

Detecting chronic kidney disease by electrocardiography

Jeroen P. Kooman¹✉

Although chronic kidney disease (CKD) can be detected by relatively simple blood and urine tests, it remains underdiagnosed even in patients at high risk for the disease. Deep learning-based approaches are now being developed to detect CKD based on electrocardiogram (ECG) data.

Chronic kidney disease is a long-term condition involving abnormalities of kidney structure or function that can impact patients' health. The diagnosis requires either an estimated glomerular filtration rate (eGFR)—a measure of kidney function—below 60 ml/min/1.73 m², based on a prediction formula which includes serum creatinine levels, or the detection of markers of kidney damage, including the presence of albumin in urine (albuminuria). According to eGFR, CKD is subdivided into five different stages, with stage 5 indicating kidney failure. CKD is estimated to be the 12th leading cause of death worldwide. The global prevalence is estimated to exceed 800 million cases¹. Changes in lifestyle factors and early treatment with angiotensin-converting enzyme inhibitors or angiotensin receptor blockers can delay progression of CKD as well as cardiovascular disease². Nevertheless, many patients with CKD remain undetected, even those with risk factors such as hypertension².

In an article now published in *Communications Medicine*, Holmstrom et al. describe a potential screening approach using a convolutional neural network-based deep learning model to detect CKD from ECG waveforms³. Deep learning is a type of machine learning-based artificial intelligence inspired by the human brain, whereby multiple layers of algorithms called convolutional neural networks learn from unstructured data to perform classification or prediction tasks.

The model developed by Holmstrom et al., and similar recently developed approaches⁴, are exciting advances which, if further validated and implemented in the clinic, have the potential to improve detection of patients with CKD using data routinely acquired for other purposes. Here, the findings and clinical implications of the study by Holmstrom et al. are discussed, along with similar studies.

The primary cohort studied by Holmstrom et al. consisted of 111,370 patients and included 247,655 ECGs, of which 100,233 were randomly allocated to the training set and 11,137 to the test set. The model achieved an accuracy of 0.767 in the primary cohort and 0.709 in an external validation cohort. Accuracy was higher with more advanced stages of CKD and in younger patients. This might be explained by the fact that on one hand, ECG alterations are more likely to be prevalent in patients with more advanced CKD, whereas in younger patients, ECG abnormalities due to causes other than CKD are less prevalent.

The definition of CKD was based on ICD-9/10 codes, identifying 7816 patients with a diagnosis of CKD in the primary cohort who had an ECG taken within a 1-year window of a CKD diagnosis. Aside from this relatively long time window, which is of potential relevance because renal function may significantly change over this time period, an important limitation of the study is that data on eGFR were available in only 49% of patients at any point in time. Thus, in 51% of cases, diagnosis only appeared to be dependent on the ICD-9 definition and no connection with the level of kidney function impairment could be made. Moreover, it cannot be excluded that in the population without an ICD-9 diagnosis of CKD, renal impairment might

¹Department of Internal Medicine, Division of Nephrology, Maastricht University Medical Centre, Maastricht, The Netherlands. ✉email: jeroen.kooman@mumc.nl

still be prevalent given the fact that CKD is underdiagnosed in the general population. The cohort might also not be representative of the general population, given the relatively high prevalence of end stage kidney failure (2.6%) and because the indication to perform an ECG by itself will introduce selection bias, as the prevalence of CKD is higher in patients with cardiovascular disease. Still, despite these limitations, the fact that model performance was similar in the population in which data on eGFR or albuminuria were present, the consistency of the model performance in different subgroups and comparable performance in the external validation cohort provides confidence that the reported data are sufficiently robust.

Subclinical cardiac abnormalities, such as myocardial fibrosis and left ventricular hypertrophy, are frequently present in patients with kidney dysfunction, even if it is mild⁵. In a population-based cohort, reduced eGFR and albuminuria were associated with an increase in the cardiac biomarkers troponin T and I indicating cardiac damage⁶. In the same cohort, changes in these cardiac biomarkers were associated with ECG alterations suggestive of cardiac damage⁷. In more advanced stages of CKD, ECG abnormalities were also related to cardiovascular mortality⁸. The ability of deep learning models to detect CKD based on ECG changes is therefore likely explained by the high prevalence of these subclinical abnormalities, which result in subtle changes that can remain undetected on routine ECG interpretation. In the study by Holmstrom et al., ECG changes identified to be associated with CKD were primarily observed in the QRS complex and PR interval.

An important possible confounder in the interpretation of ECG changes in patients with CKD are abnormalities in serum potassium. Deep learning models based on ECG interpretation have been validated for the detection of hyperkalemia⁹, and can be predictive of other electrolyte imbalances¹⁰. While detailed data on electrolytes were not available in the study of Holmstrom et al., the accuracy of the model was similar in patients with and without hyperkalemia in the subgroup where potassium levels were available, which suggest that variations in potassium levels did not have a major influence on the detection of CKD by the model.

In support of the present study, another study by Kwon et al. also assessed the prediction of CKD by ECG analysis using a deep learning model based on convolutional neural networks⁴. In that study, the model was trained to detect an eGFR level of <45 ml/min/1.73 m² (i.e. stage 3B or higher). Accuracy of the model was higher in the study of Kwon et al., which might be due to the fact that data on eGFR were available for all patients or that only patients with a more pronounced decline in renal function were included, with demographic features also included in the model. This study did not, however, evaluate the detection of earlier stage CKD, such as stage 3A disease that is less severe but nevertheless still associated with increased cardiovascular mortality.

Machine learning models based on ECG analysis have also been used in the detection of various types of heart failure, as well as other chronic diseases such as diabetes mellitus¹¹. As in CKD, left ventricular hypertrophy and myocardial fibrosis are also common in patients with diabetes and might induce comparable ECG changes. As detailed data on (pre)diabetic status and blood pressure control were missing in the study by Holmstrom et al., the question remains to which extent the model in the study is specific for CKD. As the relation between ECG changes and CKD is likely mediated by subclinical cardiac injury, it may also miss patients with CKD without cardiac damage. However, although this needs to be addressed in future studies, the model may indicate those patients with CKD who are at higher risk for adverse cardiovascular outcomes. Interestingly, in a study where a deep learning model was applied to predict

hypo- or hyperkalemia from ECGs, the risk of mortality was higher in those patients where the model indicated abnormalities in serum potassium as compared to laboratory values¹². This is also relevant for patients with CKD, given the increased prevalence of hyperkalemia and the associated mortality risk in these patients.

Both in the study of Holmstrom et al. as in the study by Kwon et al.⁴, analysis of single lead (I)-ECG resulted in a comparable model performance as compared to the 12-lead ECG. Twelve-lead ECG provide a far more complete of the heart's electrical activity compared to a single-lead ECG, but is not available in a wearable format. Their comparable performance in this study is of relevance since some newer generation smartwatches are able to perform single lead (I) ECG measurements¹³, which suggests it might one day be possible to detect CKD with a smartwatch in the general population.

At present, given the relatively low sensitivity and specificity, detection of CKD by ECG features alone might not be suitable for widespread implementation as a screening method. However, predictive power may be improved by addition of data from other sources. Recently, it was shown that a machine learning model based on physiological measurements from wearable devices was able to predict to some extent laboratory parameters including blood urea nitrogen¹⁴. Artificial intelligence models that process more granular data from different sources, including ECGs, might be useful as prescreening tools¹⁵. These could be followed by more detailed measurements of health status, including blood pressure, and measurements of glucose, renal function and albuminuria.

The remaining question is how, with further validation, the models developed by Holmstrom et al. and Kwon et al. could find their way into future clinical practice. A relatively straightforward way would be to incorporate the model into automated analysis of 12-lead ECG, indicating the need for further analysis in a patient identified at risk of CKD. As ECGs are generally performed for a specific reason, patients have already entered the healthcare system and adding another analysis step might not be too difficult, providing patients have provided consent for this. A different scenario is the one described above, in which data from wearable devices, which may include single lead ECG measurements, are used to identify persons at risk in a general population. In this case, the number of false positive cases is likely high and may be associated with health anxiety and a larger demand on the healthcare system. Moreover, there may be concerns with digital and societal equity as smart wearables may have substantial costs and therefore not be accessible for all socioeconomic groups. For smartwatch-based detection of atrial fibrillation, various ethical and data privacy concerns have also been raised, such as underrepresentation of minority groups in the training data and storage of medical data by commercial parties¹⁶.

In conclusion, the application of deep learning to detect CKD based on ECG data, as proposed by Holmstrom et al., is an interesting application of a widely used technology will need to be followed by additional validation studies, which should consider integration of different data types. These studies should be performed both in high-risk patients as well as in population-based cohorts, and in patients of different sexes or genders, ethnicities and from different geographical locations. As CKD, even in high-risk populations such as patients with hypertension, remains underdiagnosed, new methods such as the one described in *Communications Medicine* may be a welcome aid by prompting the subsequent use of conventional screening tools. However, even with successful validation, applying these tools on a population basis using wearable sensors would introduce additional ethical, societal, and regulatory challenges that would need to be carefully considered.

Received: 13 April 2023; Accepted: 15 May 2023;
Published online: 26 May 2023

References

1. Kovesdy, C. P. Epidemiology of chronic kidney disease: an update 2022. *Kidney Int. Suppl.* **12**, 7–11 (2022).
2. Shlipak, M. G. et al. The case for early identification and intervention of chronic kidney disease: conclusions from a Kidney Disease: Improving Global Outcomes (KDIGO) Controversies Conference. *Kidney Int.* **99**, 34–47 (2021).
3. Holmstrom, L. et al. Deep learning-based electrocardiographic screening for chronic kidney disease. *Commun. Med.* **3**, <https://doi.org/10.1038/s43856-023-00278-w> (2023).
4. Kwon, J. M. et al. Artificial intelligence assessment for early detection and prediction of renal impairment using electrocardiography. *Int. Urol. Nephrol.* **54**, 2733–2744 (2022).
5. Edwards, N. C. et al. Diffuse interstitial fibrosis and myocardial dysfunction in early chronic kidney disease. *Am. J. Cardiol.* **115**, 1311–1317 (2015).
6. Martens, R. J. et al. Estimated glomerular filtration rate and albuminuria are associated with biomarkers of cardiac injury in a population-based cohort study: the Maastricht study. *Clin. Chem.* **63**, 887–897 (2017).
7. Kimenai, D. M. et al. Troponin I and T in relation to cardiac injury detected with electrocardiography in a population-based cohort - The Maastricht Study. *Sci. Rep.* **7**, 6610 (2017).
8. Deo, R. et al. Electrocardiographic measures and prediction of cardiovascular and noncardiovascular death in CKD. *J. Am. Soc. Nephrol.* **27**, 559–569 (2016).
9. Galloway, C. D. et al. Development and validation of a deep-learning model to screen for hyperkalemia from the electrocardiogram. *JAMA Cardiol.* **4**, 428–436 (2019).
10. Kwon, J. M. et al. Artificial intelligence for detecting electrolyte imbalance using electrocardiography. *Ann. Noninvasive Electrocardiol.* **26**, e12839 (2021).
11. Kulkarni, A. R. et al. Machine-learning algorithm to non-invasively detect diabetes and pre-diabetes from electrocardiogram. *BMJ Innovations* **9**, 32–42 (2023).
12. Lin, C. et al. Point-of-care artificial intelligence-enabled ECG for dyskalemia: a retrospective cohort analysis for accuracy and outcome prediction. *NPJ Digit. Med.* **5**, 8 (2022).
13. Peppinkhuizen, S. et al. Accuracy and clinical relevance of the single-lead Apple Watch electrocardiogram to identify atrial fibrillation. *Cardiovasc. Digit. Health J.* **3**, S17–S22 (2022).
14. Dunn, J. et al. Wearable sensors enable personalized predictions of clinical laboratory measurements. *Nat. Med.* **27**, 1105–1112 (2021).
15. Acosta, J. N., Falcone, G. J., Rajpurkar, P. & Topol, E. J. Multimodal biomedical AI. *Nat. Med.* **28**, 1773–1784 (2022).
16. Predel, C. & Steger, F. Ethical challenges with smartwatch-based screening for atrial fibrillation: putting users at risk for marketing purposes? *Front. Cardiovasc. Med.* **7**, 615927 (2020).

Competing interests

The author declares no competing interests.

Additional information

Correspondence and requests for materials should be addressed to Jeroen P. Kooman.

Reprints and permission information is available at <http://www.nature.com/reprints>

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons license, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons license and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this license, visit <http://creativecommons.org/licenses/by/4.0/>.

© The Author(s) 2023