

NEWS & VIEWS

Open Access

# Raster-scanning Donut simplifies MINFLUX and provides alternative implement on other scanning-based microscopes

Xinzhu Xu<sup>1,2,3</sup>, Shu Jia<sup>2</sup> and Peng Xi<sup>1,3,4</sup>✉

## Abstract

A donut excitation moves around a single molecule with a zigzag configuration lattice by lattice. Such a method implemented in scanning fluorescence microscopy simplifies the conventional MINFLUX process. Consisting of hollow zero-intensity excitation, single-pixel detection, time-correlated single photon counting, and drift stabilization, the system achieves localization precision and resolution very close to conventional MINFLUX theoretically and experimentally. An averaged high-SNR reference, and pixel-registered intensity from a single molecule is essential to reconstruct localization in maximum likelihood estimation. With performance reaching nearly conventional MINFLUX's, the proposed raster-scanning MINFLUX can inspire researchers expertized in STED or confocal setup to quickly transform to MINFLUX and develop for further exploring on bio-specimens or optical applications.

The advent of super-resolution fluorescence microscopy has opened up a promising avenue to the complete understanding of cell biology, from confocal fluorescence microscopy<sup>1</sup>, which promotes signal-to-noise ratio and thus resolution, to STED<sup>2</sup> that precisely coincides with Gaussian excitation and donut depletion, and nonlinear SIM (N-SIM)<sup>3</sup> inspired by the excited saturation contributing to Fourier domain extension or even PALM<sup>4</sup>/STORM<sup>5</sup> based on single-molecule localization. They have favored researchers to directly observe the sub-cellular organelle morphology (mitochondrial cristae<sup>6</sup>), the fine subcellular structure (microtubules<sup>7,8</sup>, neurons skeleton<sup>9</sup> and active zone<sup>10</sup>), and further boosted the qualitative leap in the understanding of complex life science process (heterogeneity and dynamics of membranes<sup>11</sup> and even the first-observed enlarged fusion pores during vesicle exocytosis<sup>12</sup>).

In the recent lustrum, taking advantage of the characteristic of the central zero-intensity of donut excitation and the statistical estimation, Balzarotti developed MINFLUX<sup>13</sup> in 2017, and Gwosch published 3D-MINFLUX<sup>14</sup> in 2020. These techniques have boosted the localization precision of optical fluorescence microscopy to  $\sim 1$  nm, with the corresponding spatial resolution of  $\sim 1-3$  nm and temporal resolution of  $\sim 50$   $\mu$ s. However, the methods that achieve such ultra-precise localization precision and resolution require complicated instruments such as ultra-fast optical scanning devices and delicate FPGA circuits, which inevitably leads to a significant increase in system complexity, technical barriers, and instrumentation cost. This has been a bottleneck for other laboratories to continue to develop and innovate based on the MINFLUX system, thus posing a challenge for its broad applicability. Building a more straightforward alternative system with comparable performance is one of the issues that need attention in the super-resolution fluorescence microscopy field. In 2021, the pulsed MINFLUX<sup>15</sup> invented by Luciano et al. promised a turning point to this problem. The excitation, consisting of four parallelly spaced and equal-interval pulsed lasers, is built on an existing point-

Correspondence: Peng Xi (xipeng@pku.edu.cn)

<sup>1</sup>Department of Biomedical Engineering, College of Future Technology, Peking University, Beijing 100871, China

<sup>2</sup>Wallace H. Coulter Department of Biomedical Engineering, Georgia Institute of Technology and Emory University, Atlanta, Georgia 30332, USA  
Full list of author information is available at the end of the article

© The Author(s) 2022



**Open Access** This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons license, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons license and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this license, visit <http://creativecommons.org/licenses/by/4.0/>.

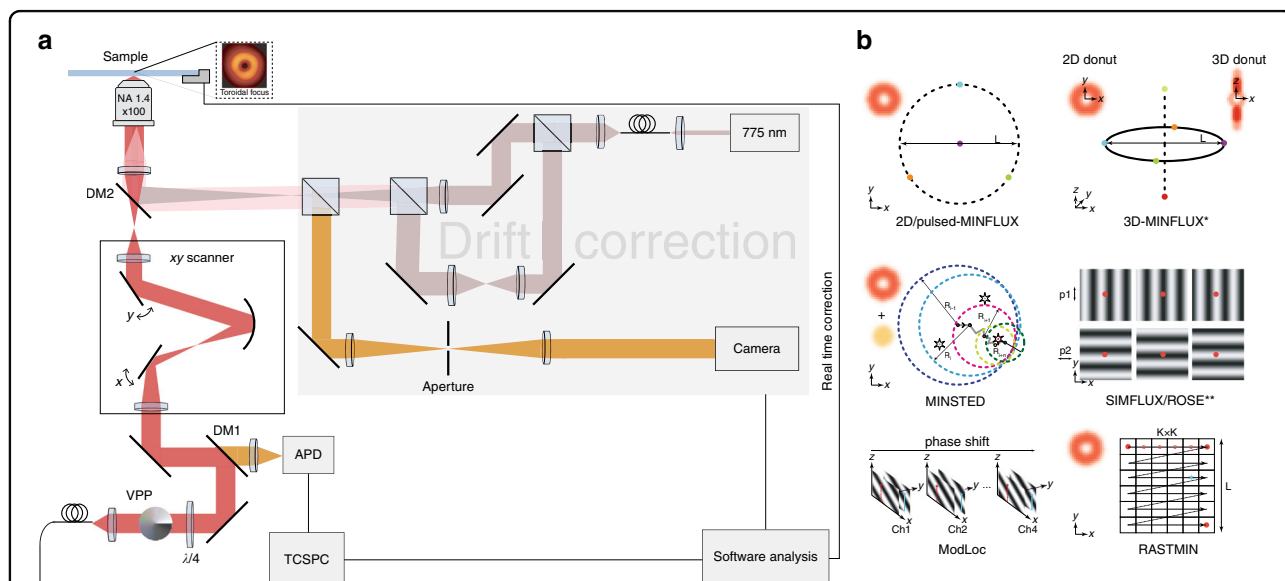
scanning confocal microscopy system. In combination with MINFLUX's four-point targeted coordinate pattern (TCP) excitation, scanning and time-correlated single-photon detection module, they achieved a localization precision of 1~2 nm under 1000–2000 photon counts and successfully demonstrated imaging of DNA origami samples with a feature distance of 12 nm. On this basis, MINFLUX fluorescence lifetime imaging is extended and realized by resolving a single fluosphere life signal from moving piezostage successively to configure a 7 nm-side-square.

To further reduce the system complexity, Luciano published RASTMIN recently<sup>16</sup>, which further simplifies the system and improves the multiplexing ability with other scanning-based microscopes. Here, an innovative single-molecule localization with sequential structured illumination<sup>17</sup> (SML-SSI) method has recently been proposed. Based upon an inverted point-scanning confocal microscope, 200 ps-pulsed-640 nm excitation is modulated into a donut after the vortex-phase plate and a quarter-wave plate. The beam then passes through the lateral scanning part with dual-axis scanning on the sample plane with nm-level accuracy. The combined up-and-down drift-corrected paths (Fig. 1(a) gray part) then meet with excitation before the objective through a dichroic mirror (DM2). The lateral scan controls the donut excitation to illuminate the pre-determined square sample area ( $L \approx 100$  nm), which is close to TCP in

MINFLUX and divided into  $K \times K$  grid points. Scanning grid-by-grid is performed, whose structure seems like a raster, thus called RASTMIN (single-molecule localization by RASTER scanning a MINimum of light). The fluorescent signal obtained by traversing each grid is de-scanned by the xy-scanner, then enters the single-photon detector, and is ultimately analyzed by the time-correlated single-photon counter module. Each grid corresponds to a certain number of photon counts, forming an intensity image of  $K \times K$  pixels. The acquired data is first screened for single-molecule emission on-state signals using the background threshold defined in the analytical model. Then, they compare it with a high signal-to-noise ratio image averaged by scanning a single fluorescent bead multiple times in advance, whose signal-to-background ratio (SBR) serves as the referee in (1)<sup>17,18</sup>, and use the maximum likelihood estimation to obtain the localization of a single molecule.

$$SBR(\mathbf{r}, L) = \frac{\sum_{i=1}^N I(\mathbf{r} - \mathbf{r}_i)}{\sum_{i=1}^N I(0 - \mathbf{r}_i)} SBR(0, L) \quad (1)$$

where  $SBR(\mathbf{r}, L)$  is the signal-to-background ratio when the emitter at position  $\mathbf{r}$  on the sample plane under the specific TCP range  $L$  (the emitter at the center of TCP  $\mathbf{r} = 0$  yields a benchmark), and  $I(\mathbf{r} - \mathbf{r}_i)$  is the signal detected when the emitter at  $\mathbf{r}$  with respect to excitation position  $\mathbf{r}_i$  ( $\mathbf{r} = 0$  yields TCP center signal). Afterward,



**Fig. 1 RASTMIN setup illustration and the main modulation patterns in some selected sequentially structured illumination(SSI)-based techniques. a** RASTMIN setup consists of excitation with donut modulation, xy-scan, drift correction and time-related single photon detection modules which has high compatibility with scanning-based fluorescent microscope, if starting from the experience on STED construction. **b** Structured excitation in 2D-MINFLUX<sup>13</sup>, pulsed-MINFLUX<sup>15</sup>, 3D-MINFLUX<sup>14</sup>, MINSTED<sup>21</sup>, SIMFLUX<sup>20</sup>, ROSE<sup>19</sup>, ModLoc<sup>22</sup>, and RASTMIN<sup>16</sup>, respectively. \*Regular focus is not displayed. \*\*Only crucial coherent modulation is illustrated; the delicate control and difference are not displayed.

Monte Carlo simulation is used to define the confidence threshold for distinguishing single-molecule blinking or simultaneous blinking of multiple molecules to eliminate the emission events of multiple fluorescent molecules that do not obey the Poisson distribution. To achieve such a high positioning accuracy without ultra-high-speed photoelectric deflection devices, the expense is to configure a drift stabilization for a real-time offset correction of the excitation within 2 nm of the three dimensions in x-y-z in the sample plane ( $x, y < 1.2$  nm;  $z < 2$  nm). Stabilization is divided into two optical paths: excitation and detection. In the excitation path, the near-infrared 775 nm TM<sub>00</sub> Gaussian mode laser is split into two light paths after passing through the beam splitter. The first path is a confocal excitation, which propagates through a pair of conjugate and tube lenses, expanding the beam and entering the back focal plane (BFP) of objective under parallel light. Thus, a convergent point on the sample excites and confocally scans the gold nanoparticles. The second beam is expanded by a telescope and then focused on the BFP of the objective. Thus, the widefield illumination is formed on the sample plane. The confocal detection consists of a pinhole placed on the Fourier surface of a pair of lenses in front of a camera to block the out-of-focus signals. Finally, the scattered signals from gold nanoparticles (GNs) were collected for imaging, as illustrated in Fig. 1(a). The system performs imaging tests on  $2 \times 3$  DNA origami arrays with a wide interval of 20 nm and a length of 15 nm, achieving super-resolution imaging with a 2-nm localization precision. At the same time, the same single 40 nm dark red fluorophore is moved in 7 nm step along the xy direction to form a square by the translation stage, and the fluorescence lifetime imaging under 7 nm resolution was obtained by the time-correlated single photon counting module.

After the invention of MINFLUX, there were methods given birth that gather signals to localize single molecules interrogated with a specific sequence of spatial modulated excitation patterns such as Repetitive Optical Selective Exposure<sup>19</sup>(ROSE), SIMFLUX<sup>20</sup>, MINSTED<sup>21</sup>, and Modulation Localization Microscopy<sup>22</sup>(ModLoc); and even early exploring on molecular dipole orientation<sup>23</sup>. In Table 1, we compared some critical parameters, and structured excitation patterns (Fig. 1(b)) among the main sequential-structured-illumination (SSI) based localization microscopy techniques. Compared with utilizing random fluorescence fluctuation information in SOFI<sup>24</sup>, ROSE and SIMFLUX take advantage of active-modulated-induced fluctuation (coherent modulation) to attain localization information, and similarly the Bessel beam bestowed with axial gradient intensity<sup>25</sup> yields another active fluorescence fluctuation localization for three-dimensional imaging. Clearly, non-ultrafast optoelectrical elements bring TCP pattern altering, specifically, the

**Table 1 Core parameters, and core ultra-fast optoelectrical elements and control devices/software in main sequential structured illumination-based localization microscopies**

	Localization precision (nm)	Spatial resolution (nm)	Scanning frequency (kHz)	Core ultra-fast optoelectrical elements and control devices/software						
2D-MINFLUX <sup>13</sup>	~1	~6	8	AOTF	EOM	EOD	Tip/Tilt Piezo	Piezo stage	FPGA	DAQ
3D-MINFLUX <sup>14</sup>	~1	1-3	20	AOTF	EOM	EOD	Tip/Tilt Piezo	Piezo stage	FPGA	DAQ
MINSTED <sup>21</sup>	1-3	1-3	125		EOD	EOD	Galvo mirrors	Piezo stage	FPGA	
SIMFLUX <sup>20</sup>	~10	<30	0.25			Pockels cell		Piezo stage	Arduino	
ROSE <sup>19</sup>	~2	<5	8	AOTF	EOM		Resonant mirror	Piezo stage	Complex programmable logic device	DAQ
ModLoc <sup>22</sup>	~7	~12	1.2		EOM	Pockels cell			Four-channel trigger generator	
RASTMIN <sup>16</sup>	~1-2	~15	1				Galvo mirrors	Piezo stage	Adwin	DAQ
p-MINFLUX <sup>15</sup>	~1-2	~12	100	Electromechanical shutters				Piezo stage	ADwin	DAQ
										Time-correlated single-photon counting unit
										Time-correlated single-photon counting unit

scanning configuration. In conventional MINFLUX, donut excitation is deflected sequentially to form a Star-like TCP. Meanwhile, it iteratively converges (dual-axis scanning with EODs up to 20 kHz), relying on the related position between the target and TCP itself until a single emitter localization process is finished. Comparatively, raster scanning reaches approximately 1 kHz without iterations and shrinks due to the limited speed and movement property of galvo mirrors. Another, the simplest RASTMIN achieves both similar localization precision and spatial resolution with only a set of core galvo-mirrors, piezo-stages and DAQ. The reason that RASTMIN achieves comparable performance to MINFLUX is because  $\sigma_{CRB}$  relies on the position of that molecule, the total detected photons for localization estimation, the signal-to-background ratio (SBR), and the size of the scanning area when the excitation intensity  $I(r)$  is assured. Since the detected photons obey Poisson distribution and the corresponding intensity on a single photon detector is linear with the photon counts from each pixel of  $K$ , in the likelihood function  $L^{13,17}$ , appropriately increasing sampling numbers and/or total detected photons result in the higher localization precision and resolution.

To reduce the engineered barrier and achieve fast construction, such as super-precision systems, RASTMIN is also an inspiration. With the popularization of the STED system review on spatial and temporal resolution<sup>26</sup> with the help of certain dyes<sup>6,27</sup>, moreover, the optically engineered STED protocol for self-building in its own lab<sup>28</sup>, the SSI-based localization system can quickly refit a prototype with performance close to MINFLUX for laboratories that have STED (especially stabilization is a commonly utilized path in observing GNS-samples' sectioning PSF along both lateral and axial plane), or even more basically, confocal fluorescence microscope constructing experience. On this basis, do some avant-garde imaging tests or explorations, such as multi-photon multi-color MINFLUX<sup>18</sup>. Luciano et al. also theoretically predict the CRB localization precision and lateral symmetry of multiphoton RASTMIN<sup>29</sup>.

Although MINFLUX is termed the post-Noble-Prize-era super-resolution technique, there is unwanted signal crosstalk. Because of the shrinking scale of donut excitation, when there are two fluorescent molecules in the vicinity of single-molecule distance, the non-zero intensity along the donut ring undesirably excites the emitter far away from another close to the zero-center, thus emerging a stronger background<sup>21</sup>. That leads to the necessity for more complex and sophisticated models, and algorithms to eliminate the wrongly excited signals from the periphery. Further, it even needs the improvements in the MINFLUX TCP, for example, increasing scan points number along TCP for delicate samplings, hence coming out more accurate localization data. The problem comes from the intrinsic

characteristic of the shrinking donut configuration. To this end, Michael. et al. invented MINSTED<sup>21</sup> in 2021, using ONB-2SiR dye<sup>30</sup> to label U-2 OS cells for imaging and addressing the legacy mentioned above problem. MINS- TED is a new generation of super-resolution fluorescence microscope technique inspired and developed by the STED system, MINFLUX algorithm and novel anti-two-photon-absorption photoswitchable dyes. Due to its donut-raster scanning simplified from STED, this may pave a new and transformative avenue for developing RASTMIN for STED-based localization microscopy.

Combining specific modulated-point spread function (PSF) scanning confocal instruments and statistical estimation-based single-molecule localization algorithms has promoted super-resolution microscopy to a single nanometer. In the near future, it will lead to optical fluorescence nanoscopy to step into the Ångstrom era. We hope the booming towards both seeking for the magnitude limitation as human beings powerful tools to reclaim unknown wilderness, and simplifying the precision nanoscopy construction barrier to facilitate global collaboration for complex life science process exploration, can flourish more research fields and extensive investigations.

#### Author details

<sup>1</sup>Department of Biomedical Engineering, College of Future Technology, Peking University, Beijing 100871, China. <sup>2</sup>Wallace H. Coulter Department of Biomedical Engineering, Georgia Institute of Technology and Emory University, Atlanta, Georgia 30332, USA. <sup>3</sup>UTS-SUStech Joint Research Centre for Biomedical Materials & Devices, Department of Biomedical Engineering, College of Engineering, Southern University of Science and Technology, Shenzhen, Guangdong 518055, China. <sup>4</sup>National Biomedical Imaging Center, Peking University, Beijing 100871, China

#### Competing interests

The authors declare no competing interests.

Published online: 10 October 2022

#### References

- White, J. & Amos, W. Confocal microscopy comes of age. *Nature* **328**, 183–184 (1987).
- Hell, S. W. & Wichmann, J. Breaking the diffraction resolution limit by stimulated emission: stimulated-emission-depletion fluorescence microscopy. *Opt. Lett.* **19**, 780–782 (1994).
- Gustafsson, M. G. Nonlinear structured-illumination microscopy: wide-field fluorescence imaging with theoretically unlimited resolution. *Proc. Natl Acad. Sci. USA* **102**, 13081–13086 (2005).
- Betzig, E. et al. Imaging intracellular fluorescent proteins at nanometer resolution. *Science* **313**, 1642–1645 (2006).
- Rust, M. J., Bates, M. & Zhuang, X. W. Sub-diffraction-limit imaging by stochastic optical reconstruction microscopy (STORM). *Nat. Methods* **3**, 793–795 (2006).
- Yang, X. S. et al. Mitochondrial dynamics quantitatively revealed by STED nanoscopy with an enhanced squaraine variant probe. *Nat. Commun.* **11**, 3699 (2020).
- Vaughan, J. C., Jia, S. & Zhuang, X. W. Ultrabright photoactivatable fluorophores created by reductive caging. *Nat. Methods* **9**, 1181–1184 (2012).

8. Jia, S., Vaughan, J. C. & Zhuang, X. W. Isotropic three-dimensional super-resolution imaging with a self-bending point spread function. *Nat. Photonics* **8**, 302–306 (2014).
9. Zhanghao, K. et al. Super-resolution imaging of fluorescent dipoles via polarized structured illumination microscopy. *Nat. Commun.* **10**, 4694 (2019).
10. Grabner, C. P. et al. Resolving the molecular architecture of the photoreceptor active zone with 3D-MINFLUX. *Sci. Adv.* **8**, eabl7560 (2022).
11. Zhanghao, K. et al. High-dimensional super-resolution imaging reveals heterogeneity and dynamics of subcellular lipid membranes. *Nat. Commun.* **11**, 5890 (2020).
12. Huang, X. S. et al. Fast, long-term, super-resolution imaging with Hessian structured illumination microscopy. *Nat. Biotechnol.* **36**, 451–459 (2018).
13. Balzarotti, F. et al. Nanometer resolution imaging and tracking of fluorescent molecules with minimal photon fluxes. *Science* **355**, 606–612 (2017).
14. Gwosch, K. C. et al. MINFLUX nanoscopy delivers 3D multicolor nanometer resolution in cells. *Nat. Methods* **17**, 217–224 (2020).
15. Masullo, L. A. et al. Pulsed interleaved MINFLUX. *Nano Lett.* **21**, 840–846 (2020).
16. Masullo, L. A. et al. An alternative to MINFLUX that enables nanometer resolution in a confocal microscope. *Light Sci. Appl.* **11**, 199 (2022).
17. Masullo, L. A., Lopez, L. F. & Stefani, F. D. A common framework for single-molecule localization using sequential structured illumination. *Biophysical Rep.* **2**, 100036 (2022).
18. Zhao, K. et al. Two-photon MINFLUX with doubled localization precision. *eLight* **2**, 5 (2022).
19. Gu, L. S. et al. Molecular resolution imaging by repetitive optical selective exposure. *Nat. Methods* **16**, 1114–1118 (2019).
20. Cnossen, J. et al. Localization microscopy at doubled precision with patterned illumination. *Nat. Methods* **17**, 59–63 (2020).
21. Weber, M. et al. MINSTED fluorescence localization and nanoscopy. *Nat. Photonics* **15**, 361–366 (2021).
22. Jouchet, P. et al. Nanometric axial localization of single fluorescent molecules with modulated excitation. *Nat. Photonics* **15**, 297–304 (2021).
23. Zhan, Z. Y. et al. Simultaneous super-resolution estimation of single-molecule position and orientation with minimal photon fluxes. *Opt. Express* **30**, 22051–22065 (2022).
24. Dertinger, T. et al. Fast, background-free, 3D super-resolution optical fluctuation imaging (SOFI). *Proc. Natl Acad. Sci. USA* **106**, 22287–22292 (2009).
25. Gao, Y. F. et al. Axial gradient excitation accelerates volumetric imaging of two-photon microscopy. *Photonics Res.* **10**, 687–696 (2022).
26. Wu, Z. Y., Xu, X. Z. & Xi, P. Stimulated emission depletion microscopy for biological imaging in four dimensions: a review. *Microsc. Res. Tech.* **84**, 1947–1958 (2021).
27. Lincoln, R. et al. A general design of caging-group-free photoactivatable fluorophores for live-cell nanoscopy. *Nat. Chem.* **14**, 1013–1020 (2022).
28. Xu, X. Z. et al. A protocol for single-source dual-pulse stimulated emission depletion setup with Bessel modulation. *Microsc. Res. Tech.* **85**, 813–823 (2021).
29. Masullo, L. A. & Stefani, F. D. Multiphoton single-molecule localization by sequential excitation with light minima. *Light Sci. Appl.* **11**, 70 (2022).
30. Weber, M. et al. Photoactivatable fluorophore for stimulated emission depletion (STED) microscopy and bioconjugation technique for hydrophobic labels. *Chemistry* **27**, 451–458 (2021).