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Ewing sarcoma dissemination and response to T-cell therapy in mice assessed by whole-body magnetic resonance imaging

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Background: Novel treatment strategies in Ewing sarcoma include targeted cellular therapies. Preclinical *in vivo* models are needed that reflect their activity against systemic (micro)metastatic disease.

Methods: Whole-body magnetic resonance imaging (WB-MRI) was used to monitor the engraftment and dissemination of human Ewing sarcoma xenografts in mice. In this model, we evaluated the therapeutic efficacy of T cells redirected against the Ewing sarcoma-associated antigen G_{D2} by chimeric receptor engineering.

Results: Of 18 mice receiving intravenous injections of VH-64 Ewing sarcoma cells, all developed disseminated tumour growth detectable by WB-MRI. All mice had lung tumours, and the majority had additional manifestations in the bone, soft tissues, and/or kidney. Sequential scans revealed *in vivo* growth of tumours. Diffusion-weighted whole-body imaging with background signal suppression effectively visualised Ewing sarcoma growth in extrapulmonary sites. Animals receiving G_{D2}-targeted T-cell therapy had lower numbers of pulmonary tumours than controls, and the median volume of soft tissue tumours at first detection was lower, with a tumour growth delay over time.

Conclusion: Magnetic resonance imaging reliably visualises disseminated Ewing sarcoma growth in mice. G_{D2}-retargeted T cells can noticeably delay tumour growth and reduce pulmonary Ewing sarcoma manifestations in this aggressive disease model.

Ewing sarcoma is a cancer of bone and soft tissue that is characterised by a molecular rearrangement of the *EWS* gene on chromosome 22 with an *ets*-type gene (Delattre *et al*, 1992). Survival of patients with localised disease has improved substantially by modern multimodal treatment regimens (Paulussen *et al*, 1998), but primary multifocal disease or disseminated relapse often remains incurable (Ladenstein *et al*, 2010). Novel treatment strategies aim to eliminate residual microscopic disease remaining after standard therapy and include molecularly targeted drugs and antibodies (Erkizan *et al*, 2009; Juergens *et al*, 2011) as

well as immunological therapies (Mackall *et al*, 2008; Kailayangiri *et al*, 2012). One approach is based on the genetic engineering of T cells with recombinant chimeric antigen receptors (CARs) directed against the ganglioside antigen G_{D2} that is overexpressed on many Ewing sarcomas (Kailayangiri *et al*, 2012). G_{D2}-specific CARs consist of the antigen-binding domain of a G_{D2}-specific antibody linked to T-cell receptor-signalling domains and mediate efficient cytolytic T-cell interaction with G_{D2}-expressing tumour cells both *in vitro* and *in vivo* (Rossig *et al*, 2001; Pule *et al*, 2008).

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In vivo preclinical data are often generated in localised tumour models, although the capacity of novel therapies to prevent the outgrowth of subcutaneous tumours in mice inadequately reflects their activity against systemic (micro)metastatic disease. To study the biology of systemic disease and to develop novel therapies including translational validation, preclinical *in vivo* models are needed that recapitulate the biology of multifocal disease and tumour dissemination. In accordance with the known haematological spread pattern of Ewing sarcoma, intravenous transplantation of single-cell suspensions of Ewing sarcoma cells into highly immunodeficient mice was found to efficiently establish multifocal sarcomas in many of the animals (Vormoor *et al*, 2001). The use of systemic disease models as preclinical tools for monitoring the antitumour activity of novel therapies requires visualisation of tumour growth in the living animal. Here, we used whole-body (WB) imaging techniques, including both standard magnetic resonance imaging (MRI) and diffusion-weighted WB imaging with background signal suppression (DWIBS) to follow-up the engraftment and systemic spread of human Ewing sarcoma xenografts in mice and to address the therapeutic efficacy of adoptive T-cell transfer against disseminated tumour cells *in vivo*.

MATERIALS AND METHODS

Cell lines. The Ewing sarcoma cell line VH-64 was a gift from Frans van Valen at the Institute of Experimental Musculoskeletal Medicine of University of Muenster, Germany. It was originally established from a malignant pleural effusion of a patient with Ewing sarcoma of the metatarsal bone. The identity of the cell line throughout the experiments was confirmed by repeated short tandem repeat profiling. VH-64 cells were cultured in collagen-coated 25 cm² tissue culture flasks in RPMI 1640 medium (Invitrogen, Darmstadt, Germany), supplemented with 10% heat-inactivated foetal calf serum (Thermo Fisher, Bonn, Germany) and 2 mM L-glutamine and maintained at 37 °C and 5% CO₂. The retroviral packaging cell lines Phoenix-ampho and FLYRD 18 were provided by Gary P Nolan (Stanford University School of Medicine, Stanford, CA, USA) and E Vanin (Center for Cell and Gene Therapy, Houston, TX, USA), respectively.

Xenogeneic NOD/scid mouse model of Ewing sarcoma. Mouse experiments were approved by the animal care committee of the local government (Bezirksregierung Muenster, Az. 87-51.04.2010.A117). NOD/scid mice (8–10-week old; Charles River Laboratories, Sulzfeld, Germany) were irradiated with a single dose of 3.5 Gy from a linear accelerator 1 day before transplantation. We chose VH-64 cells for this study, as the engraftment, dissemination, and *in vivo* proliferation of this cell line is highly representative of Ewing sarcoma xenografts (Vormoor *et al*, 2001). Single-cell suspensions of 2×10^6 tumour cells in 0.2 ml of medium were injected into the tail veins. All experimental manipulations were performed under sterile conditions in a laminar flow chamber. Animals developing clinical signs of disease (weight loss, shaggy fur, bent spine) were killed.

Whole-body MRI of mice. High resolution MR data sets were acquired on a clinical 3 Tesla WB MR system (Achieva, Philips Medical Systems, Best, the Netherlands) equipped with standard gradient coils (gradient strength 40 mT m⁻¹, slew rate 200 mT m⁻¹ ms⁻¹). A dedicated small animal solenoid receiver coil (Philips Research, Hamburg, Germany) with an inner diameter of 40 mm and an integrated heating system to regulate the body temperature of the animals was used for signal reception. The MRI protocol consisted of the following sequences: T2 TSE sagittal (TR 1732 ms, TE 60 ms, FOV 70 (tail to head) × 30 (anterior-posterior) mm, reconstruction matrix 560 × 240, number of signal averages 4, slice thickness 1 mm, number of slices 27, scan

time 3:34.8 min), T2 TSE axial (TR 2854 ms, TE 60 ms, FOV 32 (right to left) × 32 (anterior-posterior) mm, reconstruction matrix 288 × 288, NSA 4, slice thickness 1.5 mm, number of slices 45, scan time 05:53.9 min), STIR TSE sagittal (TR/TI 2445/200 ms, TE 68 ms, FOV 70 (tail to head) × 29 (anterior-posterior) mm, reconstruction matrix 512 × 214, NSA 14, slice thickness 1 mm, number of slices 25, scan time 07:59.3 min), DWIBS axial (TR/TI 16470/240 ms, TE 87 ms, FOV 50 (tail to head) × 50 (anterior-posterior) mm, reconstruction matrix 256 × 256, multi-shot EPI, EPI factor 9, number of b-factors 2 (0;1000), NSA 1, slice thickness 0.8 mm, gap 0.2 mm, number of slices 87, scan time 08:30.6 min; Takahara *et al*, 2004). Zero-filling was used to calculate the reconstruction matrix. Apparent diffusion coefficient maps were calculated from the native diffusion images with the built-in software tools of the MRI scanner. All sequences were acquired with the same geometry to assure comparability of the various sequences. First, MRIs were performed between 20 and 24 days after tumour cell transplantation independent of the development of disease symptoms. Up to four follow-up MRIs were performed to monitor tumour growth. Time points (TPs) were designated as follows: TP0, tumour cell transplantation; TP1, initial scan, median 20 days (range 20–24) after TP0; TP2, median 30 days (range 27–31) after initial scan; TP3, median 34 days (range 34–39) after initial scan; TP4, 41 days after initial scan. During examination, the mice were anaesthetised with isoflurane. Precautions to reduce the stress associated with general anaesthesia and imaging included maintenance and monitoring of the body temperature, transport to the imaging facility in suitable transport boxes, reduction of total imaging time to 1 h, and limitation to one imaging session per week. No contrast agent was given, and images were generated without respiratory gating. Two experienced radiologists independently evaluated all acquired images. Tumours were measured on the slice with their largest extent in T2 sagittal images in two directions (*x*, *y*), with an intraclass correlation of 0.958 between both investigators. Tumour volume estimation was done by manually tracing the tumours on each slice image, and then adding all the voxel volumes within the boundaries of the region of interest. Total volumes of individual tumours were calculated using Amira Software, Visage Imaging, Berlin, Germany.

Histopathology and immunohistochemistry. To confirm the presence of Ewing sarcoma xenografts, lungs, kidneys, and macroscopically detected bone and soft tissue tumours were examined by light microscopic examination and by immunohistochemistry. Tissues were fixed in 4% buffered formalin, processed and embedded in paraffin. Four- to five-micrometer sections were prepared and stained with haematoxylin and eosin or with the anti-human CD99 monoclonal antibody TÛ12 (BD Pharmingen, Heidelberg, Germany).

Production of recombinant retrovirus, transduction and expansion of T cells. Generation of the G_{D2}-specific CAR 14.G2a-CD28ζ has been described in detail in previous publications from our group (Rossig *et al*, 2001; Altvater *et al*, 2006; Kailayangiri *et al*, 2012). The receptor contains the single-chain antibody domain of the monoclonal anti-G_{D2} antibody 14.G2a (Mujoo *et al*, 1989), the transmembrane domain of CD8α, and the intracellular domains of CD28 and TCR ζ. Retroviral supernatant was generated and used to transduce *in vitro* OKT-3/anti-CD28 antibody-preactivated human T cells, as previously described (Kailayangiri *et al*, 2012). To superexpand the gene-modified T cells, 2×10^7 cells were transferred to gas-permeable culture devices with 500 ml capacity (Wilson Wolf Manufacturing, New Brighton, MN, USA) in 400 ml of medium containing IL-2 (50 U ml⁻¹) on day 5 after the prestimulation.

T-cell therapy. Following transplantation of 2×10^6 VH-64 tumour cells into the tail veins of NOD/scid mice, experimental

cohorts of mice were given intravenous injections of 1×10^7 14.G2a-CD28 ζ -transduced human T cells, whereas control cohorts received non-transduced T cells. In a first cohort of 10 mice (5 treated and 5 control mice), T-cell transfer was given on days 4, 10, 15, and 22 after tumour inoculation. A subsequent cohort of another eight mice (four treated and four control mice) received a total of six T-cell therapies on days 1, 3, 6, 9, 12, and 15. Intraperitoneal injections of human recombinant IL-2 were given twice weekly to all mice to sustain T-cell survival within the non-human environment. Mice receiving four and six injections were analysed together. Tumour development was monitored using WB-MRI as described above.

Statistical analysis. Statistical analyses were performed using IBM SPSS Statistics 21 for Windows (IBM Corporation, Somers, NY, USA) and SAS software, Version 9.3 of the SAS System for Windows (SAS Institute Inc., Cary, NC, USA). *P*-values were interpreted in Fisher's sense, representing the metric weight of evidence against the respective null hypothesis of no effect, and were considered noticeable in case $P \leq 0.05$ and highly noticeable in case $P \leq 0.01$. The intraclass correlations coefficient (ICC) was calculated as a measure of inter-rater agreement. Continuous data are reported as median, minimum, and maximum. Categorical variables are described as absolute and relative frequencies. Relationships between categorical variables were compared via contingency tables, χ^2 -, and Fisher's exact test, where appropriate. Exact χ^2 -goodness-of-fit test was applied to compare the allocation of tumour numbers between cohorts. Pairwise group comparison for tumour numbers and tumour volumes were performed using exact non-parametric Mann-Whitney *U*-tests. Wilcoxon-signed rank tests were applied to detect the statistically noticeable changes between two TPs. Kaplan-Meier analyses and log-rank tests were performed to compare event-free and overall survival between treated and control cohorts. Multivariable, mixed model analyses were conducted to analyse the impact of potentially explanatory variables on target parameters.

RESULTS

Whole-body MRI visualises disseminated tumour growth after intravenous injection of xenogeneic Ewing sarcoma cells in mice. High quality images in mice were obtained using a clinical 3 Tesla MRI scanner without respiratory triggering and without the need for contrast-enhancing agents. Among the first cohort of mice ($n = 18$) receiving intravenous injections of 2×10^6 VH-64 cells, all 18 mice developed disseminated tumours detectable by WB-MRI within 20–31 days (median of 27 days). All engrafted mice had lung tumours (100%). Sixteen mice had additional tumour manifestations in extrapulmonary sites: 55.6% of mice (10 of 18) had bone or bone marrow tumours in the lower extremities, pelvis and/or vertebral column, and 27.8% (5 of 18) had soft tissue tumours (Figure 1A). Moreover, 72.2% (13 of 18) of mice had tumours in the kidney, and three of these also had tumours within the suprarenal gland. One of five female mice and none of 13 male mice had an abdominal tumour, potentially representing an ovarian manifestation. The highest numbers of tumours were found in the lungs, with a median of 19.5 (range 1–60) per mouse (Figure 1B). Interobserver agreement was consistent with an overall ICC of 0.915 for tumour numbers and 0.967 when excluding lung tumours. The median volume of tumours at first detection varied with the tumour site (Figure 1C). Soft tissue and kidney tumours were detectable at relatively small median sizes of 8.94 mm^3 (range $2.53\text{--}25.05 \text{ mm}^3$) and 8.15 mm^3 ($1.24\text{--}40.3 \text{ mm}^3$), respectively, whereas bone tumours were relatively large upon first detection (median 33.11 mm^3 , range $13.49\text{--}117.9 \text{ mm}^3$). Lung tumours were detectable at very small volumes of $<1 \text{ mm}^3$. Dissection and

histological analysis confirmed the presence of CD99+ small, blue, round cell tumours in bones, lungs, and kidneys in all examined cases (Figure 1D).

Sequential WB-MRI allows to monitor tumour growth *in vivo*. Sequential WB-MRI scans were performed until the mice had to be killed. T2 sagittal WB sequences revealed *in vivo* growth of tumours at all sites (Figure 2A), with heterogeneous kinetics. Soft tissue tumours increased in sizes at relatively slow rates, potentially owing to the early detection of very small tumours. As reliable volumetry of individual lung tumours is complicated by their diffuse infiltrative character, pulmonary involvement was monitored by combining volumes of all individual lung tumours for each lung. Moreover, lung tumours were quantified by numbers in axial images (Figure 2B). A continuous increase of the numbers of lung tumours both per lung and per mouse was found in follow-up scans (Figure 2B and C).

Diffusion-weighted WB imaging with background signal suppression allows for functional detection of Ewing sarcoma manifestations and growth in mice. Whole-body diffusion-weighted MRI with background body signal suppression is a functional imaging technique. Tumours are visualised based on the restricted diffusion of the malignant tissue architecture (Takahara *et al*, 2004). In our cohort of 18 mice, effective background signal suppression was obtained, except for fluids in the bladder, renal pelvis, and intestinal tract. Diffusion-weighted WB imaging with background signal suppression effectively visualised disseminated Ewing sarcoma growth in bones, retroperitoneal organs, and soft tissues, but not in lungs where susceptibility artefacts and respiratory motions cause signal loss (Wang *et al*, 2012). Sequential DWIBS demonstrated increases of tumour volumes over time (Figure 3A). Four tumours (three bone tumours, one kidney tumour) were visualised by DWIBS before they appeared in MR T2 sequences. To determine the sensitivity and specificity of DWIBS, standard T2-weighted sagittal MRI sequences were defined as standard. Interobserver agreement on the presence of individual tumours by DWIBS was 92%. Limited specificity of DWIBS was found for renal manifestations (Figure 3B), explained by signal artifacts in the vicinity of liquid-filled spaces. Tumours of the suprarenal gland were not detected by DWIBS, potentially owing to their close proximity to the diaphragm (Kwee *et al*, 2008). Moreover, DWIBS failed to detect the pelvic bone lesions detected on T2 MRI sequences in 3 of 13 examinations. Tumours undetectable by DWIBS were smaller than those reliably detected with both techniques (Figure 3C). All in all, these results demonstrate feasibility of detection of disseminated Ewing sarcoma growth in a small animal model using DWIBS sequences.

***In vivo* antitumour activity of G_{D2}-retargeted T cells against established tumour xenografts.** To demonstrate the therapeutic efficacy of adoptive T-cell transfer against disseminated tumour cells, further cohorts of mice were intravenously injected with 2×10^6 VH-64 cells/mouse, followed by four ($n = 5$) to six ($n = 4$) transfusions of 1×10^7 14.G2a-CD28 ζ gene-modified human G_{D2}-specific T cells (group A, $n = 9$). Control mice (group B, $n = 9$) received analogous injections of non-transduced T cells. Analytic end points were the number of mice developing tumour manifestations and the numbers and volumes of tumours at the individual sites. Two control mice failed to develop Ewing sarcomas. All mice with lung tumours also had extrapulmonary tumour manifestations. Abdominal tumours that in female mice potentially represent ovarian manifestations were found in 2 of 6 male and in 10 of 12 female mice. As these tumours could not be assigned to specific organs, they were excluded from the analysis.

The numbers of mice developing tumours and the numbers of tumours at extrapulmonary localisation sites were not noticeably different between treated and untreated mice (Figure 4A and B).

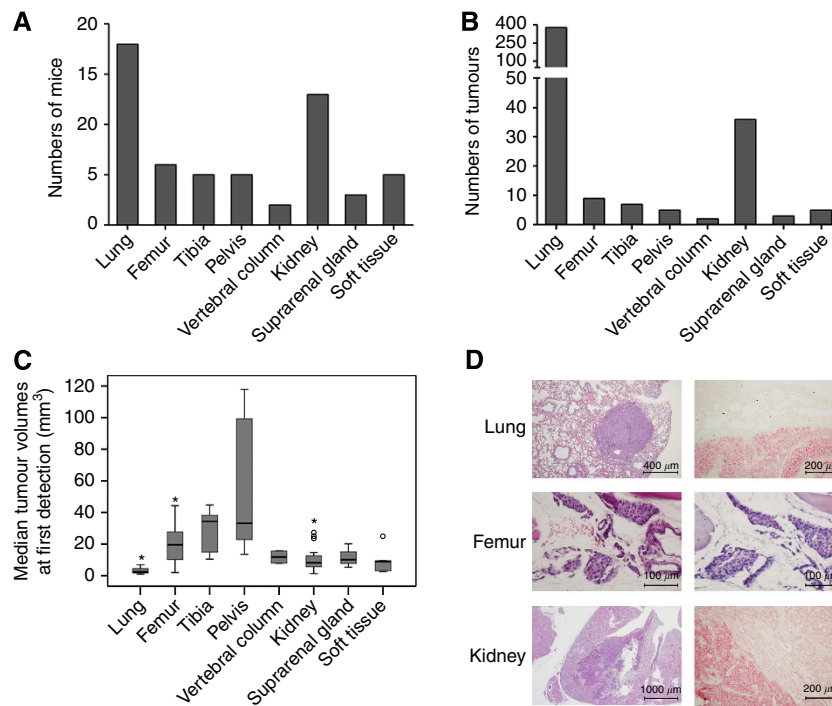


Figure 1. Visualisation of disseminated growth of Ewing sarcoma xenografts in mice by WB-MRI. VH-64 cells (2×10^6) were injected into the tail veins of 18 NOD/scid mice, followed by WB-MRI after 3 weeks, and then at weekly intervals. T2 axial sequences were used for detection of lung tumours, and T2 axial, sagittal, and STIR sequences were used for detection of manifestations at all other sites. **(A)** Numbers of mice developing detectable tumour manifestations at the indicated locations. **(B)** Total numbers of tumours per individual tumour site. **(C)** Boxplots of median tumour volumes at first detection at the various locations. The lines indicate the median sizes, and boxes represent the 25th and 75th percentiles. Circles symbolise outliers, asterisks show extreme values. **(D)** Light microscopy of haematoxylin and eosin (HE)-stained sections (left panel) and immunohistochemistry analysis by huCD99 staining (right panel) of tumours from the indicated organ and tissue sites. Altogether, the Ewing sarcoma origin was confirmed by histology and/or immunohistochemistry in four lungs with multiple lesions, five bone lesions (three in legs, two in pelvis and vertebral column, respectively), and four renal tumours.

Mice receiving gene-modified T-cell therapy had lower numbers of pulmonary tumours than control mice (Figure 4B). Soft tissue tumours at first detection had lower volumes in the treatment group (Figure 4C). Differences at further sites did not reach statistical significance. All tumour-engrafted mice in both groups had progressive disease over time (Figure 4D). For comparisons of tumour growth between the two groups, multivariable analysis according to a generalised linear-mixed model was performed to account for the complexity of the experimental system and to include the effects of time and localisation. For all localisations and TPs combined, the estimated tumour volume was reduced by 7.95 mm^3 in the treatment group, but the difference was not statistically noticeable ($P = 0.0965$; Table 1). As tumour localisation itself had a noticeable influence on tumour volume ($P < 0.0001$), we next compared tumour growth at individual localisations. At non-pulmonary sites, the maximum sizes of tumours over the entire follow-up were not noticeably different between mice receiving T-cell therapy and non-treated control mice, with the exception of reduced sizes of femoral and tibial bone tumours at the TP 4 ($P = 0.056$; $n = 7$ (A), $n = 2$ (B)). Noticeable differences between groups were identified for lung tumours (Figure 4E): Mice treated with G_{D2} -redirected T cells had a growth delay of lung tumours, with both lower numbers and smaller volumes (Figure 4B and E). No overall survival (as defined in the figure legend) advantage was found for mice receiving T-cell therapy using Kaplan–Meier analysis (Figure 4F). Thus, G_{D2} -retargeted T cells cannot completely prevent disseminated tumour growth in this systemic disease model, but are active to delay and reduce pulmonary disease manifestations.

DISCUSSION

Paediatric bone and soft tissue sarcomas tend to spread to and recur in lungs as well as in the bone and bone marrow. Multifocal disease is the hardest challenge to further improving cure rates. For the development of novel therapies and their clinical translation, *in vivo* preclinical models are needed that adequately mimic the dissemination pattern of these diseases and allow for non-invasive monitoring of tumour growth and response to treatment.

Here, we have established a small animal imaging model of systemic Ewing sarcoma growth using MRI techniques. Compared with the more broadly applied bioluminescence small animal imaging techniques, MRI directly reflects high resolution sarcoma staging in human patients and thus facilitates clinical translation of our findings.

Intravenous injection of human Ewing sarcoma cells into immunodeficient mice reliably established the disease in the majority of mice within < 5 weeks, confirming previous experience (Vormoor *et al*, 2001). Compared with the routine histology of specific organs and macroscopically affected tissues in deceased mice, sequential whole-body imaging allows more comprehensive detection of various tumour manifestations. Specifically, small tumours were detected at sites not included into routine examination in the previous study (Vormoor *et al*, 2001). Importantly, the non-invasive nature of MRI further allows for follow-up investigations of tumour growth, both during the natural course of the disease and upon therapeutic intervention. Indeed,

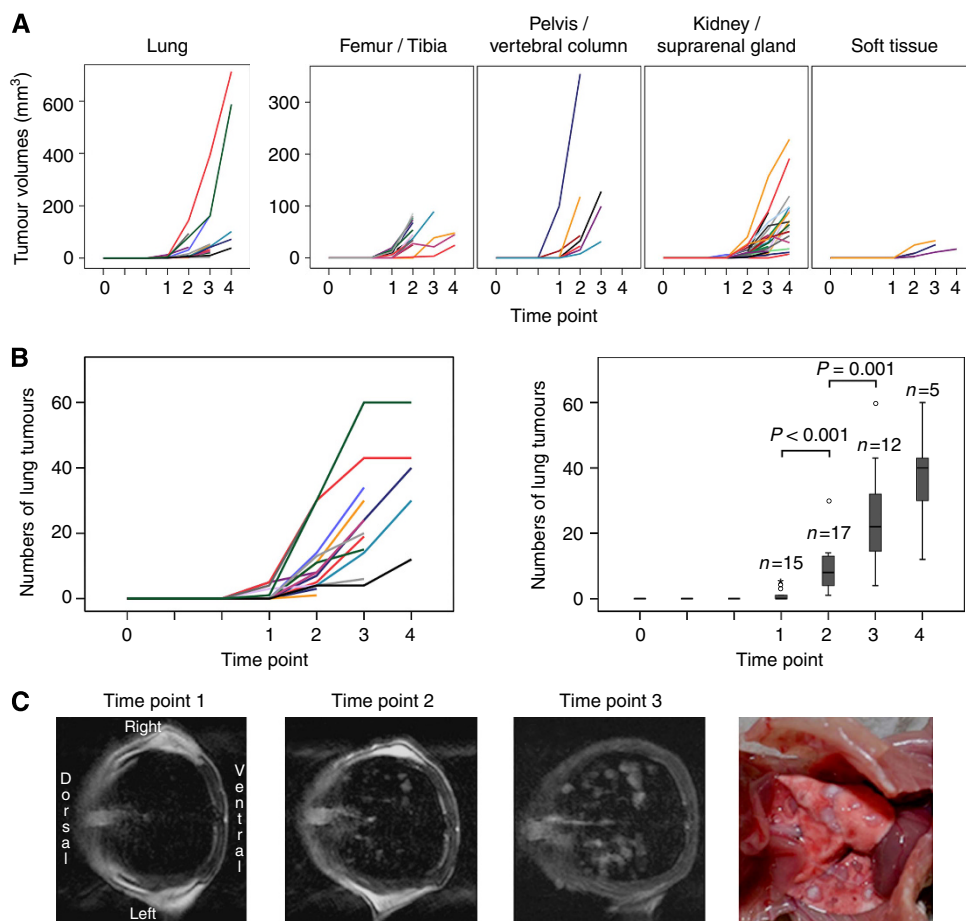


Figure 2. The kinetics of disseminated tumour growth in xenografted mice. **(A)** The volumes of individual tumours were determined in T2 axial (lung tumours) and T2 sagittal (all others) WB sequences in NOD/scid mice at time points 1, 2, 3, and 4. Extrapulmonary tumour manifestations were categorised by localisation to leg bones, skeletal trunk bones (pelvis, vertebral column), kidneys and/or suprarenal gland, and soft tissue. For lungs, each line corresponds to one mouse, as volumes of all tumour lesions were combined for each affected lung. For all other sites, each line reflects one individual tumour. Lung tumour volumes increased between TPs 1 and 2 ($P < 0.001$) and TPs 2 and 3 ($P < 0.001$). Femur/tibia tumours and pelvic tumours increased between TPs 1 and 2 ($P < 0.001$) and 2 and 3 ($P < 0.001$), and 3 and 4 ($P = 0.031$, respectively). Kidney tumours increased between TPs 1 and 2 ($P < 0.001$), 2 and 3 ($P < 0.001$), and 3 and 4 ($P < 0.001$). **(B)** Lung tumours were counted in T2 axial WB sequences in NOD/scid mice at TPs 1, 2, 3, and 4. Each line represents one mouse. In addition, boxplots represent the tumour number of the evaluable mice at each TP. Brackets represent statistically noticeable differences ($P \leq 0.05$) of the Wilcoxon-signed rank tests. Circles symbolise outliers; asterisks show extreme values. **(C)** Sequential MRI scans of one individual mouse demonstrate the progressive pulmonary involvement over time. The number and size of metastases that are detected as hyperintense manifestations in the dark lung in axial T2 images increases over time. Photodocumentation (to the right) of mice upon autopsy confirms the MRI findings, showing white-blueish metastases within the reddish lung tissue.

MRI provided a highly reproducible representation of clinical Ewing sarcoma development in mice and revealed systemic treatment efficacy of G_{D2} CAR gene-modified T cells. Our model is easy to apply and has translational potential within a wider scale for novel therapeutic developments against this malignant disease.

Besides their use in small animal models, non-invasive whole-body imaging tools are clinically needed for accurate tumour staging and assessment of treatment response. MRI is one of the most important diagnostic tools in the bone and soft tissue tumours where it provides excellent anatomical information (Lang *et al*, 1998a,b). Whole-body MRI is currently evaluated for the initial staging of patients with malignant solid tumours including Ewing sarcomas (Haubold-Reuter *et al*, 1993; Walker *et al*, 2000; Lauenstein *et al*, 2002). Its specific value lies within the early detection of bone and bone marrow disease (Eustace *et al*, 1997; Steinborn *et al*, 1999; Althoefer *et al*, 2001; Lauenstein *et al*, 2002; Hargaden *et al*, 2003; Ghanem *et al*, 2006). MRI further allows for volume-based assessment of response to cancer therapy. A limitation is that it does not assess the metabolic activity of

remaining tumour tissue. Diffusion-weighted MRI was introduced as a non-invasive technique providing functional information for both staging and response monitoring of solid tumours (Roth *et al*, 2004; Thoeny *et al*, 2005; Moffat *et al*, 2006; Schubert *et al*, 2006; Vandecaveye *et al*, 2009; Wang *et al*, 2009; Oka *et al*, 2010). In first preclinical studies in Ewing sarcomas, diffusion-weighted imaging effectively predicted early response of single subcutaneous tumours to chemotherapy in mice before the onset of morphological changes (Reichardt *et al*, 2009), and in a mouse model of ovarian cancer, DWIBS had the potential to detect peritoneal tumour dissemination (Lee *et al*, 2013). In pilot clinical studies, WB-MRI with DWIBS was found useful for detecting metastatic tumours especially in the bone (Nakanishi *et al*, 2007; Manenti *et al*, 2012; Sommer *et al*, 2012). Here, to the best of our knowledge, we are the first to demonstrate the feasibility of DWIBS for the staging of multifocal Ewing sarcoma in small animals. With the known limitation of DWIBS not detecting pulmonary metastases, the technique provided a rapid overview of extrapulmonary disease manifestations. The future value of the DWIBS technique in

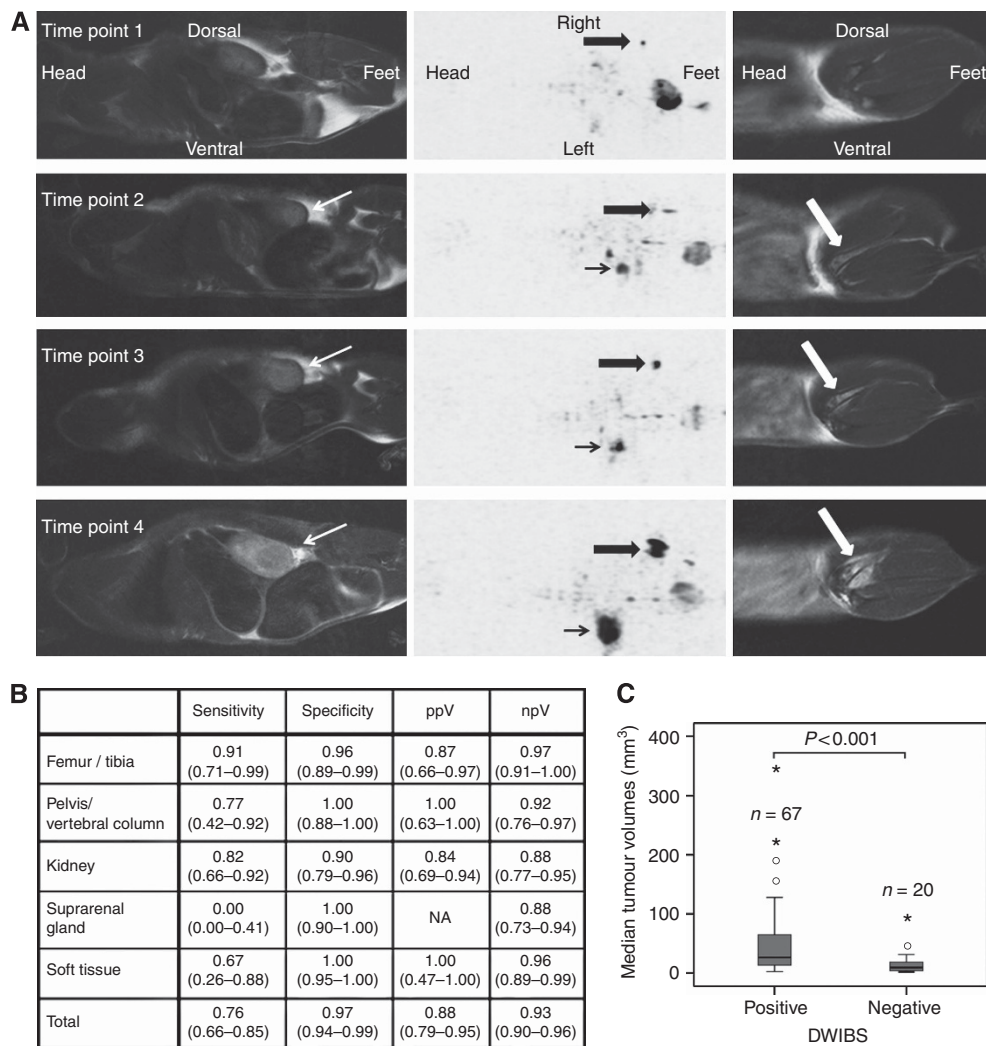


Figure 3. Whole-body MRI with DWIBS of Ewing sarcoma-engrafted mice. Sequential WB-MRI and DWIBS scans were performed in the cohort of 18 mice starting 3 weeks after tumour inoculation. **(A)** T2 sagittal MRI sequences (left and right panel) and DWIBS (central panel) images of a single mouse at sequential examinations performed 20–41 (TPs 1–4) days after tumour inoculation, as indicated. The left and right panels illustrate the growth of a kidney and a femur tumour, respectively. Images of DWIBS performed at the same time points demonstrate the two tumour manifestations in the femoral bone (larger arrow) and kidney (smaller arrow). T2 sagittal sequences were used to define the presence of tumour manifestations. The following regions were separately analysed for the presence or absence of tumours: right and left lower limbs, pelvic bones/vertebral column, left and right kidneys and suprarenal glands, and soft tissues. **(B)** Sensitivity, specificity, and positive (ppV) and negative predictive values (npV) of DWIBS were calculated for each localisation in comparison with standard T2 sagittal sequences. Numbers in brackets represent 95% confidence intervals. **(C)** Boxplots of median tumour volumes at all sites detectable and non-detectable by DWIBS, assessed by volumetry on T2 sagittal MR images. The bracket represents the result of the exact Mann–Whitney *U*-test. Circles symbolise outliers; asterisks show extreme values.

sarcoma staging may lie within providing complementary non-invasive functional tissue information for extrapulmonary sites of the disease, while avoiding exposure to ionising radiation.

Among novel experimental cancer therapies, adoptive transfer of T cells expressing recombinant antigen-specific CARs holds high promise. In patients with lymphoid malignancies, CAR-reengineered T cells mediated unequivocal clinical responses even against bulky tumours, functionally persisted *in vivo*, and established immunological memory (Kalos *et al*, 2011; Louis *et al*, 2011; Porter *et al*, 2011). However, results from individual clinical studies are variable (Brentjens *et al*, 2011; Kalos *et al*, 2011; Porter *et al*, 2011; Savoldo *et al*, 2011; Kochenderfer *et al*, 2012), and the reasons for the compelling activity of this therapy in some clinical studies but not in others are unclear. Besides the design of the individual CARs and the nature of their target antigen, host factors are thought to contribute to determining CAR treatment responses (Dudley *et al*, 2002). Although in our study, G_{D2} CAR

gene-modified T cells were not effective to prevent the disease, they had noticeable antitumour activity especially against pulmonary dissemination. Thus, our findings support further development and translational application of cellular therapies in Ewing sarcoma. A potential reason for the limited antitumour activity of the reengineered T cells is the high number of disseminated tumour cells present in the mouse organism at the time of T-cell transfer. Lower numbers of tumour cells reflecting minimal residual disease are more probably to be eradicated by this and other experimental interventions, but are also less reliable to engraft the disease in all mice. High-sensitivity imaging, as established here, may allow to detect tumour manifestations mediated by smaller numbers of tumour cells and mimic minimal disseminated disease more accurately than current models. To more adequately reflect the spectrum of local progression and organ and tissue dissemination of the disease, future experiments will include additional cell lines and low-passage cultures.

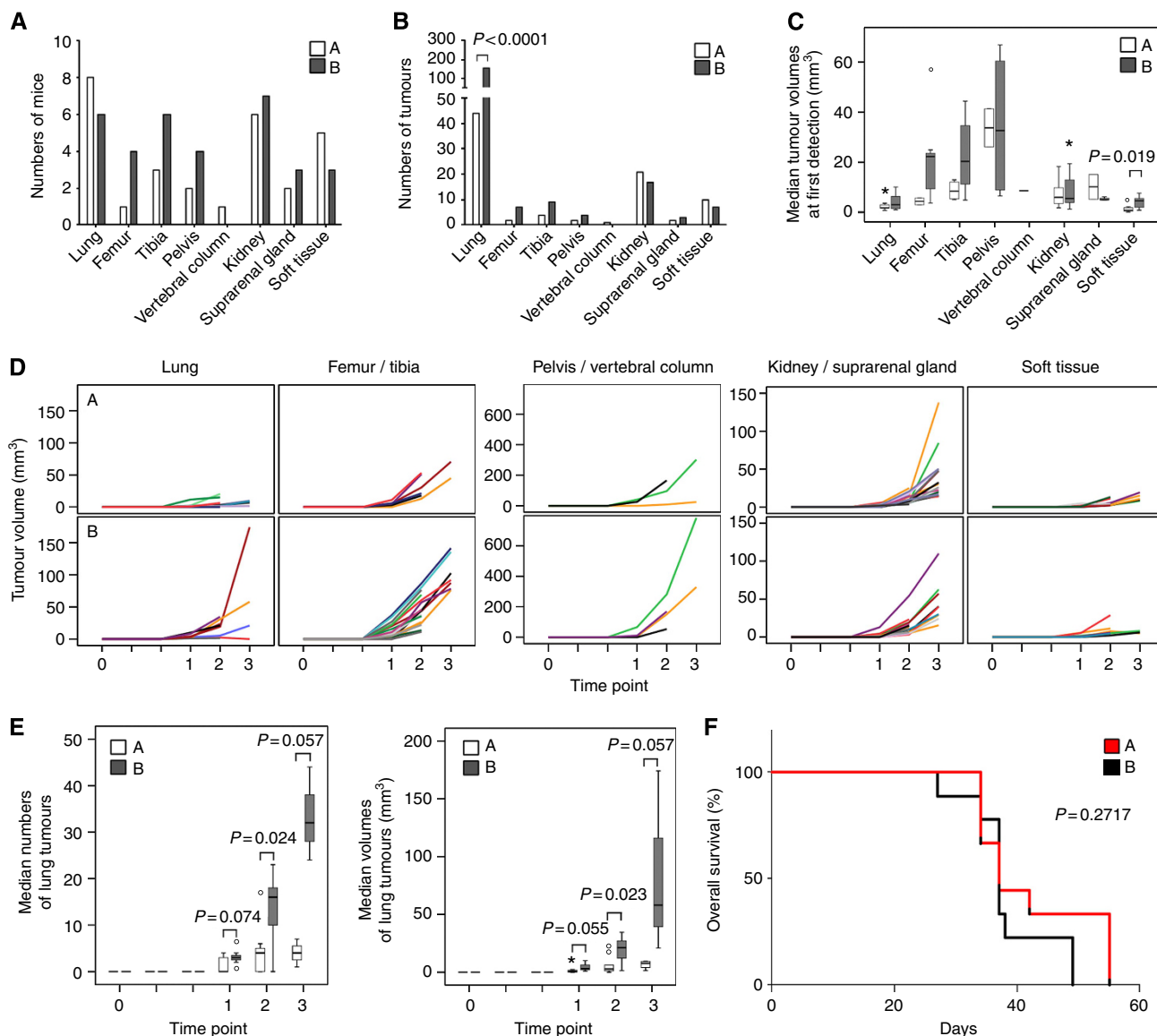


Figure 4. MRI documentation of *in vivo* activity of 14.G2a-28 ζ T cells against disseminated tumour xenografts. A cohort of nine mice were intravenously injected with 2×10^6 VH-64 cells per mouse, followed by intravenous transfer of 1×10^7 human 14.G2a-28 ζ gene-modified T cells (group A). Control mice ($n = 9$) received analogous injections of non-transduced T cells (group B). Mice were followed up by sequential T2 sagittal and axial, STIR and DWIBS WB-MRI scans. Tumour numbers were assessed at the time of termination. **(A)** Total numbers of mice of groups A and B with at least one tumour at indicated tumour sites. **(B)** Total numbers of tumours at the indicated tumour sites in groups A and B. The bracket represents a statistically highly noticeable result ($P \leq 0.01$) of the exact χ^2 -goodness-of-fit test. **(C)** Boxplots of median tumour volumes at first detection at the various locations in groups A and B. Brackets represent statistically noticeable differences ($P \leq 0.05$) between the groups determined by exact Mann–Whitney *U*-tests. **(D)** Growth of tumours at the individual sites in group A (upper panel) and group B (lower panel) over time. Volumes of lung tumours per mouse were combined and presented as the total lung tumour burden per mouse in mm^3 . For all other localisations, each line corresponds to one individual tumour. **(E)** Boxplots of median numbers (left panel) and volumes (right panel) of lung tumours at the indicated TPs. Brackets indicate differences between the groups determined by exact Mann–Whitney *U*-tests. At TPs 1 and 2, group A consisted of nine mice, and group B of seven mice. Owing to drop-out by termination or unexpected death during anaesthesia, the sizes of groups were reduced to $n = 4$ (group A) and $n = 3$ (group B) at TP 3. Circles symbolise outliers; asterisks show extreme values. **(F)** Kaplan–Meier curves of overall survival after tumour cell injection in groups A and B, and *P*-value of the log-rank test. Overall survival is defined by killing of the animals, as explained in the Materials and Methods section or by unexpected death of few animals during the anaesthesia.

The challenge now is to maximise the activity of the reengineered T cells, for example, by manipulation of costimulatory domains and optimal CAR design. Transfer of tumour antigen-specific T cells in the setting of advanced disease may be inadequate to control the disease. This is also supported by recently published *in vivo* experiments using T cells with native receptor specificity for EWS-FLI-1, which despite clear antitumour activity could not halt disease progression (Evans *et al*, 2012). Thus,

combined approaches with cytotoxic therapies may be more adequate to exploit the benefit of T-cell therapies. Moreover, recent insights into the components of the inflammatory microenvironment that contributes to local progression in Ewing sarcoma suggest that combinations with chemokine targeting may improve the efficacy of T-cell strategies (Berghuis *et al*, 2012). Although xenograft models carry limitations for immunological treatment manoeuvres as they do not completely represent the

Table 1. Analysis of tumour growth in a generalised linear-mixed model

| Parameter | Estimated volume (mm ³) (95% confidence limits) | P-value |
|---|---|----------|
| Group A vs B | -7.95 (-17.33 to 1.43) | P=0.0965 |
| Time (per day) | +1.44 (1.04 to 1.85) | P<0.0001 |
| Localisation (compared with kidney tumours) | | P<0.0001 |
| Lung | -2.03 (-15.76 to 11.69) | P=0.7707 |
| Femur/tibia | +11.06 (-1.84 to 23.95) | P=0.0925 |
| Pelvis/Vertebral column | +80.67 (61.52 to 99.83) | P<0.0001 |
| Suprarenal gland | -5.71 (-28.35 to 16.94) | P=0.6203 |
| Soft tissue | -7.32 (-20.94 to 6.29) | P=0.2905 |

Shown are estimates for tumour volume (mm³) with 95% confidence limits and P-values for the three parameters with influence on tumour volume: group, time, localisation. Owing to varying time points of follow-up scans, resulting in missing values and nested data structure, generalised linear-mixed models were fitted. The explanatory variables, such as group, time, and localisation, were modelled as fixed effects. The parameter identifying each mouse (compound symmetry covariance structure), time in days after tumour inoculation (spatial covariance structure) were modelled as random effects. Lesions were modelled as subject effect. The chosen underlying distributions were Gaussian, with identity as link function.

immunological *in vivo* complexity of interactions between host, tumour, and treatment, a comparative assessment of the antitumour activity of various constructs in our mouse model may help to choose the most promising constructs for clinical translation.

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CONFLICT OF INTEREST

HK is an employee of Philips Healthcare, the manufacturer of the MRI equipment used in this work. The remaining authors declare no conflicts of interest.

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