

## REVIEW ARTICLE OPEN



# Recent progress in the effect of magnetic iron oxide nanoparticles on cells and extracellular vesicles

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At present, iron oxide nanoparticles (IONPs) are widely used in the biomedical field. They have unique advantages in targeted drug delivery, imaging and disease treatment. However, there are many things to pay attention to. In this paper, we reviewed the fate of IONPs in different cells and the influence on the production, separation, delivery and treatment of extracellular vesicles. It aims to provide cutting-edge knowledge related to iron oxide nanoparticles. Only by ensuring the safety and effectiveness of IONPs can their application in biomedical research and clinic be further improved.

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## FACTS

- What is the fate of IONPs after they enter the cell.
- What is the effect of IONPs after they enter the extracellular vesicles.
- Improve the security and effectiveness of IONPs.

## INTRODUCTION

Iron oxide nanoparticles (IONPs) are approved by FDA and are widely used in biomedical research and clinical applications, including magnetic resonance imaging, drug delivery and disease treatment [1–7].  $\gamma\text{-Fe}_2\text{O}_3$  and  $\text{Fe}_3\text{O}_4$  nanoparticles have the advantages of biocompatibility and biodegradability [8]. They can be used to label cells and extracellular vesicles (EVs) and track and visualize them through magnetic resonance imaging (MRI) to ensure that they can reach the target site in the body and remain in the tissue, while monitoring the migration and differentiation process of stem cells in the body [9, 10]. However, the level of cytotoxicity induced by IONPs depends on the size, concentration, surface charge, coating type and functional groups of IONPs [11–13]. The uptake of IONPs by cells has an impact on cells and EVs. These effects are both positive and negative. We need to be more vigilant in identifying and responding to risks so that we can make full use of these benefits. Therefore, it is necessary to review and summarize the existing research in order to make better use of the magnetic EVs delivery system.

In the first part of this review, we describe the fate of IONPs after endocytosis in cells. The effects of IONPs on stem cells, macrophages and tumor cells were introduced in detail. The second part focuses on the key role of IONPs in the generation, separation and treatment of EVs, which can stimulate or enhance the secretion of cells to EV. The role of IONPs in the treatment mechanism of EV is of particular interest in nanomedicine. This

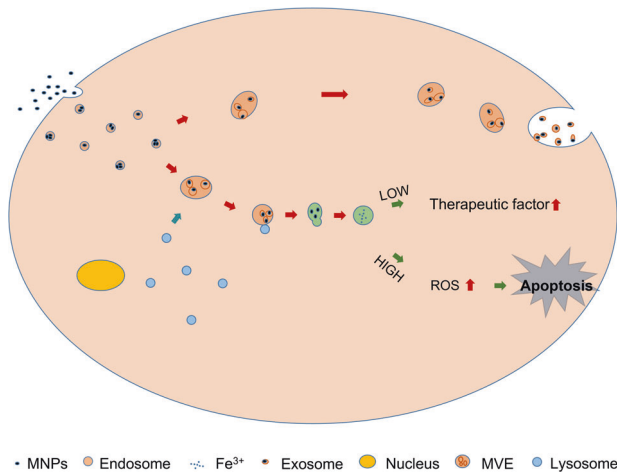
review will help deepen the understanding of how IONPs affect cells and EVs, enable readers to fully understand the application of magnetic nanomaterials in nanomedicine research, and further promote the development of natural therapeutic and diagnostic nanoplatforms.

## FATE OF IONPS IN CELLS

In vitro culture system, IONPs will be ingested by cells when incubated with cells, as shown in Fig. 1. At the same time, the application of IONPs in the complex blood flow system will also result in the initial uptake of the liver and spleen. In addition, regarding IONPs uptake by cells, researchers found that IONPs uptake was mediated by endocytosis, similar to giant cell drinking [14], after conducting subcellular analysis. The uptake of smaller IONPs is mainly mediated by clathrin- [15] and fossa-mediated endocytosis, while the uptake of larger IONPs and aggregates is mainly mediated by macrocytosis and phagocytosis [12]. In addition, the coating properties of IONPs and cell types determine the internalization mechanism of IONPs [16, 17]. After absorption, IONPs enter the inner lysosome pathway through large cytoplasmic organelles and reach the final destination of multi-layer lysosomes. The confocal microscope showed that the particles were almost completely located in the lysosome compartment after 24 h of co-culture [18]. Exposure to IONPs increases the number, permeability and alkalinity of lysosomes [19]. At the same time, the lysosomal metabolism of superparamagnetic iron oxide nanoparticles (SPION) in cells has been confirmed [20, 21]. SPIONs can be degraded by enzymes in lysosome (pH~4.5) [22, 23], thus releasing free iron in IONPs and affecting iron homeostasis. At the same time, free iron is stored in the form of protein, such as ferritin and hemosiderin, for further use by the host. The biocompatibility of IONPs is attributed to effective cellular iron metabolism, allowing iron circulation and excessive iron exocytosis [24, 25]. In addition, the cytotoxicity of SPIONs to cells largely depends on

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**Fig. 1** Fate of MNPs in cells.

their size [26, 27], shape, surface coating [17, 28, 29], dose of exposed cells [30], exposure time [31] and type [32–34]. When the exposure concentration of nano-magnetite particles is greater than 50  $\mu\text{g}/\text{ml}$ , it will produce greater cytotoxicity in the form of reduced activity, and increase ROS, reduce cell membrane potential and reduce the rate of cell apoptosis [30]. Therefore, as long as the specific parameters of IONPs are controlled, they will not have adverse effects on cell viability, metabolic activity, oxidative stress, proliferation and differentiation [9, 35, 36].

However, iron overload can trigger the generation of reactive oxygen species (ROS) [32, 37]. The main reason for the cytotoxicity of IONPs is the excessive production of ROS. ROS can cause oxidative stress in cells by activating pro-inflammatory mediators, and eventually lead to cell necrosis or apoptosis [38]. Therefore, autophagy induced by IONPs can affect cell metabolism, cytotoxicity, therapeutic effect [39], and even host immune system [40–42].

### Fate of IONPs in stem cells

The therapy based on mesenchymal stem cells (MSCs) has become a promising therapeutic strategy for tissue regeneration and repair. SPION nanoparticles can help stem cells transplant and regenerate in vivo. However, the effect of SPION labeling on the proliferation and differentiation of stem cells is still uncertain. SPION concentration for stem cell labeling is not high (<50  $\mu\text{g}/\text{ml}$ ), does not cause cytotoxicity. For example, the optimal MRI cell tracking dose (about 10  $\text{pg Fe}/\text{cell}$ ) [43]. However, SPION markers have more or less affected several cellular events of mesenchymal stem cells [44–46]. Researchers have found that SPION not only marks cells, but also regulates the differentiation, activity and treatment of stem cells.

### Migrate

After uptake by cells, IONPs are degraded by the nuclear body to release iron ions and further regulate the molecular expression in MSC. CXCR4 and SDF-1 are important factors to induce the homing of MSCs. In order to improve the effectiveness of MSC homing, the internalized SPION in MSC induces the new biological functional characteristics of MSC homing by adding CXCR4 [47–50]. Huang et al. [49] increased CXCR4 expression in MSC and enhanced CXCR4-SDF-1 $\alpha$  axis through  $\text{Zn}_{0.4}\text{Fe}_{2.6}\text{O}_4$ , it is the first time to prove that iron-based can actively increase the expression of chemokine receptor CXCR4 in bone marrow derived MSCs without gene modification, and improve the homing of MSCs to injury sites and tumors. Li et al. [48] also found that  $\text{Fe}_3\text{O}_4@\text{PDA}$  The incorporation of NPs into MSCs up-regulates the expression level of C-X-C chemokine receptor type 4 (CXCR4) to

enhance the migration of MSCs to the site of laser burn injury. In addition, the labeled MSC group showed increased cytokines and decreased pro-inflammatory factors. They also increased the expression of healing-related genes. It is known that SPION can induce reactive oxygen species (ROS), while ROS can increase CXCR4 expression in bone marrow derived MSCs [51]. The magnetic retention of SPION-labeled MSCs increases the migration and homing efficiency of MSCs with SPION nanoparticles in olfactory bulb injured mice [50]. Schulze et al. [52] found that A-PVA-SPIONS accumulated in bone marrow and increased the metabolic activity and migration rate of BMSCs. After Frank et al. [53] labeled with A-PVA-SPION, the migration of MSCs increased.

### Differentiation

The bovine serum albumin ( $\text{Fe}_3\text{O}_4/\text{BSA}$ ) particles of iron oxide nanoparticles significantly promoted the bone formation of mesenchymal stem cells under the action of external magnetic field, while the magnetic particles and external magnetic field alone did not affect the differentiation of stem cells [54]. With the increase of SPION incorporation, cartilage formation, differentiation and chemotaxis are significantly impaired [55]. The damage of cartilage formation may be caused by high intracellular iron load [44, 56]. Ferucarbotran has no toxicity to human mesenchymal stem cells (hMSCs). However, Ferucarbotran causes dose-dependent inhibition of osteogenic differentiation of human mesenchymal stem cells, cancels osteogenic differentiation at high concentrations, promotes cell migration, and activates signal molecules  $\beta$ -Catenin, cancer/testicular antigen, SSX and matrix metalloproteinase 2 (MMP2) [21]. It can also stimulate the proliferation of human mesenchymal stem cells (hMSCs) in the form of particles and ions (free iron, Fe) by reducing intracellular  $\text{H}_2\text{O}_2$ , and can affect the expression of cyclin regulators [46].

### Therapy

Connexin 43 (Cx43) induces intercellular coupling between adjacent cells. The formation of gap junction channels containing Cx43 triggered by ionizing IONPs is enhanced. In the treatment of myocardial infarction, IONPs significantly increased the expression of Cx43 in cardiomyocytes (H9C2) [57]. At the same time, IONPs can enhance the selective transfer of intercellular mitochondria from human mesenchymal stem cells (hMSCs) to diseased cells, significantly reducing the process of fibrosis [58]. In addition, SPIONS induce MSCs to secrete angiogenesis, anti-apoptosis and anti-inflammatory factors, such as angiopoietin-1 (Ang-1) and transforming growth factor- $\beta$ 1 (TGF- $\beta$ 1) And vascular endothelial growth factor (VEGF) [47, 48, 59–61]. Therefore, this strengthens the regeneration and repair ability of MSCs.

### Fate of IONPs in macrophage

There is still limited research on the effects of magnetic iron oxide nanoparticles on immune cells. Current studies have found that IOPs activate many biological processes of macrophages, including many immune reactions, endoplasmic reticulum (ER) stress and oxidative stress. SPION processes macrophages to produce reactive oxygen species [62], activates extracellular signal-regulated kinase and AKT pathway [63], JNK signal pathway [18], and promotes the production of IL-10. In addition, IL-1 $\beta$  of bone marrow-derived macrophages (BMMs) in mice was induced in a size-dependent and dose-dependent manner Release [27]. IONPs also induce BMMs to produce IL-6 and tumor necrosis factor  $\alpha$  (TNF- $\alpha$ ) [64]. Iron in SPION induces THP1-derived M2 macrophages to high CD86<sup>+</sup> and high TNF  $\alpha$ <sup>+</sup> Macrophage subtype transformation [65].  $\text{Fe}_3\text{O}_4$  nanoparticles can reduce the activity of macrophages and induce the polarization of macrophages to M1 phenotype after 48 h of treatment [66]. In addition,  $\text{Fe}_3\text{O}_4$  nanoparticles induce iron death in macrophages. P53 may contribute to iron death of macrophages induced by  $\text{Fe}_3\text{O}_4$  nanoparticles. It provides a theoretical basis for the molecular

mechanism of iron death of macrophages and Fe-induced biological toxicity *in vivo*.

### The fate of IONPs in cancer cells

Iron death is an iron-dependent cell death caused by excessive oxidation of polyunsaturated fatty acids. It can be activated by iron-based nanoparticles for cancer treatment. Fe<sub>3</sub>O<sub>4</sub> magnetic nanoparticles are more sensitive to weak acids. When entering cancer cells, it can release abundant Fe (II) ions to participate in Fenton reaction in combination with acidic tumor microenvironment and internal body conditions, and then catalyze H<sub>2</sub>O<sub>2</sub> to become highly toxic OH•, which will increase cell oxidative stress, damage mitochondria and cell membrane and induce tumor cell iron death [67], induce autophagy [68, 69], apoptosis and necrosis [70]. However, it is usually difficult to produce enough •OH, which is limited by intracellular H<sub>2</sub>O<sub>2</sub> concentration to induce iron death of cancer cells [71]. In order to achieve sufficient anti-tumor effect. It is reported that the intracellular cascade reaction can increase the concentration of H<sub>2</sub>O<sub>2</sub> in cells, thus improving the high-level production of •OH through the joint transport of metal catalysts and H<sub>2</sub>O<sub>2</sub> producers [72, 73]. Cisplatin can indirectly produce H<sub>2</sub>O<sub>2</sub> to further accelerate Fenton reaction. It can induce intracellular cascade reaction to produce enough •OH for iron death treatment [74]. In addition, the liposome is embedded with PEG-coated The liposome bilayer of γ-Fe<sub>2</sub>O<sub>3</sub> nanoparticles improves the permeability of H<sub>2</sub>O<sub>2</sub> and •OH [75], resulting in the effective activation of lipid peroxidation [76]. Moreover, 808 nm laser irradiation heat-induced Fe<sub>3</sub>O<sub>4</sub> *in situ* burst release produces effective reactive oxygen species through Fenton reaction in tumor microenvironment [77].

The cytotoxicity of superparamagnetic particles depends on the size, concentration, particle shape and coating type [78]. With the increase of particle concentration within the range of cytotoxicity [79]. With the increase of the number of IONPs, the released iron level will increase, which will catalyze the formation of oxidative free radicals, leading to cell death. Before reaching the high exposure level, although there is no obvious cytotoxicity, it has an impact on cells. For example, Watanabe et al. [80] found that lower concentrations would increase the production of reactive oxygen species, increase oxidative damage to DNA [22], and reduce the level of reduced glutathione. MgNPs-Fe<sub>3</sub>O<sub>4</sub> only at high concentration (100 μg/mL), the release of lactate dehydrogenase (LDH) was used to evaluate the cell membrane damage [80]. In addition, with the deepening of research, Fe ions generate a lot of toxic ROS. It also promoted the down-regulation of GPX4 [81] and xCT [82], and lipid peroxide began to accumulate. Apoptosis of caspase-8 activated cells after short time exposure to AC magnetic field [36]. Zhou et al. [83] showed that gold-plated iron oxide particles(Fe<sub>3</sub>O<sub>4</sub>@Au SPs) can induce non-cytotoxicity and gene expression in tumor cells, which are mainly involved in cell proliferation, differentiation and apoptosis. At clinically relevant doses, ferumoxytol has no direct cytotoxic effect on cancer cells. Adenocarcinoma cells incubated with ferumoxytol and macrophages showed increased caspase-3 activity. Zanganeh et al. [39] found that ferumoxytol caused tumor growth inhibition through indirect influence on tumor microenvironment.

At present, the joint action of SPION and external magnetic field has a far-reaching impact in many fields of nanotechnology. It can not only achieve long-distance and accurate targeted delivery, but also transform energy into force or heat for disinfection and sterilization tumor cells under the action of alternating magnetic field [84, 85]. Because SPION retained in lysosomal compartment can cause lysosomal membrane permeability (LMP) in cancer cells to cause mechanical destruction of lysosomes through high intensity dynamic magnetic field [86]. The contents of apoptotic lysozyme infiltrated into the cytoplasm and the intracellular pH value decreased [87]. Among them, lysosomal pathway with cathepsin-B activity simultaneously mediates tumor cell death [88]. In addition, the external alternating magnetic field can also

cause the Neil relaxation loss of magnetic nanoparticles to generate heat. This causes the temperature in the tumor tissue to rise to more than 43 °C, causing cancer cell necrosis [89]. To sum up, this opens up new opportunities for cancer treatment.

### EFFECT OF IONPS ON EVS

EVs are small vesicles secreted by various cells. They can carry a variety of signal biomolecules, including protein, mRNA and microRNA. In the past decade, EVs derived from stem cells have become promising tools for information transmission, treatment and marker detection in medical research. EVs are produced by budding from the inner chamber or plasma membrane and are composed of exosomes (50–150 nm) and microvesicles. In particular, the study of exosomes has attracted more and more attention in the fields of cancer and tissue regeneration due to their unique biological characteristics. However, the low separation rate and insufficient targeting ability limit their therapeutic applicability. In order to understand the regeneration mechanism caused by stem cell-derived EVs, researchers introduced magnetic particles. SPION with magnetic navigation can enhance the aiming ability of EVs.

### Effect of IONPs on EVs generation

EVs are produced or released spontaneously in response to biological, chemical or physical triggers during cell culture [90]. Therefore, cells can release magnetic vesicles when they are co-incubated with IONPs [91]. Magnetic labeling of extracellular vesicles derived from stem cells for MRI imaging [92]. The experiment shows that Fe<sub>3</sub>O<sub>4</sub> magnetic nanoparticles with a certain dose and exposure times can enhance cell proliferation when co-incubated with cells [12, 34]. In addition, the cells treated with IONPs show high activity, and the nanoparticles may stimulate the biogenesis of EVs. However, this situation is different in different cell types. In an experiment to study the transmission of magnetic EVs to the mouse brain, Kutchy et al. [93] It was found that USPIO had no significant effect on the release of astrocytes and EVs. The reason and potential mechanism for the increase of EVs particle concentration are still unclear. However, the mRNA expression of some vesicle-associated transporters has changed [12]. In conclusion, the uptake of IONPs by cells can enhance the secretion of EVs. This can improve the problem of low secretion productivity.

The labeled cells will lose magnetic nanoparticles when pressed, resulting in a decrease in the magnetic properties of the donor cells. In addition, microvesicles are released and transferred to other cells of the host organism through the mechanism of cross-transfer between cells [18]. Therefore, after internalization by monocytes or macrophages, magnetic nanoparticles can be released by cells in the form of vesicles under pressure or activation [94]. These vesicles are absorbed by immature macrophages and trigger magnetic labeled intercellular transfer. During the differentiation of magnetically labeled monocytes into macrophages, they also lead to the redistribution of magnetic markers. Silver et al. [95] also found that the microvesicles shed by stress cells were involved in the redistribution of magnetic labeled immature cells. They were detected by MRI.

### Effect of IONPs on EVs separation

The study of exosomes is of great significance to the diagnosis and prognosis of cancer and has potential in the medical field. The noninvasive separation of exosomes is a crucial step because their concentration in complex body fluids is extremely low and their volume is small [96]. Therefore, it is very important to obtain a good recovery rate and maintain the physical properties for the diagnosis and treatment of cancer [97]. The introduction of magnetic nanoparticles can improve the delivery efficiency of exosomes, thereby improving the therapeutic effect and reducing side effects. At the same time, it can provide a new method for rapid, efficient and high purity exosome separation in cell culture

supernatants or complex biological fluids. EVs were isolated and captured from different clinical samples using an external magnetic field, maintaining their biological integrity and further facilitating the application of exosomes in the required fields.

At present, the methods used to separate EVs include ultracentrifugation (UC), electroporation, magnetoacoustic perforation, magnetic sorting and immunoaffinity capture. However, the integrity of EVs can be damaged if magnetic particles are loaded by electroporation and ultrasound. This direct loading method can be considered if the EVs are only used to transport drugs. There is no special requirement for EV-specific endogenous substances. Another top-down method is to produce magnetic EVs by simultaneously incubating cells and magnetic nanoparticles. EVs are separated through UC. However, ultrahigh-speed centrifugal force may cause EV fragmentation, cargo leakage and protein sedimentation. Therefore, to avoid damage to EVs, magnetic separation can be used [90, 98]. This method involves absorption by a magnet, which is relatively mild. Guo et al. [99] prepared exosome mimics (EM) directly by magnetic extrusion after the cells engulfed the magnetic particles. EM has the same biological origin, composition, biological functions and similar morphology as natural exosomes. The main advantage of the magnetic extrusion method is the ability to harvest a large number of therapeutic vesicles. In addition, immune affinity capture can be selected. EVs carry various biomarkers. The magnetic nanoparticles are modified to form immunoaffinity magnetic nanoparticles [100–103]. Then, the exosome markers (CD63, CD9 and CD81) [104] can be recognized and combined, effectively separated and released with high efficiency [105–108].

For example, Brambilla et al. [97] immobilized DNA based on an anti-CD63 antibody and released EVs by using the endonuclease activity of DNase I. Zhang et al. [109] rapidly separated microvesicles from the supernatant of cells by streptomycin-modified iron oxide nanoparticles (SA-IONPs). In addition, blood is one of the most commonly collected biological fluids [108]. For example, María et al. [110] successfully used an exosome-binding antibody (anti-CD9) to functionalize magnetic nanoparticles to capture exosomes from the whole blood of pancreatic cancer patients. Cai et al. [96] successfully functionalized IONPs with exosome-binding antibodies (anti-CD9) and separated exosomes from whole blood through a new microfluidic device. Liu et al. [111] modified IONPs with the antibody CD63 to bind with an antigen and capture exosomes. Yang et al. [112] showed that superparamagnetic nanoparticles labeled with transferrin (Tfs) can accurately bind to blood TfR<sup>+</sup> exosomes. In addition, Chang et al. [113] removed the contamination of soluble proteins (such as albumin and fibrinogen) and lipoprotein particles to achieve the purification of exosomes by coating IONPs with the network structure of PEG. Moreover, compared with the exosomes separated by classical ultracentrifugation, the exosomes separated and released by continuous immunomagnetic separation maintained structural integrity and good biological activity.

In summary, only high concentrations of EVs can ensure the analysis of downstream proteins and nucleic acid components. Therefore, we discuss the methods of exosome isolation currently used. Different extraction methods have their own advantages and disadvantages. Researchers should select appropriate IONPs methods to highly enrich and purify EVs according to specific conditions and constantly optimize the separation method.

### Therapeutic of the magnetic EVs

Magnetic targeting drug delivery systems are of great significance in biomedical applications, as they are used to improve therapeutic efficiency. IONPs have also proven to be an effective drug delivery platform for both BBB and ischemic stroke treatment. These EVs are designed to wrap different therapeutic agents and iron oxide nanoparticles together. These magnetic vesicles can perform dynamic regulation and spatial control under

a magnetic field [114], enrich at the target location, enhance cell uptake, and thus enhance the therapeutic effect of EVs [115].

MiRNA is one of the main functional components of exosomes, which may play a key role in cell communication and ultimately the regulation of biological functions. Wu et al. [116] revealed that the abundance of miR-1260a in exosomes released by BMSCs pretreated with Fe<sub>3</sub>O<sub>4</sub> nanoparticles and SMFs was greatly increased. At the same time, the upregulation of miR-21-5p in mag-BMSC-Exos may promote wound healing [117] and tendon bone healing through the miR-21-5p/SMAD7 pathway [118]. In a heart repair experiment, Lee et al. [119] found that the NVs of MSCs derived from IONPs (IONP NVs) contain more heart repair therapeutic molecules (RNA and proteins) than normal MSC-derived NVs, which are mediated by the intracellular signal transduction modification triggered by the incorporation and ionization of iron oxide. With the slow ionization and assimilation of IONPs in vivo [120], the treatment of MSCs by IONP can improve the expression of anti-inflammatory and tissue repair cytokines by activating the JNK signal pathway [119, 121, 122]. At the same time, the level of therapeutic molecules in the prepared magnetic EVs increased. In the treatment of infarcted heart, IONP up-regulates the therapeutic molecules in IONP-MSC, including ANG1, FGF2, HGF, VEGF and Cx43, and these up-regulated molecules are also retained in IONP-NV [119]. In addition, exosomes coated with magnetic nanoparticles can be enriched at the tumor site under the guidance of an external magnetic field. The application of near-infrared radiation will cause local hyperthermia and trigger the release of goods loaded in the exosome [123, 124], thus enhancing the therapeutic effect [125].

In summary, we reviewed the influence of internalized IONPs on the therapeutic mechanism of EVs. In particular, we investigated whether IONP-Exos have a more significant therapeutic effect than normal exosomes. Although some achievements have been made, more experimental evidence is still sought to prove this effect.

### CONCLUSION AND PROSPECTS

In this paper, we reviewed the way in which IONPs were absorbed by cells and the mechanism of transport, degradation and toxicity of IONPs in cells. Therefore, IONPs can exert positive effects on cells by controlling the dosage. But it can also kill tumor cells. In stem cell therapy, the introduction of IONPs will make the ionization of IONPs trigger more therapeutic molecules (RNA and protein) for repair. Therefore, the fate of IONPs in cells is fully described to further promote the application of magnetic nanomaterials in the biomedical field. Extracellular vesicles have been proved to be suitable for the treatment of various diseases in vitro and in vivo. On this basis, the introduction of magnetic particles presents various research opportunities and challenges for the field of nanomedicine. In addition, this article briefly introduces the effects of IONPs on the production, separation and treatment mechanism of EVs. Most of the current work involves the combination of magnetic vesicles and magnetic fields to provide tissue-specific EVs delivery for therapeutic applications. However, the introduction of magnetic particles will also induce the triggering and release of cell therapeutic factors in EVs to achieve more effective disease treatment. However, more data are needed to prove the impact of IONPs on cells and EVs.

This overview aims to solve the existing problems and fully understand the effect of IONPs on cells and EVs delivery system. It is still necessary to further study the effect of IONPs on cells and EVs at multiple levels to better understand their mechanism of action and ensure the proper use of IONPs in the field of precision medicine. The therapeutic application of EVs based on IONPs also has high clinical conversion potential. Therefore, further efforts are needed in the future.



## DATA AVAILABILITY

The data used to support the findings of this study are available from the corresponding author upon request.

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#### AUTHOR CONTRIBUTIONS

YC carried out data statistics and drafted the manuscript. SH was responsible for manuscript supervision. All authors read and approved the final manuscript.

#### COMPETING INTERESTS

The authors declare no competing interests.

#### ADDITIONAL INFORMATION

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