# SCIENTIFIC REPORTS

Received: 30 July 2018 Accepted: 11 January 2019 Published online: 28 February 2019

## **OPEN** Comparison Between Performances of In<sub>2</sub>O<sub>3</sub> and In<sub>2</sub>TiO<sub>5</sub>-Based EIS **Biosensors Using Post Plasma CF<sub>4</sub> Treatment Applied in Glucose and Urea Sensing**

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In this study, the effect of post-deposition tetrafluoromethane (CF4) plasma treatment on the physical and electrical characteristics of an In<sub>2</sub>TiO<sub>5</sub> based electrolyte-insulator-semiconductor (EIS) sensor was investigated. Post-deposition CF<sub>4</sub> plasma treatment typically improved the crystalline structure and repaired dangling bonds at the grain boundaries. We used the newly fabricated device to detect several ions, such as sodium and potassium, which are essential for many biological processes. The asdeposited and CF4 plasma treated In2TiO5 sensing window with an EIS structure was also able to detect the pH of a solution, different alkali ions (Na<sup>+</sup> and K<sup>+</sup>), glucose, and urea. The sensing membrane after a 60-sec CF<sub>4</sub> plasma treatment displayed improved biosensing characteristics, such as higher sensitivity (59.64 mV/pH), better drift rate, and a smaller hysteresis voltage of approximately 0.424 mV/h. The In<sub>2</sub>TiO<sub>5</sub> sensing membrane treated with CF<sub>4</sub> plasma is a promising material for use in EIS biosensing applications.

Over the last few decades, major advances have been made in the field of biosensors for the monitoring and control of many biochemical activities. Biosensors are extensively used for monitoring food and soil quality, as well as human biochemistry and other medical applications<sup>1</sup>. Ion-sensitive field-effect transistors (ISFETs) are considered excellent transducers for sensing biochemical reactions due to their small size, fast response, and reliability. Electrolyte-insulator-semiconductor (EIS) materials operate with the same working principle as ISFETs, but their fabrication process is relatively simple and inexpensive as compared to that of ISFETs<sup>2</sup>. The surface potential of the exposed insulator sensing area changes in response to the H<sup>+</sup> concentration of the solution<sup>3</sup>. Therefore, selecting a proper insulating material with suitable characteristics is important to achieve high sensitivity and long-term reliability of the device.

Several metal oxides like indium-gallium-zinc oxide (InGaZnO, IGZO), zinc oxide (ZnO), and indium tin oxide (InSnO, ITO) have been developed as sensor membranes owing to their excellent sensing characteristics<sup>4-6</sup>. Indium oxide  $(In_2O_3)$  thin films have attracted significant attention as a sensing membrane because of its higher mobility  $(160 \text{ cm}^2/(\text{V}\cdot\text{s}))^7$ , higher melting point (1910 °C), larger band gap  $(3.5-3.7 \text{ eV})^8$ , and insolubility in water. In<sub>2</sub>O<sub>3</sub> films can easily be reduced to create an oxygen deficiency, where insufficient oxygen atoms are contained in the crystal structure<sup>9</sup>. This results in the formation of a nonstoichiometric  $In_2O_{3-x}$  film with an increased number of defects. Thus, the main free carriers in  $In_2O_{3-x}$  are the internal oxygen vacancies of the film, which also affect the chemical stability of the film. As a potential solution,  $CF_4$  plasma treatment of the  $In_2O_3$  and  $In_2TiO_5$  film can enhance the In-O bonding. In<sub>2</sub>O<sub>3</sub> is widely used for gas sensing<sup>10</sup>, transparent conducting oxides<sup>11</sup>, and thin film transistors<sup>12</sup> because of its excellent material characteristics.

The performance of a biosensor is conferred by doping with a transition metal, such as titanium (Ti). Ti affects the sensing membrane through the passivation of the defects in the bulk to the sensing performance and

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#### Figure 1. Process flow for the fabrication of $In_2O_3$ and $In_2TiO_5$ EIS with $CF_4$ plasma treatment.



**Figure 2.** XRD spectra of the (**a**)  $In_2O_3$  and (**b**)  $In_2TiO_5$  membranes with  $CF_4$  plasma treatment for 15, 30, and 60 sec.



**Figure 3.** AFM of the surface of the (**a**) as-deposited In<sub>2</sub>O<sub>3</sub> sample ( $R_{rms} = 0.557 \text{ nm}$ ), (**b**) In<sub>2</sub>O<sub>3</sub> sample CF<sub>4</sub> plasma treated for 60 sec ( $R_{rms} = 1.77 \text{ nm}$ ), (**c**) as-deposited In<sub>2</sub>TiO<sub>5</sub> sample ( $R_{rms} = 0.628 \text{ nm}$ ), (**d**) In<sub>2</sub>TiO<sub>5</sub> sample CF<sub>4</sub> plasma treated for 60 sec ( $R_{rms} = 2.92 \text{ nm}$ ), and (**e**) AFM of the sensing membrane with CF<sub>4</sub> plasma treatment for various times.

production of dangling bonds at the oxide interface<sup>13,14</sup>. Ti internalization also enhances device capacitance and reduces the reactivity with the surrounding moisture<sup>15,16</sup>.

Recent evidence demonstrated  $CF_4$  plasma treatment that improves the sensing performance of oxide materials for biosensing applications<sup>17</sup>. Fluorine incorporation improves the dielectric properties of the material by fixing the dangling bonds and replacing the weak bonds at the grain boundaries<sup>18</sup>. Fluorine introduces a net negative surface charge owing to its high electronegativity and improves the ability to capture positively charged H<sup>+</sup> ions<sup>19</sup>. Moreover, pre- and post-deposition  $CF_4$  plasma treatment reduces metal-silicate formation at the oxide/ silicon (Si) interface<sup>20</sup>.

Here, we used a post-deposition  $CF_4$  plasma treatment on  $In_2O_3$  and  $In_2TiO_5$  thin films to improve their electrical and physical characteristics. We describe the consequence of the post-deposition  $CF_4$  plasma treatment on the sensing and physical characteristics of a deposited  $In_2TiO_5$  thin film as a sensing membrane. The detailed process flow of the EIS structure fabrication is shown in Fig. 1. After fabricating the device, sensing characteristics, including sensitivity, hysteresis, and drift of the device were measured. To determine the physical characteristics, X-ray diffraction (XRD) atomic force microscopy (AFM), and secondary ion mass spectroscopy (SIMS) analyses were done.

### **Results and Discussion**

**Physical characteristics.** XRD was used to probe the crystalline structure of the materials. Figure 2(a,b) depicts XRD patterns of as-deposited and post-deposition  $CF_4$  plasma treated  $In_2O_3$  and  $In_2TiO_5$  membranes, respectively. The diffraction angles (2 $\theta$ ) ranged from 20 to 60°. All the  $In_2O_3$  membrane samples displayed a cubic crystalline phase with two diffraction peaks, (222) and (321), at a diffraction angle of 30.5° and 33.10°, respectively<sup>21</sup>. A strong  $In_2O_3$  (321) peak was observed for the sample annealed at 60 sec.  $In_2TiO_5$  displayed a strong peak at (222) at a 2 $\theta$  of 30.5. The major phase changed from (321) to (222) in XRD pattern of  $In_2TiO_5$ . The intensities of these three peaks were enhanced by the  $CF_4$  plasma treatment and further increased by increasing







**Figure 5.** Normalized C-V curve of the sensing membrane of (**a**) as-deposited  $In_2O_3$  sample and (**b**)  $In_2O_3$  sample  $CF_4$  plasma treated for 60 sec, and (**c**) as-deposited  $In_2TiO_5$  sample and (**d**)  $In_2TiO_5$  sample  $CF_4$  plasma treated for 60 sec.

the plasma treatment time from 15 to 60 sec due to the improvement in the crystalline structure. The crystallinity improvement arises from the formation of a stronger fluorinated bond between indium and oxygen<sup>18</sup>. Therefore, after  $CF_4$  plasma treatment for 60 sec the  $In_2O_3$  and  $In_2TiO_5$  membranes would display higher intensity peaks than those prepared under other conditions. The XRD data indicated that internalization of Ti upgrades the thin film stoichiometry because it minimizes the number of dangling bonds on the dielectric surface and improves the temperature stability compared with  $In_2O_3$  thin film<sup>22,23</sup>.

AFM was used to study the surface morphology of the devices treated with post-deposition plasma. Figure 3(a-d) show two-dimensional (2D) AFM images of the as-deposited and post-deposition CF<sub>4</sub> plasma treated In<sub>2</sub>O<sub>3</sub> and In<sub>2</sub>TiO<sub>5</sub> samples. The AFM images of as-deposited In<sub>2</sub>O<sub>3</sub> and In<sub>2</sub>TiO<sub>5</sub> membranes revealed surface roughness of 0.557 nm and 0.628 nm, respectively. The roughness increased with In<sub>2</sub>O<sub>3</sub> and In<sub>2</sub>TiO<sub>5</sub> samples with increased CF<sub>4</sub> plasma treatment time from 15 to 60 sec, as shown in Fig. 3(e). Samples doped with Ti achieve better surface roughness compared to bare In<sub>2</sub>O<sub>3</sub>. Ti has a higher affinity toward oxygen, and thus provides a larger grain size. This produces a rougher surface<sup>23,24</sup>. CF<sub>4</sub> plasma treatment increases the interior grain size and causes plasma-induced morphological changes, which increase surface roughness and the number of surface sites, which in turn increase the sensitivity and linearity<sup>25</sup>.



**Figure 6.** (a,c) Hysteresis of  $In_2O_3$  and  $In_2TiO_5$  sensing membranes for the as-deposited and samples with  $CF_4$  plasma treatment of various times during the pH loop of  $7 \rightarrow 4 \rightarrow 7 \rightarrow 10 \rightarrow 7$  over a period of 30 min. (b,d) Drift rate of  $In_2O_3$  and  $In_2TiO_5$  sensing membranes for the as-deposited and samples with  $CF_4$  plasma treatment for various times in pH 7 buffer solution.

Secondary ion mass spectrometry analysis data of the  $In_2O_3$  and  $In_2TiO_5$  thin films with and without  $CF_4$  plasma treatment are shown in Fig. 4. The as-deposited sample displayed no trace of fluorine atoms. For all the samples with  $CF_4$  plasma treatment, fluorine atoms were evenly distributed throughout the entire oxide bulk areas. Fluorine content increased as the  $CF_4$  plasma treatment time increased from 15 to 60 sec. Ti-doped  $In_2O_3$  membranes have less excess etching of the sensing membrane. Fluorine incorporation reduces interfacial defect states at the oxide/silicon interface and increases the overall quality of the deposited oxide layer<sup>26</sup>.

**Sensing characterization.** The most important parameter of EIS structure is its flat-band voltage, which is defined as the voltage applied to produce a silicon surface potential of zero. The flat-band voltage of EIS is calculated as<sup>27</sup>:

$$V_{FB}=E_{ref}~-~\Phi^{Si}~-\Psi_0~-~Q_i/C_i~+~\chi^{Sol}~+~\delta_{\chi}$$

where  $E_{ref}$  is the reference electrode potential with respect to vacuum;  $\frac{1}{q}\Phi^{Si}$  is the work function of Si, which is equal to 4.7 V;  $\Psi_0$  is the potential drop in the electrolyte at the insulator-electrolyte interface;  $C_i$  and  $Q_i$  are the insulator capacitance and effective charge per unit area, respectively,  $\chi^{Sol}$  is the surface dipole potential of the solvent; and  $\delta_{\chi}$  is the number of variations of  $\chi$  potentials. The surface potential  $\Psi_0$  changes by changing the pH of the solutions, which causes a change in flat-band voltage at the different pHs. The surface potential  $\Psi_0$  is calculated as<sup>25,28</sup>:

$$\Psi_0 = 2.3 \frac{kT}{q} (\text{pHpzc} - \text{pH}) \frac{\beta}{\beta + 1}$$

where  $pH_{pzc}$  is the value of pH for which the oxide surface is electrically neutral and  $\beta$  is the parameter that depends on the sensitivity of the sensing surface. The site-binding model can also be explained using the equation for capacitance, Q = CV, where Q is the surface charge, C is the double layer capacitance at the insulator interface, and V is the surface potential ( $\Psi_0$ ). The surface potential can be expressed as:

$$\Delta \Psi_0 = -2.3 \alpha \frac{kT}{q} \Delta p H_{\text{bull}}$$



**Figure 7.**  $H^+$ ,  $Na^+$ , and  $K^+$  sensing properties of as-deposited  $In_2O_3$  and  $In_2TiO_5$  membrane ((**a**,**c**) respectively) and  $In_2O_3$  and  $In_2TiO_5$  membrane ((**b**,**d**), respectively) treated with  $CF_4$  plasma for 60 sec.

where  $\alpha$  is the dimension-less sensitivity parameter consisting of the differential double layer capacitance. The ability of the oxide surface to protonate and deprotonate can be represented by the symbol  $\beta$ .

Figure 5(a-d) represent the capacitance versus substrate bias (C-V) curves of the In<sub>2</sub>O<sub>3</sub> and In<sub>2</sub>TiO<sub>5</sub> sensing membranes with and without CF<sub>4</sub> plasma treatment. The inset of the figures shows the pH sensing properties of the films extracted from the C-V curves. The as-deposited In<sub>2</sub>O<sub>3</sub> sample displayed a very low sensitivity of 21.67 mV/pH and linearity of 91.66%. The  $In_2O_3$  sample treated with  $CF_4$  plasma for 15 sec displayed higher sensitivity and linearity of 47.03 mV/pH and 98.76%, respectively. The sensitivity and linearity increased to 52.43 mV/pH and 98.83% for samples treated for 30 sec. When samples were treated for 60 sec, the sensitivity and linearity further increased to 56.15 mV/pH and 98.18%, respectively. The as-deposited  $\text{In}_2\text{TiO}_5$  sample displayed a decent sensitivity of 36.34 mV/pH and linearity of 97.65%. For CF<sub>4</sub> plasma treatments of 15 and 30 sec, the sensitivity and linearity increased to 49.98 mV/pH and 94.23% at 15 sec, respectively, and 55.06 mV/pH and 99.67% at 30 sec, respectively. With a 60-sec CF<sub>4</sub> plasma treatment, In<sub>2</sub>TiO<sub>5</sub> samples displayed highest sensitivity and linearity values of 59.64 mV/pH and 99.68%, respectively. The CF<sub>4</sub> plasma treatment increased the overall sensing surface area by increasing the surface roughness. Thus, the larger sensing surface area will lead to higher sensitivity with more surface sites being present and capable of binding ions present in the electrolyte solution<sup>18</sup>. Therefore, pH sensing membrane treated with  $CF_4$  plasma for 60 sec can possess high sensitivity and excellent linearity. These properties can be attributed to the formation of a greater number of fluorinated bonds (F-In bonds) on the In<sub>2</sub>O<sub>3</sub> and  $In_2 TiO_5$  film surface due to CF<sub>4</sub> plasma treatment. The deviation in surface potential of the sensing surface after the surface is dipped into solutions with different pH values was determined by the C-V shift. H<sup>+</sup> and OH-attachment at the corresponding binding sites at the sensing surface can alter the surface potential<sup>29</sup>. The present results demonstrate that Ti doping increases the numbers of binding sites on the sensing surface. The grain size becomes larger with higher surface roughness due to incorporation of Ti. Correspondingly the number of binding sites increases with the larger surface area<sup>23</sup>. Therefore, the sensitivity and linearity of  $In_2 TiO_5$  membranes that are plasma-treated for 60 sec is much higher than those aspects of In<sub>2</sub>O<sub>3</sub> membranes.

To investigate the hysteresis effects of the membrane, the samples were immersed in buffer solutions with different pH values in an alternating cycle (pH 7  $\rightarrow$  4  $\rightarrow$  7  $\rightarrow$  10  $\rightarrow$  7). Moreover, to test the long-term reliability of the devices, the drift effect of the In<sub>2</sub>O<sub>3</sub> with CF<sub>4</sub> plasma treated sensing membrane was measured by a C-V curve in a pH 7 buffer solution for 12 h. The hysteresis voltage and drift rate under the different CF<sub>4</sub> plasma treatment conditions reveal that the 60-sec In<sub>2</sub>O<sub>3</sub> film plasma treatment produced the lowest hysteresis voltage and lowest drift rate (4.33 mV and 0.95 mV/h, respectively (Fig. 6(a–d)). In<sub>2</sub>TiO<sub>5</sub> CF<sub>4</sub> plasma-treated sensing membrane displayed a hysteresis voltage 25.75, 9.32, 6.85 and 2.72 mV in the as-deposited condition and following 15, 30, and 60 sec of annealing, respectively. Figure 6(d) shows the drift rate for In<sub>2</sub>TiO<sub>5</sub> devices with CF<sub>4</sub> plasma treatment. The drift rate of the as-deposited sample was 9.23 mV/h, whereas drift rates of 4.92, 1.09, and 0.42 mV/h were



**Figure 8.** Glucose sensing properties of (**a**) as-deposited  $In_2TiO_5$  membrane and (**b**) membrane treated with  $CF_4$  plasma for 60 sec.

obtained following annealing for 15, 30, and 60 sec, respectively. This was likely because fluorine compensated for the dangling bonds and replaced weaker bonds in the grain boundaries. Thus, the  $CF_4$  plasma treatment can reduce the trap states in the oxide/silicon interface and improve the hysteresis and drift rate characteristics of the films<sup>18</sup>. The dangling bonds are negated by Ti ions and the defects located underneath of the dielectric surface are compensated<sup>16,23</sup>.

To analyse the sensing performance of our sensing membrane in the presence of potassium and sodium, we prepared a solution using a micropipette to control the concentrations of sodium and potassium ions ranging between  $10^{-5}$  and  $10^{-1}$  M by injecting 1 M NaCl/Tris-HCl and 1 M KCl/Tris-HCl into buffer electrolyte. Comparisons of H<sup>+</sup>, Na<sup>+</sup>, and K<sup>+</sup> sensing performances of the as-deposited In<sub>2</sub>O<sub>3</sub> and In<sub>2</sub>TiO<sub>5</sub> membrane, and the membrane treated with CF<sub>4</sub> plasma for 60 sec are presented in Fig. 7(a–d). In<sub>2</sub>TiO<sub>5</sub> sample treated with CF<sub>4</sub> plasma for 60 sec are presented in Fig. 7(a–d). In<sub>2</sub>TiO<sub>5</sub> sample treated with CF<sub>4</sub> plasma for 60 sec CF<sub>4</sub> plasma treated In<sub>2</sub>O<sub>3</sub> sample (13.77 mV/pNa and 12.78 mV/pK). For sodium and potassium sensing, considerably lower sensitivity was obtained compared to H<sup>+</sup> sensing. This can be explained by the heavier and larger Na<sup>+</sup> and K<sup>+</sup> ions compared to H<sup>+</sup> ions.

We also measured the essential human biochemistry data of glucose and urea. They were detected by incorporating appropriate enzymes on the sensing oxide surface. The chemical equations for the reactions that can be used for glucose detection are<sup>30,31</sup>:

$$\beta - D - Glucose + O_2 + H_2O \xrightarrow{glu \cos eoxidase} D - glucose - \delta - lactone + H_2O_2$$

 $D - glucose - \delta - lactone \rightarrow D - gluconoate + H^+$ 

The chemical equation for the reactions that can be used for urea detection is<sup>30,31</sup>:

$$\rm NH_2CONH_2 + 3H_20 \xrightarrow{urease} 2\rm NH_4^+ + OH^- + HCO_3^-$$

The glucose sensing properties of the  $In_2TiO_5$  sensing membrane on the EIS structure with and without the 60-sec  $CF_4$  plasma treatment are presented in Fig. 8(a,b). The glucose concentration was controlled over the range of 2 to 7 mM. The as-deposited  $In_2TiO_5$  sensing membrane exhibited a low glucose sensitivity of 2.85 mV/mM and linearity of 85.23%. After Ti doping and 60-sec  $CF_4$  plasma treatment, the sensitivity increased to 6.63 mV/mM and the linearity increased to 92.35%.



**Figure 9.** Urea sensing properties of (a) as-deposited  $In_2 TiO_5$  membrane and (b) membrane treated with  $CF_4$  plasma for 60 sec.

Sensing membrane	pH sensitivity (mV/pH)	Hysteresis voltage (mV)	Drift rate (mV/h)	Glucose	Urea	References
TbY <sub>x</sub> O <sub>y</sub>	59.79	5.00	0.26	4.81	—	33
CeO <sub>2</sub>	57.60	8.43	1.21	4.74	2.49	34
ZnO	42.54	7.37	1.78	3.14	1.81	35
Sm <sub>2</sub> O <sub>3</sub>	56.20	6.20	1.29		2.45	36
Ti-ZnO	57.56	2.79	0.29	6.42	1.4~3.62	37
CeO with						
CF <sub>4</sub> plasma	53.38	—	—	5.83	2.30	38
$\begin{array}{c} {\rm In_2TiO_5with} \\ {\rm CF_4plasma} \end{array}$	59.64	2.72	0.42	6.63	2.69	_

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 Table 1. Comparative data of the obtained sensing parameters of drift rate, pH sensitivity, hysteresis voltage, glucose, and urea sensing for different EIS devices.

The urea concentration was controlled in a range between 5 and 40 mM (Fig. 9(a,b)). The sensitivity values of the  $In_2TiO_5$  sensing membrane above as-deposited and  $CF_4$  plasma treatment in samples treated for 60 sec were 1.55 and 2.69 mV/mM, respectively. Therefore, the 60-sec  $CF_4$  plasma treated  $In_2TiO_5$  sensing membrane has better sensitivity and linearity for the detection of urea. These results indicate that the  $CF_4$  plasma treatment can increase the interior grain size and increase the number of surface sites, resulting in better sensing performance for the detection of H<sup>+</sup>, Na<sup>+</sup>, K<sup>+</sup>, glucose, and urea.

The test sample of commercially available glucose devices, such as the ACCU-CHECK glucometer, uses a precious metal (Ag/AgCl)<sup>32</sup>. In this study, we used In and Ti as the sensing film. Their use can reduce the purchase price and enable reuse of material. These advantages also include a sensing membrane with high glucose sensitivity and the capability to accurately and sensitively measure other molecules.

Table 1 provides comparative data of the sensing parameters of drift rate, pH sensitivity, hysteresis voltage, glucose, and urea sensing for different EIS devices with TbY<sub>x</sub>O<sub>y</sub><sup>33</sup>, CeO<sub>2</sub><sup>34</sup>, ZnO<sup>35</sup>, Sm<sub>2</sub>O<sub>3</sub><sup>36</sup>, Ti-doped ZnO<sup>37</sup>, and CeO with CF<sub>4</sub> plasma treatment<sup>38</sup>. The pH sensitivity, hysteresis, drift rate, glucose and urea sensing of the EIS device prepared with In<sub>2</sub>TiO<sub>5</sub> and incorporating a CF<sub>4</sub> plasma sensing membrane was superior. CF<sub>4</sub> incorporated into In<sub>2</sub>TiO<sub>5</sub> film can enhance the In-O bonding at the In<sub>2</sub>TiO<sub>5</sub> sensing membrane, which improves the sensing characteristics.

#### Conclusion

A CF<sub>4</sub> plasma treated In<sub>2</sub>TiO<sub>5</sub>-based EIS sensor was fabricated for H<sup>+</sup>, Na<sup>+</sup>, K<sup>+</sup>, and glucose sensing applications. The effect of the post-deposition CF<sub>4</sub> plasma treatment on the physical and electrical characteristics of the sensors was studied. The In<sub>2</sub>TiO<sub>5</sub> EIS sensor with a 60-sec post-deposition plasma treatment exhibited good sensitivity of 59.64 mV/pH and linearity of 99.68%. Post-deposition CF<sub>4</sub> plasma treatment improves the crystalline structure and repairs the dangling bonds at the grain boundaries. Furthermore, the 60-sec plasma treatment produced the best material and electrical properties, and achieved ideal sensing capabilities, likely due to defect passivation by fluorine. Furthermore, the Ti-doped In<sub>2</sub>O<sub>3</sub>-based EIS sensor treated with CF<sub>4</sub> plasma treatment also had better sensitivity and linearity than the as-deposited sample for glucose and urea detection.

#### Methods

The EIS incorporated  $In_2O_3$  and  $In_2TiO_5$  sensing membranes were fabricated on 4-inch n-type (100) silicon wafers with a resistivity of 5–10  $\Omega$ -cm. After a standard RCA cleaning process, the samples were dipped into a 1% hydrofluoric acid solution to remove native oxide from the surface. A 50 nm-thick SiO<sub>2</sub> substrate was thermally oxidized on the silicon wafer. Then, (a) a 50 nm-thick  $In_2O_3$  film was deposited on the SiO<sub>2</sub>/Si substrate by reactive radio frequency sputtering. (b) Both  $In_2O_3$  and Ti were used to co-sputter  $In_2TiO_5$  film on SiO<sub>2</sub>/Si stacks in a diluted argon flow (Ar/O<sub>2</sub> = 20 sccm/5 sccm) with a radio frequency power and process pressure of 100 W and 20 mTorr, respectively. After deposition, the  $In_2O_3$  and the  $In_2TiO_5$  films were subjected to a post-deposition CF<sub>4</sub> plasma treatment in a plasma-enhanced chemical vapor deposition system with a radio frequency power of 30 W and a pressure of 500 mTorr for 15, 30, and 60 sec. The back-contact was made by depositing a 300 nm-thick aluminium film on the back side of the Si wafer. The sensing area of the deposited  $In_2O_3$  films was defined by an automatic robot dispenser with an adhesive silicone gel to build the final EIS structure on the printed circuit board using a silver gel to form conductive lines. An epoxy package was used to separate the EIS structure and the copper line. The detailed process flow of the EIS structure fabrication is shown in Fig. 1.

Morphological analyses of the  $In_2O_3$  and  $In_2TiO_5$  sensing membranes included XRD, AFM, and SIMS. These analyses were done to investigate the link between structural and electrical characteristics properties. SIMS instruments use an internally yielded beam of either positive or negative ions focused on a sample surface to generate secondary ions. The generated ions are then transferred into a mass spectrometer across a high electrostatic potential. The depth profiling of elemental and molecular species, as well as isotopic ratios of compounds was evaluated by SIMS analysis. The surface morphologies of the  $In_2O_3$  and  $In_2TiO_5$  nano-layers were observed using AFM in Bruker Dimension Icon modes with intermittent contact using a silicon tip with a 10 pN/nm spring constant. A sample area of  $3 \times 3 \mu m$  was scanned with actuation rates up to 8 kHz in air and fluid. For XRD analysis of the samples, grazing incidence of X-ray beam CuKa (k = 1.542 Å) radiation was used with an incidence angle step of  $0.5^{\circ}$  in the diffraction angle range (2 $\theta$ ) from 20° to 60°.

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#### Acknowledgements

This work was supported by the Ministry of Science and Technology under the contract of MOST 107–2221-E-182-036-. This work was supported by the Chang Gung University under contract CMRPD2H0181.

#### **Author Contributions**

Chun-Fu Lin, Chyuan-Haur Kao, and Chan-Yu Lin, designed the research. Chun-Fu Lin and Chia Shao Liu graphed the device structure. Chun-Fu Lin and Yi Wen Liu devised the crystal growth method, and grew and characterized the materials. Chun-Fu Lin, Chyuan-Haur Kao, and Chan-Yu Lin analysed the data and wrote the paper.

#### **Additional Information**

Competing Interests: The authors declare no competing interests.

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