

Polyethylene Glycol-Surfactant for Lavage Lung Injury in Rats

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ABSTRACT

Addition of ionic and nonionic water-soluble polymers to pulmonary surfactants in the presence of inactivating substances prevents surfactant inactivation *in vitro* and improves lung function in several models of lung injury. However, a recent report found opposite effects when surfactant plus polyethylene glycol (PEG) was used to treat lung injury caused by saline lung lavage. Therefore, we examined the reasons why the polymer effect is less evident in the saline lung lavage lung injury model. We treated rats with lavage lung injury with a commercial lung surfactant extract derived from bovine lung (Survanta) with or without addition of PEG. Groups treated with Survanta + PEG had significantly higher static post mortem lung volumes than groups treated with Survanta. However, groups treated with Survanta + PEG had more tracheal fluid and no significant

benefit in arterial oxygenation compared with the group treated with Survanta, despite our use of measures to reduce pulmonary edema. Measurements after intravascular injections of ¹²⁵I-labeled albumin confirmed that addition of PEG increased extravascular lung water and that this effect is mitigated by furosemide. We conclude that surfactant + PEG mixtures are less effective in lavage injury than in other forms of lung injury because of increased extravascular lung water. (*Pediatr Res* 58: 913–918, 2005)

Abbreviations

ALI, acute lung injury
ARDS, acute respiratory distress syndrome
PEEP, positive end-expiratory pressure
PEG, polyethylene glycol

ALI results from a variety of insults as diverse as meconium aspiration in newborns, hydrochloric acid reflux, sepsis, and ventilator trauma. In turn, injury predisposes the patient to acute (or adult) respiratory distress syndrome (ARDS) (1–4). Pulmonary surfactant replacement, now a mainstay in the treatment of respiratory distress syndrome in premature infants, has not enjoyed comparable success in treating ARDS (5–7). Inadequate dosage or distribution, and inactivation of surfactant have been postulated for its poor performance in treating these injuries (8–11).

Multiple reports indicate improved surfactant function when polymers such as dextrans, PEG, and hyaluronan are added to surfactant preparations *in vitro* (12–15). Animals with ALI have improved lung function when treated with surfactant polymer mixtures *versus* surfactant alone. Lu *et al.* (16–18)

found that adult rats receiving surfactant + PEG, dextran, or hyaluronan mixtures have better gas exchange, pulmonary mechanics, and histologic appearance of the lungs when compared with rats treated with Survanta (beractant) alone after HCl-, meconium-, and endotoxin-induced lung injuries. Kobayashi *et al.* (19,20) have shown that addition of dextran to surfactant improves responses in two additional lung injury models (albumin inhibition in immature rabbits and acid milk aspiration in rats).

The specific model used to induce ALI, however, may affect treatment responses to surfactant and surfactant + PEG, as different models of lung injury produce different alveolar environments. A lavage model of lung injury, for example, removes variable amounts of alveolar surfactant (21), whereas a meconium model of lung injury inactivates but does not remove surfactant. Puligandla *et al.* (22) have demonstrated the varied effects of different lung injury models on the properties of exogenous surfactants, noting differences in large aggregate pool sizes, surface activity, and alterations in phospholipid and protein content in recovered exogenous surfactant.

Providing an illustration of this point, a recent study by Campbell *et al.* (23) of lavage-injured adult rabbits has produced results inconsistent with the positive results seen with

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PEG in a different lung injury model. Animals treated with surfactant + PEG in their study exhibited more hypoxemia, lower lung compliance, and hypercapnia when compared with animals receiving only surfactant. Why addition of polymers to surfactants improved responses after meconium, endotoxin, HCl, and albumin-immaturity injuries but worsened responses in lavage injury is not clear. Our initial hypothesis, like that of Campbell *et al.*, was that PEG surfactant mixtures would improve lung mechanics and gas exchange in a lavage model of lung injury. When we found results that were less dramatic than we had found using this treatment in other lung injuries, we tested whether the suboptimal effects were associated with increased lung water that could be attributable to the osmolality of the added PEG.

METHODS

The animal protocol used was approved by the committee on animal research at the University of California–San Francisco. The general design of these experiments was to anesthetize and paralyze adult rats, create lung injury by saline lung lavage until target Po_2 values were achieved, administer furosemide, then treat the rats with different doses of Survanta or Survanta + PEG. The seven experimental groups consisted of no treatment ($n = 3$), Survanta 20 mg/kg \pm PEG (10 kD, 5% wt/vol), Survanta 25 mg/kg \pm PEG, and Survanta 50 mg/kg \pm PEG (treatment groups: $n = 6$ –7). With results of these experiments in hand, using a slightly modified protocol, we studied the specific effects of PEG and furosemide on extravascular lung water and capillary leak using ^{125}I -labeled albumin as a marker.

Lavage procedure. We chose to use rats for these experiments based on our extensive experience with lung injuries in this species (16,18). After randomization, white adult male Sprague-Dawley rats weighing 267–411 g were anesthetized by intraperitoneal injection of 100 mg/kg pentobarbital at 50 mg/mL. After tracheostomy, the rats were supported on a Harvard volume-controlled ventilator (Harvard small rodent ventilator, model 683; Harvard Apparatus, South Natick, MA) with initial settings of frequency = 40 breaths/min, tidal volume = 9 mL/kg body weight, PEEP = 4 cm water, $\text{Fio}_2 = 1.0$, and flow rate = 0.5 L/min. The right carotid artery was catheterized for monitoring of systemic arterial blood pressure, collection of blood gas samples, and drug and fluid administration. Systemic arterial blood pressure and tracheal pressure measurements were recorded every 30 min throughout the experiment. Rats with a systemic blood pressure <100 mm Hg after 30 min on the ventilator were observed for an additional 45 min and removed from the study if the blood pressure remained <100 mm Hg. The carotid catheter was flushed with a 10 units heparin/mL normal saline solution after arterial blood gas collection and drug administration. Blood pressure and tracheal pressures were measured using Viggo-Spectromed transducers (Gould model P23XL) attached to a recorder (Gould Windowgraf, Gould, Valley View, OH).

Intra-arterial pancuronium (1 mg/kg) was administered at the start of the experiment (18), and 0.5 mg/kg was given every hour. Intra-arterial pentobarbital (7 mg/mL) was given in 0.1 mL increments throughout the experiment to maintain systolic blood pressure <125 mm Hg and for response to skin pinch. The rats were maintained under an overhead heat lamp (50 W) with measurements of rectal temperature (Digi-Sense, Cole-Parmer, Vernon Hills, IL). A baseline arterial blood gas was recorded 15 min after placement on the ventilator and every 10–15 min thereafter until stable values were obtained (target $\text{Pco}_2 = 35$ –50 mm Hg). The respiratory frequency was adjusted by five breaths per minute every 15 min to maintain Pco_2 within the desired limits. Rats for which we could not achieve stable Pco_2 s after three respiratory rate changes were excluded from the study.

Thirty minutes after placement on the ventilator, tracheal lavage with 0.9% NaCl at 37°C was carried out by disconnecting the animals from the ventilator and carrying out the lavage procedure. Rats were lavaged three times with 10 mL/kg per lavage. The chest was compressed twice and the rats were reconnected to the ventilator for 5–10 s and aspirated lavage fluid volume was recorded. This procedure was carried out an additional five times. PEEP was increased to 8 cm H_2O and maintained at that level for the duration of the experiment. The rats were then placed back on the ventilator for 5 min and placed on their sides if hypotension occurred (blood pressure <75 mm Hg) to decompress the great vessels. Blood and tracheal pressures were recorded immediately before and after each lavage series. Five minutes after the sixth lavage procedure, an arterial blood gas was obtained. If the blood gas revealed a $\text{Po}_2 > 100$ mm Hg (which was rare), the rats were subjected to additional lavage procedures until a $\text{Po}_2 < 100$ mm Hg was obtained (24).

Thirty minutes after the last lavage, an arterial blood gas was recorded and 10 mg/kg of intra-arterial furosemide (10 mg/mL) was administered. We use diuretic for several reasons: we used it in our meconium lung injury model adapted from the work of Sun *et al.* (25), and we thought it especially relevant to include with the wet lung injury produced by lavage. If the osmotic effects of PEG are important *in vivo*, then inclusion of diuretic could be relevant to eventual clinical use. Thirty minutes later, another arterial blood gas was recorded and treatment was given. Treatment consisted of Survanta at 20, 25, or 50 mg/kg. The stock 25 mg/mL Survanta solution was diluted to a treatment volume of 4 mL/kg with 0.45% NaCl and mixed by Vortex for 30 s (Fisher Vortex, model G-560; Fisher Scientific, Pittsburgh, PA). Survanta was supplied by Ross Laboratories (Columbus, OH). Surface tension of the Survanta was tested in a modified pulsating bubble surfactometer (Electronics, Buffalo, NY) at a concentration of 1.25 mg/mL. Minimal surface tension in the pulsating bubble surfactometer was assessed at 37°C on the 10th cycle and in all cases was <10 mN/m. PEG (molecular weight, 10 kD; Lot 115H26011) was obtained from Sigma Chemical Co. (St. Louis, MO) as dry crystalline flakes. Dry PEG (5% wt/vol) was added to the diluted treatment mixtures and mixed by Vortex. The treatment mixture was instilled into the trachea, with half the dose given while the rats were on each side. Control rats received no treatment. Arterial blood gases were recorded 30 and 60 min after treatment, then hourly until the end of the experiment. Tracheal fluid was aspirated with a 3-mL syringe attached to a PE 50 catheter introduced into the tracheal tube to the level of the carina (16) 1 h after treatment and hourly thereafter.

Volume of tracheal fluid was measured and the fluid assayed for total protein using the Bradford protein assay (26). Survanta + PEG samples were compared with a standard curve constructed with 5% PEG and bovine albumin (lyophilized BSA, #68530A; Bio-Rad, Hercules, CA). Control and Survanta samples were compared with standard curves constructed with bovine albumin alone.

Three hours after treatment, intra-arterial pentobarbital (33 mg/kg) was administered and the trachea was clamped. Twenty minutes after pentobarbital administration, the abdomen and diaphragm were opened widely. Adequate degassing of the lungs was confirmed by the appearance of maroon-colored (airless) lungs. Lungs from rats who died before the end of the experiment or whose lungs did not appear airless were degassed in a bell jar connected to a vacuum pump (Maxima Vacuum, Model D8A, Fisher Scientific).

Deflation pressure-volume measurements. Postmortem quasi-static deflation pressure-volume measurements on open-chested animals were performed by inflating the lungs to a pressure of 35 cm H_2O using a 20-mL syringe. After a 30-s period of stabilization, volume was measured to define total lung capacity. Pressure was reduced in steps of 5 cm H_2O with at least a 10-s stabilization period at each step, and the corresponding volumes were measured. Volume was corrected for compression in the dead space of the apparatus and expressed as milliliters per kilogram of body weight (16).

Histology. After the standardized lung inflation for pressure-volume measurements, lungs were removed and weighed, and a mid-sagittal slice of the left lung was fixed in 4% formaldehyde, embedded in paraffin, and stained with hematoxylin and eosin. The sections were coded so that the specimens were graded by two investigators without knowledge of the experimental groupings. The sections were examined by light microscopy and assessed for the presence of hemorrhage, atelectasis, and leukocytes. Each characteristic was scored 0 to 3 (0 = absent; 1 = mild; 2 = moderate; 3 = prominent). Scores by the two observers did not differ by more than 15%.

Electron microscopy. Transmission electron microscopy was performed on Survanta with or without 5% PEG. Pellets (10,000 rpm, 1 h) of Survanta or Survanta + PEG were fixed in 2% glutaraldehyde, 1% OsO_4 in 0.1M cacodylate buffer (pH 7.4) for 24 h at 4°C. The samples were further stabilized and stained *en bloc* in 2% aqueous uranyl acetate for 48 h. The pellets were dehydrated quickly in cold acetone, brought to room temperature in 100% acetone, then slowly infiltrated with increasing concentrations of LX 112 (Ladd Research Industries, Burlington, VT), left overnight in 100% LX 112, and finally embedded. Thin sections were cut and stained with 5% uranyl acetate and 0.8% lead citrate, then examined in a Zeiss 10 transmission electron microscope (Carl Zeiss, Thornwood, NY).

Lung water experiments. An additional series of animals was studied to assess the effects of PEG added to surfactant and/or furosemide on pulmonary edema (excess extravascular lung water in milliliters) measured by the gravimetric method, and endothelial permeability to albumin measured by extravasation of vascular ^{125}I -labeled albumin (27). Rats were prepared and given lung injury as described above, but the lavage was standardized to give five lavages of 30 mL/kg body weight. Six experimental groups ($n = 3$) were studied consisting of 1) uninjured and untreated (U, U); 2) uninjured and PEG (U, P); 3) Survanta 25 mg/kg and furosemide after injury (I, S, F); 4) Survanta 25 mg/kg with PEG and furosemide after injury (I, S, P, F); 5) Survanta 25 mg/kg with PEG after injury (I, S, P); and 6) injury and PEG (I, P). In these experiments, Survanta was diluted to the appropriate concentration with 0.9% NaCl (not 0.45% NaCl as used in the initial experiments). At the time of

treatment, 1 μ C of 125 I-labeled albumin in 1 mL saline was injected into the artery, with blood samples taken at 5 min, 1 h, and 2 h thereafter. At the end of the experiment, the lungs were removed and weighed. 125 I counts per minute, Hb, and wet/dry weights were obtained on lung homogenates, and excess lung water was calculated by the gravimetric method. No aspiration of tracheal fluid was done in these experiments.

Extravascular plasma equivalents (EVPE) were measured by the following formula:

$$\text{EVPE} = [C_H - (C_{\text{pend}} \times Q_B)]/C_{\text{Pave}}$$

where, EVPE = μ l/g dry lung weight; C_H = counts per min/g in the homogenized lung; C_{pend} = the count per min/g in plasma samples at the end of the experiment; Q_B = the blood volume in the lungs determined by the gravimetric method; and C_{Pave} = the average counts per min/g in the plasma samples collected at 5 min, 1 h, and 2 h.

Analyses. Data are expressed as mean \pm SEM. Serial measurements were analyzed by two-way ANOVA modified for repeated measures using Sigma-Stat software (SPSS Science, Chicago, IL). Univariate analyses were done for nonserial data and differences were compared using the *t* test, with $p < 0.05$ considered statistically significant.

RESULTS

General findings. Four of the 40 rats randomized in the initial study died during the experiment (1 from the Survanta 25 mg/kg group, 1 from the Survanta 25 mg/kg + PEG group, and 2 from the Survanta 50 mg/kg + PEG group). The number of lavages ranged between seven and nine per rat, with 88–91% of the lavage fluid recovered (no statistically significant differences among groups). There were no significant differences between groups treated with Survanta or Survanta + PEG with regard to blood pressure, peak inspiratory pressures, body weight, fluid administration, rectal temperature, or urinary output. No significant differences existed between Survanta and Survanta + PEG for pretreatment pH, P_{CO_2} , P_{O_2} , or base deficit.

Oxygenation. Average values for arterial oxygenation for the various groups are shown in Figure 1. A significant dose response was noted only when the 25 and 50 mg/kg groups were compared with the 20 mg/kg group. There were no significant differences between Survanta and Survanta + PEG group at any dose. Average oxygenation for groups treated with Survanta or Survanta + PEG was significantly better than oxygenation for the control (untreated) group.

Pressure-volume relationships. In general, pressure-volume measurements indicated that lung volumes were higher in the groups treated with Survanta + PEG. Pressure-volume curves were significantly improved for Survanta + PEG groups (50 and 25 mg/kg) but not for 20 mg/kg when compared with

Survanta alone (ANOVA for repeated measures) (Fig. 2). Pressure-volume curves were significantly left-shifted for the Survanta 50 mg/kg + PEG group when compared with the Survanta 25 mg/kg + PEG group ($p = 0.025$) and the 20 mg/kg + PEG group ($p < 0.001$).

Histology. In control animals, lavage injury was similar to that reported by Berggren *et al.* (28), with atelectasis and an influx of white and red cells. Significantly reduced scores ($p < 0.05$) for atelectasis and presence of white and red blood cells were found as the dose of Survanta was increased from 20 or 25 mg/kg to 50 mg/kg. There was no difference for any histologic variable between Survanta and Survanta + PEG groups at corresponding doses.

Lung water and capillary leak. The Survanta + PEG groups had greater volumes of tracheal fluid recovered in the 3 h after treatment at each dose when compared with Survanta groups ($p < 0.01$ for all three groups) (Fig. 3). Less tracheal fluid was obtained from animals treated with 50 and 25 mg/kg Survanta + PEG than from those treated with 20 mg/kg Survanta + PEG ($p < 0.05$).

Protein concentrations of the tracheal fluids were significantly higher in the Survanta 20 mg/kg group than the Survanta 20, 25, and 50 mg/kg + PEG groups ($p < 0.01$) (Fig. 4). There was no difference in protein concentration among the three Survanta + PEG groups. Since no tracheal fluid was recovered from Survanta 25 mg/kg or Survanta 50 mg/kg animals, protein measurements were not possible for these groups.

Wet lung weights (expressed as a percentage of body weight) appeared higher in all Survanta + PEG groups when compared with the corresponding Survanta groups, but differences were not significant. When the volume of tracheal aspirate recovered from each rat was added to the wet lung weight (and expressed as a percentage of body weight), all Survanta + PEG groups had significantly higher lung weight/body weight ratios than the corresponding Survanta groups ($p < 0.01$ for all groups).

Results from experiments designed specifically to study capillary leak are shown in Figure 5. Excess extravascular lung water (EELW) was significantly increased when injured animals receiving furosemide were treated with Survanta + PEG or PEG and were compared with Survanta (Fig. 5A). Furosemide significantly diminished the amount of lung water in the Survanta + PEG group (Fig. 5A). Wet/dry ratios are

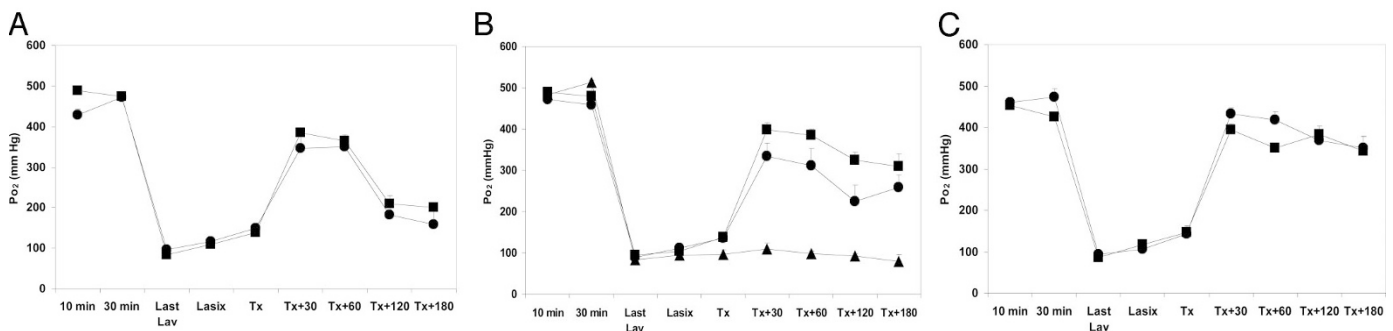


Figure 1. Comparisons of mean P_{O_2} values between Survanta (circles) and Survanta + PEG (squares) at (A) 20, (B) 25, and (C) 50 mg/kg ($n = 6$ –7/treatment group). No significant differences between Survanta and Survanta + PEG at any dose are found (Lasix = furosemide). Triangles in B represent the means for the control (untreated) group ($n = 3$).

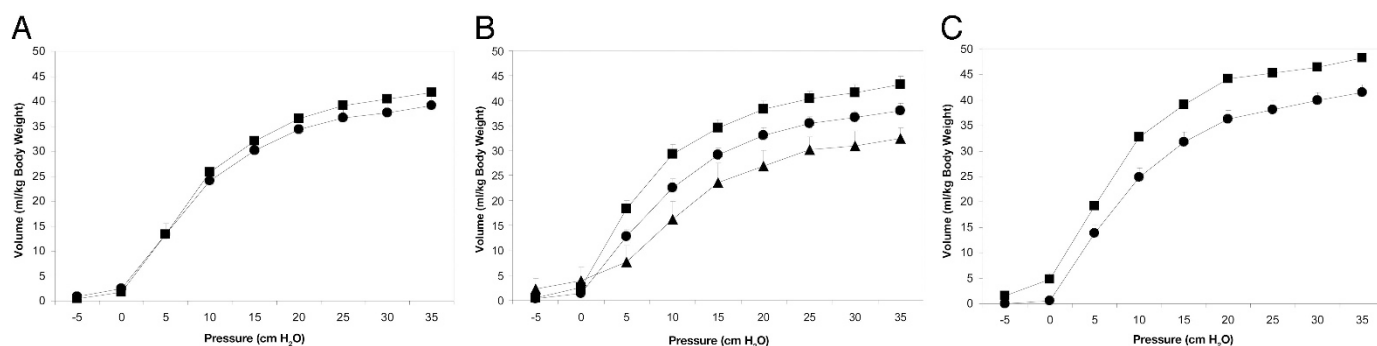


Figure 2. Deflation pressure/volume curves comparing Surfactant (circles) and Surfactant + PEG (squares) at doses of (A) 20 mg/kg, (B) 25 mg/kg, and (C) 50 mg/kg ($n = 6-7$ /treatment group). Triangles in B represent the means for the control (untreated) group ($n = 3$). Lung volumes are significantly improved with Surfactant + PEG at 25 ($p = 0.03$) and 50 mg/kg ($p = 0.001$) compared with those treated with Surfactant alone.

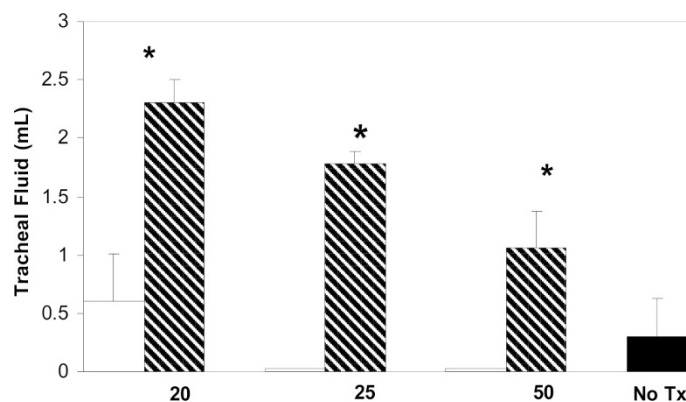


Figure 3. Aspirated tracheal fluid volumes are shown. Statistical significance ($p < 0.01$) denoted with an asterisk. Those treated with Surfactant + PEG had an increased amount of tracheal fluid at all three surfactant dosages compared with Surfactant alone. Open bars, Surfactant; hatched bars, Surfactant + PEG; solid bar, control (untreated) group.

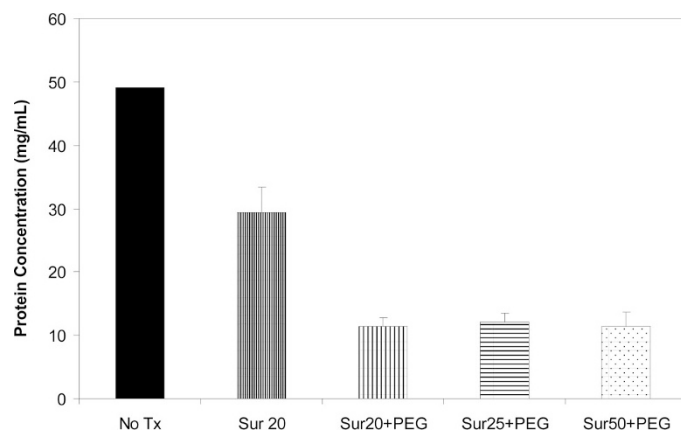


Figure 4. Protein concentrations of tracheal fluid are shown. Animals treated with Surfactant 20 mg/kg had higher protein concentrations than any PEG-treated group ($p < 0.01$). No difference was found among the Surfactant + PEG-treated groups. Animals in the Surfactant 25 and 50 mg/kg groups produced no tracheal fluid.

significantly greater in the injured Surfactant + PEG groups with or without furosemide when compared with the uninjured and untreated. The comparison between the injured group versus the noninjured group, both treated with PEG, was also significantly different (Fig. 5B). Average EVPE were not significantly different among the six groups.

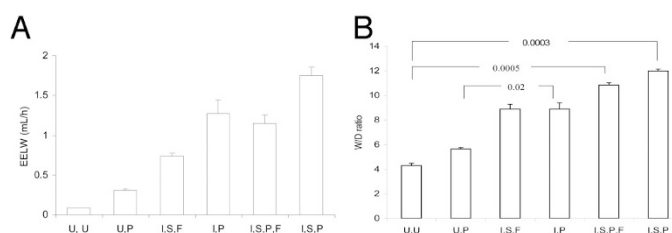


Figure 5. Data are from experiments specifically designed to study lung water ($n = 3$). (A) Excess extravascular lung water (EELW, mL/h) is significantly greater in the injured group treated with Surfactant + PEG and furosemide (I, S, P, F) vs the group treated with Surfactant and furosemide (I, S, F) ($p = 0.04$) or when the Surfactant + PEG group (I, S, P) is compared with Surfactant + PEG with furosemide (I, S, P, F) ($p = 0.01$). When comparing uninjured and untreated (U, U) animals with those that were uninjured and treated with PEG (U, P), $p = 0.005$. (B) Lung wet and dry weight ratios are shown. Wet/dry ratios are significantly greater in the injured Surfactant + PEG groups with or without furosemide (I, S, P, F or I, S, P) when compared with the uninjured and untreated (U, U). The comparison between the injured group vs the noninjured group, both treated with PEG (I, P vs U, P), was also significantly different.

Electron microscopy. Comparison of electron photomicrographs of Surfactant and Surfactant + PEG indicated more multilamellar structures were seen in the Surfactant/PEG mixtures. (Fig. 6). These changes imply that the vesicles coalesce into membranous structures in the presence of PEG.

DISCUSSION

The addition of PEG to Surfactant in this study improved quasistatic mechanical properties but not serial measures of gas exchange. Significant increases of lung volumes during performance of deflation pressure-volume curves were found with Surfactant + PEG groups at doses of 25 and 50 mg/kg. Several lines of evidence suggest increased alveolar fluid volume occurs when PEG is added to surfactant. Aspirated tracheal fluid volume increased with lower dosage of surfactant in the presence of PEG. In addition, extravascular lung water but not alveolar protein was increased in animals receiving Surfactant + PEG or PEG alone. In contrast to the results of Campbell *et al.* (23), we found no worsening of gas exchange in Surfactant + PEG-treated animals compared with animals treated with Surfactant.

Increased pulmonary fluid may be secondary to an osmotic effect of PEG reducing clearance of pulmonary edema. Also, epithelial injury in the face of continued accumulation of alveolar fluid may overwhelm the ability of the epithelium to

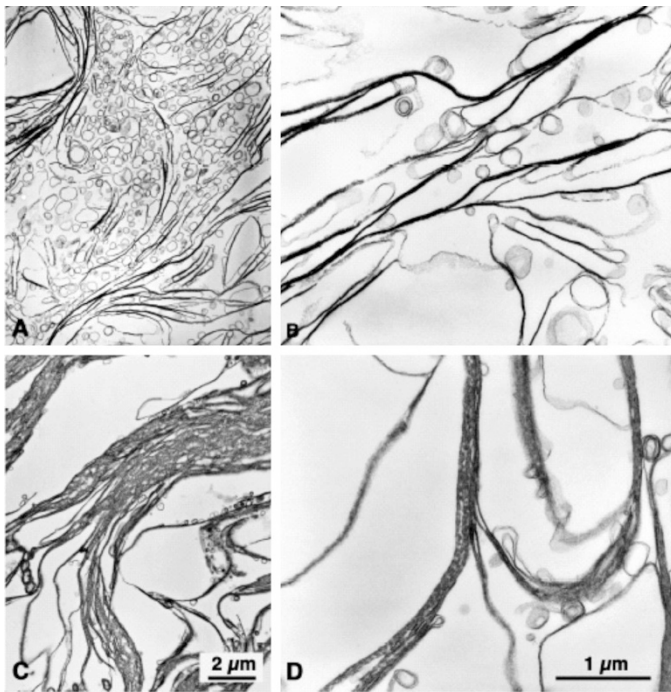


Figure 6. Transmission electron micrographs of Surfactant are shown. (A and B) Surfactant; (C and D) Surfactant + PEG. A and C are low magnification and B and D are high magnification. More membranous structures are seen after adding PEG to Surfactant.

transport fluid out of the alveoli (29,30). Interpolating from measurements reported by MacDonald (31), we estimate osmolarity of 5% PEG to be two to three times that of plasma colloid osmotic pressure. Therefore, depending on a variety of factors (PEEP, plasma oncotic and hydrostatic pressures, alveolar surface tension, degree of epithelial and endothelial damage, effectiveness of cellular clearance mechanisms for alveolar water, and amount of water bound to PEG), alveolar water could be increased by the presence of an osmotically active agent like PEG. All groups in this study had estimates of lung fluid at the end of the experiment in the range of 14–40% of total lung volumes (at pressures of 35 cm H₂O). This excess fluid burden, in an animal expected to develop additional alveolar fluid from this kind of lung injury itself, may prove too much for the animal to clear in the presence of PEG.

Our results differ to some degree from those of Campbell *et al.* (23). They found diminished serial measures of P_O₂ in rabbits treated with either 100 or 25 mg/kg Surfactant with PEG compared with Surfactant alone. Differences may be explained by use of different species, the degree of injury, and alterations in ventilator use. Our use in the initial studies of a hypoosmotic vehicle for diluting surfactant, a diuretic, relatively high PEEP, and regular tracheal suctioning may also have mitigated the buildup of pulmonary fluid with PEG, and hence explain the discrepancies in gas exchange seen between our study and that of Campbell *et al.* (23).

The rationale for adding PEG (or dextran) to surfactants is that PEG reduces inactivation of surfactant and enhances rates of surfactant transfer from bulk lipid to air liquid surfaces (15,32). Treatment of ALI with inactivation-resistant surfactants may im-

prove responses to therapy. However, if addition of PEG increases alveolar water, then positive effects may be attenuated. Good evidence indicates that alveolar fluid is increased in some patients with ARDS and that mechanisms for clearance of alveolar water are impaired, especially in those patients with poor outcomes (33). However, in prior work, we and others have found that addition of polymers to surfactant improves responses in different animal models of ALI, suggesting that they have positive, not detrimental, effects in these forms of ALI although detailed measurements of lung water were not carried out (16,18–20).

The osmotic effects of PEG and dextran may be, in part, responsible for their effects on surfactant function. Polymers cause dehydration of spaces between lipid vesicles setting up depletion forces that cause lipid aggregation as well as improved function of surfactants *in vitro* (15,31,32,34). Electron micrographs indicate that PEG is associated with a change in form of Surfactant, from vesicles to thickened membranous structures.

For surfactants improved by addition of PEG or other polymers (12,17,19,35) to be clinically useful, our data, coupled with the observations of Campbell *et al.* (23), indicate that careful matching of surfactant quality with the specific intraalveolar pathology may be necessary as implied by the work of Puligandla *et al.* (22). This approach may in time significantly improve surfactant therapy for ALI/ARDS. In summary, after measures were taken to reduce lung water, we find no evidence that PEG-Surfactant mixtures worsen pulmonary function after lavage-high tidal volume injury. In two of the three treatment groups, addition of PEG to Surfactant improved pressure-volume relationships. Nonetheless, lung lavage produces a form of ALI in which responses to surfactant plus polymer mixtures are less than with other experimental models of ALI, probably due to increases in lung water. Although evidence remains strong that addition of nonionic and ionic polymers can reduce inactivation of surfactant and improve lung function after some types of ALI, osmotic effects may constitute a risk with these additives. More study is needed to understand how polymers affect function of pulmonary surfactants *in vitro* and *in vivo*, and to identify polymer-surfactant mixtures that have positive, or, at least, negligible, effects on fluid balance in the lungs of animals with acute lung injury.

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