# Micro-magnetic resonance imaging (µ-MRI) study on the sepsis effected eyeball of zebrafish

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#### Abstract

We have studied the normal and sepsis effected zebrafish eyeball with micro-magnetic resonance imaging (micro-MRI).  $T_2$  weighted image was studied and pixel-wise  $T_2$  maps were co registered among the normal and sepsis effected eye. From the micro-image the sepsis effect in the eye has been demonstrated. The pixel-wise brightness distribution is not so scattered in the normal eyeball image, whereas it is very scattered in case of sepsis affected eyeball image. Also the  $T_2$  mapping on the eye has given valuable information that would be a potential tool for the study of diseased organ in the micro level. From  $T_2$  mapping, it has shown that the T2 in normal eyeball have low values in comparison to the sepsis affected eyeball.

Keywords: Zebrafish; Eyeball; Micro-Magnetic Resonance Imaging; T<sub>2</sub> weighted image;

T<sub>2</sub>-map.

# Introduction

The zebrafish, one of the favourite animals of developmental biologists, is rapidly gaining ground in infection models [1,2]. With the zebrafish, genetic screens in a vertebrate host with a fully developed immune system are possible [3,4]. In addition, bacterial infections can be analyzed in real-time in zebrafish embryos [5]. This fish is a unique and important animal model in which the power of mutagenesis is applied to the study of vertebrate development [6,7]. Zebrafish genome mutagenesis has provided important insights into genes related to cardiac, vascular, and erythrocyte development, including models of disease such as congenital sideroblastic anemia and hepatoerythropoietic porphyria [6-9]. Given the development of appropriate screening assays, the power of the zebrafish model can be harnessed for the study of other vertebrate functions such as hemostasis, thrombosis and sepsis [10-13]. Previous research with zebrafish ensured that a variety of human disease conditions are can be studied utilizing the zebrafish model [14,15].

It is well known that  $T_2$  plays a role in almost every aspect of nuclear magnetic resonance [16]. Clinical  $T_2$ -weighted images were exquisitely sensitive to neuro pathology, giving rise to much optimism that  $T_2$  relaxation would lead to pathological specificity [17].  $T_2$ relaxation rates can be correlated to the pathological changes observed in neurodegenerative diseases including edema (increased intra- or extracellular water), blood–brain barrier collapse (tight junction leakage), inflammation (proliferation of inflammatory cells), demyelination (breakdown of the myelin sheath), gliosis

(proliferation of glial cells) and axonal loss (breakdown of the axon) [18]. The level to which these pathologies can be measured by MRI depends upon whether they have a unique impact on the proton NMR signal; if these pathological changes affect the organisation of nonaqueous molecules in cellular structures, water T<sub>2</sub> relaxation should also be affected. The features allied with pressure ulcers that may affect muscle proton density and relaxation times are inflammation, edema, necrosis, hemorrhage, fibrosis, and fatty infiltration[19-21]. These diseases like inflammation, edema, and also hemorrhage can lead to an increased proton density which is caused by an increased in both intracellular and extracellular free water. T<sub>2</sub> is very sensitive to tissue changes [22] which were noted in animal model Brown-Norway rats where tibialis anterior (TA) was condensed by means of an indenter. After 24 h, muscle tissue variation was observed by using MRI. It was shown that affected tissue localized by T<sub>2</sub>-weighted MRI correlated well with damaged areas determined by histological examination. A raise in the transverse relaxation time  $(T_2)$  is generally established as a measurement of tissue injury [23].

However, there no previous report to study the zebrafish diseases model using MRI. So, it is very relevant to study the sepsis model using MRI. Here we have investigated the sepsis induced eyeball of zebrafish (*Danio rerio*) by MR micro-imaging giving special emphasis on the transverse relaxation mapping and we took an opportunity also to shed light on micro-level for the study of sepsis effect on the eyeball with the help of micro-MRI.

### **Materials and methods**

Zebrafish model. Adult zebrafish were obtained from the lab stock maintained according to the guidelines given in the zebrafish book [24]. The fish used in these experiments were about 4-6 months old and approximately 3 cm in length which were kept in 5-10 lit glass aquariums. The aquaria had a continuous re-circulating system, consisting of biological filters. Additional oxygen was provided by placing air-stones in the water and 1/3 of water was replaced weekly. Aquariums water temperature was maintained at 28.5°C-32°C and a constant 14/10-h light/dark cycle.

Sepsis effected zebrafish. All zebrafish were injected at the age of 4-6 months old. BD ultra-fine II insulin syringe (1-2 cc capacity) was used for injection (Becton Dickinson). Fishes were admitted to the study ward at 8:00 am after an overnight fast. The volume of injection was maintained constant at 10  $\mu$ l, and the amount of LPS was 2 ng/kg LPS (Sigma, USA). The fishes were taken out of the water and provided anesthesia with MS-222 (a methane sulfonate salt of 3-aminobenzoic acid ethyl ester, Sigma Chemical Company, St. Louis, MO, USA) at a concentration of 50 mg/100 ml for 5-10 minutes and then an intra-muscular injection was given approximately in the end region

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of the dorsal fin on one flank of the fish. Identical volumes of saline were given in the control group.

*Collection of samples.* We have operated and collected zebrafish's eyeball for (1) normal and (2) sepsis affected, very carefully to collect the eyeball. The eye was kept in liquid nitrogen for quick freezing. Within 24 hours we have used the sample for study.

*Micro-imaging.* All MR images of the zebrafish eyeball were obtained with a Varian Unity INOVA 500 MHz NMR spectrometer with 11.4 Tesla magnetic fields in vertical bore Oxford 500 magnet system at a 500-MHz proton Larmor frequency. The system was interfaced to a Linux PC running Solaris 9 operating environment on Sun SPARC host workstation. T<sub>2</sub>-weighted images [25] were acquired using spin echo multi scan (SEMS) pulse sequence. Subsequent T<sub>2</sub>- weighted images were acquired using multiple echo time (TE). The MR parameters were: repetition time (TR) = 1000 msec (90° flip angle), effective echo time (TE) = 12, 16, 20, and 25 msec, spectral width = 50 kHz, 8 averages, field of view (FOV) = 0.3 cm × 0.3 cm, data matrix = 128 × 128, and number of transients (NT) = 32.

Data Analysis. T<sub>2</sub> have been calculated pixel-by-pixel of the region of interest (ROI) according to the relation,

$$S(TE) = S_0 g \exp(-TE/T_2) \qquad \dots (1)$$

where TE is the effective echo time at the center of the echo-train length, and  $S_0$  is the signal intensity at TE = 0.  $T_2$  were derived using nonlinear least squared regression with Mathematica 5.0. In the regression process, for each pixel, we have taken the signal intensity for different TE values. Thus we can find the  $T_2$  values for each pixel.

## Results

The zebrafish eyeball, one is normal and other as sepsis effected, were used to collect micro-MR images with three different TE weightings (TE = 12, 16 and 20 ms). We have taken dorsal -median plane section of the eyeball (Fig. 1D). The FOV was  $0.3 \times 0.3 \text{ cm}^2$ . Nearly uniform brightness appeared in different parts of the normal eyeball (Fig. 1 A, B and C). Also the images for sepsis affected eye are shown in Fig. 2 A, B and C. The histograms of the pixel-wise brightness distribution in the image with TE=12 ms for normal and sepsis effected eyes are shown respectively in Fig. 3 A and B. It is understood from the histogram for the normal eye that more or less the pixels are around the intensity value 0.0002 (in arbitrary unit) with median 0.0002307 and standard deviation 0.0001684 (Table 1). We have considered total 6717 pixels in the image. But there is remarkable variation in brightness in the different parts in T<sub>2</sub>-weighted image of the sepsis affected eyeball (Fig. 2 A, B and C). The histogram of the pixel-wise

For precise understanding, a ROI was taken just in the backside of the lens in between the lens and the retina (Fig. 2 D). We have taken the ROI both for normal and sepsis effected eye for comparison. The histograms of the pixel-wise brightness distribution in the ROIs are depicted in Fig. 3, C and D for normal and sepsis affected eye respectively. The histogram shows for the normal eye that the pixels are around the intensity value 0.0009 (in arbitrary unit) with median 0.0009154 and standard deviation 0.0001451 (Table 2). For sepsis effected ROI, the distribution is comparatively more scattered with median 0.00113 and standard deviation 0.0001253 (Table 2).

T2 have been calculated pixel-by-pixel as explained in the data analysis section. The  $T_2$  mappings for normal eye and the sepsis affected one are shown in Fig 4 A and B. The mapping indicates that  $T_2$  have greater values in case of sepsis affected eye. Most of the part in the sepsis affected one is characterized with  $T_2$  values greater than 200 ms. But in the normal eye,  $T_2$  values are in the range from 75 ms to 200 ms.

#### Discussion

The major findings of this study are: (1)  $T_2$ -weighted images and (2)  $T_2$  mapping of normal and sepsis effected eye of zebrafish. From  $T_2$ -weighted images, it is found that there is a more variation in the brightness in sepsis effected eyeball image. But there is

not so much variation in the normal eyeball image. Also it is clear from the histogram that the pixel-wise brightness distribution is not so scattered in the normal eyeball, whereas it is very scattered in case of sepsis effected eyeball. From T<sub>2</sub> mapping, it is shown that the  $T_2$  in normal eyeball have comparatively low values. But the  $T_2$  have the larger values in sepsis affected eyeball. It can be understood from the T2 weighted anatomical and T<sub>2</sub> mapping images, that T<sub>2</sub> is very sensitive to the pathological change in tissues. The relaxation properties of water, which may be characterized by a longitudinal or spin-lattice relaxation time  $T_1$  and a transverse or spin-spin relaxation time  $T_2$ , play a crucial role [26]. These values depend in a characteristic way on molecular environment of water molecules, because of different molecular mobility and structures. Also, water protons can exchange themselves or the magnetization with mobile protons of external functional OH- or NH-groups of the proteins leading also to contributions of these environments to water relaxation times [27,28]. Nevertheless, these quantities can provide interesting information on changes of protein hydration and mobility, which are themselves related to biological changes [29,30]. The spin-spin relaxation time  $T_2$  is a specific attribute of spins that depends on their surroundings. Interaction between spins (e.g., coupling of neighboring nuclei) destroys the phase coherence, and therefore the  $T_2$ relaxation time can be a sensitive indicator of impaired cell physiology. In the sepsis effected region on the eyeball, it causes the ingression of intracellular and extracellular free water which in turn results in an increase in  $T_1$  (longitudinal relaxation time) and  $T_2$ .  $T_2$  is very sensitive to tissue changes. An increase in the transverse relaxation time ( $T_2$ ) is an expression of tissue damage.

However, MRI can measure structural, physiological (like blood flow and oxygenation) and, metabolic data in a single setting, which are generally not possible with present techniques and that is the great advantage of MRI. It has no depth limitation also. Therefore, MRI has the potential to complement existing techniques to study the eyeball.

In conclusion, the pathological changes due to the sepsis in the zebrafish eyeball were resolved using multiple MRI contrasts. To the best of our knowledge, this is the first micro-MRI study in demonstrating the damage in the sepsis affected eyeball of zebrafish. Further improvements are expected for this model. MRI has the potential to provide sepsis affected physiological (such as tissue blood flow and oxygenation) and functional information on the organ of micro-dimension in a single setting without depth limitation and, thus, it could complement existing techniques to study very small size organ.

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# Table 1

Histogram of the pixel wise intensity distribution in the eyeball.

Eyeball	Number of	Minimum	Maximum	Median	Mean	Standard
	Pixels/Area	intensity	intensity			Deviation
		(arbitrary	(arbitrary			
		unit)	unit)			
Normal	6717/0.0369	4.719e-	0.0008	0.000230	0.000273	0.000168
		06		7	7	4
Sepsis	6971/0.03829	2.14e-06	0.0014	0.000631	0.000654	0.000350
effected				8	4	4

# Table 2

Histogram of the pixel wise intensity distribution in the ROI.

ROI	Number of	Minimum	Maximum	Median	Mean	Standard
	Pixels/Area	intensity	intensity			Deviation
		(arbitrary	(arbitrary			
		unit)	unit)			
	1673/0.00919	0.000391	0.001257	0.000915	0.000890	0.000145
Normal		8		4	1	1
	1353/	0.000722	0.001484	0.00113	0.001128	0.000125
Sepsis	0.007432	6				3
effected						

## **Figure captions**

Fig. 1. T<sub>2</sub> weighted Micro-MR images of normal zebrafish eye with TE (A) 12, (B) 16 and (C) 20 ms and (D) schematic dorsal -median plane section.

Fig. 2. T<sub>2</sub> weighted Micro-MR images for sepsis effected zebrafish eye with TE (A) 12, (B) 16 and (C) 20 ms and (D) ROI in the backside of the lens in between the lens and the retina (indicated as dotted line loop) in the normal eye.

Fig. 3. The histograms of the pixel-wise brightness distribution in the image with TE=12 ms for (A) normal and (B) sepsis effected eyes (C) the ROI in Normal (D) the ROI in sepsis effected eye.

Fig. 4. The  $T_2$  mappings for normal and the sepsis effected eye. ( $T_2$  values are indicated as black colour code)



Fig. 2.



Fig. 3.



Α





В





D

Fig. 4.



А

В