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OPEN Extension of human GCSF serum half-life by the fusion of albumin binding domain

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Granulocyte colony stimulating factor (GCSF) can decrease mortality of patients undergo chemotherapy through increasing neutrophil counts. Many strategies have been developed to improve its blood circulating time. Albumin binding domain (ABD) was genetically fused to N-terminal end of GCSF encoding sequence and expressed as cytoplasmic inclusion bodies within Escherichia coli. Biological activity of ABD-GCSF protein was assessed by proliferation assay on NFS-60 cells. Physicochemical properties were analyzed through size exclusion chromatography, circular dichroism, intrinsic fluorescence spectroscopy and dynamic light scattering. Pharmacodynamics and pharmacokinetic properties were also investigated in a neutropenic rat model. CD and IFS spectra revealed that ABD fusion to GCSF did not significantly affect the secondary and tertiary structures of the molecule. DLS and SEC results indicated the absence of aggregation formation. EC50 value of the ABD-GCSF in proliferation of NFS-60 cells was 75.76 pg/ml after 72 h in comparison with control GCSF molecules (Filgrastim: 73.1 pg/ml and PEG-Filgrastim: 44.6 pg/ml). Animal studies of ABD-GCSF represented improved serum half-life $(9.3 \pm 0.7 h)$ and consequently reduced renal clearance (16.1 ± 1.4 ml/h.kg) in comparison with Filgrastim (1.7 ± 0.1 h). Enhanced neutrophils count following administration of ABD-GCSF was comparable with Filgrastim and weaker than PEG-Filgrastim treated rats. In vitro and in vivo results suggested the ABD fusion as a potential approach for improving GCSF properties.

Inflammatory cytokines such as tumor necrosis factor alpha (TNF-α), and interleukin 1 beta (IL-1B) are being released early during the course of microbial infections. These factors stimulate NF-κB and C/EBPβ pathways which enhance granulocyte colony-stimulating factor (GCSF) expression¹ and consequently higher production of granulocytes and stem cells from bone marrow. This hematopoietic cytokine is produced by endothelial and mesothelial cells, macrophages, fibroblasts and monocytes² and is usually administered to neutropenic individuals after chemotherapy³. This growth factor consists of four antiparallel α -helices compromising 174 amino acids (19.6 kDa)^{4,5} with two disulfide bonds (Cys36-Cys42 and Cys64-Cys74), one free cysteine (Cys17) and one O-linked carbohydrate chain attached to Thr133. It has been proved that the carbohydrate moiety has little or no impact on 3D structure and biological activity of GCSF⁶ but the disulfide bonds are necessary for the stability and biological activity of molecule^{7,8}. Due to the small size of the molecule, it is usually destroyed with serum proteases and eliminated by the kidney infiltration. Because of its high clearance rate (0.5 to 0.7 ml/min/kg), patients should receive daily which cause patients dissatisfaction and increase treatment costs⁹. Therefore, several strategies have been developed to improve its serum-half life and pharmacokinetic properties. One approach is the attachment of polyethylene glycol (PEG) to the molecule. Although, PEGylation has low immunogenicity, high stability, no electrical charge and high flexibility, it shows some disadvantages including metabolic accumulation within the kidneys and high cost of purification^{10,11}. Other suggested approaches are genetically fusion of the target molecule to Fc domain of IgG1¹², human serum albumin (HASylation)¹³, albumin-binding domain¹⁴⁻¹⁶, or addition of PAS motif (PASylation)¹⁷, lipids (Acylation)¹⁸, XTENylation¹¹.

Albumin is the most abundant protein of the plasma¹⁹ and its serum half-life increases by its attachment to the FcRn^{20,21}. It has been well documented that albumin-binding domains (ABDs) can non-covalently bind to the serum albumin^{22,23} and increase the durability of the genetically attached molecule within blood circulation^{24–26}.

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Figure 1. Schematic view of the expression cassette.

Different types of albumin binding domains are being expressed on the surface of several bacterial families including Staphylococci, and Streptococci²⁷. *Finegoldia magna*, an anaerobic gram-positive coccoid bacterium, also expresses ABD (G148-ABD)²⁸ which was manipulated to ADB035, a highly stable but highly immunogenic molecule²⁷. Further studies developed ABD molecules which were safer and had desirable affinity towards albumin (ABD088, ABD094 and ABD095)²⁹. Among these ABD derivatives, ABD094 showed the lowest sensitivity during T-cell proliferation assay³⁰. High stability of these domains even after thermal or chemical denaturation may be due to the lack of cysteine amino acid residues and post translational modifications²⁷.

Therefore, in the present study, GCSF was genetically fused to the ABD094 domain to study the possible structural and functional changes of GCSF protein in comparison to the commercially available GCSF molecules.

Results

Protein expression. The expression cassette (Fig. 1) was subcloned in pET28a expression vector and confirmed by restriction digestion and sequencing (data not shown). The optimum expression level of the fusion protein was achieved at 30 °C using 0.25 mM IPTG 6 h post-induction (Fig. 2a and Supplementary Fig. 1a) which was nearly 60% of the total bacterial protein content. The recombinant protein (25.46 kDa) was successfully purified using Ni-agarose resin (Fig. 2b and Supplementary Fig. 1b) yielding to an 8 mg/l of bacterial medium and was confirmed by Western blotting with anti-His tag antibody (Fig. 2c and Supplementary Fig. 1c). According to the endotoxin assessment by Pyrotell test, LPS content of the purified ABD-GCSF protein was lower than the detection limit of the kit (<0.25EU/ml) when 2EU/mg LPS of the Filgrastim (Ph. Eur. Method 2.6.14) was set as endotoxin limit of this recombinant GCSF derivative.

Confirmation of ABD-GCSF refolding. The obtained results from Ellman's assay showed that free sulfhydryl concentration in refolded ABD-GCSF protein was similar to the Filgrastim molecule which is assumed to be a native refolded GCSF protein. Optical densities revealed that the number of thiol residues within unfolded ABD-GCSF are more than its refolded form after dialysis which indicated that cysteine residues were participated in the formation of correct disulfide bonds (Supplementary Fig. 2). In addition, a computer generated 3-D image of ABD-GCSF protein represented no free cysteine residue on the surface of the protein (Supplementary Fig. 3a,b). This observation could explain the unchanged optical absorbance of the Ellman's reagent in the case of refolded ABD-GCSF after dialysis.

Size exclusion chromatography (SEC). Hydrodynamic volume of the protein is one of the most important parameters affecting its renal infiltration and half-life¹¹. The mobility of monomeric forms of Filgrastim and ABD-GCSF was analyzed on a calibrated SEC-HPLC column. The observed molecular weights were higher than those deduced from corresponding amino acid sequences which may be due to the ability of SEC column in separation of proteins based on their shape (hydrodynamic radius) as well as molecular weight³¹. SEC-HPLC results demonstrated that the addition of ABD to the GCSF protein almost did not change its hydrodynamic volume (Fig. 3). The obtained chromatogram revealed that there are no major impurities including truncated or aggregated forms of ABD-GCSF surrounding the main peak (monomer form) of the molecule which was appeared in retention time of about 19 min which is little different from Filgrastim control sample due to their molecular weight difference. The peak eluted at 22 min is derived from the sample dilution buffer.

Dynamic light scattering measurements. To assess the possibility of aggregation formation within the recombinant fusion protein and to determine the effect of ABD on GCSF hydrodynamic radius, DLS experiments were performed. Based on calculated PdI index (PdI: 0.48) and DLS graph (Supplementary Fig. 4), aggregation of ABD-GCSF was not significant. It was also shown that ABD fusion to the GCSF molecule could significantly increase the hydrodynamic radius of GCSF in comparison with Filgrastim (Fig. 4).

Intrinsic fluorescence measurements. Following excitation and emission of tryptophan residues (Trp59 and Trp119) within GCSF protein at 295 nm and 300–450 nm, fluorescence spectra represented a similar maximum peak at 350 nm confirming the unchanged structural conformation of GCSF molecule by the fusion of ABD moiety (Fig. 5).

Circular dichroism measurements. Far and near-UV CD spectra have been shown in (Fig. 6a,b). In far-UV spectra, a positive peak at 195 nm and two minima at 208 and 222 nm were observed representing α -helical structures. According to the acquired near-UV spectra, it was concluded that three proteins had similar tertiary structures (Fig. 6b).

Cell proliferation assay. Proliferation of NFS-60 cell line depends on the presence of GCSF as a growth factor. The cells were treated with dilutions of Filgrastim, PEG-Filgrastim and ABD-GCSF for 72 h. Stimulus





Figure 2. ABD-GCSF protein. (a) Protein expression: M: Protein Mw marker; #1, 3: Recombinant bacterial lysates before induction; #2, 4: Recombinant bacterial lysates after induction. (b) Protein purification: #1: Initial sample (IS); #2: Flow through (FT) sample; #3: Washing sample; M: Protein Mw marker; #4-8: Eluted samples. (c) Western blotting: M: Protein Mw marker; #1, 2: Bacterial lysates before and after induction; #3, 4: Eluted proteins. The full-size original gels and the blot are presented in supplementary Fig. S1a,b,c, respectively.

response graphs and the corresponding calculated EC50 values of Filgrastim, PEG-Filgrastim and ABD-GCSF were 73.1, 44.6, and 75.76 pg/ml (Fig. 7).

Affinity of ABD-GCSF towards human serum albumin. In a home-made ELISA assay the affinity of refolded ABD-GCSF protein for HSA was observed (Fig. 8) which can confirm the theoretical role of this domain in increasing serum half-life of the fusion protein through binding to the serum albumin.

Animal studies. To investigate pharmacodynamic and pharmacokinetic parameters of ABD-GCSF protein, 100 µg/kg of GCSF derivatives were injected to the rats one day after inducing neutropenia except PBS control group (Group 1). As illustrated in (Fig. 9), CPA-induced reduction of neutrophils and total WBCs was gradually improved from day 6 by the administration of GCSF derivatives especially within the rats received PEG-Filgrastim but these molecules could not increase red blood cells (RBC), lymphocytes and monocytes (Supplementary Fig. 5a,b,c).

Based on ELISA results, the time points in which 50% of the proteins were eliminated $(t_{1/2})$ were calculated as 1.7 ± 0.1 , 10.0 ± 0.5 and 9.3 ± 0.7 h for Filgrastim, PEG-Filgrastim and ABD-GCSF, respectively. The lowest rate of protein clearance rate was calculated for PEG-Filgrastim which was significantly different from Filgrastim and ABD-GCSF (Table 1). On the other hand, subcutaneous administration of each protein resulted in maximum concentrations at 2, 24 and 10 h for Filgrastim (552.3 ± 47.7 ng/ml), PEG-Filgrastim (481.7 ± 45.2 ng/ml) and ABD-GCSF (353±32 ng/ml). Calculated area under the protein concentration-time curves (AUC) suggested that ABD fusion to GCSF may improve the protein concentration within body in comparison with Filgrastim (Table 1). Filgrastim, PEG-Filgrastim, and ABD-GCSF were cleared from blood samples 10, 96 and 24 h postinjection according to the limit of quantification (LOQ) index of human GCSF ELISA kit (Fig. 10). Mean residence time (MRT) values were estimated to be 3.4 ± 0.1 , 17.9 ± 2.2 and 9.9 ± 0.4 h for Filgrastim, PEG-Filgrastim







Figure 4. Dynamic light scattering measurements of ABD-GCSF and PEG-Filgrastim in comparison with Filgrastim. Data presented as mean ± SD. *Considered *P* values less than 0.05 in comparison to Filgrastim protein.

and ABD-GCSF, respectively. Calculated AUC_{0- ∞} value of Filgrastim (2315.33 ± 129.3 ng.h/ml) showed that maintenance of Filgrastim within the body is lower than ABD-GCSF and PEG-Filgrastim (6232.1 ± 531.5 and 16,773.8 ± 2371.8 ng.h/ml, respectively) representing the decreased total clearance rates of GCSF derivatives (Filgrastim: 43.3 ± 2.3; PEG-Filgrastim: 6.056 ± 0.8341; ABD-GCSF: 16.1 ± 1.4 ml/kg.h, respectively).



Figure 5. Fluorescence emission spectra of GCSF derivatives.





Figure 6. CD spectra of GCSF derivatives. (a) Far-UV spectrum (190–250 nm). (b) Near-UV spectrum (250–350 nm). Filgrastim and ABD-GCSF are represented in green and black lines, respectively.

Discussion

Although GCSF molecule is commonly used to reduce the neutropenic side effects of myeloid suppressive anticancer drugs³² its rapid clearance has forced development of several strategies to improve its pharmacokinetic properties^{12,32,33} Increasing the GCSF size by fusing the protein to another protein or to a polymer such as polyethylene glycol (PEG) was one of the options. For this purpose, several studies have been conducted to see if N or C terminal amino acids of this molecule can be modified. In the case of PEG-Filgrastim, the long-acting Filgrastim, it was confirmed that the attachment of a single linear 20 kDa PEG molecule to the N-terminal



Figure 7. Dose response curves for GCSF derivatives on NFS-60 cells. Data are given as mean ± SD values of triplicate wells.



Figure 8. ELISA showing HSA binding of ABD-GCSF. The graph represents the mean ± SD of duplicates.

Methionine can not significantly interfere with GCSF/GCSF-R interaction³⁴. Previous studies have shown that the attachment of albumin binding domains (ABDs) could enhance protein half-life^{24,25,28}. For example, this domain has been genetically fused to Exenatide and improved its short half-life (30 min to 16 h)²⁵. Serum stability of an anti-cancer bispecific diabody was also extended five–six fold by the fusion of ABD (10 vs. 64 min)²⁴. Therefore, in the present study ABD peptide with improved stability and safety (ABD094)^{24,25,27,29} was genetically attached to the N-teminus of the Filgrastim molecule by the use of a flexible Gly₄Ser linker peptide of 15 amino acids in order to have the minimum structural change of GCSF/GCSF-R interface. Also six histidine residues were inserted at upstream of ABD-GCSF gene in order to be purifed with Ni–NTA affinity column. It has been confirmed that His-tag does not change the expression level, solubility, folding and biological function of the recombinant proteins due to its small size^{35,36}.

According to the previous studies, *Escherichia coli* can be considered as a suitable expression host cell in comparison with mammalian cells due to its short doubling time, well-known genome, easy scale-up and low cost of growth conditions³⁷⁻³⁹. Although many studies have revealed that *E. coli* can be selected as the expression host for the proteins which have no complex post translational modifications (PTM)³⁹, disulfide bond formation





Proteins	T _{max} (h)	C _{max} (ng/ml)	AUC _(0-t) (ng h/ ml)	$\begin{array}{c} AUC_{\ (0-\infty)}\ (ng\ h/\\ml) \end{array}$	K _a (h ⁻¹)	K _e (h ⁻¹)	t _{1/2} (h)	CL/F (ml/h/ kg)	MRT (h)
Fil- grastim	2.0 ± 0.0	552.3 ± 47.7	2406.6 ± 218.0	2315.3±129.3	1.22 ± 0.11	0.4 ± 0.00	1.7 ± 0.1	43.3 ± 2.3	3.4 ± 0.1
PEG-Fil- grastim	$24.0 \pm 0.0^{*}$	481.7±45.2*	16,773.8±2371.8*	16,773.8±2371.8*	0.103 ± 0.001	$0.07 \pm 0.00^{*}$	$10.0 \pm 0.5^{*}$	$6.056 \pm 0.83^{*}$	17.9±2.2*
ABD- GCSF	$10.0 \pm 0.0^{*}$	353±32.0*	6038±520.7*	6232.1±531.5*	0.187 ± 0.004	$0.08\pm0.0^*$	9.3±0.7*	16.1±1.4*	$9.9\pm0.4^{*}$

Table 1. Major pharmacokinetic parameters of administered ABD-GCSF in a neutropenic rat model. Data is represented as the means ± SD of 5 rats/group. T_{max} , Time to reach the peak plasma concentration; $t_{1/2}$, Elimination half-life; C_{max} , Maximum observed plasma concentration; K_e , Elimination rate constant; *CL/F*, Apparent total clearance; *AUC*, Area under the serum concentration–time curve; *MRT* Mean residence time. **P* < 0.05 in comparison with the Filgrastim group.



Figure 10. Plasma concentration–time profile of Filgrastim, PEG-Filgrastim and ABD-GCSF in rats. 5 rats/ group subcutaneously received GCSF derivatives. All points report the mean±SD of animals.

and appropriate refolding can be challenging issues which should be considered for *E. coli* expression systems. In the case of GCSF molecule, development of Filgrastim and its biosimilar forms which are produced in *E. coli* suggest this host as a suitable expression system.

Size exclusion HPLC chromatography (SEC) showed that multimeric forms of ABD-GCSF were not significant confirming the good quality of the dialyzed recombinant protein. Complete removal of the denaturant agent and correct refolding of the protein was further approved by DLS PdI index and SDS-PAGE (Supplementary Fig. 6). Tryptophan, phenylalanine and tyrosine residues usually contribute in intrinsic fluorescence properties of proteins⁴⁰. Based on tryptophan fluorescence properties, intensity of this amino acid could predict the tertiary structure of the proteins. In the case of PEG-Filgrastim, the increased fluorescence intensity may be due to the Trp relocation towards outside of PEG-fused GCSF confirming previously published results⁴¹. The obtained IFS spectra of ABD-GCSF protein did not represent any significant shift confirming unchanged structural conformation of the protein in comparison with the commercially available GCSF proteins. In addition, the increased height of the peaks for PEGylated and ABD-GCSF could interpret the buried tryptophan residues of Filgrastim causing a more compacted structure of this molecule. Also, in Far-UV spectrum of ABD-GCSF, 2 minima peaks at 208 and 222 nm and one positive peak at 195 nm were observed which were similar to Filgrastim. CD spectra of ABD-IFNα and ABD-Ciliary neurotrophic factor (CNTF) also confirmed that ABD could not change secondary structure of these molecul^{15,42}.

Herein, on molar basis according to the molecular weight of protein monomers, the calculated EC50 values represented 2.83, 3.89 and 1.14 μ M for Filgrastim, PEG-Filgrastim and ABD-GCSF, respectively. The results are in accordance to the previously published data of GCSF-Fc¹², GCSF-transferin⁴³ and PEG-GCSF^{12,44,45}.

In the present study neutropenic rats were used to evaluate biological activity of recombinant ABD-GCSF in analogy between two commercial forms. Any changes in pharmacodynamic curves strongly depends on potency of the administered drug in reduction of CPA side-effects. It was also revealed that duration of neutropenia in rats received PEG-Filgrastim and ABD-GCSF was shorter than the group received Filgrastim which may be due to their prolonged blood circulation. To get more detailed view, clinical effects (PD) should be studied along with pharmacokinetics properties (PK). Previous studies have shown that the efficacy of GCSF on inducing neutrophil production depends on its serum concentration and total clearance rate⁴⁶⁻⁴⁸. Plasma concentration-time profile of ABD-GCSF protein was wider than Filgrastim which resulted to a prolonged T_{max} (10.0±0.0 h for ABD-GCSF vs. 2.0 ± 0.0 h for Filgrastim) representing different clearance patterns and confirmation of more efficiency of ABD-GCSF in stimulation of neutrophils compared to the Filgrastim-treated group. On the other hand, different maximum concentration (C_{Max}) of ABD-GCSF protein (63.91% of Filgrastim; 353 ± 32.0 vs. 552.3 ± 47.7 ng/ml) could suggest different pathways in protein absorption^{49,50}. In contrast, plasma half-life and C_{Max} of PEG-Filgrastim (10.0 ± 0.5 h, 481.7 ± 45.2 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 ng/ml) was more than ABD-GCSF (9.3 ± 0.7 h, 353 ± 32.0 h, 350 ± 0.7 h, 350 \pm 0.7 h, 350 ml) and Filgrastim $(1.7 \pm 0.1 \text{ h}, 552.3 \pm 47.7 \text{ ng/ml})$ which could be explained by its hydrated polyether chain preventing protease degradation and macrophage uptake of the molecule. Consequently, its total clearance rate $(6.056 \pm 0.8341 \text{ ml/h.kg})$ was lower than ABD-GCSF and Filgrastim $(16.1 \pm 1.4 \text{ and } 43.3 \pm 2.3 \text{ ml/h.kg})$. As a result, maximum neutrophil count in PEG-Filgrastim group was higher than two other groups which decreased neutropenic days in these rats. The calculated time for reaching to the maximum concentration (T_{Max}) of PEG-Filgrastim and ABD-GCSF (24 vs. 10 h) could refer to their hydrodynamic radius and/or lymphatic absorption

which result to slower release of the molecule after s.c adminstration^{49,50}. According to the previous studies, elimination of GCSF is mostly through non-renal clearance by the neutrophils^{12,51-54}. In brief, GCSF binds to its receptors mainly located on the surface of peripheral neutrophils follows with internalization and degradation of GCSF protein^{51,52,55}. Therefore, GCSF serum concentration will be mainly associated to the number of neutrophils and the other cells possessing GCSF receptor especially in bone marrow and spleen⁵⁴. In the present study, higher AUC (0-∞) value of ABD-GCSF (6232.1±531.5 ng.h/ml) in comparison to Filgrastim (2315.3±129.3 ng.h/ml) indicated the improved ABD-GCSF plasma circulation. This phenomenon was supported by the confirmed affinity of ABD-GCSF towards HSA in a home-made ELISA assuming recycled protein through FcRn with reduced lysosomal degradation and kidney uptake. On the other hand, plasma half-life of ABD-GCSF could be associated with its albumin attachment characteristics and reduced cellular internalization^{21,51}. The obtained pharmacokinetic indices of PEG-Filgrastim are in accordance with previous studies in which a single dose of PEG-Filgrastim act as effective as multiple doses of Filgrastim because of its increased hydrodynamic radius^{56,57}. Altogether, total clearance rates, time of obtaining GCSF plasma peak (24 h) and AUC (0.00) values can suggest that PEG-Filgrastim is more stable than ABD-GCSF. The observed improved plasma circulation of ABD-GCSF confirmed previously published studies on this domain. The short serum half-life of IFN- α was increased by genetically fusion of ABD to its C and/or N terminus (from 3 to 19.3 and 32.8 h; 6.5 and 11-fold)¹⁵. In another study, the attachment of HER2-binding affibody to ABD035 could increase its half-life to 80-fold (0.5 vs. 41 h)²⁸. ABD fusion to IL-2 decreased clearance rate (from 176.4 ± 4.0 to 77.4 ml/h/kg) while increased serum half-life (46 vs. 150 h, 3 fold)⁵⁸. In the case of doxorubicin, the chemotherapy drug, the clearance rate enhanced from 4.38 to 23 h (five fold) after its attachment to ABD⁵⁹. Serum half-life of a receptor blocking anticalin protein (OX40 Ac) could increase from 0.5 to 60 h (12-fold) by genetically fusion to ABD094 in a mouse model⁶⁰. In another study, N-terminal ABD035 could extend half-life of ciliary neurotrophic factor (CNTF) from 34 to 483 min (14-fold)⁴². Low serum half-life of recombinant hTRAIL was also enhanced from 0.32 to 14.1 h (28-fold) by the fusion of ABD035 to the N-terminus. Their results showed that hTRAIL-ABD format could not efficiently attach to the albumin and no change of circulation half-life of the hTRAIL was observed⁶¹. This finding supports that fusion of ABD moiety to the N or C terminus of the candidate protein should be studied carefully to achieve the longer serum half-life.

Conclusions

Our results showed that attachment of ABD moiety could increase circulating half-life and stability of GCSF protein without affecting its hematopoietic characteristics. It seems that genetically fusion of safe polypeptides like ABD to the small drug proteins may have promising results in development of biobetter biologics.

Methods

Ethics statement. All experiments and procedures were approved by the Ethics Committee of Pasteur Institute of Iran (IR.PII.REC.1399.013) and performed in accordance with the approved guidelines and regulations.

Expression cassette. GCSF (Filgrastim) encoding amino acid sequence was extracted from drug bank (Accession No. DB00099). ABD094 amino acid sequence compromising of 46 amino acids (Mw: ~ 5.8 kDa) was obtained from published patents (US10206975B2 and JP2014557602A). The two amino acid sequences were fused using a flexible Gly₄Ser linker peptide compromising 15 amino acids ((G₄S)3). A histidine tag was designed at upstream of the ABD-GCSF gene cassette (Supplementary Fig. 7), synthesized after *E. coli* codon optimization and subcloned into pET28a expression vector (Novagen, USA) at *NcoI* and *HindIII* restriction sites.

Protein expression. The expression of recombinant protein was induced in *E. coli* BL21 (DE3) (Novagen, USA) host cells. Luria–Bertani (LB) broth medium supplemented with kanamycin 30 μ g/ml was inoculated with the recombinant bacteria and incubated at 37 °C shaker incubator until optical density of the medium reached 0.5 at 600 nm. Isopropyl β -d-1-thiogalactopyranoside (IPTG) was used as expression inducer (0.25 mM) and bacteria were incubated for further 6 h at 30 °C. Bacterial pellet was collected by centrifugation at 9000 rpm for 3 min and protein expression level was quantified on 12% SDS-PAGE stained with Coomassie Brilliant Blue G250 dye.

Bacterial lysates were run on 12% SDS-PAGE and transferred to nitrocellulose membrane (Amersham, UK) in a semi-dry transfer system (Bio-RAD) (18v, 25 min). After overnight (o/n) blocking the membrane with 2% (w/v) skim milk in phosphate buffered saline (PBS) at 4 °C, 1:2000 dilution of Horse Radish Peroxidase (HRP) conjugated anti-His antibody (Sigma, USA) was added to the membrane for 2 h at room temperature (RT). The membrane was washed 4 times with PBS/Tween-20 (0.05%) and the corresponding His-tagged fusion protein band was visualized using 3,3'-diaminobenzidine (DAB) substrate (Sigma, USA).

Protein purification. To purify the recombinant protein, colonies was inoculated into 500 ml LB broth medium under the above-mentioned culture condition. Bacterial pellet was resuspended in lysis buffer I (50 mM NaH₂PO₄, 10 mM Imidazole, 300 mM NaCl; pH8.0) and sonicated by 20 pulses (20 s with the same interval time) and centrifuged at 10,000 rpm for 20 min at 4 °C. The pellet was resuspended in lysis buffer II (50 mM NaH₂PO₄, 300 mM NaCl, 10 mM Imidazole, 8 M Urea; pH8.0) and sonicated for further 3 pulses (20 s/pulse) and centrifuged again. The supernatant was filtered through 0.45 µm syringe filter and was loaded to the Ni-agarose resin (ABT Agarose Bead Technologies, Spain) under denaturing conditions. The column was washed with 30 volume of washing buffer I (50 mM NaH₂PO₄, 300 mM NaCl, 30 mM Imidazole, 8 M Urea, 0.1% Triton-X114; pH8.0) to remove weakly bounded proteins and bacterial lipopolysaccharides (LPS) followed by the second washing step

(50 mM NaH₂PO₄, 300 mM NaCl, 30 mM Imidazole, 8 M Urea, pH8.0) to remove residual Triton-X114. The recombinant protein was eluted by the elution buffer (50 mM NaH₂PO₄, 300 mM NaCl, 250 mM Imidazole, 8 M Urea; pH8.0) at a flow rate of 1.5 ml/min.

Refolding of the eluted protein was performed through dialysis in order to gradually remove urea (from 8 M to 0). The dialyzed protein was finally kept in phosphate-buffer (PB) (8 mM Na₂HPO₄, 1 mM KH₂PO₄, 137 mM NaCl, 3 mM KCl; pH7.4). Protein concentration was performed using Centriprep-3 kDa (Amicon, USA) and the protein concentration was measured by NanoDrop[™] 3000 spectrophotometer (Bio-RAD).

The pyrogenicity of the purified recombinant protein was quantified by Pyrotell gel clot LAL kit (USA; Sensitivity 0.25EU/ml of analyzed solution) according to the manufacturer's instruction. Briefly, Limulus Amebocyte lysate was incubated with serially diluted ABD-GCSF protein samples at 37 °C for 60 min and a positive test will be indicated by the formation of gel which does not collapse when the tube is inverted.

DTNB colorimetric analysis (Ellman). Ellman's reagent, 5, 5'-dithiobis-(2-nitrobenzoic acid) (DTNB), was used for quantification of free sulfhydryl groups in ABD-GCSF protein in comparison with Filgrastim. In brief, the reaction buffer (0.1 M sodium phosphate, 1 mM EDTA; pH8.0) containing 5 mM Filgrastim or different concentrations of ABD-GCSF (5, 3, 2, 1 mM) and DTNB was incubated at RT for 15 min. The change in optical absorbance was measured at 412 nm. The concentration of free thiol groups was measured using molar extinction coefficient of chromophore $(1.415 \times 10^4 \text{ M}^{-1} \text{ cm}^{-1})$. The negative control sample was DTNB in the absence of any protein. Different concentrations (1.5, 1.25, 1.0, 0.75 and 0.25 mM) of cysteine amino acid solution were used as positive control.

Size exclusion chromatography (SEC). For comparing the hydrodynamic volume of commercially available GCSF protein (Filgrastim; Pooyesh Darou, Iran) and ABD-GCSF, size exclusion chromatography (SEC) was carried out according to the European Pharmacopoeia version 9.1. In brief, proteins were diluted in 0.06 M sodium acetate (pH4.0) to 200 μ g/ml. In the next step, 8 μ g of each protein was injected into TSK gel G3000SWxl column (Tosoh Bioscience, Japan) connected to a Shimadzu HPLC system (Kyoto, Japan) and eluted by an isocratic mobile phase of 0.03 M (NH₄)₂HPO₄ (pH7.0) at a flow rate of 0.5 ml/min at 30°C. The ultraviolet (UV) absorbance was recorded at 215 nm. Molecular weight of the proteins was also estimated based on the retention time of gel filtration standard protein (Bio-RAD, Cat No. 151-1901).

DLS. Dynamic light scattering experiments were performed to determine the effect of ABD tag on hydrodynamic radius of the GCSF protein. In brief, 0.5 mg/ml of each protein (Filgrastim, PEG-Filgrastim manufactured by CinnaGen, Iran, and ABD-GCSF) was prepared in double distilled water (ddH₂O) and analyzed by Zetasizer ZEN3600 system (Malvern, Germany) at 25 °C. All results were reported as hydrodynamic radius in nm.

IFS. To investigate tertiary conformational changes, intrinsic fluorescence emissions of proteins were measured using Cary Eclipse Varian Spectrophotometer (Agilent Technologies, Germany) in emission wavelength ranging from 300 to 400 nm. 300 µg/ml concentration of the proteins was prepared in PBS (pH7.4) in 1 cm path length quartz cells. Fluorescence emission was excited at 295 nm. Excitation and emission slits of 5 and 10 nm were considered.

CD analysis. For finding possible secondary structural changes of ABD-GCSF protein in comparison to the commercially available GCSF molecules (Filgrastim and PEG-Filgrastim), Circular dichroism (CD) analysis was performed using J-810 Spectropolarimeter (Jasco Instruments, Japan). In brief, 0.2 mg/ml protein in double distilled water (ddH₂O) was exposed to far (190–260 nm) and near (250–320 nm) UV spectra within 1 mm path length quartz cell at 25 °C. CD spectra were recorded by the average of two scans, 1 nm band width and scanning speed of 500 nm/min.

Albumin binding assay. A home-made ELISA assay was developed to measure the affinity of ABD-GCSF towards human serum albumin (HSA). In brief, 96-well plate was coated with HSA (1 μ g/well) in carbonate-bicarbonate buffer at 4 °C (o/n). The plate was blocked with 2%w/v skim milk for 2 h at 37 °C. After washing step with PBS supplemented with 0.05% Tween-20, serial dilution of ABD-GCSF (0-1000 nM) was added to the wells and incubated for 2 h RT. HRP-conjugated anti-His antibody (1: 2000) was used as the secondary antibody. Assessment of binding reaction was done using 3,3',5,5'-Tetramethylbenzidine (TMB) substrate (Sigma, USA).

 $\rm H_2SO_4$ was added to the wells to stop the reaction and optical density was measured at 450 nm by a microplate reader (BioTeK, USA).

Pharmacodynamics. The effect of ABD-GCSF in acceleration of neutrophil count was investigated in normal Sprague Dawley male rats (6–7 weeks, 250–300 g weight). The research protocols and animal studies were approved by the Ethics Committee of Pasteur Institute of Iran (IR.PII.REC.1399.013) and followed ARRIVE reporting guidelines⁶². Animals were adopted to the conditions of light and humidity for one week and were randomly divided into five groups (five rats/group). The animals except control group (Group 1) intraperitoneally (*i.p.*) received 100 mg/kg of cyclophosphamide (CPA) for induction of neutropenia on day zero^{12,63}. On day 1, the rats in Groups 2 to 4 subcutaneously (*s.c.*) received 100 μ g/kg of Filgrastim, PEG-Filgrastim, or ABD-GCSF, respectively and the 5th group received PBS alone as control^{12,30,64}. Blood samples were collected from tail vein in non-vacuumed K₂EDTA Nex tubes (Nexamo Technoplast, India) according to the designed time schedule on 0, 1, 2, 3, 4, 5, 6, 7, 8, 9 and 11 days post GCSF injection. Complete blood counting (CBC) of neutrophils, lymphocytes, eosinophils, monocytes, red and white blood cells was done by hematology analyzer Celltac alpha (Nihon Kohden, Japan).

Pharmacokinetics. To determine the basic pharmacokinetic parameters of Filgrastim, PEG-Filgrastim and recombinant ABD-GCSF, plasma samples were used to quantitate GCSF concentration in the above-mentioned rat groups using human Quantikine GCSF ELISA kit (R&D Systems, USA). Briefly, blood samples were collected at 0, 0.5, 1, 2, 4, 8, 10, 24, 48, 76, 92, 120, 144, 168, 192 and 240 h post *s.c* drug injection and centrifuged at 3,000 rpm for 15 min to separate plasma. GCSF level was measured using the kit. Pharmacokinetic parameters were calculated using the log linear trapezoidal method. Half-life ($t_{1/2}$), maximum concentration (C_{max}), time of maximum concentration (T_{max}), apparent total clearance rate (CL/F), area under the plasma concentration–time curve (AUC) and AUC from time zero to the time that protein is detectable in the blood (AUC_{0-t}), AUC up to unlimited time (AUC_{0-c}), AUC up to the last measurable concentration (AUMC_{0-t}), and mean residence time (MRT) were calculated. Linear regression of terminal log-linear phase and residual method were respectively used for obtaining of terminal rate constant (K_{el}).

Statistical analysis. GraphPad Prism (v. 8.0) and SPSS software (v. 21) were used. All data were reported as mean \pm SD. *P* values less than 0.05 were considered significant.

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Author contributions

Y.T., and Y.H.A were chief investigators and revised the manuscript. Y.T., and L.N involved in design of the study. F.Y.N., was responsible for the major experimental work and contributed in writing the manuscript. E.M. and Y.H.A were responsible for animal experiments. S.S. contributed in CD analysis. S.Sh., E.B., M.S., and H.A.M.A assisted in data collection.

Competing interests

The authors declare no competing interests.

Additional information

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