



OPEN

Au nanoparticles modified CuO nanowire electrode based non-enzymatic glucose detection with improved linearity

Ashwini Kumar Mishra¹, Deepak Kumar Jarwal¹, Bratindranath Mukherjee², Amit Kumar¹, Smrity Ratan¹, Manas Ranjan Tripathy¹ & Satyabrata Jit¹✉

This paper explores gold nanoparticle (GNP) modified copper oxide nanowires (CuO NWs) based electrode grown on copper foil for non-enzymatic glucose detection in a wide linear ranging up to 31.06 mM, and 44.36 mM at 0.5 M NaOH and 1 M NaOH concentrations. The proposed electrode can be used to detect a very low glucose concentration of 0.3 μM with a high linearity range of 44.36 mM and sensitivity of 1591.44 $\mu\text{A mM}^{-1} \text{cm}^{-2}$. The electrode is fabricated by first synthesizing Cu(OH)₂ NWs on a copper foil by chemical etching method and then heat treatment is performed to convert Cu(OH)₂ NWs into CuO NWs. The GNPs are deposited on CuO NWs to enhance the effective surface-to-volume ratio of the electrode with improved catalytic activity. The surface morphology has been investigated by XRD, XPS, FE-SEM and HR-TEM analysis. The proposed sensor is expected to detect low-level of glucose in urine, and saliva. At the same time, it can also be used to measure extremely high sugar levels (i.e. hyperglycemia) of ~806.5454 mg/dl. The proposed sensor is also capable of detecting glucose after multiple bending of the GNP modified CuO NWs electrode. The proposed device is also used to detect the blood sugar level in human being and it is found that this sensor's result is highly accurate and reliable.

According to the world health organization (WHO), the number of diabetic patients is expected to reach up to 500 million by 2030^{1,2} in the world. Diabetic causes some severe complications like heart attack, stroke, kidney failure, vision loss and nerve damage³. The normal range of blood glucose concentration lies in the range of 80–120 mg/dl (4.4–6.6 mM) for a healthy person³. In general, blood glucose levels greater than 126 mg/dl when fasting and greater than 200 mg/dl at 2 h after meals are considered to be hyperglycemia³ which is dangerous from the health point of view. On the other hand, glucose level below 54 mg/dl is known as hypoglycemia which also needs immediate medical attention. Thus, it is required, especially for the diabetic persons with glucose levels above the normal range, to check the glucose level in blood regularly. As a result, glucose sensors have covered nearly 85% of the entire biosensors markets³. However, accurate and fast assessment of glucose level in blood is still challenge in biological and medical analysis^{4,5}. Different techniques have been explored in electronic biosensors for detecting various chemical analytes like glucose, cholesterol, other fluids, gases etc^{6–11}. In general, the resonance and capillary-zone electrophoresis methods are used in electronic glucose sensors^{11–13}. However, the electrochemical based glucose level estimation techniques have drawn considerable attention of the researchers due to its natural simplicity, high sensitivity and good selectivity^{14–16}.

Electrochemical glucose sensors are of two types depending on the electro-catalyst used on the sensor electrodes¹⁰. The first is enzymatic type glucose sensors that requires an enzyme like glucose oxidase (GOx), GDH, etc. on the electrode while the second type is called non-enzymatic glucose sensors which requires no enzymes in electrode for detection^{10,17,18}. Although the enzymatic glucose sensors possess high sensitivity, high selectivity, and low detection limit¹⁹, but they suffer from poor stability resulted from variations of operating temperatures, pH values and relative humidity. Further, the enzymatic glucose sensors are costlier than the non-enzymatic glucose sensors due to requirement of costly enzymes^{20–23}. Thus, a significant emphasis has been given on the development of low-cost, accurate and fast-response based non-enzymatic glucose sensors^{24–26}.

¹Department of Electronics Engineering, Indian Institute of Technology (BHU) Varanasi, Varanasi 221005, India. ²Department of Metallurgical Engineering, Indian Institute of Technology (BHU) Varanasi, Varanasi, India. ✉email: sjit.ece@iitbhu.ac.in

It is reported that performance improvement of such non-enzymatic glucose sensors can be achieved using electrodes with high conductivity, large specific surface area, high stability, good selectivity and good reproducibility with high capability of effective electron transfer from the electro-catalyst to the conductive surface of the electrode²⁷. Several noble metals such as Pd, Au and Pt as well as their composites like Pt–Pd, Pt–Au, Au–Pd etc. have explored for glucose sensing^{28–30}. However, the cost of these metals have encouraged to explore the possibility of metal oxides such as CuO, NiO, ZnO, Cu₂O, MnO₂, Fe₂O₃, SnO₂ and Ag₂O for developing low-cost non-enzymatic glucose³¹. Among them, CuO has been widely used for developing low-cost glucose sensors due to its good electrochemical and electro-catalytic properties, and abundant availability^{11,16,25,27,32,33}. The intrinsically p-type semiconductor CuO with a band-gap of ~1.2 eV has also been extensively used in electrochemical sensors, photoelectric devices, gas sensors and lithium-ion batteries due to its interesting electrical and optical properties^{15,34–36}. Various CuO nanostructures (e.g. nanowires, nanorods, nano flower, etc.) grown on a copper foil using easy and simple synthesis techniques have been reported for low-cost glucose sensors with a fast response, high sensitivity, and stable detection due to their enhanced catalytic property over the other metal oxide nanostructures¹¹.

Li et al.²⁷ have synthesized CuO nanowires (NWs) on 3-D copper foam by anodization process for glucose detection. They²⁷ have achieved high sensitivity and wider linear range up to 18.8 mM at a concentration of 1 M NaOH. The high catalytic activity of the metal oxide and high conductivity of the noble metals have also encouraged to use nanocomposites of ≥95% metal oxide and ≤5% noble metal for glucose-sensing applications. Li et al.³⁷ have tried Au/CuO (metal and metal oxide) nano-composite (nano-cauliflower) to sense glucose for the first time.

They³⁷ have achieved a detection limit of 0.3 μM, the sensitivity of 708.7 μA mM⁻¹ cm⁻² and linear range from 0.0001 mM to 30 mM at a concentration of 1 M of NaOH. Xio et al.³⁸ have used Au/CuO Nanohybrids to get a sensitivity of 374 μA mM⁻¹ cm⁻² with linearity up to 12 mM at a concentration of 0.1 M NaOH (pH = 13) while Wang et al.¹⁹ have got the sensitivity of 709.52 μA mM⁻¹ cm⁻² and linearity up to 8 mM at a concentration of 0.1 M NaOH. The nano-composite of CuO (metal oxide) nanostructure and Au (metal) nanostructure shows the enhancement of conductivity to accelerate the rate of electron transfer, selectivity and sensitivity of glucose sensing³⁷. In such glucose sensors, the direct electron transfer property of CuO NWs acts as catalysts whereas the large surface-to-volume ratio of Au nanoparticles can act as co-catalyst for enhancing the linearity and sensitivity in a drastic manner of the glucose sensors.

There are still challenges to develop glucose sensors with a wide range of linearity and high sensitivity for detecting the glucose levels in moderate to severe diabetic patients. Recently, Mishra et al.³⁹ have observed a significant increase in sensitivity, linearity, and selectivity in gold nanoparticles (GNPs) modified CuO NWs based glucose sensors at low-concentration of 0.1 M of NaOH solvent. In this article, we have demonstrated the improvement of linearity and sensitivity of the GNPs modified CuO NWs electrode based glucose sensor using the higher levels of electrolyte (NaOH) concentrations at 0.5 M and 1 M.

Results and discussions

Characterizations of electrodes. Synthesis and electrode fabrication is briefly illustrated in Fig. 1(a) along with detail explanation in experimental sections. Figure 2a shows the XRD patterns of Cu foil, Cu(OH)₂ NWs, CuO NWs, and CuO NWs with GNP which are compared with standard JCPDS file numbers 04–0836, 35–0505, 80–1917, and 04–0784 of Cu, Cu(OH)₂, CuO NWs, and GNPs modified CuO NWs, respectively. The crystalline sharp peaks found at 43.37 degrees, 50.61 degrees, and 74.27 degrees correspond to (111), (200) and (220) of FCC Cu confirming composition of the foil. The other two minor peaks at 35.39 degrees and 38.65 degrees are due to impurities of native oxide of copper. The XRD of Cu(OH)₂ NWs sample also shown in Fig. 2(a) matches well with the orthorhombic phase (JCPDS 35–0505) thereby confirming the successful growth of Cu(OH)₂ NWs on the Cu foil. Heating induced dehydroxylation leadsto re-crystallization and formation of CuO nanowires as evident from the XRD plot (JCPDS 80–1917) which is also shown in Fig. 2a. The comparison of the XRD pattern of the CuO NWs with GNP in Fig. 2a with those of CuO NWs confirm that other minor peaks in the XRD of the CuO NWs with GNP have resulted from the small amount of gold nanoparticles (GNP) uniformly grown on the CuO NWs. The FE-SEM image obtained for low magnification to high magnification for CuO NWs with GNP grown on Cu foil is shown in Fig. 2b–d.

The Field Emission Scanning electron microscopy (FE-SEM) images to illustrate morphology of CuO NWs with GNP under study are shown in Fig. 1b with low resolution. Moderate and high resolutions of CuO NWs with gold nanoparticles are shown in Fig. 2c–d. On the basis of Fig. 2c–d the diameter of the nanowire was observed in the range of 150–250 nm.

HRTEM image analysis gives us better investigations of the surface morphology of CuO NWs with GNP as shown in Supplementary Fig. S1. The free-standing of TEM images of CuO NWs with GNP is obtained after scrapping from the Cu substrate shown in Supplementary Fig. S1(a). The image of Supplementary Fig. S1(b) clearly shows the dark spot of well-distributed gold nano-particles on CuO NWs. In Supplementary Fig. S1(b) the presence of dark spot was due to higher atomic weight of gold (Au) in comparisons Cu and O. The average diameter of gold nanoparticles are found in the range of 10–30 nm and the diameter of the CuO NWs are found in the range of 100–150 nm. The selected area electron diffraction (SAED) pattern of the gold CuO NWs with GNP from the scanning image area is shown in Supplementary Fig. S1(c). The diameter of the first three circles corresponds to CuO (202), CuO (111)/Au (111), and CuO (002), with a d-spacing of 1.58 Å, 2.32 Å, and 2.5 Å, respectively. Further, the image is magnified as shown in Supplementary Fig. S1(d) and S1 (e) where dark spot shows the gold (Au) Nanoparticles and the white spot shows the presence of CuO NWs. Supplementary Fig. S1(f) shows the lattice spacing measurements for dark and white regions as 2.32 Å, and 2.5 Å, respectively which confirm the presence of Au (111) and CuO (002). Bright field TEM image of CuO NWs has been shown in

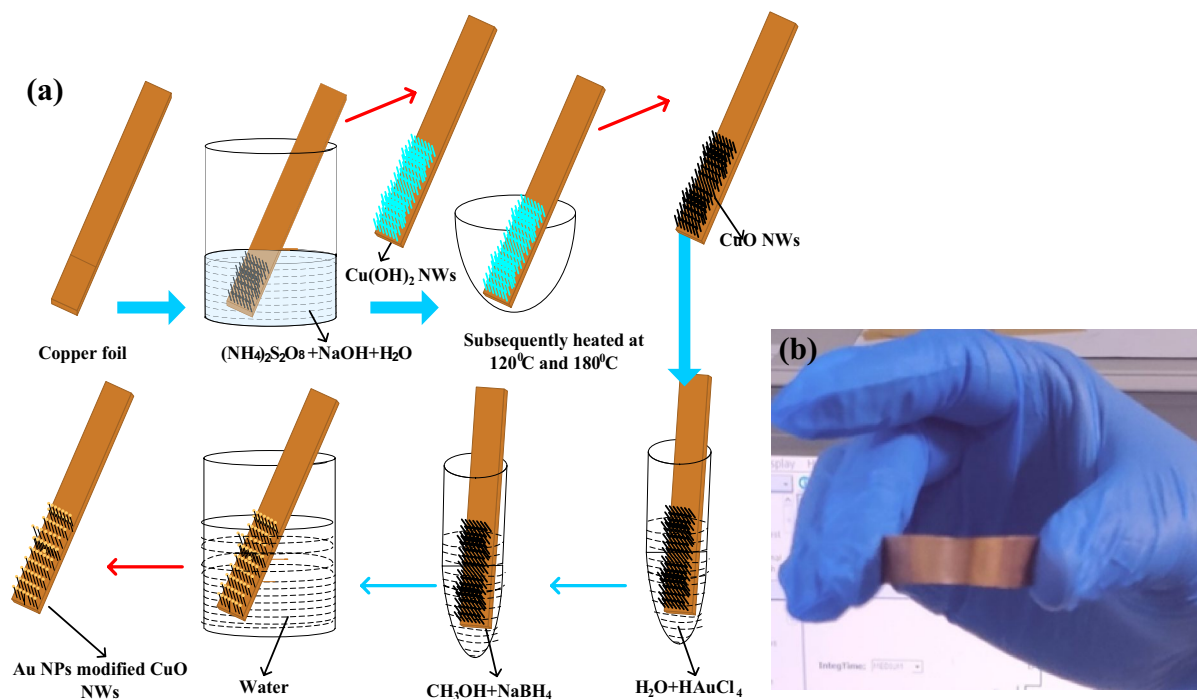


Figure 1. (a) Fabrication step of gold modified CuO NWs on Cu foil electrode, and (b) Bendable copper foil.

Supplementary Fig. S2. There are no dark spot in the Supplementary Fig. S2(a) to (c), as it was present in Supplementary Fig. S1. SAED pattern shown in Supplementary Fig. S2(d) also confirms the absences of gold in the CuO NWs. Material composition and EDS spectra of the CuO NWs with GNP are shown in Supplementary Fig. S4.

The characterization details of the surface composition of CuO NWs and CuONWs with GNP (gold nanoparticles) were shown in Fig. 3. The whole spectrum of CuO NWs GNP shows the presence of Cu, O, Au, C, and Na atoms, which is shown in Fig. 3(a). The high resolutions spectra for O 1s are shown in Fig. 3(b) which depicts two peaks in CuO NWs GNP at 531.16 eV and 532.27 eV equivalent to the oxygen vacancies or defect (O_v) present because of O_2 species in the lattice (O_L) and dissociated (O_C) oxygen species^{40–42}. The XPS of Cu 2p core level is expressed in Fig. 3(c) where two peaks of energy 934 eV and 954 eV are shown in Fig. 3(c) which corresponds to Cu 2p_{3/2} and Cu 2p_{1/2} respectively which confirms the existence of the Cu⁺². Two more peaks present at 941.8 eV and 961.9 eV are the satellite peaks of Cu2p_{3/2} and Cu2p_{1/2} respectively. They show the presence of the unfilled shell of 3d which again proves the presences of Cu⁺² in the sample. Gold (Au) 4f core of the Au/CuO nanostructure (shown in Fig. 3(d) has been filled with two peaks i.e. Au 4f_{7/2} and Au 4f_{5/2} with binding energy 84.0 eV and 87.7 eV which prove the presences of gold on CuO nanowires. For the selection of the better electrode the different copper oxide has been chosen like Cu (OH)₂ NWs, CuO NWs and CuO NWs with GNP. The current which is observed in the case of Cu(OH)₂ NWs is very low, moderate for CuO NWs and extremely high for CuO NWs with GNP in the solution of 0.5 M NaOH and 1 mM glucose concentrations.

Due to the very high current observed in CuO NWs with GNP, we can use it as a working electrode for this research work. The drastic improvement with CuO NWs with GNP is due to intensive increments in surface to volume ratio for CuO NWs with GNP electrode. The C–V graph of the different working electrodes has been shown in Fig. 4(a).

CuO NWs with GNP electrode are dipped in the solution of 0.5 M NaOH with different concentrations of glucose at 0 mM, 1 mM, 2 mM, 3 mM 4 mM, and 5 mM. It is observed that the current increases with an increase in glucose concentration and linearity is found to be maintained as elucidated in Fig. 4(b). Figure 4(c) again shows the C–V plot same as Fig. 4(b) which covers the complete range of glucose for the working electrode at a solution concentration of 0.5 M NaOH up to till 31.05 mM which linearity is maintained. The final relation between current and concentration is shown in Fig. 4(d). It shows the sensitivity of the sensors 1429.43 $\mu\text{A cm}^{-2}$ with $R^2 = 0.9927$ and linearity shows a maximum value of 31.05 mM.

The current–voltage graphs for the GNPs modified CuO NWs based electrodes with different scan rates are shown in Fig. 5(a). This figure confirms the redox reaction model. The linearity graph of the cathodic peak current and anodic peak current with different scan rates (5 mV s^{-1} to 500 mV s^{-1}) is shown in Fig. 5(b). In view of the above discussion, it can be easily observed that the redox reaction model is surface-confined process^{43,44} and the glucose molecule directly oxidizes the composite surface of CuO NWs with GNP and the electrons were directly transferred without any mediators.

The studied electronics properties over the surface are corroborated from the measurements of the electrochemical impedance spectra (EIS). EIS measurements are clearly shown in Fig. 5(c) depicts the gradual enhancement of conductivity from Cu (OH)₂NWs electrode to CuO NWs with the GNP electrode. Figure 5(c)

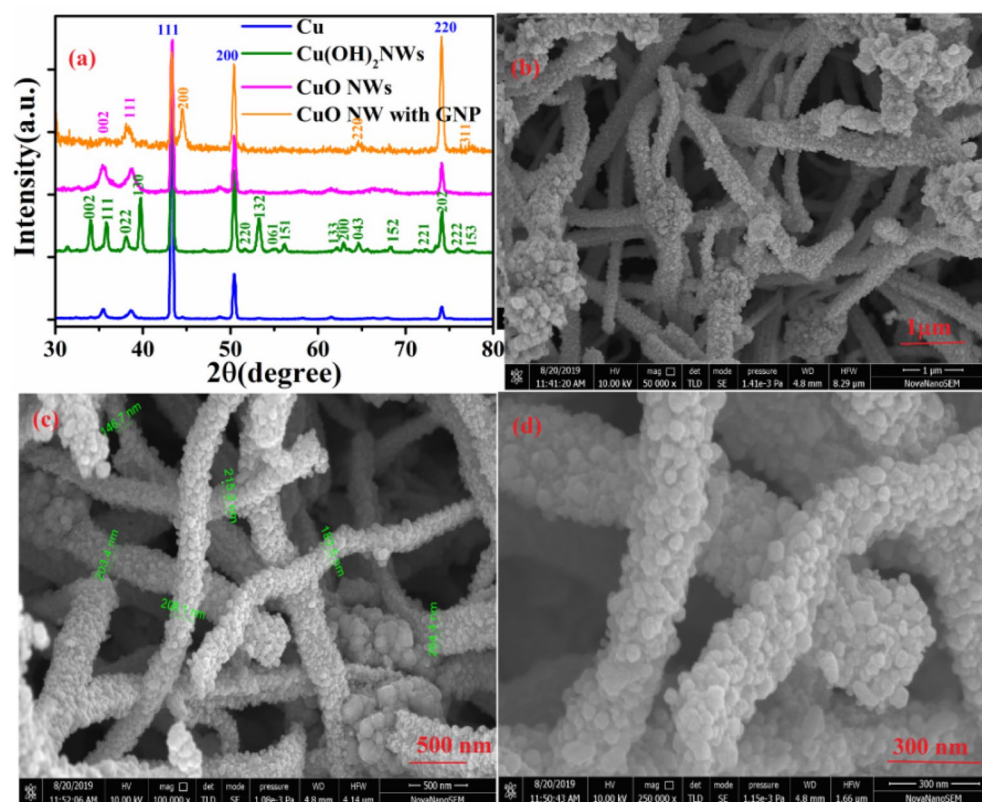


Figure 2. (a) XRD pattern of as synthesis Cu foil electrode, $\text{Cu}(\text{OH})_2\text{NWs}$, CuONWs and CuO NWs with GNP. (b) Low resolution of FESEM image of CuO NWs with GNP. (c) Moderate-resolution of FESEM image of CuO NWs with GNP. (d) High resolution of FESEM image of CuO NWs with GNP.

also reveals that the resistance is getting reduced and conductivity is getting enhanced due to decoration of gold nanoparticles on CuO NWs . EIS measurements have been taken place by considering a frequency range from 10^5 Hz to -0.1 Hz with an open circuit potential of 26 mV. Nyquist plot of the ($\text{Cu}(\text{OH})_2$) NWs, ($\text{Au}/\text{Cu}(\text{OH})_2$) NWs, Copper Oxide (CuO) NWs, and CuO NWs with GNP are shown in Fig. 5(c). The smallest semicircle of CuO NWs with GNP clearly shows the lowest resistance and higher conductance which confirms the accelerated rate of electrons transfer in the presence of gold nanoparticles.

Uric acid (UA), ascorbic acid (AA), dopamine (DA), sucrose, lactose, and maltose are the various interferences components along with glucose present in human blood serum. The concentration of glucose in human blood serum is approximately 30 times more than the components of the above interference^{45,46}. Due to the aforesaid reasons, the selectivity of CuO NWs with GNP electrode-based glucose sensor under study was examined at 1 mM glucose with these interfering elements of 0.2 mM each of lactose, sucrose, and maltose, UA, AA, and DA. Due to increased oxidation of glucose in comparison to other interferences components, the change in current was significantly high for glucose in comparison to other interferences species⁴⁷ which is as shown in Fig. 5(d). At the concentration of 1 M NaOH solution, working electrode CuO NWs with GNP has been used for measuring the current with an increase in glucose concentration. At the fixed voltage of 0.55 V, the increment in current was directly proportional to the amount of glucose added in the solution.

Reusability, reproducibility, and stability tests. The important factors for measuring the efficiency of the sensing devices are reusability, reproducibility, and stability. For the reusability, CuO NWs with the GNP electrode was dipped into a freshly prepared sample containing 1 mM of glucose in 0.5 M NaOH solutions at 50 mVs^{-1} scan rate and the resultant data were shown in Supplementary Fig. S3(a) and (b). The electrode was dipped in the solution for at least 10 times in the same solution or 10 different solutions. It is observed that CuO NWs GNP glucose sensing electrode retains more than 99% of its original response which shows its reusability. To test reproducibility, 10 freshly prepared Au/CuONWs with GNP electrode have been used in 1 mM of glucose solution of 0.5 M NaOH with a scan rate of 50 mVs^{-1} . The peak current of each electrode is mentioned in the C–V graph as shown in Fig. Supplementary Fig. S3(c) and (d). The response of these electrodes is found to have a relative standard deviation of 5%. It can be concluded from the above discussion that the sensors based on CuO NWs with GNP electrode are good enough to reproduce approximately the same results which show the sensor reproducibility. To add more functionality to the sensor, stability test was evaluated by the C–V response of the CuONWs with the GNP electrode at an interval of 3 days for a month as shown in Supplementary Fig. S3 (e). The electrode was stored at room temperature upto the completion of the measurement. After the completion

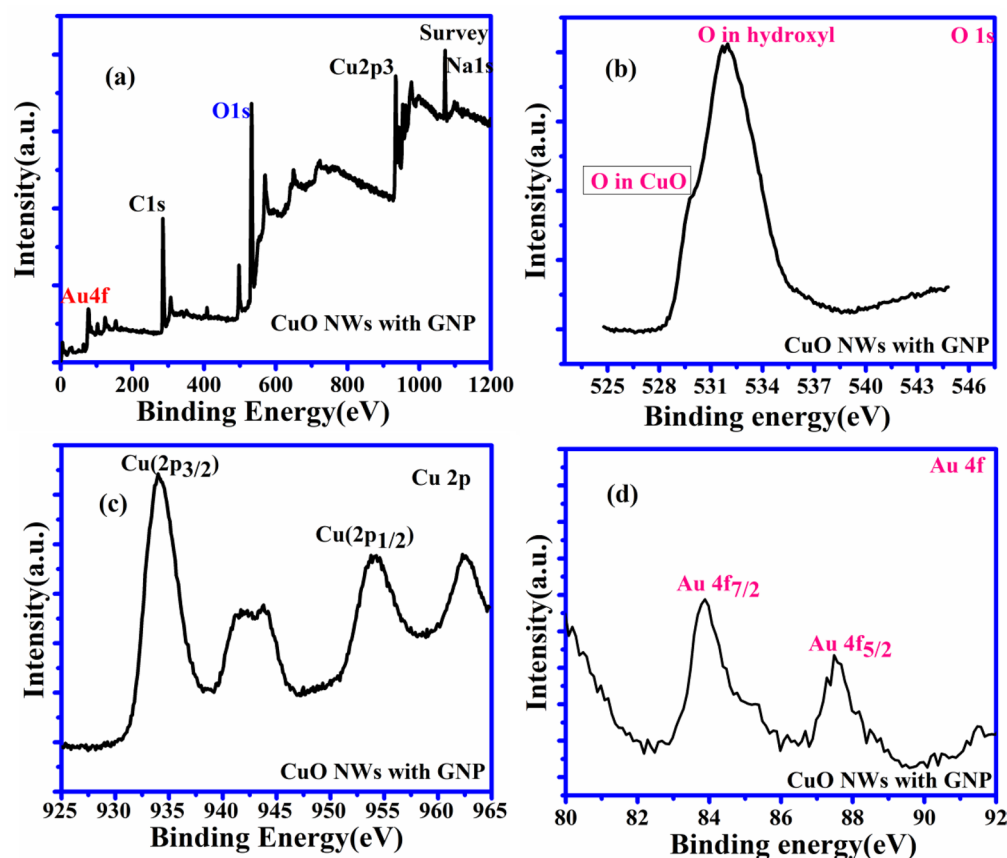


Figure 3. XPS analysis. (a) XPS spectrum of CuO NWs with GNP showing full scan survey (b) and corresponding de-convoluted peaks in the high-resolution spectra for O 1s (c) Cu 2p (d) Au 4f.

of 30 days, the response of the proposed CuO NWs with the GNP electrode was compared with the response of the electrode on the first day. The result is shown in Supplementary Fig. S3(f) as a histogram plot which conveys the information that the proposed sensor is very much stable which is able to retain 95% (measured on day 30) of its original response (measured on day 0). The excellent stability response of the electrode was due to the stable grown of CuO NWs with GNP on the surface of the electrode which provides strong mechanical stability to the sensing device.

In all the above discussion the C–V measurement is done at 0.5 M NaOH. To test the sensor feasibility, we have also measured the C–V characteristics at 1 M NaOH solution as shown in Fig. 6(a) along with different concentrations of glucose. At a fixed potential of 0.55 V and the scan rate of 50 mV s⁻¹, it is observed that the increment in current density is directly proportional to the amount of glucose added in the solutions. The linearity between current density and glucose concentration is shown in Fig. 6(b). The sensitivity of 1591.44 mA M⁻¹ cm⁻² with a wide linear range up to 44.36 mM is observed for the proposed sensor with 1 M NaOH. Due to this significant improvement in linearity with 1 M NaOH, the sensor is capable enough to detect the glucose level in highly diabetic patients. Figure 6(c) shows the C–V characteristics with different scan rates. The significance of this plot is to show that the proposed sensor is also showing linearity with varying scan rates. Figure 6(d) shows C–V characteristics with varying scan rates keeping the potential (voltage) constant. Here also we can observe that the linearity is still maintained by varying scan rates.

Sensitivity and linearity of the different Au-nanoparticles decorated CuO NWs (working electrode) have been given in Table 1. From the Table 1 it can be easily conclude that at 0.5 M and 1M NaOH solutions, this sensors are works for an extremely serious diabetic patients(linearity up to 31.05 mM and up to 44.36 mM) with good sensitivity.

To see the practical application of proposed device, real blood samples have been taken from our research group for testing in a private pathology laboratory named Dr. Lal Pathology Lab just located outside of our institute. The real time blood reports have been compared with the results obtained from our proposed sensor in Table 2. Approximately 100 μ L blood is added into 9.90 ml of 0.5 M NaOH solutions, and the current density-concentrations responses are measured at Voltage = 0.55 V. The blood glucose concentration in the human blood serum is measured through the calibrated curve shown in Fig. 4(d). Each sample has been used 3 times and the average value has been taken for the comparison. It has been observed that our proposed sensor data are closely matched with the data provided by the Dr. Lal Pathology Lab. The maximum difference between our proposed

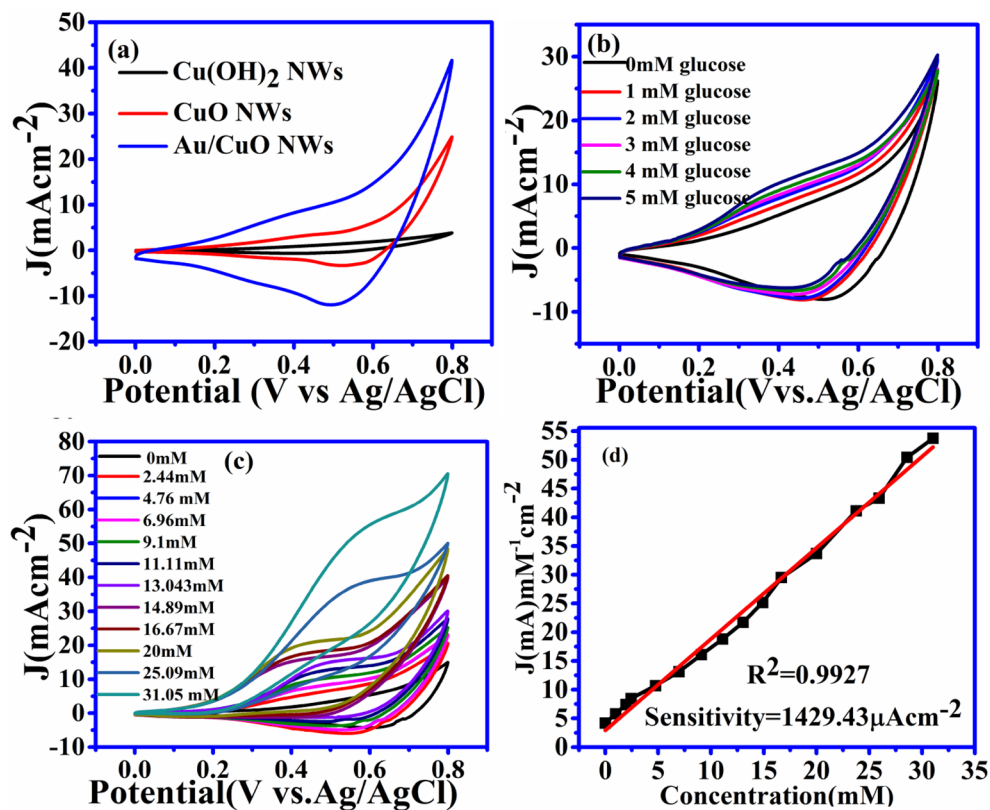


Figure 4. C–V curve of the electrode. (a) Current density versus potential graph for different type of electrode. (b) Current density of CuO NWs electrode with different concentration of glucose from 0 to 5 mM. (c) CV curve of Au/CuO type electrode with different concentration from 0 to 31.05 mM. (d) Corresponding calibration between concentration and current density at 0.55 V of reference voltages.

sensor data and the data provided by the Lal Pathology Lab is ~ 3.6%. Thus, we safely conclude that our proposed sensor can be used for commercial glucose sensing applications.

In the summary, a facile step is involved in the fabrication of GNPs modified CuO NWs electrode-based non-enzymatic glucose sensors. GNPs coated CuO NWs enhance the effective surface-to-volume ratio of the electrode with respect only CuO, NWs based electrodes. This improves the catalytic property of the electrodes which, in turn, enhances the oxidation and reduction properties of the GNPs coated CuO NWs electrode. These enhanced properties in the proposed sensor gives a sensitivity of $1591.44 \mu\text{A mM}^{-1} \text{cm}^{-2}$ and $1,440.63 \mu\text{A mM}^{-1} \text{cm}^{-2}$ at a concentration of 1 M and 0.5 M NaOH, respectively. The linearity ranges of the glucose sensor are 44.36 mM and 31.05 mM at 1M and 0.5 M NaOH solvent concentrations respectively. The low detection limit of the sensor at different concentrations shows that the sensors can be used to detect extremely low glucose levels in saliva and urine. The results reported here are highly accurate and stable.

Experimental section

The fabrication and characterization methods of the electrode are nearly similar to our previous works reported elsewhere³⁸. However, we have briefly discussed the fabrication and characterization of the electrode here for the clarity of the readers. We have also included some new characterization results for the better understanding of the readers.

Materials

Alfa Aesar, Thermo Fisher Scientific (India) has provided the highly pure copper foil (99.9%) used as substrate for CuO NWs. Sodium hydroxide (NaOH), hydrochloric acid (HCl), ammonium persulfate [(NH₄)₂S₂O₈], acetone, isopropanol, and Malt extract powder have been bought from Merck Life Science Private Limited (India). Sisco Research Laboratories Private Limited (India) has provided glucose, sucrose, and uric acid. All the chemicals used are ultra-pure and of analytical grade, hence there is no need for further cleaning. DI water of high resistivity (18MΩ-cm) obtained from Merck Millipore system is used for cleaning purposes.

Electrodes preparation. *Formation of Cu(OH)₂ NWs electrode.* Small pieces of (5 mm × 5 mm) of copper foil have been prepared from the bulk copper sheet. These copper foils are first cleaned ultrasonically in DI water and HCl. Again these copper foils have been cleaned by acetone and isopropanol sequentially. After the

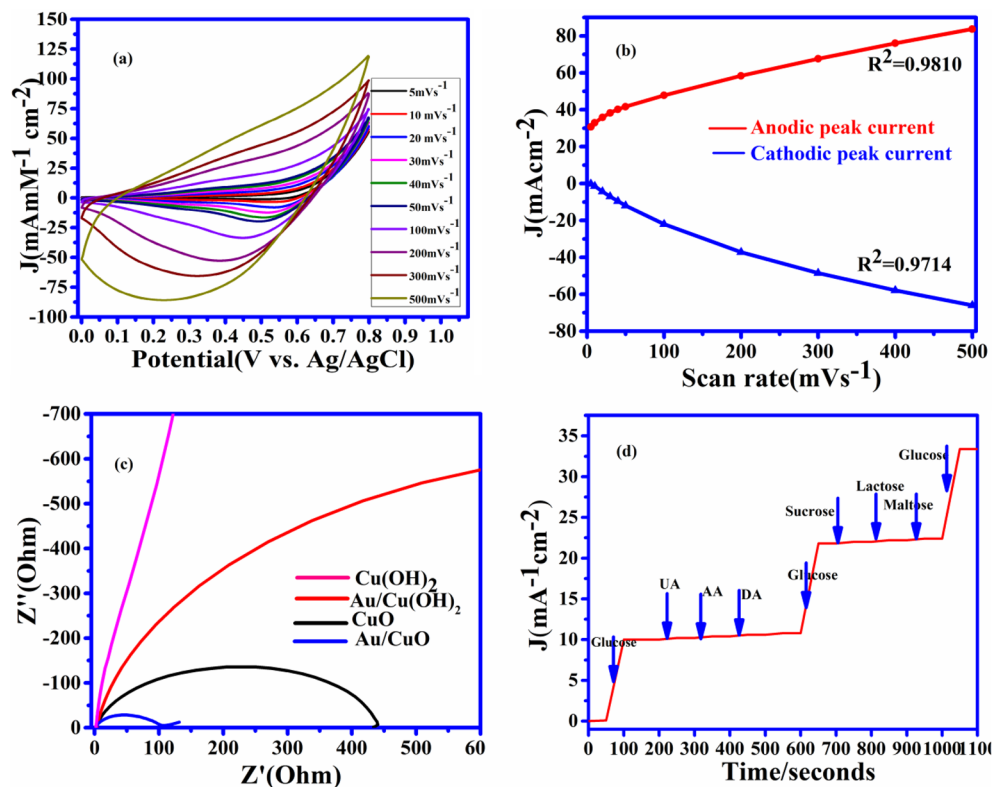
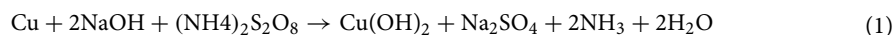


Figure 5. Electrochemical characterization (a) C–V obtain at 1 mM glucose in 0.5 M NaOH solution at different scan rates. (b) The graph between peak current density versus scan rate (c) Nyquist plot for different copper electrode $\text{Cu}(\text{OH})_2$ NWs, Au/CuO NWs, CuO NWs, and Au/CuO NWs at OCP (open circuit potential). (d) Anti-interference property of the CuO NWs decorated by GNP electrode with 1 mM of glucose and with 0.1 mM each of UA, AA, and DA. Then 1 mM of glucose with 0.05 mM sucrose, lactose, and maltose and 1 mM of glucose added in the last.

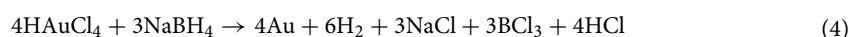
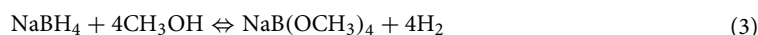
completion of the cleaning process, these foils have been dried in the air. These foils are then dipped in a solution consisting of 180 μl of DI water (H_2O), 80 μl of 10 M Sodium Hydroxide (NaOH), and 40 μl of 1 M Ammonium Thiosulphate ($(\text{NH}_4)_2\text{S}_2\text{O}_8$). After the completion of half an hour, these foils are taken out from the solution and dried in the flow of air. A deep blue film of $\text{Cu}(\text{OH})_2$ NWs on Cu foils has been obtained³³.



Formation of CuO NWs electrode. Deep blue colors of $\text{Cu}(\text{OH})_2$ on Cu foil were kept in alumina boat inside the furnace till half an hour in presences of Ar gas. The flow of Ar gas has been stopped after 30 min and foils are heated at 120 $^\circ\text{C}$ for three hours. For better crystallization, the foils were heated further at temperature 180 $^\circ\text{C}$ for two hours. The blue film of copper foils converted into black one and this is CuO NWs in the Cu foils³³.



Formation of gold NPs decorated CuO NWs electrode. CuO NWs were dipped in the solution of 3 ml DI water containing 8 mg tetra chloro auric Acid (HAuCl_4) for 10 min. After that rinse these foil in DI water. Again these foils were dipped in a solution containing 9 mg sodium borohydride (NaBH_4) dissolve in 3 ml methanol. Finally, the foil is again rinsed with DI water for 2 min, to get gold nanoparticle decorated CuO NWs electrode on copper foil. The following reaction takes place during the formation of a gold nanoparticle on the CuO NWs electrode³⁹.



Electrode characterizations and electrochemical set-up. The copper foils, $\text{Cu}(\text{OH})_2$ NWs, CuO NWs, and GNP modified CuO NWs are characterized using X-ray diffraction (XRD) (RIGAKU-SmartXDMAX, PC-20, 18-kW Cu rotating anode, Rigaku, Tokyo). The surface morphology of GNP modified CuO NWs is investigated by

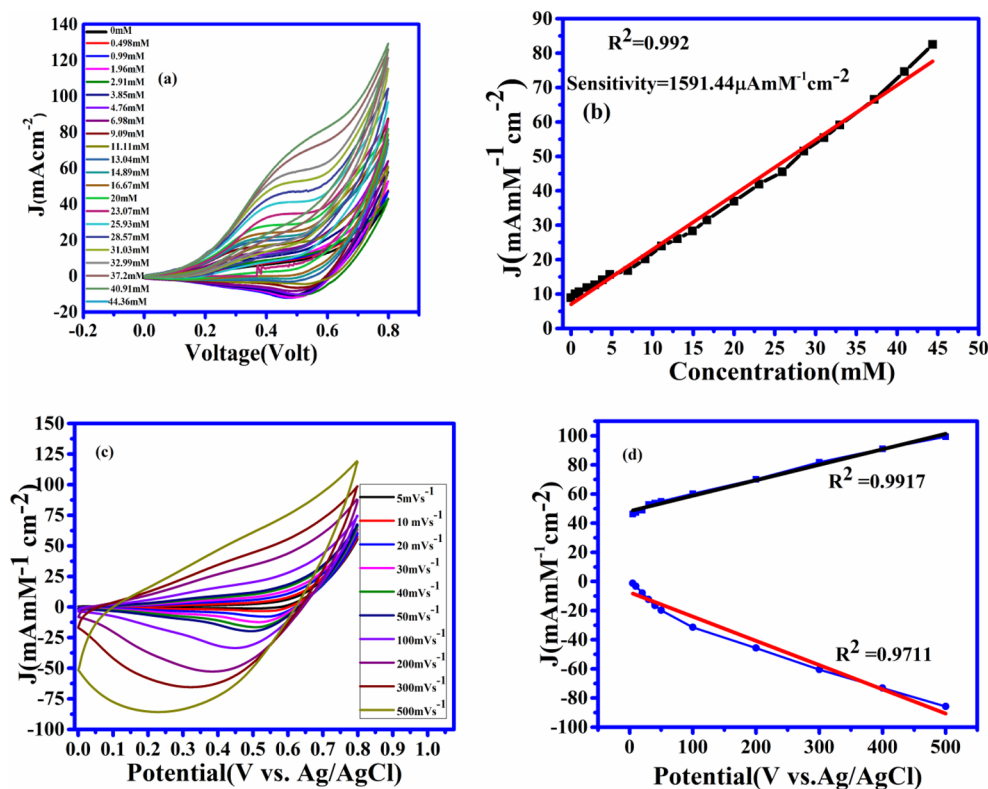


Figure 6. (a) C–V graph at 1 M NaOH solution with successive addition of glucose from 0 mM to 44.36 mM glucose solution. (b) Linearity graph between current density and concentration at 0.55 V of the reference voltage. (c) C–V graph with 1 M NaOH solution and 1 mM glucose concentration with different scan rates. (d) The linearity graph between current density and potential with different scan rates.

Sample	Sensitivity ($\mu\text{A mM}^{-1} \text{cm}^{-2}$)	Linear range (mM)	Detection limit (μM)	Solution concentrations (M)
CuO NWs with(GNP) ³⁸	4,398.8	0.005–5.9	0.5	0.1
CuO nanowires/ copper foam ²⁷	2,217.41	0.001–18.8	0.3	1
Au/CuO nanocauliflower ³⁷	708.7	0.001–30	0.3	1
3D Cu@ Cu ₂ O aerogels ⁴⁸	194.88	0.001–17.12	0.6	0.1
Cuo Nano Particles/Ag ⁴⁹	2,762.5	0.05–18.45	0.5	0.0001
ZnO Nano rod decorated by CuONPs ⁵⁰	2,961.8	0.001–8.45	0.40	0.1
CuO NWs with Au NPs (This work)	1,425.69	0.001–31.05	0.3	0.5
CuO NWs with Au NPs (This work)	1591.44	0.001–44.36	0.3	1

Table 1. Comparation of the non-enzymatic glucose sensors based on direct modification of working electrode.

Sample	Glucose concentration(mM) Spectrophotometric method(provided by health centre)	Proposed method(mM)	Recovery%	Error%
1	6.847(123 mg/dl)	6.6	96.4	3.6
2	5.34(97 mg/dl)	5.21	97.56	2.44
3	5.73(103 mg/dl)	5.64	98.42	1.57

Table 2. Detections of glucose in blood samples.

FE-SEM (Model-Nova Nano SEM FEI Company of USA (S.E.A.) PTE, LTD) and (HR-TEM) (Model-Tecnai G2 20 TWIN FEI Company of USA (S.E.A.) PTE, LTD). The electrochemical measurements were performed in a 3-electrode electrochemical cell configuration with CuO based electrodes as working electrodes, a platinum wire as counter electrode, and Ag/AgCl as a reference electrode with an electrochemical workstation (ModelCS: 350, S/N: 1,609,178, Corr test Instrument, China). The electrode preparation processes have been shown in Fig. 1(a) in which the steps involved in the formation of CuO NWs with GNP have been shown. Different concentration of NaOH (0.5 M and 1 M NaOH) solution has been used an electrolyte for measurement of cyclic voltammetry (C–V) at room temperature. In Fig. 1(b), bendable clean strip of copper foil is shown which is used in Fig. 1(a).

Received: 29 February 2020; Accepted: 1 June 2020

Published online: 10 July 2020

References

1. WHO Global Report. Global report on diabetes. *Isbn* 978, 6–86 (2016).
2. Zhao, N., Ma, L., Bai, S. & Wang, C. Correlation of blood glucose level and blood pH value with cardiac enzyme, amylase and other markers in patients with diabetes ketoacidosis. *Int. J. Clin. Exp. Med.* **11**, 10208–10214 (2018).
3. Wang, J. Electrochemical glucose biosensors. *Chem. Rev.* **108**, 814–825 (2008).
4. Aini, B. N., Siddiquee, S., Ampon, K., Rodrigues, K. F. & Suryani, S. Development of a glucose biosensor based on ZnO nanoparticles film and glucose oxidase-immobilized eggshell membrane. *Sens. Bio-Sens. Res.* **4**, 46–56 (2015).
5. Meher, S. K. & Rao, G. R. Archetypal sandwich-structured CuO for high-performance non-enzymatic sensing of glucose. *Nanoscale* **5**, 2089–2099 (2013).
6. Giusy, M. *et al.* Advances in wearable chemical sensors design for monitoring biological fluids. *Sens. Actuat.* **B211**, 403–418 (2015).
7. Singh, A. K., Pandey, A. & Chakrabarti, P. Fabrication, modeling and characterization of green light photosensitive p-channel-Poly[2,5-bis(3-tetradecylthiophen-2-yl)thieno[3,2-b]thiophene] organic semiconductor-based phototransistors. *Organic Electron.* **75**, 1 (2019).
8. Jarwal, D. K. *et al.* Efficiency improvement of TiO₂ nanorods electron transport layer based Perovskite solar cells by Solvothermal. *Etching.* **99**, 1–9 (2019).
9. Kumar, A. *et al.* Effect of PQT-12 interface layer on the performance of PCDTBT: PCBM bulk heterojunction solar cells. *Mater. Res. Express* **6**, 115514 (2019).
10. Zhu, H., Li, L., Zhou, W., Shao, Z. & Chen, X. Advances in non-enzymatic glucose sensors based on metal oxides. *J. Mater. Chem.* **B4**, 7333–7349 (2016).
11. Zhang, Y. *et al.* CuONWs Based sensitive and selective non-enzymatic base glucose detection. *Sens. Actuat. B* **191**, 86–93 (2014).
12. Jin, L. *et al.* Biomolecule stabilized Au nanoclusters as fluorescence probe for the detection of glucose. *Biosens. Bioelectron.* **26**, 1965–1969 (2011).
13. Wang, S., Su, P. & Hongjun E. & Yang, Y. Polyamidoamine dendrimer as a spacer for the immobilization of glucose oxidase in the capillary enzyme microreactor. *Anal. Biochem.* **405**, 230–235 (2010).
14. Quoc Dung, N., Patil, D., Jung, H. & Kim, D. A high-performance nonenzymatic glucose sensor made of CuO-SWCNT nanocomposites. *Biosens. Bioelectron.* **42**, 280–286 (2013).
15. Reitz, E., Jia, W., Gentile, M., Wang, Y. & Lei, Y. CuO nanospheres based non-enzymatic glucose sensor. *Electroanalysis* **20**, 2482–2486 (2008).
16. Lu, W., Qin, X., Asiri, A. M., Al-Youbi, A. O. & Sun, X. Ni foam: A novel three-dimensional porous sensing platform for sensitive and selective nonenzymatic glucose detection. *Analyst* **138**, 417–420 (2013).
17. Parlak, O. *et al.* structuring of Au nanoparticles on two-dimensional MoS₂ nanosheet for electrochemical glucose sensors. *Biosens. Bioelectron.* **89**, 545–550 (2017).
18. Wang, H. C. & Lee, A. R. Recent developments in blood glucose sensors. *J. Food Drug Anal.* **23**, 191–200 (2015).
19. Wang, X. Sensing of Cuo nanostructure and their application for non-enzymatic glucose sensing. *Sens. Actuat. B* **144**, 220–225 (2010).
20. Wang, Z., Liu, S., Wu, P. & Cai, C. Detection of glucose based on direct electron transfer reaction of glucose oxidase immobilized on highly ordered polyaniline nanotubes. *Anal. Chem.* **81**, 1638–1645 (2009).
21. Mani, V., Devadas, B. & Chen, S. M. Direct electrochemistry of glucose oxidase at electrochemically reduced graphene oxidemultiwalled carbon nanotubes hybrid material modified electrode for glucose biosensor. *Biosens. Bioelectron.* **41**, 309–315 (2013).
22. Bo, L. *et al.* Direct electron transfer glucose biosensors based on glucose oxidase self-assembled on electrochemically reduced. *Carboxyl Graph. Biosens. Bioelectron.* **43**, 131–136 (2013).
23. A sensitive Ag NPs/CuO nanofiber non-enzymatic glucose sensors based electrospinning technology **195**, 431–438 (2014).
24. Jin, L. *et al.* Biomolecule-stabilized Au nanoclusters as a fluorescence probe for sensitive detection of glucose. *Biosens. Bioelectron.* **26**, 1965–1969 (2011).
25. Gnana Kumar, G., Amala, G. & Gowtham, S. M. Recent advancements, key challenges and solutions in non-enzymatic electrochemical glucose sensors based on graphene platforms. *RSC Adv.* **7**, 36949–36976 (2017).
26. Zhang, Y. *et al.* Electrochemical deposition of nickel nanoparticles on reduced graphene oxide film for nonenzymatic glucose sensing. *Electroanalysis* **25**, 959–966 (2013).
27. Li, Z., Chen, Y., Xin, Y. & Zhang, Z. Sensitive electrochemical nonenzymatic glucose sensing based on anodized CuO nanowires on three-dimensional porous copper foam. *Sci. Rep.* **5**, 16115 (2015).
28. Chen, X. Non-enzymatic glucose sensors based on flower-shaped Au@pd Core-shell nanoparticles-ionic liquid composite film modified glassy carbon electrodes. *Electrochemical Acta* **56**, 636–643 (2010).
29. Habrioux, A. *et al.* Activity of platinum-gold alloys for glucose electrooxidation in biofuel cells. *J. Phys. Chem. B* **111**, 10329–10333 (2007).
30. Niu, X., Nonenzymatic glucose biosensors based on pt-pd nanoflakes. *Talanta* **99**, 1062–1067 (2012).
31. Cherevko, S. *et al.* The porous copper electrode fabricated by hydrogen bubble evolution and its application to highly sensitive non-enzymatic glucose detection. *Talanta* **80**, 1371–1377 (2010).
32. Chiang, C. Y. *et al.* Copper oxide photocathodes prepared by a solution-based process. *Int. J. Hyd. Energy* **37**, 8232–8239 (2012).
33. Ni, P. *et al.* Facile fabrication of CuO nanowire modified Cu electrode for non-enzymatic glucose detection with enhanced sensitivity. *RSC Adv.* **4**, 28842–28847 (2014).
34. Zhu, G. *et al.* Facile fabrication and enhanced sensing properties of hierarchically porous CuO architectures. *ACS Appl. Mater. Interfaces* **4**, 744–751 (2012).
35. Wang, B., Wu, X. L., Shu, C. Y., Guo, Y. G. & Wang, C. R. Synthesis of CuO/graphene nanocomposite as a high-performance anode material for lithium-ion batteries. *J. Mater. Chem.* **20**, 10661–10664 (2010).

36. Zhuang, Z. *et al.* An improved sensitivity non-enzymatic glucose sensor based on a CuO nanowire modified Cu electrode. *Analyst* **133**, 126–132 (2008).
37. Li, Z., Xin, Y., Zhang, Z., Wu, H. & Wang, P. Rational design of binder-free noble metal/metal oxide arrays with nanocauliflower structure for wide linear range nonenzymatic glucose detection. *Sci. Rep.* **5**, 1–10 (2015).
38. Xio, *et al.* Non-enzymatic glucose sensors based on controllable nanoporous gold/copper oxide nanohybrids. *Talanta* **125**, 366–371 (2014).
39. Mishra, A. K. *et al.* Superficial fabrication of gold nanoparticles modified CuO nanowires electrode for non-enzymatic glucose detection. *RSC Adv.* **9**, 1772–1781 (2019).
40. Zhang, X. *et al.* Effect of aspect ratio and surface defects on the photocatalytic activity of ZnO nanorods. *Sci. Rep.* **4**, 4–11 (2014).
41. Ahmad, R. *et al.* Ammonium ion detection in a solution using vertically grown ZnO nanorod based field-effect transistor. *RSC Adv.* **6**, 54836–54840 (2016).
42. Wang, Y. *et al.* Visible-light-responsive TiO₂-coated ZnO: I nanorod array films with enhanced photoelectrochemical and photocatalytic performance. *ACS Appl. Mater. Interfaces* **7**, 6093–6101 (2015).
43. Bai, Y. F., Xu, T. B., Luong, J. H. T. & Cui, H. F. Direct electron transfer of glucose oxidase-boron doped diamond interface: A new solution for a classical problem. *Anal. Chem.* **86**, 4910–4918 (2014).
44. Zhou, J., Liao, C., Zhang, L., Wang, Q. & Tian, Y. Molecular hydrogel-stabilized enzyme with facilitated electron transfer for determination of H₂O₂ released from live cells. *Anal. Chem.* **86**, 4395–4401 (2014).
45. Zhang, J., Ma, J., Zhang, S., Wang, W. & Chen, Z. A highly sensitive nonenzymatic glucose sensor based on CuO nanoparticles decorated carbon spheres. *Sens. Actuat. B Chem.* **211**, 385–391 (2015).
46. Mishra, A. K. *et al.* CuO nanowire-based extended-gate field-effect transistor (FET) for pH sensing and enzyme-free/receptor-free glucose sensing applications. *IEEE Sens. J.* <https://doi.org/10.1109/JSEN.2020.2966585> (2020).
47. Wang, J. & Zhang, W. D. Fabrication of CuO nanoplatelets for highly sensitive enzyme-free determination of glucose. *Electrochim. Acta* **56**, 7510–7516 (2011).
48. Gao, Y. *et al.* Three-dimensional porous Cu₂O aerogels for the direct voltammetric sensing of glucose. *Microchimica Acta* **186**, 192 (2019).
49. Ahmad, R., Vaseem, M. & Tripathy, N. Y. B. Wide linear range detecting non-enzymatic glucose biosensors on CuO nanoparticles inkjet printed on the electrode. *Anal. Chem.* **85**, 10448–10454 (2013).
50. Ahmad, R. *et al.* Highly efficient non-enzymatic glucose sensors based on CuO modified vertically grown ZnO nanorods on electrode. *Scientific report.* *Sci. Rep.* **7**, 5715 (2017).

Acknowledgements

The authors are also grateful for getting the opportunity to characterizations the facility for this work from the Central Instrument Facility Center, IIT (BHU) Varanasi. Authors are also thankfully acknowledged MEITY for the research scholarship to Ashwini Kumar Mishra; A. Kumar, and D.K. Jarwal under Visvesvaraya Ph.D. Scheme.

Author contributions

S.J. and A.K.M. have formulated the concepts and designed the experiments. B.N.M. has prepared the materials. D.K.J., A.K., A.K.M., and S.R. helped in characterizing the materials. A.K.M., M.R.T., and S.J. wrote the manuscript. All the authors discussed the manuscript.

Competing interests

The authors declare no competing interests.

Additional information

Supplementary information is available for this paper at <https://doi.org/10.1038/s41598-020-67986-4>.

Correspondence and requests for materials should be addressed to S.J.

Reprints and permissions information is available at www.nature.com/reprints.

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons license, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons license and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this license, visit <http://creativecommons.org/licenses/by/4.0/>.

© The Author(s) 2020