



OPEN

Absorbance biosensors-based hybrid MoS₂ nanosheets for *Escherichia coli* detection

Son Hai Nguyen¹, Phan Kim Thi Vu² & Mai Thi Tran^{2,3}✉

Detecting *Escherichia coli* is essential in biomedical, environmental, and food safety applications. In this paper, we have developed a simple, rapid, sensitive, and selective *E. coli* DNA sensor based on the novel hybrid-type MoS₂ and (NH₄)₆Mo₇O₂₄ nanosheets. The sensor uses the absorbance measurement to distinguish among the DNA of *E. coli*, *Vibrio proteolyticus*, and *Bacillus subtilis* when implemented in conjunction with NH₂-probes. Our experiments showed that the absorbance increased when sensors detected *E. coli* DNA, whereas it decreased when sensors detected *V. proteolyticus* and *B. subtilis* DNA. To the best of authors' knowledge, there are no reports using the novel hybrid-MoS₂ and (NH₄)₆Mo₇O₂₄ materials for differentiating three types of DNA using cost-effective and rapid absorbance measurements. In addition, the label-free *E. coli* DNA biosensor exhibited a linear response in the range of 0 fM to 11.65 fM with a limit of detection of 2 fM. The effect of NH₂-probes on our sensors' working performance is also investigated. Our results will facilitate further research in pathogen detection applications, which have not been fully developed yet.

The gram-negative bacterium *Escherichia coli* causes enteritis, blood sugar infections, urinary tract infections, and meningitis in infants¹, as well as deafness, blindness, and death². Prompt and effective detection of *E. coli* is necessary to save lives^{2,3}. To detect *E. coli*, researchers usually extract them into double-stranded DNA (ds-DNA) or single-stranded DNA (ss-DNA)⁴, then use the techniques such as polymerase chain reaction (PCR) and enzyme-linked immunosorbent assay (ELISA) for DNA detection. However, these methods are time-consuming and costly and cannot be used for on-site diagnosis^{5,6}. Hence, a biosensor based on nanomaterials, a new point-of-care method that detects pathogens with high selectivity and sensitivity, is attracted huge attention recently⁷. Some biosensing technologies have been developed, such as electrochemistry^{8,9}, colorimetry^{10,11}, and field effect transistors¹². Among these techniques, optical biosensors based on nanomaterials are commonly used to detect DNA due to their abilities in real-time monitoring of measuring the DNA with high sensitivity, selectivity, and multi-analyte detection¹³. It has also been reported that the probe can enhance the sensitivity and selectivity to detect targeted DNA^{12,14}. Despite these numerous advantages, it's important to consider potential challenges associated with optical biosensors based on nanomaterials, including potential toxicity of some nanomaterials, the need for careful control over nanomaterial synthesis and modification, and challenges related to the scale-up and commercialization of these technologies.

Pure Molybdenum disulphide (MoS₂) nanosheets is a 2D transition metal dichalcogenide, a typical graphene-like material^{15–18}. They show strong adsorption ability for single-stranded DNA (ssDNA)^{8,10,12,19–22}. Apart from the properties, MoS₂ also gains attention based on its easy-to-find materials and uncomplicated protocol²³. Moreover, MoS₂ has been observed to have biological compatibility with human bodies in its applications, such as curing cancer and Alzheimer's²⁴. Recently, the nanostructured hybrid of MoS₂ attracted much attention due to the ability to change the composition and properties of the excitation light²⁵ and process ultrafast and nonlinear optical properties²⁶. Hybrid MoS₂ nanosheets have several advantages over pure MoS₂ nanosheets, such as improved sensitivity, selectivity, and stability, and they can enable the detection of a broader range of analytes^{27–29}. Furthermore, hybrid-type MoS₂ nanosheet is better than pure semiconductor materials in safely injecting into the human body^{16,20,22,30}. These hybrid nanomaterials intrigue properties and potential applications in sensing point-of-care. Therefore, using this hybrid material as a sensing material for optical biosensors is an area of our interest. This hybrid 2D structures with a robust light-mater intercalation motivated us to design new and cost-effective composite 2D materials to detect pathogenic DNA. We aim to prepare an affordable,

¹School of Mechanical Engineering, Hanoi University of Science and Technology, Hanoi 100000, Vietnam. ²College of Engineering and Computer Science, VinUniversity, Hanoi 100000, Vietnam. ³VinUni-Illinois Smart Health Center, VinUniversity, Hanoi 100000, Vietnam. ✉email: mai.tt@vinuni.edu.vn

compatible, and simple fabricated hybrid MoS₂-3R nanosheets and then utilizing them to detect DNA based on the optical measurements.

In the next section, we prepared a new hybrid-type of MoS₂ nanosheets by a simple and fast hydrothermal method. Their structures and morphologies were examined by X-ray diffraction (XRD) and Scanning Electron Microscope (SEM) images. Then the hybrid MoS₂ nanosheets, in conjunction with an amine-probe, provided a rapid and sensitive sensing platform for differentiating *E. coli*, *V. proteolyticus*, and *B. subtilis* DNAs based on UV-vis spectroscopy measurement. In our experiments, the amine-probe-MoS₂ nanosheet system is built as a biosensor. The performance of the biosensors with different MoS₂ concentrations with *E. coli* DNA was also studied.

Results and discussion

The morphology and structure of the materials. The synthesized materials' structure, morphology, and absorbance properties were examined by XRD and SEM observations. In Fig. 1A, the composition of hybrid-type MoS₂ includes MoS₂-3R (card no PDF#17-0744) and (NH₄)₆Mo₇O₂₄ (PDF#23-0784). MoS₂-3R shows the diffraction peaks from (101), (012), (015), (110), and (113) planes, which correspond to the peaks centered at the 2θ angles of 33.03°, 34.06°, 41.11°, 58.32°, and 60.50°, respectively (PDF#17-0744, using JADE software by MDI Materials Data). Because the hydrothermal process happened in a short period of time, 5 hours at 180 °C; hence along with MoS₂-3R, the precursor chemical Ammonium Heptamolybdate Tetrahydrate ((NH₄)₆Mo₇O₂₄) is still found in the resultant composite. However, based on the SEM image shown in Fig. 1B, the hybrid material clearly shows the multi-layer sheets of nanomaterials. Hence, we hypothesized that (NH₄)₆Mo₇O₂₄ in the formation of lamellar structure MoS₂ species in which adjacent layers are filled with NH₄⁺ ions. Therefore, it can be concluded that either (NH₄)₆Mo₇O₂₄ functionalizes the MoS₂ surface or (NH₄)₆Mo₇O₂₄ molecule fragments.

The absorbance of biosensors with different types of DNA. In this section, the absorbance properties of the hybrid-type MoS₂ nanosheets in the range of 220–700 nm are investigated. In our experiments, the sensing materials with a concentration of 0.031 g/L hybrid MoS₂ nanosheet solution were exposed to different concentrations of three types of DNA, *B. subtilis*, *V. proteolyticus*, and *E. coli*. It is worth noting that *V. proteolyticus* and *E. coli* are gram-negative bacteria, while *B. subtilis* is a gram-positive bacterium³¹. As shown in Fig. 2A,B, the absorbances of *B. subtilis* and *V. proteolyticus* decreased when the DNA concentration increased for the whole wavelength range from 220 to 700 nm. On the other hand, in Fig. 2C, the absorbances increased with the concentrations of *E. coli* DNA in the range of 234 nm to 284 nm wavelength. The experimental result proposes a new selective method for differentiating the three types of DNAs. In the presence of NH₂-5'-GGTCCGCTT GCT CTC GC-3' probe, when the excitation light is from 234 to 284 nm, *E. coli* DNA is easily detected from the others. The interpretation of the different absorption spectra might be due to the differences in the adsorption of dsDNA and ssDNA on the hybrid MoS₂ nanosheets. It has been reported that the adsorption energy of dsDNA is much less than that of ssDNA³². When the different DNAs were added, only *E. coli* DNA was complementary with the probes to form dsDNA. The weak interaction of dsDNA weakens the dielectric screening from the ssDNA case, leads to a shift in absorbance peak and enhances the absorbances.

To further explain the detection mechanism, Fig. 2D depicts the schematic illustration of the adsorbed ssDNA on the hybrid MoS₂ surface³³. The ssDNA could bind to the surface of hybrid MoS₂ and modulate the dielectric environment of MoS₂. As the ssDNA is hybridized with its complementary DNA, the interaction between the formed dsDNA and hybrid MoS₂ is so weak that it would be far away from the surface of MoS₂, resulting in the dielectric environment transforming from DNA to water. Furthermore, in the combined system, the resonance absorbance of the DNA molecule and MoS₂ nanosheets are coupled, leading to hybridized quantum molecule-classical materials³⁴. Hence, the absorbance increases with the *E. coli* DNA concentrations. On the other hand, if the DNA cannot be coupled with the MoS₂ nanosheets, when we add more DNA, the concentration of MoS₂ is reduced and more ssDNA bind to the surface of hybrid MoS₂; thus, the absorbance is diminished, corresponding to the experimental results of the probe and mismatched ssDNA due to the absorbance of DNA is significantly weaker than the absorbance peak of hybrid MoS₂ nanosheets. In addition to differentiating between *E. coli*, *V.*

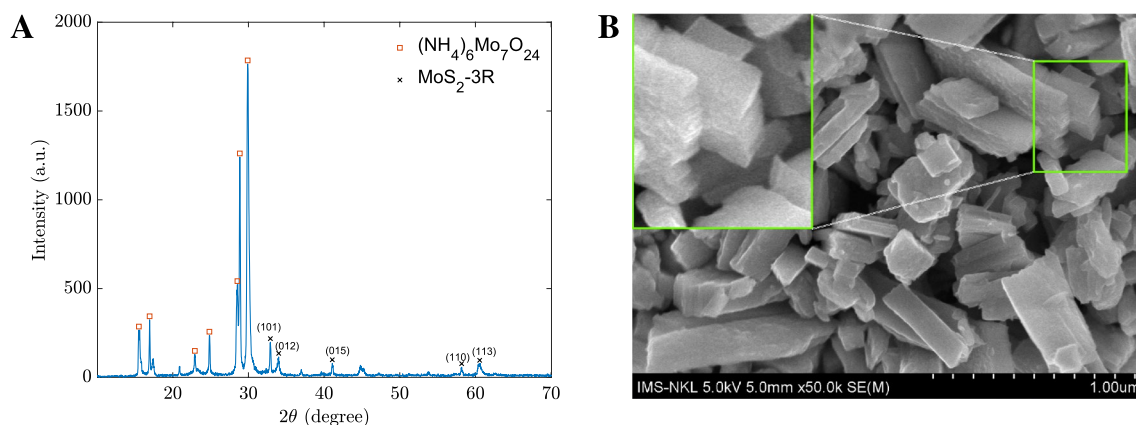


Figure 1. (A) XRD patterns and (B) SEM image of synthesized materials. The inset is an enlarged portion with applied contrast enhancement.

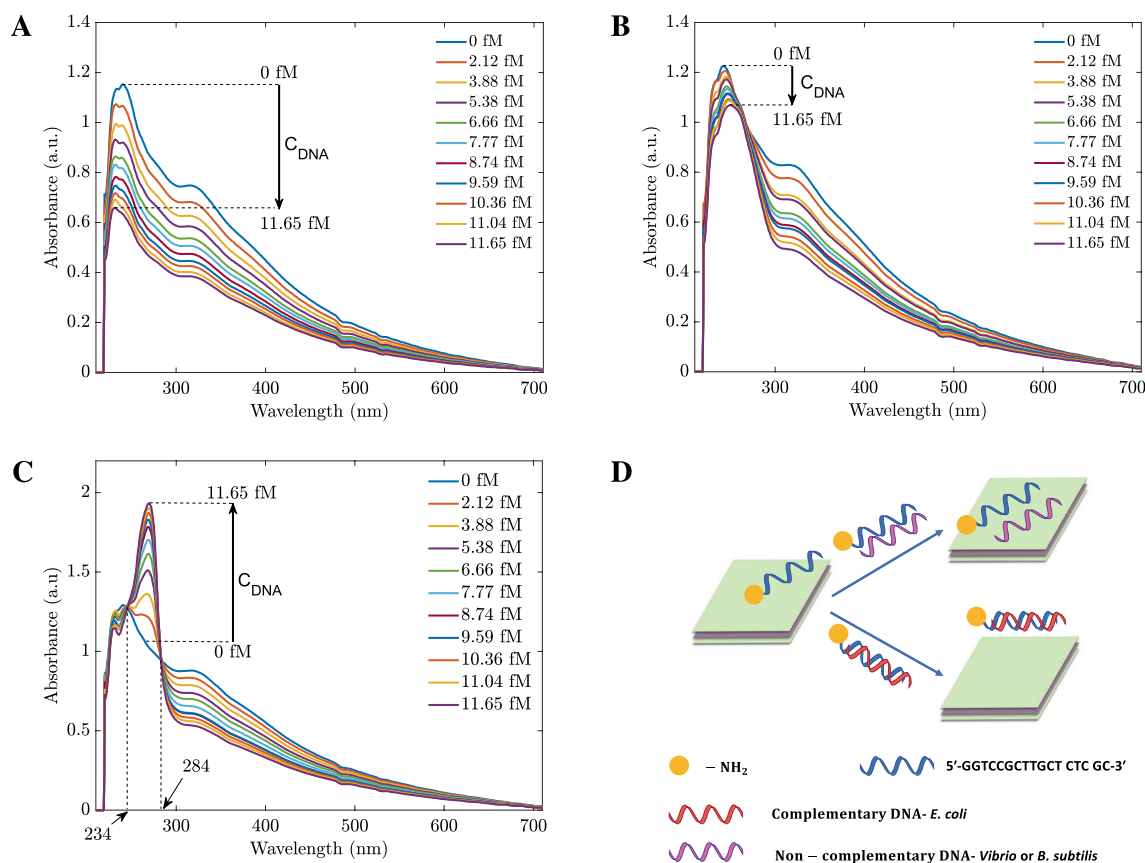


Figure 2. Adsorption spectra of hybridization of 0.031 mg/L hybrid MoS₂ nanosheet solution with various concentrations of *B. subtilis* (A), *V. proteolyticus* (B) and *E. coli* (C) DNAs from 0 to 11.65 fM, respectively. (D) The schematic of *E. coli* DNA sensing mechanism.

proteolyticus, and *B. subtilis*, the absorbances of the biosensors varied linearly with the DNA concentration in the range of 0 fM to 11.65 fM in the resonant region of 234–284 nm wavelength. Figure 3 demonstrates the sensors' performances with different DNA concentrations at 255 nm. This figure also shows that only *E. coli* has a positive slope, confirming the boosting phenomenon in absorbance. The result was obtained from the average of 15 measurements and the hybrid-type MoS₂ nanosheet concentration was 0.031 g/L.

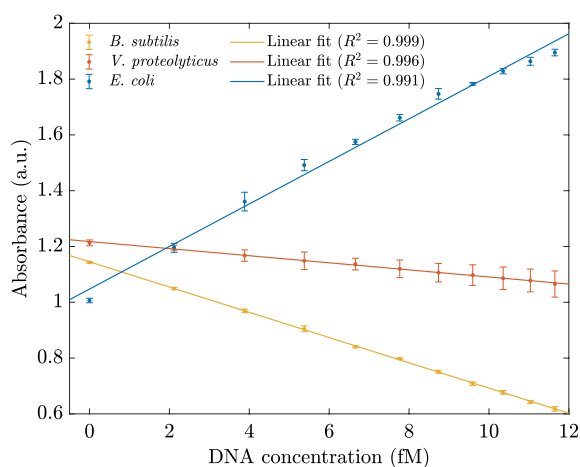


Figure 3. The linear relationship between DNA concentrations and the absorbance of three types of DNA in the range of 0–11.65 fM was taken at the wavelength of 255 nm. Error bars represent the standard deviations of fifteen measurements.

Absorbance biosensor based on hybrid-type MoS₂-3R with *E. coli*. As demonstrated in the previous section, the complementary amine probe can be used to detect *E. coli* by the enhancing effect between 234 and 284 nm. In this section, the sensitivity of *E. coli* DNA sensors with different sensing material concentrations is studied. For quantitative analysis, the biosensors were prepared with varying hybrid-type MoS₂ nanosheets concentration ranging from 0.005 to 0.0625 g/L and the *E. coli* DNA concentrations were from 2 to 11.65 fM. First, the absorbances of the sensors before contacting with DNA were determined and are shown in Fig. 4A. From the result, the absorbance of sensors increases as the concentration of sensing materials increases. Next, these *E. coli* DNA sensors were examined with different *E. coli* DNA concentrations. The absorbance spectra of four different hybrid-type MoS₂ nanosheet concentrations are displayed in Fig. 4B–E. The plots indicate that the higher the sensing material concentration is, the less change in the responded absorbance.

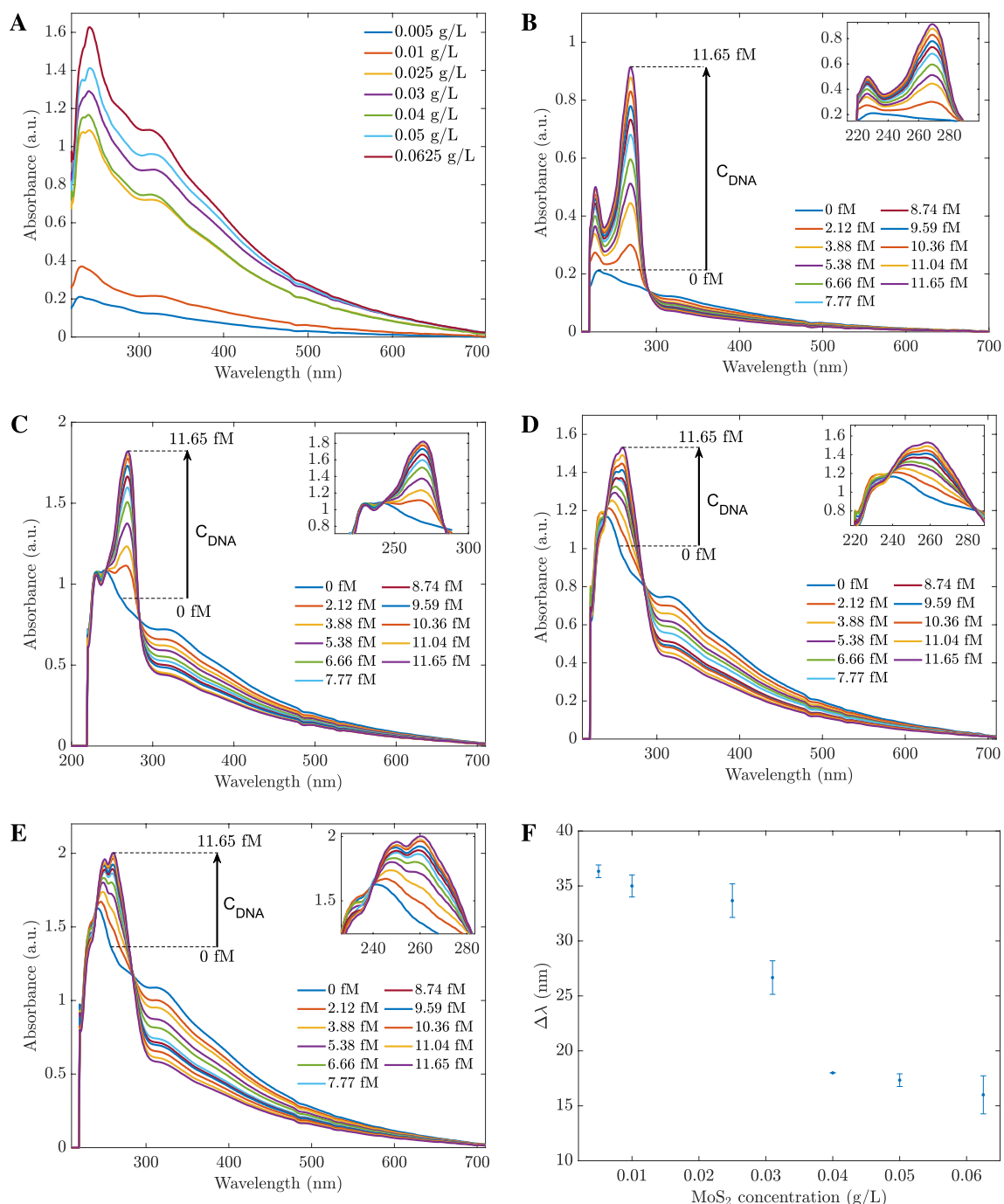


Figure 4. (A) The absorbances of the hybrid MoS₂ based sensors with various sensing concentrations before contacting with DNA. Absorbance changes of *E. coli* DNA sensors with different hybrid-type MoS₂ nanosheets concentrations: (B) 0.005 g/L, (C) 0.025 g/L, (D) 0.04 g/L, (E) 0.0625 g/L. (F) The peak shift for different types of hybrid-types MoS₂ nanosheet sensors in contact with *E. coli* DNA. 0 fM lines are associated with the hybrid MoS₂ nanosheet spectra before contact with DNA. The values were calculated from 6 measurements.

As observed in Fig. 4B–E, the origin peaks of sensing materials are located at roughly 234 nm, even with different concentrations. After contacting with *E. coli* DNA, depending on the origin sensing concentrations, either the spectra have two peaks, or the location of a higher intensity peak changed. In addition, the locations of the highest peaks in the absorbance spectra changed when the sensor contacted *E. coli* DNA. For instance, when the sensing concentration level was as low as 0.005 g/L, the enhancing effects were observed at 234 and 270 nm peaks, and the peak shift $\Delta\lambda$ was 36 nm. The peak shift is demonstrated in Fig. 4F. The higher concentration of sensing material is, the narrower the peak shift is. This phenomenon can be explained by the fact that DNA nucleobases have a limited optical absorption, in comparison to that of hybrid-MoS₂. Hence, with the higher sensing concentration, the induced absorbance in the presence of DNA nucleobases shows less absorbance peaks and wavelength shifting of the MoS₂ absorbance peak³⁴.

The 0.01 g/L hybrid MoS₂ sensor was examined as an example for further study. The absorbances were measured at 234 nm, 268 nm, 284 nm, and 324 nm. Here, 234 nm is the origin peak of sensing materials, 268 nm is the peak when in contact with *E. coli* DNA, 284 nm is the peak where the less change in absorbance (isosbestic point) and 324 nm is the other peak of origin material (outside the resonant bandwidth), always shows the quenching effects in response to any DNAs. The absorbances at four wavelengths are shown in Fig. 5A. With the highest slope, the enhancing effect at 268 nm is an excellent indicator to detect *E. coli*. Therefore, we introduced two quantities to use for calibration lines. The first quantity is a ratio of A₂₆₈/A₂₆₈₍₀₎, where A₂₆₈ and A₂₆₈₍₀₎ are the absorbances of sensors after and before adding *E. coli* DNA. The second quantity is a ratio of A₂₆₈/A₃₂₄, where A₂₆₈ and A₃₂₄ are the absorbances at 268 nm and 324 nm on the same absorbance spectrum. As shown in Fig. 5B, both ratios increased linearly with the concentrations of *E. coli* DNA. Since A₂₆₈/A₃₂₄ shows a higher slope; hence, the ratio A₂₆₈/A₃₂₄ can be used to determine the *E. coli* DNA concentration. The experiments were repeated for other sensors with different hybrid MoS₂ concentrations to build the calibration lines. As shown in Fig. 6, sensors of 0.005 g/L and 0.01 g/L have the highest slopes. However, the error bars are broader than the other sensors with lower starting absorbance. Hence, the 0.025 g/L or 0.031 g/L hybrid MoS₂ nanosheets are recommended for *E. coli* DNA sensors.

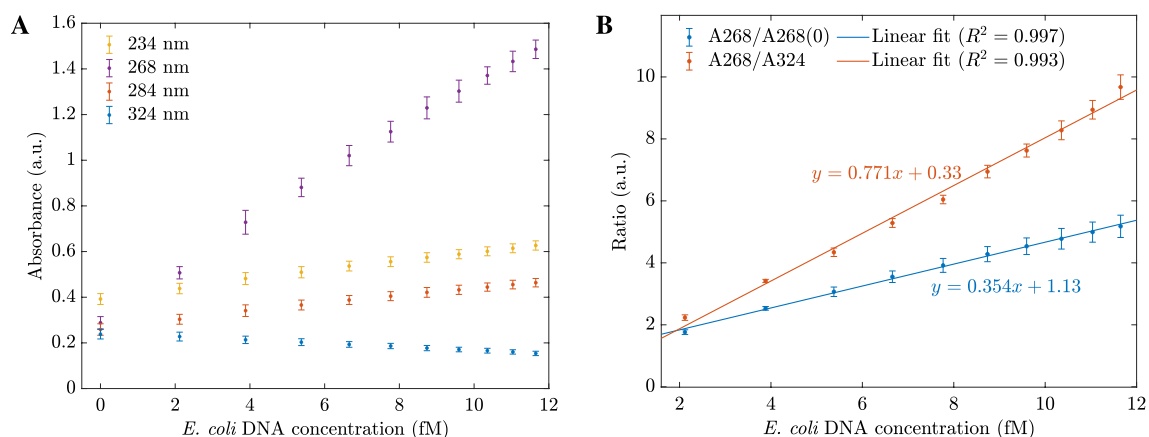


Figure 5. (A) The absorbances changed with *E. coli* DNA concentrations taken at different wavelengths; (B) The calibration lines of *E. coli* DNA sensors were based on two different ratios.

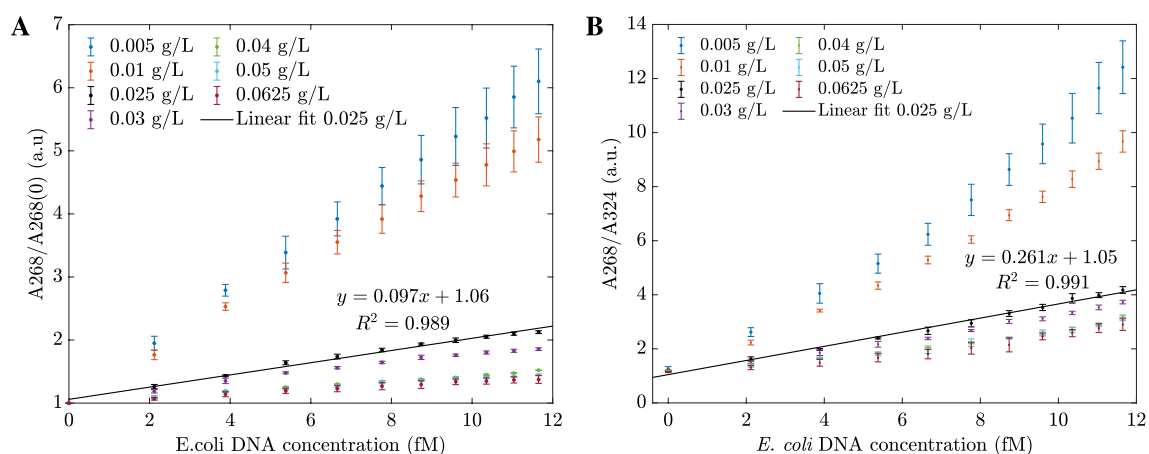


Figure 6. (A) The A₂₆₈/A₂₆₈₍₀₎ calibration lines for different *E. coli* DNA sensors; (B) The A₂₆₈/A₃₂₄ calibration lines for different *E. coli* DNA sensors.

Effect of an amine-probe on the absorption of 2D hybrid MoS₂ biosensors. In the previous section, our results show that hybrid MoS₂ nanosheets combined with amine-probe can provide a rapid and sensitive sensing platform for detecting *E. coli* DNA based on UV-vis spectroscopy measurement. The probe-amine-hybrid MoS₂ nanosheet system is built as a sensor. Here, the probe NH₂-5'-GGTCCGCTTGCT CTC GC-3' is selected to detect the complementary target *E. coli* DNA according to the Watson–Crick base-pairing rules³⁵. The probe was modified with amine (-NH₂) to bond with the MoS₂ surface and thus can enhance the absorbance. To verify our hypothesis, we repeated the experimental steps to measure UV-vis measurements with three different sensors: the first one without a probe (Fig. 7A), the second one with a probe without NH₂ (Fig. 7B), and the third one with the amine probe (Fig. 7C). In all cases, the absorbances were enhanced. However, the shapes of the spectra and the rate of change were different. In particular, without a probe, the absorbance changes were slight (less than 0.05). When the added probe was 5'-GGTCCGCTTGCT CTC GC-3' (without NH₂), the first peak at 234 nm disappeared when adding DNA, and at the wavelength of 260 nm, the absorbance changed significantly (Fig. 7B). Lastly, when we used the amine-5'-GGTCCGCTTGCT CTC GC-3', the enhancement was observed at two peaks of 234 nm and 268 nm. After adding 2 fM DNA, the second absorbance at 268 appeared, and the absorbance increase was even higher than the case in Fig. 7B.

For comparison, the absorbance changes of the sensors at different peak wavelengths are plotted in Fig. 8A. The figure shows that the amine probe enhanced the sensitivity of the sensors at the resonant peak, while the slope was minimal in the case without the probe. Because for each biosensor, the enhanced absorbance peaked at different wavelengths, 255 nm, 260 nm, and 268 nm for biosensors without the probe, sensors with the probe but without NH₂, and sensors with amine probe, respectively. Then, we plotted the graph for the introduced ratio of $A_{\text{peak}}/A_{\text{peak}(0)}$ as shown in Fig. 8B. The amine probe boosted the sensitivity of the sensors (the slopes were more extensive) and increased the precisions. Our experiments showed that the simple configuration of amine probe-hybrid MoS₂ nanosheets had great potential for *E. coli* DNA detection with high sensitivity and selectivity in the range of 0–11.65 fM with a limit of detection (LOD) of 2 fM, which is much lower than other sensors based on hybrid MoS₂ nanosheets. For example, Xiang et al. reported a MoS₂ nanosheet-based fluorescent biosensor for protein detection with a detection limit of 0.67 ng/mL³⁶. Alexaki et al. reported two-dimensional dichalcogenide materials, MoS₂ and WS₂, with the LOD of 5 M³⁷. Huang et al. reported a novel MoS₂-based fluorescent biosensor for DNA detection via hybridization chain reactions (HCRs) with the LOD of 15 pM³⁸. The applications of hybrid-MoS₂ are still in their early stages and have not been fully explored. To the best of the authors' knowledge, there are no existing reports on the use of the novel hybrid-MoS₂ and (NH₄)₆Mo₇O₂₄ materials for differentiating three types of DNA using cheap and fast UV-vis spectroscopy. Our result will facilitate other works in pathogen detection applications that are not fully developed yet.

Conclusion

In this study, we successfully created a simple biosensor for *E. coli* DNA using hybrid MoS₂ nanosheets and demonstrated its absorbance-enhancing ability. The absorbance of *V. proteolyticus* and *B. subtilis* DNA was quenched during the working processes. The sensor can detect DNA at 0–11.65 fM without any amplification strategy or dopant process. The biosensing platform could also detect DNA with high sensitivity and repeatability, with a detection limit of 2 fM. Hence, a homogeneous quantitative DNA analysis was provided with a short turnaround time, simple operation, and relatively high sensitivity. Furthermore, the complementary target DNA could be distinguished from mismatched DNA through the absorbance spectra of Amino-probe hybrid MoS₂. This work could promote the research of novel sensing platforms by coupling nanomaterials with biomolecular recognition events. Therefore, the findings suggest that such a biosensor is promising for nucleic acid detection, particularly quantitative DNA methylation analysis at the point of care. The following steps will explore the sensor's performance with photoluminescence measurements. We will also adjust the prepared conditions or dope other compositions to boost the sensitivity and selectivity more.

Methods

Chemicals and probe to detect *E. coli* DNA. The chemicals used in this research without further purification were Ammonium Heptamolybdate Tetrahydrate ((NH₄)₆Mo₇O₂₄, 99.0%, Tianjin Chemical Reagent Factory, Tianjin, China), Thioacetamide (C₂H₅NS, 99.0%, Shanghai Zhanyun Chemical Co., Ltd, Shanghai, China), Ethanol (C₂H₅OH, 99.5%, Xilong Scientific Co., Ltd., Guangdong, China), and deionized (DI) water. The oligonucleotide probe was designed to specifically target *E. coli*, using the sequence: amine-5'-GGTCCGCTTGCT CTC GC-3'³⁵. *E. coli*, *V. proteolyticus*, and *B. subtilis* DNAs were pretreated by heating at 95 °C for 5 min and then placed in an ice bath for 1 min. All probes were purchased from PHUSA genomics Co., Ltd, Can Tho, Vietnam.

Synthesis of hybrid-type MoS₂–3R nanosheets and absorbance measurement. Hybrid-type MoS₂ nanosheets were prepared using the hydrothermal method³⁹. The process was as follows. First, 5 g of (NH₄)₆Mo₇O₂₄ · 4H₂O and C₂H₅NS were completely dissolved in 20 mL of deionized water and stirred separately for 10 min. Then we mixed and stirred them for 5 min. Next, the mixture was slowly added 20 mL Ethanol and stirred for 30 min. The precipitation was transferred to an 80 mL Teflon-lined stainless-steel autoclave, kept at 180 °C for 5 h, and then allowed to cool naturally to room temperature. Finally, the products were collected by centrifugation at 5000 rpm for 4 min, washed three times with DI water and Ethanol, and dried in a vacuum at 60 °C for three hours. The structure and morphology of synthesized materials were characterized by Rigaku MiniFlex600 (for X-ray patterns) and HITACHI-S4800 (for SEM images).

DNA extraction method. Three bacteria are provided by the microbiology and genetics lab at Hanoi University of Science and Technology, Hanoi, Vietnam. The chemicals were used for these extractions includes the

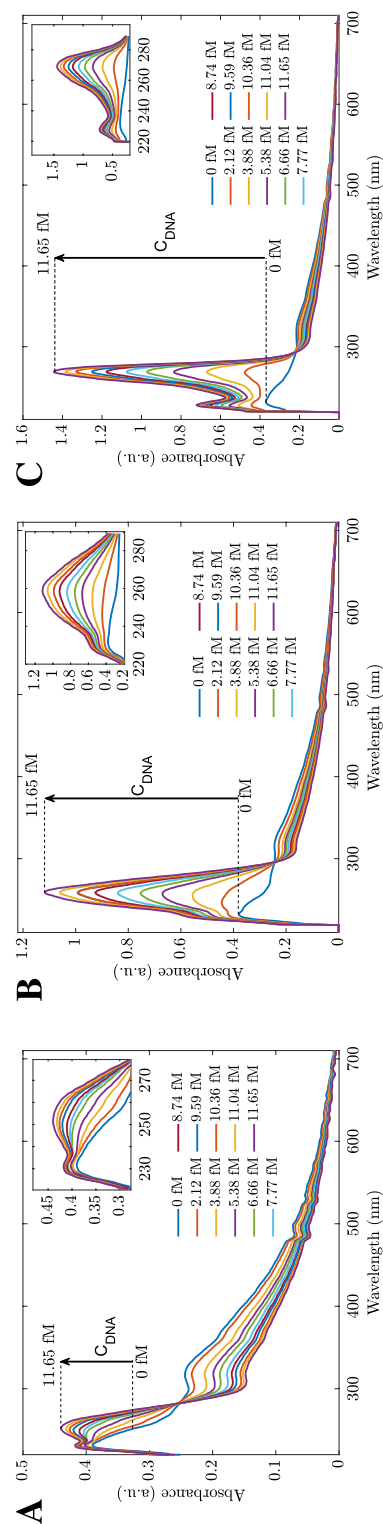


Figure 7. The absorbance spectrum of *E. coli* DNA sensors (A) without the probe, (B) with the probe but without NH_2 , (C) with NH_2 -probe. The concentration of sensors was 0.01 g/L hybrid MoS_2 nanosheets. 0 fM lines are associated with the hybrid MoS_2 nanosheet spectra before contact with DNA.

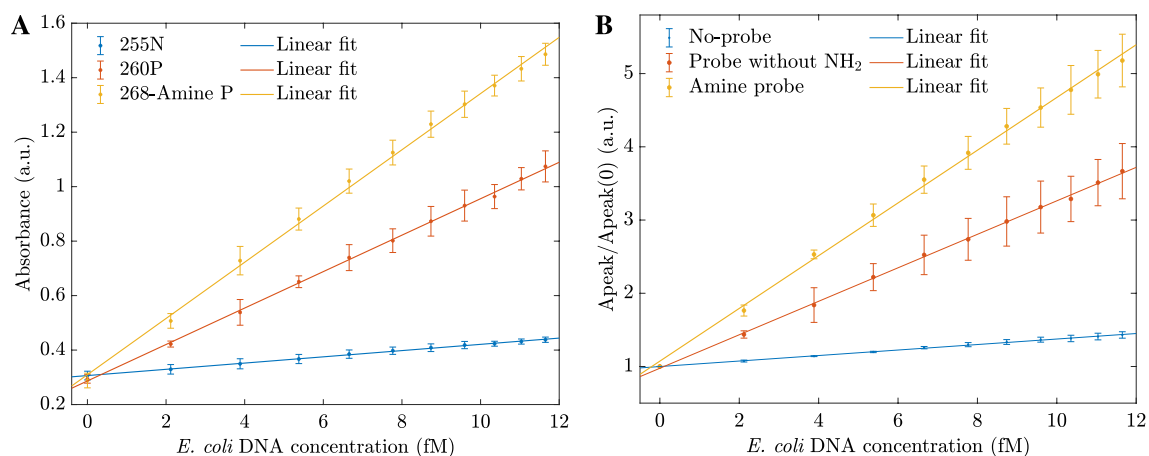


Figure 8. (A) The absorbance changes with the various concentrations of DNA of three types of sensors: 255 N denotes for absorbance at 255 nm of the sensor without the probe, 260P denotes the absorbance at 260 nm of the sensor with the probe but without NH₂, and 268-amine P stands for the absorbance at 268 nm of the sensor with amine probe. (B) Comparison of three sensors without a probe, with a probe but without NH₂, and with amine-probe using ratios at the second peaks derived from Fig. 7.

2% w/v CTAB (Biobasic, Canada), 100 mM Tris-HCl pH 8.0 (Biobasic, Canada), 20 mM EDTA (Biobasic, Canada) and 1.4 M NaCl (Merck, Germany). Before the sterilization process, the pH of the lysis buffer was adjusted to 5.0. 1.0 mL bacteria were added to a 2.0 mL Eppendorf tube and centrifuged at 12,000×g for 5 min at 4 °C. Supernatants were transferred to fresh 2 mL microcentrifuge tubes, and 600 μL of phenol: chloroform: isoamyl alcohol (Sigma, Aldrich) with the ratio of 25: 24: 1, respectively, pH 6.7, was added for each extraction. Samples were incubated at room temperature for 10 min. Phase separation occurred during the centrifugation at 12,000×g for 5 min at 4 °C. Then, the upper aqueous phase was transferred to a new tube and added 450 μL of isopropanol (Biobasic, Canada). The samples were incubated at 20 °C overnight before being centrifuged at 12,000×g for 5 min at 4 °C, and supernatants were discarded. Finally, DNA pellets were washed in 1 mL of 70% (v/v) ethanol (Merck, Germany). The final pellet was dried in air and re-suspended in 100 μL of 75 mM TE buffer pH 8.0. DNA was stored at −20 °C prior to use. All the DNA used in this study was measured the OD_{260/280}, the results showed the ratios about 2.0. These indicators proved that the DNAs are pure.

Absorbance measurements of DNA using UV-Vis method. In our experiments, 100 μL of the probe and 1400 μL of MoS₂ with concentrations of 0.0625, 0.05, 0.04, 0.031, 0.025, 0.01, and 0.005 g/L were added to the curvet 10mm using TE buffer as solvent. These mixtures were ready to use as a sensing platform immediately. Then 100 μL of DNA was repeatedly added to the cuvette to achieve different concentration levels (from 2 to 11.65 fM). At each level, the UV-Vis absorption spectrum was measured. In all our real-time experiments, the probe concentration was 35 nM. We evaluated the performance of seven sensors with various concentrations of the sensing material, to determine the optimal sensor configuration.

Data availability

The datasets used and analysed during the current study available from the corresponding author on reasonable request.

Received: 21 April 2023; Accepted: 21 June 2023

Published online: 23 June 2023

References

- Kaper, J. B., Nataro, J. P. & Mobley, H. L. Pathogenic *Escherichia coli*. *Nat. Rev. Microbiol.* **2**, 123–140 (2004).
- Ahmed, A., Rushworth, J. V., Hirst, N. A. & Millner, P. A. Biosensors for whole-cell bacterial detection. *Clin. Microbiol. Rev.* **27**, 631–646 (2014).
- Van de Beek, D., de Gans, J., Tunkel, A. R. & Wijdicks, E. F. Community-acquired bacterial meningitis in adults. *N. Engl. J. Med.* **354**, 44–53 (2006).
- Law, J.W.-F., Ab Mutalib, N.-S., Chan, K.-G. & Lee, L.-H. Rapid methods for the detection of foodborne bacterial pathogens: Principles, applications, advantages and limitations. *Front. Microbiol.* **5**, 770 (2015).
- Li, F. *et al.* Detection of *Escherichia coli* O157:H7 using gold nanoparticle labeling and inductively coupled plasma mass spectrometry. *Anal. Chem.* **82**, 3399–3403 (2010).
- Yamada, K. *et al.* Single walled carbon nanotube-based junction biosensor for detection of *Escherichia coli*. *PLoS ONE* **9**, e105767 (2014).
- Chalklen, T., Jing, Q. & Kar-Narayan, S. Biosensors based on mechanical and electrical detection techniques. *Sensors* **20**, 5605 (2020).
- Zhou, Y. *et al.* Electrochemical aptasensing strategy for kanamycin detection based on target-triggered single-strand dna adsorption on mos2 nanosheets and enzymatic signal amplification. *Sens. Actuators B Chem.* **296**, 126664 (2019).
- Dai, Z., Hu, X., Wu, H. & Zou, X. A label-free electrochemical assay for quantification of gene-specific methylation in a nucleic acid sequence. *Chem. Commun.* **48**, 1769–1771 (2012).

10. Oreshkin, V. & Tsizin, G. Atomic absorption determination of cadmium, lead, and mercury in sea and river suspensions using an electrothermal atomizer with two vaporization zones. *J. Anal. Chem.* **64**, 1221 (2009).
11. Geng, Y., Wu, J., Shao, L., Yan, F. & Ju, H. Sensitive colorimetric biosensing for methylation analysis of p16/cdkn2 promoter with hyperbranched rolling circle amplification. *Biosens. Bioelectron.* **61**, 593–597 (2014).
12. Singh, P., Gupta, R., Sinha, M., Kumar, R. & Bhalla, V. Mos 2 based digital response platform for aptamer based fluorescent detection of pathogens. *Microchim. Acta* **183**, 1501–1506 (2016).
13. Abu-Salah, K. M. *et al.* Dna-based nanobiosensors as an emerging platform for detection of disease. *Sensors* **15**, 14539–14568 (2015).
14. Maki, W. C. *et al.* Nanowire-transistor based ultra-sensitive dna methylation detection. *Biosens. Bioelectron.* **23**, 780–787 (2008).
15. Voiry, D. *et al.* Conducting mos2 nanosheets as catalysts for hydrogen evolution reaction. *Nano Lett.* **13**, 6222–6227 (2013).
16. Ma, H., Shen, Z. & Ben, S. Understanding the exfoliation and dispersion of mos2 nanosheets in pure water. *J. Colloid Interface Sci.* **517**, 204–212 (2018).
17. Qu, R. *et al.* A mos 2 nanosheet-coated mesh for ph-induced multi-pollutant water remediation with in situ electrocatalysis. *J. Mater. Chem. A* **6**, 6435–6441 (2018).
18. Abinaya, R. *et al.* Ultrathin layered mos 2 nanosheets with rich active sites for enhanced visible light photocatalytic activity. *RSC Adv.* **8**, 26664–26675 (2018).
19. Zhu, C. *et al.* Single-layer mos2-based nanoprobe for homogeneous detection of biomolecules. *J. Am. Chem. Soc.* **135**, 5998–6001 (2013).
20. Xi, Q. *et al.* Highly sensitive and selective strategy for microRNA detection based on ws2 nanosheet mediated fluorescence quenching and duplex-specific nuclease signal amplification. *Anal. Chem.* **86**, 1361–1365 (2014).
21. Yang, Y. *et al.* Mos2-based nanoprobe for detection of silver ions in aqueous solutions and bacteria. *ACS Appl. Mater. Interfaces* **7**, 7526–7533 (2015).
22. Ramakrishna Matte, H. *et al.* Mos2 and ws2 analogues of graphene. *Angew. Chem. Int. Ed.* **49**, 4059–4062 (2010).
23. Iwai, H., Kakushima, K. & Wong, H. Challenges for future semiconductor manufacturing. *Int. J. High Speed Electron. Syst.* **16**, 43–81 (2006).
24. Sobańska, Z., Zapor, L., Szparaga, M. & Stepnik, M. Biological effects of molybdenum compounds in nanosized forms under in vitro and in vivo conditions. *Int. J. Occup. Med. Environ. Health* **33**, 1–19 (2020).
25. Jagminas, A. *et al.* Mos2 with organic fragment—A new hybrid material for laser writing. *Sci. Rep.* **9**, 7839 (2019).
26. Liu, H.-Q., Yao, C.-B., Jiang, C.-H. & Wang, X. Preparation, modification and nonlinear optical properties of semiconducting mos2 and mos2/zno composite film. *Opt. Laser Technol.* **138**, 106905 (2021).
27. Cui, S., Wen, Z., Huang, X., Chang, J. & Chen, J. Stabilizing mos2 nanosheets through sno2 nanocrystal decoration for high-performance gas sensing in air. *Small* **11**, 2305–2313 (2015).
28. Liu, L. *et al.* Edge-exposed mos2 nanospheres assembled with sns2 nanosheet to boost no2 gas sensing at room temperature. *J. Hazard. Mater.* **393**, 122325 (2020).
29. Wang, J. *et al.* Mos2-based nanocomposites for cancer diagnosis and therapy. *Bioact. Mater.* **6**, 4209–4242 (2021).
30. Tang, W. Electrical, electronic and optical properties of MoS₂ & WS₂. Master's thesis, New Jersey Institute of Technology (2017).
31. Karp, M. Expression of bacterial luciferase genes from *Vibrio harveyi* in bacillus subtilis and in *Escherichia coli*. *Biochim. Biophys. Acta Gene Struct. Expr.* **1007**, 84–90 (1989).
32. Jin, K., Xie, L., Tian, Y. & Liu, D. Au-modified monolayer mos2 sensor for dna detection. *J. Phys. Chem. C* **120**, 11204–11209 (2016).
33. Yan, L., Shi, H., Sui, X., Deng, Z. & Gao, L. Mos 2-dna and mos 2 based sensors. *RSC Adv.* **7**, 23573–23582 (2017).
34. Faramarzi, V., Ahmadi, V., Fotouhi, B. & Abasifard, M. A potential sensing mechanism for dna nucleobases by optical properties of go and mos 2 nanopores. *Sci. Rep.* **9**, 6230 (2019).
35. Jaiswal, N., Pandey, C. M., Solanki, S., Tiwari, I. & Malhotra, B. D. An impedimetric biosensor based on electrophoretically assembled zno nanorods and carboxylated graphene nanoflakes on an indium tin oxide electrode for detection of the dna of *Escherichia coli* o157: H7. *Microchim. Acta* **187**, 1–8 (2020).
36. Xiang, X. *et al.* Mos2 nanosheet-based fluorescent biosensor for protein detection via terminal protection of small-molecule-linked dna and exonuclease iii-aided dna recycling amplification. *Biosens. Bioelectron.* **74**, 227–232 (2015).
37. Alexaki, K. *et al.* A dna sensor based on upconversion nanoparticles and two-dimensional dichalcogenide materials. *Front. Chem. Sci. Eng.* **15**, 935–943 (2021).
38. Huang, J. *et al.* Molybdenum disulfide-based amplified fluorescence dna detection using hybridization chain reactions. *J. Mater. Chem. B* **3**, 2395–2401 (2015).
39. Nguyen, S. H., Vu, P. K. T. & Tran, M. T. Glucose sensors based on chitosan capped Zns doped Mn nanomaterials. *IEEE Sens. Lett.* **7**, 1–4 (2023).

Acknowledgements

The authors would like to thank Dr. Hang Dam of HUST for her support in extracting DNA and other group members, including Huy Nguyen, Tien Nguyen, and Hiep Nguyen, for supporting this work. This work was funded by VinUni-Illinois Smart Health Center.

Author contributions

M.T.T. conceptualized the method and conceived the experiments, P.K.T.V. conducted the experiments, S.H.N. and M.T.T. analyzed the results and prepared the manuscript. All authors reviewed the manuscript.

Competing interests

The authors declare no competing interests.

Additional information

Correspondence and requests for materials should be addressed to M.T.T.

Reprints and permissions information is available at www.nature.com/reprints.

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>.

© The Author(s) 2023