BD FACS Calibur, San Jose, CA, USA). Briefly, 5 mg of rhodamine was dissolved in 1 mL of DI water. 1 mL of the MNMs suspensions were mixed with rhodamine solution overnight at room temperature and dark. Then, sodium carbonate buffer (1 M) was added to the mixture and stirring was continued for 20 min. Finally, unbound rhodamine was removed with an Amicon filter (molecular weight cut-off 100 kDa, Millipore, UK). After that, rhodamine-labeled M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs were incubated with MCF-7 and MCF-10A cell lines ( $5 \times 10^5$  cells per well) for 4 h and their cellular uptake was evaluated.

In addition, to measure the content of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs in MCF-7 and MCF-10A cells, the cells were seeded in Petri dishes ( $\emptyset$  6 cm) with a density of  $5 \times 10^5$  cells. After 48 h of seeding, the cells were incubated with MNMs ( $50 \mu g/mL$ ) for 6 h. Then, the cells were washed three times with 10 mL of cold PBS and detached with trypsin/EDTA. The Mn content in each cell line was determined by ICP-MS. Protein concentration, proportional to the number of cells, was defined from cell lysates by the Bradford method.

**Relaxivity measurement.** MRI measurements using a 1.5 T MRI scanner (Prisma, Siemens Healthcare, Erlangen, Germany) with a head neck coil at room temperature were performed to determine the potential use of the prepared MNMs as MRI contrast agents. The M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs were dispersed on the agarose gel at various concentrations (0.04, 0.08, 0.16, 0.32, and 0.64 mM). Dotarem was used at the same concentration as the control group. The T<sub>1</sub>-weighted image was obtained with the following parameters using a conventional spin echo sequence: TR/TE = 50, 200, 400, 600, 800, 1100, 1300, 1500, 1800, 2000/11 ms, slice thickness = 5 mm, field of view (FOV) = 250 mm × 250 mm, field of view =  $128 \times 128 \text{ mm}^2$ , matrix size of  $256 \times 256$ . The T<sub>2</sub>-weighted images were obtained using a multi-spin echo sequence with the same parameters as T<sub>1</sub>-weighted images acquisition except TR/TE = 3000/10, 30, 60, 90, 130, 170, 210, 240, 270, 350 ms, slice thickness = 5 mm. After image acquisition, the region of interest (ROI) signal strength was defined by ImageJ software (version 1.410). The relaxivity measurements were averaged to obtain single T1 and T<sub>2</sub> values. The T<sub>1</sub> and T<sub>2</sub> relaxation rate (R<sub>1</sub> and R<sub>2</sub>) was determined using the optimal single exponential function. Finally, r<sub>1</sub> and r<sub>2</sub> relaxation capacity was determined by linear curve fitting of R<sub>1</sub> (1/T<sub>1</sub>) and R<sub>2</sub> (1/T<sub>2</sub>) versus the MNMs concentrations.

**Cellular MR imaging.** MCF-7 and MCF-10A cell lines were grown in cell culture flasks under standard conditions (37 °C and 5% CO<sub>2</sub>), and the plates were incubated in DMEM and RPMI 1640 medium, respectively. MCF-7 and MCF-10A cells ( $10 \times 10^6$  cells/well) were exposed to different concentrations (0, 1, and  $10 \mu \text{g mL}^{-1}$ ) of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs for 6 h. Following incubation, the cells were washed three times with PBS buffer and re-suspended in PBS buffer before MR imaging. Cell phantoms were prepared using  $10 \times 10^6$  cells in agarose gel and placed in a rectangle tube with 0.5% agarose gel. All MRI measurements were performed with a 1.5 Tesla MRI system. For obtaining T<sub>1</sub>-weighted images, a spin-echo sequence was performed using the following parameters: TR/TE = 500/12 ms, matrix size =  $220 \times 320$ , slice thickness = 3 mm, FOV =  $82 \times 120$  mm, bandwidth = 140 Hz/Px. Finally, R<sub>1</sub> ( $1/T_1$ ) values were estimated by a monoexponential fitting algorithm.

**Statistical analysis.** The one-way analysis of variance (ANOVA) was used to determine statistical significance using the GraphPad Prism version 9.1.1 (GraphPad, San Diego, CA). All the data were reported as mean  $\pm$  standard deviation (SD). *P* value < 0.05 was considered statistically significant.

### **Results and discussion**

**Characterization of the synthesized MNMs.** UV-visible analysis was employed to evaluate completion of the reaction. After completion of the reaction, the characteristic absorption band of  $KMnO_4$  was disappeared at about 530 nm (Fig. 1a). In the meantime, the purple color of the  $KMnO_4$  solution was disappeared and, the color of the mixture turned dark brown. Also, the characteristic absorption band of  $Mn(NO_3)_2$  in the range of 200–300 nm disappeared. The synthesized M1-MnO<sub>2</sub> NMs showed a maximal absorbance around 410 nm, ascribed to the d–d transition of Mn ions in  $MnO_2^{30,31}$ . This is a clear indication of the formation of  $MnO_2$  NMs. Figure 1b shows that after adding NaOH to the KMnO<sub>4</sub> solution, the characteristic absorption band of KMnO<sub>4</sub> at 530 nm was also disappeared, and the color of the mixture turned brown. The synthesized M2-MnO<sub>2</sub> NMs



Figure 1. UV-visible spectra of (a)  $M1-MnO_2$  and (b)  $M2-MnO_2$  NMs.

showed maximum absorption at about 360 nm. The significant blue shift for M2-MnO<sub>2</sub> compared to M1-MnO<sub>2</sub> could be related to the different morphology of these nanostructures.

The chemical composition of the prepared MNMs was investigated by FTIR analysis. A broad band was appeared at around 3430 cm<sup>-1</sup> in both spectra, which could be attributed to the O–H stretching vibration. The weak band around 1630 cm<sup>-1</sup> could be also related to the O–H bending vibrations (Fig. 2a)<sup>32</sup>. These bands could be related to the adsorbed water molecules and the free hydroxyl groups in the structure of MnO<sub>2</sub> NMs. The peaks around 1384 and 731 cm<sup>-1</sup> could be attributed to the vibrations of the O–Mn–O bonds in the MnO<sub>2</sub> structure<sup>33</sup>. For both samples, the characteristic bands at 500–800 cm<sup>-1</sup> were observed. The peaks that appeared at 533 and 580 cm<sup>-1</sup> in the spectrum of M1-MnO<sub>2</sub> could be related to the Mn–O lattice vibration<sup>33,34</sup>. However, the position of the characteristic bands displayed some apparent changes in M2-MnO<sub>2</sub>. The absorption band related to the Mn–O–Mn vibration was appeared at around 553 cm<sup>-1</sup> in M1-MnO<sub>2</sub> and 607 cm<sup>-1</sup> in M2-MnO<sub>2</sub>.

XRD analysis was used to study the crystallinity of the prepared MNMs and to identify the phase of the crystals. It is well known that  $MnO_2$  has several polymorphs (types of  $\alpha$ ,  $\beta$ ,  $\gamma$ ,  $\delta$ , etc.), which are different in crystal structures<sup>35</sup>. The XRD patterns of the samples are shown in Fig. 2b. The XRD pattern of M1-MnO<sub>2</sub> NMs shows predominant peaks at  $2\theta = 12.59$ , 18.06, 28.67, 36.10, 37.54, 42.0, 49.80, 58.86, and 60.08 °, which are attributed to the (110), (200), (310), (400), (211), (301), (411), (600), and (521) crystal planes, respectively (Fig. 2bA). The presence of these diffraction peaks is ascribed to the  $\alpha$ -MnO<sub>2</sub> crystal phase, which is consistent with the database in the Joint Committee on Powder Diffraction Standards (JCPDS) card number of 44-0141<sup>36</sup>. No other peaks related to the impurity phases were observed. The crystallite diameter of M1-MnO<sub>2</sub> calculated by Debye-Scherer was 16.94 nm. Furthermore, the XRD peaks of M2-MnO<sub>2</sub> were appeared at  $2\theta = 12.42$ , 24.92, and 36.69°, which could be attributed to the crystal planes of (001), (002), and (111), respectively (Fig. 2bB). The presence of these sharp peaks in the XRD pattern of M2-MnO<sub>2</sub> NMs confirmed formation of the predominant phase of  $\delta$ - MnO<sub>2</sub> according to JCPDS card number of 80–1098<sup>37,38</sup>. The crystallite diameter of M2-MnO<sub>2</sub> calculated by Debye-Scherer was 14.55 nm. The results revealed that the applied method for the synthesis has a significant effect on the crystalline lattice of the prepared MnO<sub>2</sub> nanostructures<sup>37</sup>. Moreover, the sharp diffraction peaks indicate that the MnO<sub>2</sub> nanostructures are crystalline in nature.

To investigate the state of Mn, XPS analysis was performed. Figure 2c illustrates the scan XPS survey spectrum recorded from the M1-MnO<sub>2</sub> NMs in the range of 0–1100 eV. The appearance of Mn binding energy peaks (2*s*,  $2p^{3/2}$ ,  $2p^{1/2}$ , 3p, 3s) and O1s suggests the formation of MnO<sub>2</sub> without any contaminants and impurity peaks. The high-resolution XPS spectrum of Mn 2p reveals the spin–orbit doublet components located at ~ 656.87 and 645.47 eV, corresponding to the different binding energies of Mn  $2p^{1/2}$  and Mn  $2p^{3/2}$ , respectively (Fig. 2d). The spin energy separation between these two peaks is 11.40 eV, which is consistent with the literature reported XPS spectrum of MnO<sub>2</sub><sup>39,40</sup>. Moreover, the broad Mn  $2p^{1/2}$  and  $2p^{3/2}$  peaks are deconvoluted into two peaks due to the overlapping of Mn<sup>3+</sup> and Mn<sup>4+</sup> ions. Additionally, the Mn 3*s* spectrum consists of two peaks positioned at ~ 91.10 and 86.25 eV, corresponding to Mn 3*s* (2) and Mn 3*s* (1), respectively, with an energy separation of



**Figure 2.** (a) FT-IR spectra of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs. (b) XRD patterns of (A) M1-MnO<sub>2</sub>, (B) M2-MnO<sub>2</sub>. (c) A wide-scan XPS spectrum of M1-MnO<sub>2</sub>. Core level high-resolution XPS spectrum of (d) Mn 2p, (e) Mn 3s, and (f) O 1s energy levels.

4.85 eV (Fig. 2e). The splitting of Mn 3s spectrum can be due to the coupling of 3s electron and 3d valenceband electrons. Therefore, the results reveal that the sample includes mainly  $Mn^{4+}$  with some  $Mn^{3+}$  ions. In addition, the three binding energy peaks of the O 1s spectrum at 528.24, 531.02, and 533.83 eV, attributed to the Mn–O–Mn, Mn–OH, and H–O–H bonds, respectively (Fig. 2f), indicate the –2 oxidation state of oxygen<sup>13</sup>.

FESEM was used to evaluate morphology of the samples. As shown in Fig. 3a,b, M1-MnO<sub>2</sub> NMs showed a porous flower-like morphology, which created a porous structure with interconnected pores. The possible mechanism for the formation of this morphology could be the growth of manganese oxide nuclei during the Ostwald ripening process, resulting in the formation of a flower-like structure<sup>41</sup>. M2-MnO<sub>2</sub> NMs showed a nearspherical morphology, which tended to agglomerate (Fig. 3g). The calcination process increases the crystallinity. Also, it removes impurities resulting in the crystalline materials with better properties compared to their amorphous structures<sup>42</sup>. Moreover, an organic template such as TA, which is removed in the calcination process, can be used to prepare nanostructures with a unique porous morphology<sup>24</sup>. The corresponding TEM images of the MNMs are shown in Fig. 3c and Fig. 3h. Through the analysis of TEM images by imageJ software, the average size of flower-like and near-spherical MNMs was estimated to be 259 and 115 nm, respectively. The elemental composition of the MNMs was identified using EDX analysis. As shown in Fig. 3d, neither K nor N signals were detected in the EDX spectrum of M1-MnO2, and only Mn and O atoms were present, confirming formation of M1-MnO<sub>2</sub> NMs without any impurity. The absence of C peaks in the EDX spectrum confirmed the removal of TA during the calcination process. Similarly, the EDX spectrum of M2-Mn $O_2$  showed no peaks related to the presence of K (Fig. 3i). The data extracted from the EDX analysis of the MNMs (tables inset in Fig. 3d,i) indicates that the prepared MNMs have a composition of Mn and O atoms, which corresponds to the MnO<sub>2</sub> formula<sup>43</sup>. The elemental mapping images showed uniform distribution of Mn as well as O in the prepared MNMs (Fig. 3e,j). Besides, the hydrodynamic diameter of the MNMs in water was determined by DLS analysis (Fig. 3f,k). The mean size diameter of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs were  $285 \pm 24.17$  and  $129 \pm 10.48$  nm, respectively. Average size of the NPs used in MRI is about 3.0 to 350 nm<sup>44</sup>. Since the colloidal stability of nanostructures is a critical issue for biological application, the stability of flower-like MnO<sub>2</sub> NMs was also evaluated by DLS analysis in different media (Fig. S1). The size of flower-like  $MnO_2$  NM did not change significantly during 7 days of incubation in both PBS (pH = 7.4) and DMEM containing 10% FBS. However, flocculation of flower-like MnO<sub>2</sub> in DI water resulted a little change in the hydrodynamic diameter, indicating the relatively poor stability of flower-like MnO<sub>2</sub> in water over time. The results confirmed the stability of flower-like MnO<sub>2</sub> for in vivo biomedical applications.

The surface area and pore size distribution of the synthesized MNMs with different morphologies are shown in Fig. 4. The BET surface area was investigated by measuring the N<sub>2</sub> adsorption–desorption isotherms, and the pore size distribution was determined from the BJH analysis of N<sub>2</sub> adsorption isotherms<sup>45</sup>. The measurements showed that the BET surface area of M1-MnO<sub>2</sub> NMs was 78.47 m<sup>2</sup> g<sup>-1</sup> and the pore size distribution was 5.27 nm. The BET surface area of M2-MnO<sub>2</sub> NMs was estimated to be 20.05 m<sup>2</sup> g<sup>-1</sup> and there was a small pore distribution peak at 2.73 nm. Values of the surface area, total pore volume, and mean pore size of the MnO<sub>2</sub> samples can be found in Table 1. The results suggest that with the increase of the specific surface area, the pore volume and pore size increase. This could be due to the presence of interconnected pores<sup>46</sup>. M1-MnO<sub>2</sub> NMs showed the highest BET surface area, probably because the pores were large enough to host N<sub>2</sub> molecules<sup>45</sup>. The morphology of M2-MnO<sub>2</sub> which consists of agglomerates of near-spherical particles can negatively affect the formation of pores in the material and reduce the total pore volume, which leads to N<sub>2</sub> molecules to be adsorbed mainly on the external surface. It could also be implied that after calcination and removal of TA, the surface area increases due to the appearance of new pores, which increases total pore volume and average pore size<sup>47</sup>. Furthermore, porous nanostructures possess significant properties, such as high surface area, making them valuable for various applications<sup>48</sup>.

The magnetic hysteresis (M-H) curve of the MNMs at 300 K using VSM method is shown in Fig. S2. The  $MnO_2$  nanostructures, synthesized in this work, displayed an early linear relationship between their magnetization and applied field, indicating that the MNMs had the paramagnetic state<sup>49</sup>. However, a small coercivity at the low applied manetic fields (-2 kOe - 2 KOe) was detected in the M2-MnO<sub>2</sub> sample, suggesting a very weak ferromagnetic-like state<sup>50</sup>. The magnetic saturation (Ms) of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> was 0.2 and 0.4 emu/g, respectively. Based on previous studies, it is believed that the Ms of magnetic NMs depends not only on the particle size but also on their surface properties<sup>51,52</sup>. Flower-like NMs behave differently compared to similar single-core nanoparticles. They are composed of different cores having similar aspects, so they show better magnetic properties due to the reduced anisotropy and large surface area<sup>53,54</sup>. Therefore, the better magnetic performance of flower-like M1-MnO<sub>2</sub> NMs could be attributed to their large specific surface area compared to M2-MnO<sub>2</sub> NMs.

**Dual-enzyme mimetic activities of MNMs.** Peroxidase- and oxidase-like nanozymes catalyze the oxidation of TMB to an aqueous oxidized product (oxTMB) in the presence and absence of  $H_2O_2$ , respectively, with a major absorption peak at 652 nm. M1-MnO<sub>2</sub> NMs with flower-like morphology showed relatively higher peroxidase-like activity than M2-MnO<sub>2</sub> NMs with near-spherical morphology (Fig. 5a). The properties of the nanoenzymes depend on the reaction conditions<sup>55</sup>. As shown in Fig. 5b,c, the absorbance at 652 nm increased with increasing the concentration of the MNMs. The effect of pH, temperature, and concentration of the samples on peroxidase-like activity were also evaluated, and absorbance at 652 nm was recorded for each condition. As shown in Fig. 5d, the peroxidase-like activity reached a higher level in an acidic buffer (pH 4–5.5) than near neutral buffer. The highest peroxidase-like activity was obtained at 43 °C (Fig. 5e). The optimal dose of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs was 100 µg/mL (Fig. 5f). Therefore, the optimal conditions for the maximum peroxidase-like catalytic activity were observed as pH=5.5, T=43 °C, and 100 µg/mL of the MNMs.



**Figure 3.** FESEM images of (**a**, **b**) M1-MnO<sub>2</sub> (scale bar: 1  $\mu$ m and 500 nm) and (**g**) M2-MnO<sub>2</sub> (scale bar: 500 nm). TEM images of (**c**) M1-MnO<sub>2</sub> and (**h**) M2-MnO<sub>2</sub> (scale bar: 300 nm, inset in **c**: 100 nm). EDX elemental analysis of (**d**) M1-MnO<sub>2</sub> and (**i**) M2-MnO<sub>2</sub>; Insets: Quantitative analysis. Elemental mapping of (**e**) M1-MnO<sub>2</sub> and (**j**) M2-MnO<sub>2</sub> (scale bar: 10  $\mu$ m): red and green points represent manganese and oxygen, respectively. Hydrodynamic diameter of (**f**) M1-MnO<sub>2</sub> and (**k**) M2-MnO<sub>2</sub> characterized by DLS.

Subsequently, TMB was used as a substrate to investigate the oxidase-like activity of the MNMs in the absence of  $H_2O_2$ . Figure 6a shows that both M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs catalyze the rapid oxidation of TMB in the absence of  $H_2O_2$ . The intensity of blue color and absorption at 652 nm increased with increasing the concentration of the MNMs (Fig. 6b,c). The oxidase mimics exhibited high activity at pH = 6.8 and T = 37 °C (Fig. 6d,e). When



**Figure 4.** (A) The  $N_2$  adsorption–desorption isotherms of (a) M1-MnO<sub>2</sub> and (b) M2-MnO<sub>2</sub> in different morphologies. (B) BJH pore size distribution.

Samples	BET surface area (m <sup>2</sup> g <sup>-1</sup> )	Total pore volume (cm <sup>3</sup> g <sup>-1</sup> )	BJH pore size (nm)
M1-MnO <sub>2</sub>	78.47	0.35	5.27
M2-MnO <sub>2</sub>	20.05	0.07	2.73

Table 1. Surface areas and pore structures of the synthesized MNMs with different morphologies.



**Figure 5.** (a) Comparison of peroxidase-like activity between M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> after adding 1.25 mM TMB in the presence of  $H_2O_2$ . The absorbance spectra of (b) M1-MnO<sub>2</sub> and (c) M2-MnO<sub>2</sub>, where the peak at 650 nm indicates the oxTMB (Inset: visual color changes of peroxidase-like activity proportional to increasing the concentration). Effects of (d) pH, (e) temperature, and (f) concentration of the MNMs. The maximum activity in each graph of the same variable was set to 100% (n=3, P < 0.05).



**Figure 6.** (a) Comparison of oxidase-like activity between M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> after adding TMB (1.25 mM) in the absence of  $H_2O_2$ . The absorbance spectra of (b) M1-MnO<sub>2</sub> and (c) M2-MnO<sub>2</sub>, where the peak at 650 nm indicates the oxTMB (Inset: visual color changes of oxidase-like activity proportional to increasing the concentration). Effects of (d) pH, (e) temperature, and (f) concentration of the MNMs. The maximum activity in each graph of the same variable was set to 100%. (n = 3, P < 0.05).

the concentration of M1-MnO<sub>2</sub> NMs was in the range of 1–100 µg/mL, the absorption increased by increasing the concentration (Fig. 6f). When the M1-MnO<sub>2</sub> NMs concentration was higher than 100 µg/mL, the absorption decreased at 652 nm. This could be caused by the catalytic oxidation of oxTMB to biphenyl quinone in the presence of excess amount of M1-MnO<sub>2</sub><sup>56</sup>. In the case of M2-MnO<sub>2</sub> NMs, the maximum oxidase-like catalytic activity was at a concentration of 50 µg/mL and the absorption decreased above this concentration. This could be due to the high tendency of near-spherical M2-MnO<sub>2</sub> NMs to agglomeration, affecting the catalytic activity of nanozymes<sup>55</sup>. Accordingly, the optimal conditions for the maximum oxidase-like catalytic activity were pH = 6.8, T = 37 °C, 100 µg/mL for M1-MnO<sub>2</sub> and 50 µg/mL for M2-MnO<sub>2</sub> NMs. The results suggest that M1-MnO<sub>2</sub> NMs show more peroxidase- and oxidase-like activities compare to M2-MnO<sub>2</sub> NMs. These characteristics are mainly due to its morphology with a large BET surface area, allowing it to have a higher affinity towards TMB<sup>57</sup>. The crystal structure, morphology, and specific surface area significantly affect the activity of enzyme mimics<sup>56,58</sup>. It has been found that a larger surface area and better dispersion of NMs significantly improve their catalytic activity<sup>55</sup>. Altogether, flower-like M1-MnO<sub>2</sub> NMs can maintain aceptable nanozyme activity in a range of pH, temperature, and concentration, providing a bright prospect for future applications, especially cancer therapy.

Cell cytotoxicity and apoptosis assay. To evaluate safety of the MNMs, a cytotoxicity assay was performed using MTT in both cancerous MCF-7 and normal MCF-10A cell lines. The dose-(10, 25, 50, and 100 µg/mL) and time-dependent (24 and 48 h) cytotoxicity profiles were obtained for each sample, M1-MnO<sub>2</sub> and  $M2-MnO_2$ . As shown in Fig. 7, no significant cytotoxicity was observed at various concentrations of  $M1-MnO_2$ and M2-MnO<sub>2</sub> during 24 h of incubation (Fig. 7a,c). Even at a concentration of 100  $\mu$ g/mL, the cell viability remained above 88%, indicating the biocompatibility of the MNMs. In our study, the decrease in cell survival with increasing the concentration was not significant in both samples compared to the control group (untreated cells), making the MnO<sub>2</sub> NMs more favorable for biomedical applications compared to Mn<sup>2+</sup>-based CAs. Besides, by increasing the incubation time to 48 h, the cell viability decreased with a concentration-dependent trend. Cell viability in normal cells after 48 h of incubation for both samples was higher than that of in cancer cells. The highest cytotoxicity of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs on cancer cells was observed at concentrations above 50 and 100  $\mu$ g/mL, respectively (\*P<0.05) (Fig. 7b,d). At a concentration of 100  $\mu$ g/mL, a decrease in cell viability in cancer cells treated with M1-MnO2 was probably due to the acidic internal environment of cancer cells. In addition, we demonstrated that M1-MnO<sub>2</sub> NMs had dual enzyme-mimetic activities at acidic pH (5.5–6.8). The cell viability of MCF-7 cells in the presence of spherical MnO<sub>2</sub> was reported to be  $45\%^{59}$ . Wang et al.<sup>60</sup> demonstrated that the nanoflowers had little cytotoxicity on normal cells, but they could induce cancer cell death, indicating that the flower-like nanostructures can inhibit cancer cell growth. The performance



**Figure 7.** Cell viability of MCF-10 A and MCF-7 cells after incubation with M1-MnO<sub>2</sub> NMs (**a**: 24 and **b**: 48 h) and M2-MnO<sub>2</sub> NMs (**c**: 24 and **d**: 48 h) at varying concentrations (\*P<0.05). Flow cytometry assay shows the apoptotic rates of MCF-7 cells after treatment; (**e**) control, (**f**) M1-MnO<sub>2</sub>, and (**g**) M2-MnO<sub>2</sub> NMs; Q1: necrotic cells, Q2: late-stage apoptotic cells, Q3: early-stage apoptotic cells, Q4: viable cells.

of the flower-like mesoporous  $MnO_2$  NMs was better than the reported values<sup>61,62</sup>. Therefore, the M1-MnO<sub>2</sub> NMs have the potential to be used as MRI CA to identify cancer cells, and since they are selectively cytotoxic to cancer cells, they can also be used against cancerous cells, without harming normal cells. Flow cytometry was performed to evaluate the cell death mechanism for MCF-7 cells treated with 50 µg/mL of MNMs (Fig. 7e–g). Although more than 80% of the cells survived, the late-stage apoptosis rate of the cells after incubation with flower-like M1-MnO<sub>2</sub> was slightly higher than that of incubation with near-spherical M2-MnO<sub>2</sub> NMs. The results clearly showed that the flower shape promotes the cytotoxicity of MNM in cancer cells. It has been reported that flower-like nanostructures can disrupt the cell wall better than spherical ones, thereby increasing the death of human endothelial cells<sup>63-65</sup>. Sultana et al. found that flower-shaped NPs have a higher surface area than spherical NPs, so they are more potent to interact with the cell membrane due to the spiky surface. The morphology-dependent cell death mechanism supports the hypothesis that surface roughness is responsible for

cell membrane disruption, and is a critical parameter in cellular internalization of nanostructures<sup>64</sup>. In this study, the flower-like mesoporous M1-MnO<sub>2</sub> exhibited a relatively high surface area for biological interactions, which can increase the ability to kill cancer cells. These findings are consistent with the results obtained from the MTT assay. Therefore,  $MnO_2$  NMs with flower shape can be a potential candidate, improving diagnostic sensitivity and therapeutic efficiency.

Cellular uptake. Prior studies approved that the physical parameters of NPs, including size, shape, porosity, surface area, pore volume, and stable aqueous dispersibility affect the interaction between NPs and cell membrane, controlling the cell penetration<sup>66,67</sup>. Nanostructures with a well-defined shape are internalized by non-specific cellular uptake<sup>68</sup>. In this study, in vitro cellular uptake was evaluated using fluorescence microscopy and amount of M1-MnO2 and M2-MnO2 NMs taken up by MCF-7 and MCF-10A cells was estimated (Fig. 8a,b). The fluorescence intensity of cell uptake in cancer cells was stronger than normal cells. The increase in cellular uptake may be due to the higher activity of cancer cells than normal cells which could absorb the MNMs via interactions on the cell membrane. Moreover, the permeability of the nanostructures is influenced by the contact surface with the lipid layer<sup>69</sup>. In non-spherical structures, due to the greater contact surface, the interaction with the membrane increases, and subsequently the cell internalization efficiency improves compared to spherical structures<sup>70</sup>. Therefore, the higher cellular uptake of flower-like M1-MnO<sub>2</sub> NMs could be due to the higher surface area and more surface roughness compared to near-spherical M2-MnO<sub>2</sub> NMs. The content of M1-MnO<sub>2</sub> and M2-MnO2 in MCF-7 and MCF-10A cells was also determined by ICP-MS. Fig. S3 shows the amount of the internalized Mn normalized to the total protein content of the cell. Internalized Mn values were significantly higher for MCF-7 incubated in the presence of M1-MnO<sub>2</sub> than M2-MnO<sub>2</sub> (P<0.05). On the contrary, Mn content in MCF-10A cells was low, with no significant difference for two types of MNMs (P > 0.05). Our findings suggest that flower-like mesoporous MnO<sub>2</sub> NMs exhibit more Mn content in cancer cells due to the more nonspecific cellular uptake and faster internalization rate compared to the spherical shape.

**Relaxivity.** To investigate the effectiveness of the MNMs as a  $T_1$  MRI contrast agent,  $T_1$ -weighted images were obtained using a clinical 1.5 T MRI scanner. The M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> showed slightly brighter  $T_1$ -weighted images than commercially approved MRI contrast agent (Dotarem) in a phantom model (Fig. 9a).







**Figure 9.** (a)  $T_1$ -weighted images, (b) the longitudinal relaxivity, (c)  $T_2$ -weighted images, (d) and the transverse relaxivity of M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs dispersed in water.

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It was found that M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs effectively shortened the longitudinal relaxation time  $(T_1)$  and significantly increased the signal intensity in T<sub>1</sub>-weighted images in comparison with Dotarem. Also, the degree of the bright contrast enhancement in T<sub>1</sub>-weighted images was directly related to the concentration of Mn ions. The longitudinal relaxivity values (r1) for M1-MnO2, M2-MnO2, and Dotarem were achieved at 5.73, 3.17, and 2.39 m $M^{-1}$  s<sup>-1</sup>, respectively (Fig. 9b). The obtained r<sub>1</sub> value was comparable to the previously reported Mn nanoparticles<sup>71,72</sup>. The difference between the prepared MnO<sub>2</sub> NMs in this study could be due to the significant difference in morphologies, pore volume, specific surface area, and subsequently potential H<sub>2</sub>O absorption sites of the MNMs. Some studies showed that samples with large pore volume provide high  $r_1^{12,73}$ . This trend could be described by different rotational dynamics, where the large NPs are likely to rotate more slowly than smaller NPs with lower moments of inertia<sup>74,75</sup>. According to SEM and BET results, M1-MnO<sub>2</sub> NMs have a uniform porous structure with a higher specific surface area and pore volume than M2-MnO<sub>2</sub> NMs. Therefore, the morphology of M1-MnO<sub>2</sub> NMs could result in the absorption of more water molecules in the structure, which leads to an increase in the  $r_1$  relaxivity value. The decrease in the  $r_1$  relaxivity value in M2-MnO<sub>2</sub> compared to M1-MnO<sub>2</sub> could be due to its slightly higher polydispersity. In addition, the aggregation of M2-MnO<sub>2</sub> NMs could reduce the  $T_1$  contrast ability<sup>76</sup>. However, no significant signal intensity changes were observed in  $T_2$ - weighted images of the MNMs, indicating that MNMs had a small T<sub>2</sub> effect (Fig. 9c). The transverse relaxivity values (r<sub>2</sub>) for M1-MnO<sub>2</sub>, M2-MnO<sub>2</sub> NMs and Dotarem were 5.49, 3.78, and 3.36 mM<sup>-1</sup> s<sup>-1</sup>, respectively (Fig. 9d). The low  $r_2/$  $r_1$  ratio value for M1-MnO<sub>2</sub> indicated that the  $T_1$ -shortening effect was dominant over the  $T_2$  effect, indicating a strong contrast enhancement in the T<sub>1</sub>-weighted images. In this regard, the obtained results suggest that M1-MnO<sub>2</sub> NMs have the potential to be used as  $T_1$  MRI contrast agents.

**Cellular MR imaging.** To confirm the diagnostic ability of the  $MnO_2$  NMs as a  $T_1$  MRI contrast agent, MCF-7 and MCF-10A cells were incubated with MNMs at different concentrations (0, 0.1, and 1 µg/mL), and MR signal intensity was evaluated. As shown in Fig. 10a,  $T_1$ -weighted MR images gradually became brighter as the concentration of the MNMs increased in the treated cells. The concentration-dependent brightening effect in  $T_1$ -weighted MR images is more obvious in the lower pH environment of MCF-7 cells, while the MR



**Figure 10.** (a)  $T_1$ -weighted images and longitudinal relaxation rate of (b) MCF-7 and (c) MCF-10A cells treated with M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> NMs at different concentrations (n = 3, \**P*<0.05, \*\**P*<0.01).

signals appear relatively weaker in MCF-10A normal cells with the natural pH of 7.4. Moreover, the longitudinal relaxation rate ( $R_1$ ) of MCF-7 cells treated with M1-MnO<sub>2</sub> and M2-MnO<sub>2</sub> was significantly higher than that of MCF-10A cells (Fig. 10b). The increase in  $R_1$  value in MCF-7 cells could be related to the accumulation of paramagnetic  $Mn^{+2}$  in MCF-7 cells, induced by the MnO<sub>2</sub> nanostructures, resulted from the acidic internal environment of the cancer cells compared to the normal cells. MnO<sub>2</sub> is known to be stable at neutral and basic pH, but it could be decomposed to  $Mn^{+2}$  and  $O_2$  under acidic pH<sup>59</sup>. Furthermore, since  $Mn^{+2}$  with five unpaired electrons could shorten the  $T_1$  of water protons and enhance the  $T_1$  signal intensity, the presence of  $Mn^{+2}$  in the developed  $MnO_2$  NMs enables  $T_1$ -based metabolic imaging<sup>59,77</sup>. Figure 10 shows that the  $R_1$  of M1-MnO<sub>2</sub> in the presence of MCF-7 cancer cells was higher than that of M2-MnO<sub>2</sub> NMs, which could be ascribed to the high accessibility of water molecules to the  $Mn^{+2}$  paramagnetic centers. Hence, M1-MnO<sub>2</sub> are more suitable as a  $T_1$  MRI contrast agent. M1-MnO<sub>2</sub> may act as a promising pH-sensitive cellular and metabolic MR imaging agent, particularly useful for tumor imaging having the acidic tumor microenvironment. The obtained results of this study was comparable to what achieved in previous works (Table S1).

#### Conclusion

In thgis work a simple and green method using TA as a template was introduced for the preparation of novel flower-like mesoporous MnO<sub>2</sub> nanomaterials (M1-MnO<sub>2</sub>), with hydrodynamic size of ~ 285 nm, and relatively large surface area, high pore volume, as well as appropriate paramagnetic behavior compared to near-spherical M2-MnO<sub>2</sub>. The paramagnetic property of the MNMs was strongly dependent on the shape and surface area of the prepared samples, so the flower-like M1-MnO<sub>2</sub> with the higher surface area showed better paramagnetic properties than near-spherical M2-MnO<sub>2</sub>. It was found that M1-MnO<sub>2</sub> NMs had inetresting peroxidase-and oxidase-like activities. Based on the in vitro MRI studies, M1-MnO<sub>2</sub> NMs with mesoporous flower-like morphology showed promising longitudinal relaxivity value ( $r_1 = 5.73 \text{ mM}^{-1} \text{ s}^{-1}$ ), with more efficient contrast enhancement effect compared to M2-MnO<sub>2</sub> NMs having near-spherical morphology. The longitudinal relaxation rate of M1-MnO<sub>2</sub> NMs was higher in the presence of MCF-7 cancer cells, which could be attributed to their more porous structure and high accessibility of water molecules to the Mn<sup>+2</sup> paramagnetic centers. The obtained results revealed that by controlling the shape, size, and specific surface area of the MNMs as CA, the efficiency of MR imaging could be improved. *In vivo* studies on the synthesized flower-like M1-MnO<sub>2</sub> NMs with dual-enzyme mimetic activities for targeted photodynamic cancer therapy will be our future purposes.

#### Data availability

The datasets used and/or analysed during the current study available from the corresponding author on reasonable request.

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#### References

- Ning, S. et al. Cancer cell membrane-coated C-TiO<sub>2</sub> hollow nanoshells for combined sonodynamic and hypoxia-activated chemotherapy. Acta Biomater. 152, 562–574 (2022).
- Liu, D. et al. Liquid exfoliation of ultrasmall zirconium carbide nanodots as a noninflammatory photothermal agent in the treatment of glioma. Biomaterials 292, 121917 (2023).
- 3. Guo, W. *et al.* Platelet membrane-coated C-TiO<sub>2</sub> hollow nanospheres for combined sonodynamic and alkyl-radical cancer therapy. *Nano Res.* **16**, 782–791 (2023).
- 4. Weissleder, R. & Pittet, M. J. Imaging in the era of molecular oncology. Nature 452, 580-589 (2008).
- Zhang, K. et al. Marriage strategy of structure and composition designs for intensifying ultrasound & MR & CT trimodal contrast imaging. ACS Appl. Mater. Interfaces 7, 18590–18599 (2015).
- 6. Frangioni, J. V. New technologies for human cancer imaging. Clin. Oncol. 26, 4012 (2008).
- 7. Cheong, B. Y., Wilson, J. M., Preventza, O. A. & Muthupillai, R. Gadolinium-based contrast agents: Updates and answers to typical questions regarding gadolinium use. *Tex. Heart Inst. J.* 49, e217680 (2022).
- 8. Pan, D., Schmieder, A. H., Wickline, S. A. & Lanza, G. M. Manganese-based MRI contrast agents: Past, present and future. *Tetrahedron* 67, 8431 (2011).
- 9. Peng, X.-H. et al. Targeted magnetic iron oxide nanoparticles for tumor imaging and therapy. Int. J. Nanomed. 3, 311 (2008).
- Gholibegloo, E. et al. Folic acid decorated magnetic nanosponge: An efficient nanosystem for targeted curcumin delivery and magnetic resonance imaging. J. Colloid Interface Sci. 556, 128–139 (2019).
- Zhou, Z. & Lu, Z. R. Gadolinium-based contrast agents for magnetic resonance cancer imaging. Wiley Interdiscip. Rev. Nanomed. Nanobiotechnol. 5, 1–18 (2013).
- 12. Cai, X. *et al.* Manganese oxide nanoparticles as MRI contrast agents in tumor multimodal imaging and therapy. *Int. J. Nanomed.* 14, 8321 (2019).
- Wang, X. et al. A novel manganese chelated macromolecular MRI contrast agent based on O-carboxymethyl chitosan derivatives. Colloids Surf. B. 183, 110452 (2019).
- Pan, D. *et al.* Revisiting an old friend: Manganese-based MRI contrast agents. Wiley Interdiscip. Rev. Nanomed. Nanobiotechnol. 3, 162–173 (2011).
- 15. Wen, M. *et al.* Multifunctional hemoporfin-Cu9S8-MnO2 for magnetic resonance imaging-guided catalytically-assisted photothermal-sonodynamic therapies. *J. Colloid Interface Sci.* **626**, 77–88 (2022).
- Pan, D. *et al.* Ligand-directed nanobialys as theranostic agent for drug delivery and manganese-based magnetic resonance imaging of vascular targets. J. Am. Chem. Soc. 130, 9186–9187 (2008).
- 17. Liu, X. et al. BSA-templated MnO2 nanoparticles as both peroxidase and oxidase mimics. Analyst 137, 4552-4558 (2012).
- Qin, R. et al. Fe-coordinated carbon nanozyme dots as peroxidase-like nanozymes and magnetic resonance imaging contrast agents. ACS Appl. Bio Mater. 4, 5520–5528 (2021).
- Han, L., Shi, J. & Liu, A. Novel biotemplated MnO<sub>2</sub> 1D nanozyme with controllable peroxidase-like activity and unique catalytic mechanism and its application for glucose sensing. Sens. Actuators B Chem. 252, 919–926 (2017).
- Liu, J. et al. MnO2 nanosheets as an artificial enzyme to mimic oxidase for rapid and sensitive detection of glutathione. Biosens. Bioelectron. 90, 69–74 (2017).
- Chevallier, P. *et al.* Tailored biological retention and efficient clearance of pegylated ultra-small MnO nanoparticles as positive MRI contrast agents for molecular imaging. *J. Mater. Chem. B.* 2, 1779–1790 (2014).
- 22. He, D. *et al.* Redox-responsive degradable honeycomb manganese oxide nanostructures as effective nanocarriers for intracellular glutathione-triggered drug release. *Chem. Commun.* **51**, 776–779 (2015).
- Luo, Y. et al. Facile synthesis and functionalization of manganese oxide nanoparticles for targeted T1-weighted tumor MR imaging. Colloids Surf. B. 136, 506–513 (2015).
- 24. Ahmad, T. Reviewing the tannic acid mediated synthesis of metal nanoparticles. J. Nanotechnol. 2014, 1-11 (2014).
- Hou, C., Wang, Y., Zhu, H. & Wei, H. Preparation of mesopourous Fe<sub>3</sub>O<sub>4</sub> nanoparticle with template reagent: Tannic acid and the catalytic performance. J. Taiwan Inst. Chem. Eng. 60, 438–444 (2016).
- Javdani, H. et al. Tannic acid-templated mesoporous silica nanoparticles as an effective treatment in acute ferrous sulfate poisoning. Microporous Mesoporous Mater. 307, 110486 (2020).
- Gao, Z. & Zharov, I. Large pore mesoporous silica nanoparticles by templating with a nonsurfactant molecule, tannic acid. Chem. Mater. 26, 2030–2037 (2014).
- Saowalak, K., Titipun, T., Somchai, T. & Chalermchai, P. Iron (III)-tannic molecular nanoparticles enhance autophagy effect and T1 MRI contrast in liver cell lines. Sci. Rep. 8, 1–13 (2018).
- Wang, X. et al. Liquid exfoliation of TiN nanodots as novel sonosensitizers for photothermal-enhanced sonodynamic therapy against cancer. Nano Today 39, 101170 (2021).
- Hoseinpour, V., Souri, M. & Ghaemi, N. Green synthesis, characterisation, and photocatalytic activity of manganese dioxide nanoparticles. *Micro Nano Lett.* 13, 1560–1563 (2018).
- Jaganyi, D., Altaf, M. & Wekesa, I. Synthesis and characterization of whisker-shaped MnO<sub>2</sub> nanostructure at room temperature. *Appl. Nanosci.* 3, 329–333 (2013).
- 32. Zhang, H. *et al.* Efficient removal of Pb (II) ions using manganese oxides: The role of crystal structure. *RSC Adv.* 7, 41228–41240 (2017).
- Ashokkumar, K., Dhanapandian, S., Suthakaran, S., Krishnakumar, N. & Anandan, M. Synthesis of MnO<sub>2</sub> nanoparticles and its effective utilization as high-performance of supercapacitor. *Mater. Today.* 49, 2675–2678 (2022).
- Kang, L., Zhang, M., Liu, Z.-H. & Ooi, K. IR spectra of manganese oxides with either layered or tunnel structures. Spectrochim. Acta A Mol. Biomol. Spectrosc. 67, 864–869 (2007).
- Nawaz, F. *et al.* Selection of active phase of MnO<sub>2</sub> for catalytic ozonation of 4-nitrophenol. *Chemosphere* 168, 1457–1466 (2017).
   Sannasi, V. & Subbian, K. Influence of *Moringa oleifera* gum on two polymorphs synthesis of MnO<sub>2</sub> and evaluation of the pseudo-
- capacitance activity. J. Mater. Sci. Mater. **31**, 17120-17132 (2020). 37. Huang, X., Cui, W., Yu, J., Lu, S. & Liao, X. Preparation of mesoporous MnO2 catalysts with different morphologies for catalytic
- ozonation of organic compounds. Catal. Lett. 152, 1441–1450 (2022).
  7. Fidang, X., Sui, W., J., Lu, S. & Elab, X. Heparatholo interoptions into 2 catalysis with uniferent interprinting is in catalysic ozonation of organic compounds. Catal. Lett. 152, 1441–1450 (2022).
  8. Zhoo, B., Dan, Wu, Y., Sui, Y., Barto, K., Karabarta, C., Karabarta, S., Kara
- Zhao, B., Ran, R., Wu, X. & Weng, D. Phase structures, morphologies, and NO catalytic oxidation activities of single-phase MnO<sub>2</sub> catalysts. *Appl. Catal. A-Gen.* 514, 24–34 (2016).
- 39. Wang, Z. et al. Biomimetic nanoflowers by self-assembly of nanozymes to induce intracellular oxidative damage against hypoxic tumors. *Nat. Commun.* 9, 3334 (2018).
- Deng, R., Xie, X., Vendrell, M., Chang, Y.-T. & Liu, X. Intracellular glutathione detection using MnO<sub>2</sub>-nanosheet-modified upconversion nanoparticles. J. Am. Chem. Soc. 133, 20168–20171 (2011).
- Chen, Q. et al. Dopamine-assisted preparation of Fe<sub>3</sub>O<sub>4</sub>@ MnO2 yolk@ shell microspheres for improved pseudocapacitive performance. *Electrochim. Acta* 317, 628–637 (2019).

- 42. Kim, M. G. *et al.* Effects of calcination temperature on the phase composition, photocatalytic degradation, and virucidal activities of TiO<sub>2</sub> nanoparticles. *ACS Omega* **6**, 10668–10678 (2021).
- Panahi-Kalamuei, M., Motevalli, K. & Aliabadi, M. Rice-like MnO2 nanoparticles: simple and novel thermal decomposition synthesis, characterization and photocatalytic activity using new precursor. J. Mater. Sci. Mater. 27, 4631–4635 (2016).
- 44. Shokrollahi, H. Contrast agents for MRI. Mater. Sci. Eng. C 33, 4485-4497 (2013).
- Zhang, Y., Yang, Y., Zhang, Y., Zhang, T. & Ye, M. Heterogeneous oxidation of naproxen in the presence of α-MnO<sub>2</sub> nanostructures with different morphologies. *Appl. Catal. B.* 127, 182–189 (2012).
- 46. Estrada-Flores, S., Martínez-Luévanos, A., Perez-Berumen, C. M., García-Cerda, L. A. & Flores-Guia, T. E. Relationship between morphology, porosity, and the photocatalytic activity of TiO<sub>2</sub> obtained by sol-gel method assisted with ionic and nonionic surfactants. *Bol. Soc. Esp. Ceram. Vidr.* 59, 209–218 (2020).
- Huang, W. L., Liang, K. M., Cui, S. H. & Gu, S. R. Influence of calcination procedure on porosity and surface fractal dimensions of silica xerogels prepared under different evaporation conditions. J. Colloid Interface Sci. 231, 152–157 (2000).
- 48. Khan, I., Saeed, K. & Khan, I. Nanoparticles: Properties, applications and toxicities. Arab. J. Chem. 12, 908–931 (2019).
- 49. Li, W. et al. Performance modulation of α-MnO<sub>2</sub> nanowires by crystal facet engineering. Sci. Rep. 5, 8987 (2015).
- 50. Sebayang, K. et al. in IOP Conference Series: Materials Science and Engineering, 012119 (IOP Publishing, 2018).
- Jun, Y.-W. et al. Nanoscale size effect of magnetic nanocrystals and their utilization for cancer diagnosis via magnetic resonance imaging. J. Am. Chem. Soc. 127, 5732–5733 (2005).
- Roca, A. G., Marco, J. F., Morales, M. D. P. & Serna, C. J. Effect of nature and particle size on properties of uniform magnetite and magnemite nanoparticles. J. Phys. Chem. C. 111, 18577–18584 (2007).
- 53. Hugounenq, P. et al. Iron oxide monocrystalline nanoflowers for highly efficient magnetic hyperthermia. J. Phys. Chem. C 116, 15702-15712 (2012).
- Saeed, M. et al. Controllable synthesis of Fe<sub>3</sub>O<sub>4</sub> nanoflowers: Enhanced imaging guided cancer therapy and comparison of photothermal efficiency with black-TiO<sub>2</sub>. J. Mater. Chem. B 6, 3800-3810 (2018).
- Ballesteros, C. A. S. et al. Recent trends in nanozymes design: From materials and structures to environmental applications. Mater. Chem. Front. 5(20), 7419–7451 (2021).
- 56. Meng, Y. et al. Effects of crystal structure on the activity of MnO2 nanorods oxidase mimics. Nano Res. 13, 709-718 (2020).
- Wan, Y., Qi, P., Zhang, D., Wu, J. & Wang, Y. Manganese oxide nanowire-mediated enzyme-linked immunosorbent assay. *Bioelectron.* 33, 69–74 (2012).
- Liu, S., Lu, F., Xing, R. & Zhu, J. J. Structural effects of Fe<sub>3</sub>O<sub>4</sub> nanocrystals on peroxidase-like activity. *Chem. Eur. J.* 17, 620–625 (2011).
- 59. Xu, X. *et al.* Multi-stimuli responsive hollow MnO<sub>2</sub>-based drug delivery system for magnetic resonance imaging and combined chemo-chemodynamic cancer therapy. *Acta Biomater.* **126**, 445–462 (2021).
- Wang, Z. et al. Biomimetic nanoflowers by self-assembly of nanozymes to induce intracellular oxidative damage against hypoxic tumors. Nat. Commun. 9, 1–14 (2018).
- Alhadlaq, H. A., Akhtar, M. J. & Ahamed, M. Different cytotoxic and apoptotic responses of MCF-7 and HT1080 cells to MnO<sub>2</sub> nanoparticles are based on similar mode of action. *Toxicology* **411**, 71–80 (2019).
- Fredericks, J., Senapati, S. & Wannemuehler, M. J. Cytotoxic effects of manganese oxide nanoparticles in combination with microbial components on intestinal epithelial cells. *F1000Research* 9, 975 (2020).
- Rupa, E. J. et al. Dendropanax morbifera extract-mediated ZnO nanoparticles loaded with indole-3-carbinol for enhancement of anticancer efficacy in the A549 human lung carcinoma cell line. Materials 13, 3197 (2020).
- Sultana, S. et al. Comparative toxicity evaluation of flower-shaped and spherical gold nanoparticles on human endothelial cells. Nanotechnology 26, 055101 (2015).
- 65. Zhu, X., Vo, C., Taylor, M. & Smith, B. R. Non-spherical micro-and nanoparticles in nanomedicine. *Mater. Horiz.* 6, 1094–1121 (2019).
- 66. Chithrani, B. D., Ghazani, A. A. & Chan, W. C. Determining the size and shape dependence of gold nanoparticle uptake into mammalian cells. *Nano Lett.* **6**, 662–668 (2006).
- 67. Gratton, S. E. et al. The effect of particle design on cellular internalization pathways. PNAS 105, 11613–11618 (2008).
- 68. Huang, X., Teng, X., Chen, D., Tang, F. & He, J. The effect of the shape of mesoporous silica nanoparticles on cellular uptake and cell function. *Biomaterials* **31**, 438–448 (2010).
- 69. Liu, Y., Tan, J., Thomas, A., Ou-Yang, D. & Muzykantov, V. R. The shape of things to come: Importance of design in nanotechnology for drug delivery. *Ther. Deliv.* **3**, 181–194 (2012).
- 70. Chen, J., Clay, N. E., Park, N.-H. & Kong, H. Non-spherical particles for targeted drug delivery. *Chem. Eng. Sci.* **125**, 20–24 (2015). 71. Arian, M., Zamanian, A. & Taheri, S. Highly water-dispersible calcium lignosulfonate-capped MnO nanoparticles as a T1 MRI
- contrast agent with exceptional colloidal stability, low toxicity and remarkable relaxivity. RSC Adv. 9, 40498–40506 (2019).
- 72. Lai, J. *et al.* MnO nanoparticles with unique excitation-dependent fluorescence for multicolor cellular imaging and MR imaging of brain glioma. *Mikrochim. Acta.* **185**, 1–8 (2018).
- 73. Hu, H. *et al.* Surfactant-controlled morphology and magnetic property of manganese ferrite nanocrystal contrast agent. *Nanotechnology* **22**, 085707 (2011).
- 74. Basini, M. et al. Local spin dynamics of iron oxide magnetic nanoparticles dispersed in different solvents with variable size and shape: A 1H NMR study. J. Chem. Phys. 146, 034703 (2017).
- 75. Hsu, B. Y. W. *et al.* Relaxivity and toxicological properties of manganese oxide nanoparticles for MRI applications. *RSC Adv.* **6**, 45462–45474 (2016).
- Ta, H. T. et al. Effects of magnetic field strength and particle aggregation on relaxivity of ultra-small dual contrast iron oxide nanoparticles. Mater. Res. Express. 4, 116105 (2017).
- Zhang, M. et al. MnO2-based nanoplatform serves as drug vehicle and MRI contrast agent for cancer theranostics. ACS Appl. Mater. Interfaces 9, 11337–11344 (2017).

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#### Author contributions

F.S. performed data curation, participated in the characterization of the MNMs, and writing the manuscript. E.Gh. synthesized and characterized the MNMs, and participated in writing the manuscript. S.K. and T.M. performed the cytotoxic assay and MRI analyses. L.F. and A.F. provided the lab facilities, participated in statistical analyses and reviewed the manuscript. M.Kh. designed and organized the work, and revised the manuscript.

### **Competing interests**

The authors declare no competing interests.

#### Additional information

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Correspondence and requests for materials should be addressed to M.K.

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