

# Investigation of Anatomical Thalamo-Cortical Connectivity and fMRI Activation in Schizophrenia

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The purpose of this study was to examine measures of anatomical connectivity between the thalamus and lateral prefrontal cortex (LPFC) in schizophrenia and to assess their functional implications. We measured thalamocortical connectivity with diffusion tensor imaging (DTI) and probabilistic tractography in 15 patients with schizophrenia and 22 age- and sex-matched controls. The relationship between thalamocortical connectivity and prefrontal cortical blood-oxygenation-level-dependent (BOLD) functional activity as well as behavioral performance during working memory was examined in a subsample of 9 patients and 18 controls. Compared with controls, schizophrenia patients showed reduced total connectivity of the thalamus to only one of six cortical regions, the LPFC. The size of the thalamic region with at least 25% of model fibers reaching the LPFC was also reduced in patients compared with controls. The total thalamocortical connectivity to the LPFC predicted working memory task performance and also correlated with LPFC BOLD activation. Notably, the correlation with BOLD activation was accentuated in patients as compared with controls in the ventral LPFC. These results suggest that thalamocortical connectivity to the LPFC is altered in schizophrenia with functional consequences on working memory processing in LPFC.

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## INTRODUCTION

The thalamus features prominently in major hypotheses about the neural circuitry implicated in schizophrenia (Andreasen *et al*, 1996), and evidence for its involvement derives from multiple fields of investigation but remains controversial (reviewed in Byne *et al*, 2009). Abnormalities in the medio-dorsal, pulvinar, and centromedian nuclei of the thalamus, all connected to the lateral prefrontal cortex (LPFC), a site of well-documented abnormalities in schizophrenia (Weinberger *et al*, 2001), have been reported with several methods (eg, Andrews *et al*, 2006; Byne *et al*, 2002; Byne *et al*, 2007; Harms *et al*, 2007; Hazlett *et al*, 1999; Kemether *et al*, 2003; Kessler *et al*, 2009; Kumari *et al*, 2010;

Lehrer *et al*, 2005; Popken *et al*, 2000; Rose *et al*, 2006, but see, for example, Danos *et al*, 2005; Dorph-Petersen *et al*, 2004; Kreczmanski *et al*, 2007 for negative findings). Some functional MRI (fMRI) studies found abnormalities in the correlation between the activity in the thalamus and the PFC in schizophrenia (eg, Meda *et al*, 2010; Schlosser *et al*, 2003; Welsh *et al*, 2010; Zhou *et al*, 2007), which may reflect alterations in anatomical connectivity. Thus, the changes in the coordinated functioning of the PFC and the thalamus might be relevant to the pathophysiology of schizophrenia.

Whether there is an abnormality in anatomical connectivity between the thalamus and the prefrontal cortex in schizophrenia is an important knowledge gap that might be addressed with the latest advances in probabilistic tractography via diffusion tensor imaging (DTI). This technique has allowed researchers to segment the thalamus in functionally relevant connectivity-defined regions (CDRs) based on their preferential connectivity to particular cortical areas (Behrens *et al*, 2003a, b; Johansen-Berg *et al*, 2005; Klein *et al*, 2010). Here, we used this methodology to test the following hypotheses: (1) that the degree of connectivity from the thalamus to the LPFC defined via probabilistic tractography is reduced in schizophrenia,

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(2) that thalamocortical connectivity would predict performance during a working memory task and (3) associated prefrontal blood-oxygenation-level-dependent (BOLD) activation during fMRI. Both working memory performance and prefrontal activation have been found to index cortical dysfunction and to be related to genetic risk for schizophrenia (Callicott *et al*, 2003a; Egan *et al*, 2001; Meyer-Lindenberg and Weinberger, 2006).

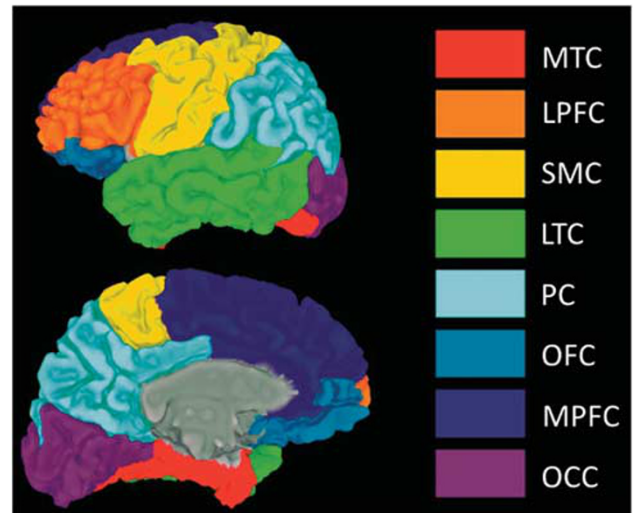
## PATIENTS AND METHODS

In all, 19 patients with schizophrenia and 26 healthy volunteers participated in the study. Participants were assessed as detailed in (Egan *et al*, 2001). Exclusions based on the history of other axis I disorders (including substance abuse), significant medical history, or excessive movement in the scanner (corrupting a substantial portion of the acquired images) resulted in the final group of 15 patients and 22 controls reported here. All participants had taken part in the Clinical Brain Disorders Branch 'Sibling Study' (NCT00001486). Five patients with schizophrenia were recruited as outpatients, whereas the rest were recruited from our inpatient ward (NCT00001247). No T2 hyperintensities were observed on the MRI scans of the participants. At the time of study, all patients were treated with second-generation antipsychotics and adjunctive medications.

DTI sessions were conducted using a GE 1.5T Signa scanner (GE, Milwaukee, WI) with an axial single shot echo planar imaging (EPI) sequence (TE 83.7 ms, 80 slices with isotropic voxel size  $2 \times 2 \times 2$  mm, NEX = 1,  $80 \times 110$  matrix, field of view: 22 cm) with cardiac gating of each individual slice (TR > 10 000 ms). In all, 107 volumes were acquired for each participant ( $b_{\max} = 1200$  s/mm<sup>2</sup>; see Supplementary Table S1), with 42 directions acquired with  $b$  values > 850 s/mm<sup>2</sup>. The directions of diffusion-weighted scans were distributed uniformly in space for each  $b$  value acquired. In order to assess the reproducibility of our measures, ten controls repeated one DTI session twice, with an average time between scans of  $61 \pm 32$  (SD) days.

In separate sessions, three-dimensional structural MRI and fMRI scans were acquired. A  $T_1$ -weighted spoiled gradient (SPGR) sequence (TR/TE = 2400/5 ms, flip angle = 45°, with 124 sagittal slices,  $256 \times 256$  matrix, FOV 24 cm,  $0.94 \times 0.94 \times 1.5$  mm<sup>3</sup> voxel size) at 1.5T (GE) was used for the structural acquisition whereas a 3T system (GE) was used for fMRI EPI acquisition with TR/TE = 2000/30 ms, flip angle = 90°, FOV 24 cm,  $64 \times 64$  matrix,  $3.75 \times 3.75 \times 6$  mm voxel size, 24 contiguous slices. The task paradigm used during fMRI was the 2-back working memory task (30 epochs of 0-back alternating with 2-back as previously described in Callicott *et al* (2003b)).

The Freesurfer software package (<http://surfer.nmr.mgh.harvard.edu>) was used to generate eight bilateral cortical (Figure 1) and one thalamic region of interest (ROIs) from the  $T_1$ -weighted structural images. ROIs were then transformed into DTI space for tractography. Affine registration (Jenkinson and Smith, 2001) using a normalized mutual information cost function with 12 degrees of freedom was used for each participant to derive transformation matrices from the non-diffusion-weighted image of the DTI series to



**Figure 1** Cortical ROIs in one healthy volunteer. The subdivisions of the cortex used in the analysis are shown for the left hemisphere in a lateral (top) and medial (bottom) view with a color bar for reference. Bilateral ROIs were used in the analysis, whereas unilateral ROIs are shown here for visualization. The following original Freesurfer parcellations (Desikan *et al*, 2006) were combined to form the larger ROIs used here: orbitofrontal cortex (OFC: pars orbitalis, medial orbitofrontal cortex, lateral orbitofrontal cortex), medial prefrontal cortex (MPFC: caudal anterior cingulate, rostral anterior cingulate, superior frontal gyrus), lateral prefrontal cortex (LPFC: pars triangularis, frontal pole, rostral middle frontal gyrus, pars opercularis), sensorimotor cortex (SMC: precentral gyrus, caudal middle frontal gyrus, post-central gyrus, paracentral lobule), parietal cortex (PC: inferior parietal cortex, supramarginal gyrus, precuneus cortex, posterior cingulate cortex, isthmus cingulate, superior parietal cortex), medial temporal cortex (MTC: entorhinal cortex, parahippocampal gyrus, fusiform gyrus), lateral temporal cortex (LTC: transverse temporal cortex, superior temporal gyrus, banks of the superior temporal sulcus, inferior temporal gyrus, middle temporal gyrus, temporal pole), and occipital cortex (OCC: pericalcarine cortex, lingual gyrus, lateral occipital cortex, cuneus cortex). Graphics were created using SUMA, part of the AFNI package (<http://afni.nimh.nih.gov/afni/suma>).

the structural  $T_1$ -weighted image. The inverse of those transformation matrices was then applied to convert the binary cortical ROIs to diffusion space with trilinear interpolation. Cortical ROIs in diffusion space were thresholded at 0.3, re-binarized, and corrected such that there were no overlapping voxels among regions. To ensure that no white matter voxels were included in the cortical ROIs, all voxels with fractional anisotropy > 0.2 were excluded from the cortical ROIs. Bilateral thalamic ROIs in diffusion space were thresholded at 0.6 and re-binarized. These thresholds were established after careful review of overlaid masks and registered  $T_1$  and non-diffusion-weighted images. We confirmed visually in each individual that the thalamic mask did not grossly exceed the borders of the thalamus after registration, while encompassing the entire  $T_1$ -weighted visible structure (the borders of the thalamus are not easily detectable in the non-diffusion-weighted image). For the cortex, a more liberal threshold for binarization was chosen to retain cortical voxels while preventing the extension of the mask into white matter.

All tools for DTI processing belonged to the FMRIB Diffusion Toolbox in the FMRIB Software Library (FSL 4.0; <http://www.fmrib.ox.ac.uk/fsl/>). The DTI series was first manually reviewed to eliminate artifacts. Volumes where

sudden motion had occurred (resulting in slices with low signal) were eliminated. We believe that the rejection of these volumes did not influence our results because all participants had at least seven volumes with  $b$  values  $< 10$  s/mm<sup>2</sup> and 42 directions with  $b > 850$  s/mm<sup>2</sup>. Images were corrected for distortion caused by eddy currents and head motion using an affine registration to the first non-diffusion-weighted volume (Jenkinson and Smith, 2001).

The brain was extracted and the diffusion parameters were estimated (Behrens *et al*, 2007), giving a probability distribution function of two fibers in each voxel of the brain. For each voxel in the thalamic mask, 5000 samples were sent through the connectivity distribution using probabilistic tractography. Probabilistic tractography was run bilaterally as pilot studies showed that reproducibility was somewhat improved over unilateral measures.

Total percent connectivity was calculated as the number of samples from any thalamic voxel reaching the corresponding cortical ROI divided by the total number of samples from all thalamic voxels reaching any cortical ROI. This is a measure of total tractography-defined connectivity from the thalamus to a particular cortical area, independent of where the tract originated from inside the thalamus.

When  $> 25\%$  of the total number of samples originating in a thalamic voxel reached a cortical ROI, that voxel was assigned to a CDR, considered to be connected to the homonymous cortical ROI. The total number of voxels belonging to a CDR divided by the total number of voxels in the thalamus of that individual was the outcome measure. This is a measure of the relative size of the thalamic CDR connected via tractography to a particular cortical area.

The two dependent variables for each cortical ROI were used as within effects in separate analyses of variance, where diagnostic group was the between effect. Two ROIs (medial temporal and orbito-frontal cortices) were dropped from this analysis due to poor reproducibility across two repeated scans of 10 normal controls (Supplementary Methods *a*). In these analyses, main effects of the region were of no interest, and will not be reported further, although we focused on main effects of diagnosis or ROI-*by*-diagnosis interactions. If the latter was significant, *post-hoc* *t*-tests were run for each ROI. These were not corrected for multiple comparisons as the overall significance protects from type I error. The effect of possible confounding variables on LPFC percent total connections was assessed as detailed in the Supplementary Methods *b*. All statistics of this kind were run with Statistica release 7 (StatSoft, Tulsa, OK).

fMRI was analyzed for a subset of 27 individuals (18 healthy subjects and 9 patients with schizophrenia: Supplementary Methods *c*, Table S3) during an n-back working memory task. All fMRI data were preprocessed and analyzed with SPM5 software (<http://www.fil.ion.ucl.ac.uk/spm>). All fMRI data sets met the criteria for quality control as described previously (Callicott *et al*, 2003b). All fMRI data were pre-processed and spatially normalized to the common stereotactic space provided by the Montreal Neurologic Institute (MNI) and analyzed using a general linear model. For each experimental condition, a box car model convolved with the hemodynamic response function at each voxel was modeled. Linear contrasts were computed producing voxel-wise *t*-statistical parameter maps for

2-back relative to 0-back and entered into second-level analyses.

Two second-level multiple regression models were tested on the contrast images (2-back–0-back), with the subject as a random factor: one to detect voxels with a significant relationship to LPFC connectivity where both groups were assumed to have equal slopes; the other to detect voxels with significantly different slopes between the diagnostic groups. The first model had LPFC connectivity, diagnosis, age, sex, and 2-back performance as covariates. The second model was constructed including the following predictors: two diagnostic group predictors, two LPFC connectivity predictors (one per diagnostic group), age, sex, and n-back accuracy. The contrast between the two LPFC connectivity vectors (adjusted by group means, age, sex, and n-back performance within each group) was then used to assess group differences in the slope of the regression.

Levels of significance to detect associations between LPFC connectivity and BOLD activation were set at  $p = 0.005$  uncorrected for multiple comparisons. Results are reported in a ROI constructed by normalizing to the MNI template and then averaging the bilateral LPFC ROIs used as tractography targets. The resulting image was smoothed with a  $3 \times 3 \times 3$  mm FWHM filter mimicking the fMRI resolution and then thresholded at a value of 0.4 for binarization. Corrections for multiple comparisons were performed at the cluster extent level, using the cluster size threshold computed via AlphaSim, a function available in AFNI (<http://afni.nimh.nih.gov/>). This program was run for each individual with 1000 iterations, within the ROI described above, and a cluster connectivity radius of 3.1 mm. AlphaSim estimated the rate of false positive voxels within a cluster that are expected given a threshold of  $p < 0.005$  uncorrected. For a specific  $\alpha$ , any cluster size larger than this number can be considered statistically significant after correction for multiple comparisons. For any group analysis, the critical cluster size is calculated averaging this measure across all individuals. In our analysis, for  $\alpha = 0.05$  the average cluster extent threshold was 621  $\mu$ l (23 voxels).

The relationship between LPFC total percent connectivity and number of correct responses on the 2-back was assessed with Pearson's *r*.

## RESULTS

The patients ( $n = 15$ ) and controls ( $n = 22$ ) did not significantly differ in age, sex, or handedness (Table 1). Overall quality of the tractography results was assessed in several ways, as detailed in the Supplementary Results (Figures S1, S2, S3, S4), and appeared to be consistent with known anatomy.

A significant diagnosis-*by*-ROI interaction was found for percent total connectivity ( $F_{5,175} = 22.4$ ,  $p = 0.03$ ) and for CDR size ( $F_{5,175} = 2.38$ ,  $p = 0.04$ ; Figures 2 and 3, and Supplementary Table S4). Patients with schizophrenia had on average lower thalamocortical connectivity and CDR size than controls in the LPFC, whereas they had elevated total connectivity to the somato-motor cortex.

There was no correlation of measures of connectivity with age, years of education or Wide Range Achievement Test in



**Table 1** Subject Characteristics

	Patients with schizophrenia (n = 15)	Healthy volunteers (n = 22)	Statistical test
Age, years (mean ± SD)	30.6 ± 12.5	34.1 ± 12.0	$t_{35} = -0.85$ , $p = 0.40$
Gender	11 M, 4 F	17 M, 5 F	$\chi^2 = 0.08$ , $p = 0.78$
Handedness <sup>a</sup>	12 R, 2 L	18 R, 4 L	$\chi^2 = 0.0935$ , $p = 0.76$
Family SES <sup>a</sup>	46.5 ± 14	52 ± 11.1	$t_{34} = -1.32$ , $p = 0.2$
<i>Cognitive measures</i>			
Years of education	13.5 ± 1.9	15.5 ± 1.9	$t_{35} = -3.10$ , $p < 0.01$
WRAT reading score	98.9 ± 14.9	109.4 ± 9.29	$t_{35} = -2.63$ , $p = 0.01$
<i>Clinical measures</i>			
Age of onset, years	19.0 ± 3.0		
Duration of illness (years) <sup>b</sup>	14.1 ± 12.0		
Chlorpromazine equiv <sup>c,a</sup>	595.8 ± 491.1		
PANSS positive factor <sup>d</sup>	12.9 ± 4.0		
PANSS negative factor <sup>d</sup>	15.4 ± 4.0		
PANSS cognitive factor <sup>d</sup>	14.1 ± 3.5		
PANSS excitement factor <sup>d</sup>	9.0 ± 1.8		
PANSS depression factor <sup>d</sup>	9.0 ± 3.1		

Abbreviations: F, female; L, left-handed; M, male; PANSS, Positive and Negative Syndrome Scale; R, right-handed; WRAT, Wide Range Achievement Test.

<sup>a</sup>Data missing for one patient. SES based on Hollingshead (1975).

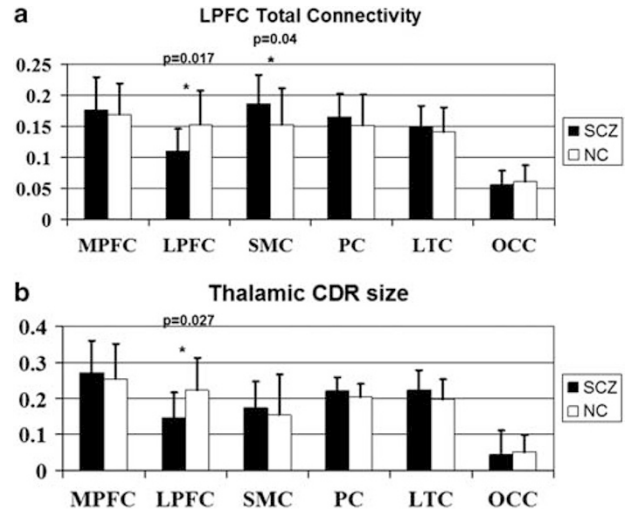
<sup>b</sup>Based on the age at first hospitalization.

<sup>c</sup>Calculated using Woods (2003).

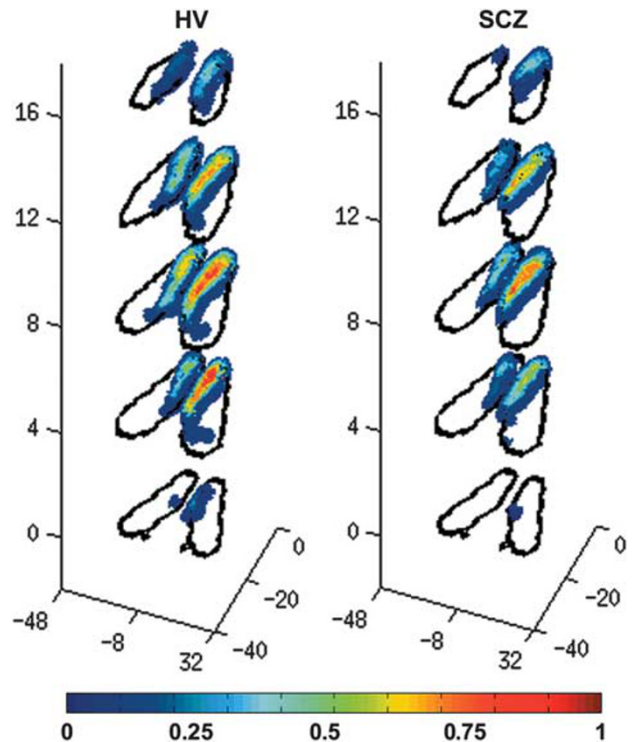
<sup>d</sup>Patients' symptoms were rated with the PANSS by an experienced nurse or a psychiatrist and were summarized in five factor scores (Lindenmayer et al, 1995).

the whole group, or with chlorpromazine equivalents and duration of illness in the patient group. There were no significant differences between groups in total thalamic or frontal cortical volumes (Supplementary Table S5: this was true both for absolute volumetric measures and for those normalized to intra-cranial volume), or in the average tract properties connecting the thalamic CDR and the LPFC (Supplementary Table S6).

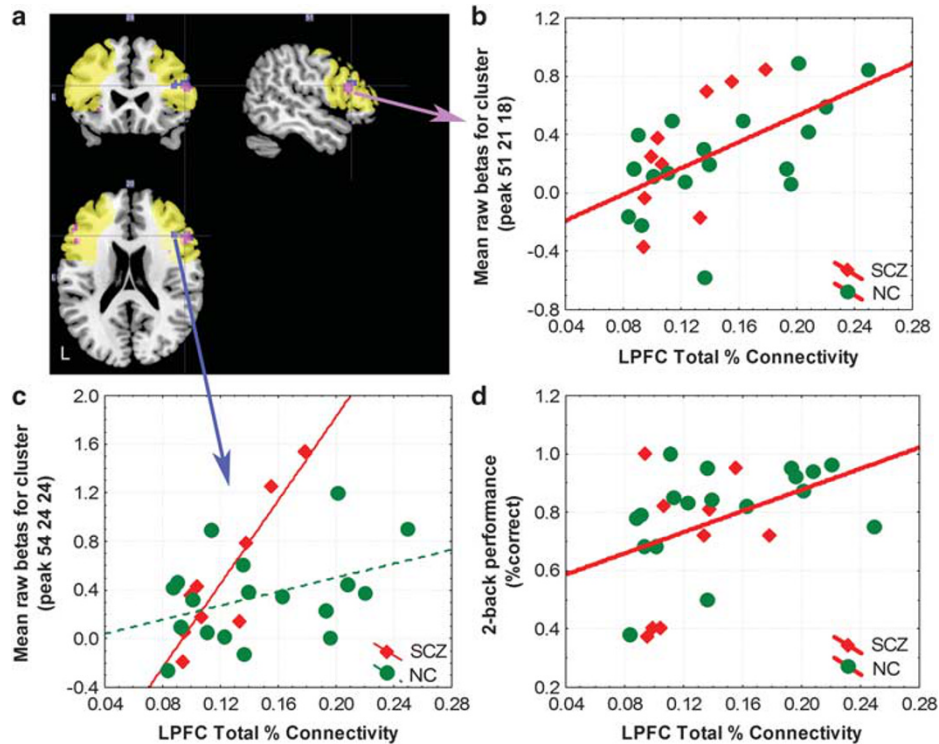
In the fMRI study of working memory, patients and controls had similar performance in terms of accuracy and reaction time ( $p > 0.15$ ) and performance was used as a covariate in the analysis. Thalamic LPFC percent total connectivity correlated with cortical activation in the LPFC bilaterally (Figure 4a, maximum effect:  $r^2 = 0.33$ ,  $p = 0.0017$  uncorrected, cluster size 648  $\mu\text{l}$ ) for the model with equal slopes across groups, although patients with schizophrenia had steeper slopes than controls in the right ventral LPFC (Figure 4b,  $p = 0.0007$  uncorrected, cluster size 648  $\mu\text{l}$ ). Both relationships occurred in clusters larger than 621  $\mu\text{l}$ , thus corrected for multiple comparisons. LPFC total percent connectivity was significantly correlated with 2-back performance in the whole group (Figure 4c,  $r^2 = 0.19$ ,  $p = 0.02$ ).



**Figure 2** Results for total percent connectivity and CDR size. (a) Total percent connectivity for the six cortical ROIs included in the analysis. (b) Thalamic CDR size for the six regions included in the analysis.  $P$  values represent *post-hoc* unpaired  $t$ -tests.  $*P < 0.05$  on the *post-hoc* tests. Error bars represent SD. LTC, lateral temporal cortex; LPFC, lateral PFC; MPFC, medial prefrontal cortex; OCC, occipital cortex; PC, parietal cortex; SMC, somato-motor cortex.



**Figure 3** Comparison of the spatial consistency of LPFC thalamic CDRs between patients with schizophrenia and controls. Binary masks of the thalamic CDRs for the healthy volunteers ( $n = 22$ ) and patients with schizophrenia ( $n = 15$ ) were normalized to a standard template (Wake Forest University PickAtlas: <http://fmri.wfubmc.edu/cms/softwarePickAtlas>), averaged, and thresholded to show only those voxels with  $> 10\%$  of the subjects represented at that location. The black border outlines five slices of the thalamus, oriented from top to bottom, with the axes showing the mm coordinates in standard MNI space. Warmer colors illustrate a higher spatial consistency across subjects, with dark red representing 100% of subjects present at a particular location. Graphics were created using Matlab (Mathworks, Natick, MA).



**Figure 4** Correlation of prefrontal BOLD activation and LPFC total percent connectivity. (a) The significant clusters are shown superimposed on the MNI single subject template. The yellow area represents the region of interest used to constrain the analysis, the pink area corresponds to the cluster (maximum at voxel coordinates 51 21 18) where both groups had similar positive slopes for the correlation between LPFC total percent connectivity and BOLD, whereas the blue area corresponds to the cluster (maximum at voxel 54 24 24) where slopes differed significantly across groups. (b) Correlation between LPFC total percent connectivity and BOLD parameter estimates for the cluster with the peak at voxel 51 21 18 (raw  $\beta$  values adjusted for the session mean of the individual subject,  $n = 27$ ,  $r = 0.56$ ,  $p = 0.0027$ ,  $z$  for peak voxel = 3.33). The cluster surrounding the peak of significance encompassed 24 voxels ( $648 \mu\text{l}$ ). This exceeded the threshold of 23 voxels ( $621 \mu\text{l}$ ) found by AlphaSim and can therefore be considered corrected for multiple comparisons. (c) Significant difference in the correlation between LPFC connectivity and BOLD activation in the cluster surrounding voxel 54 24 24 (raw  $\beta$  values adjusted for the session mean, normal controls (NC):  $n = 18$ ,  $r = 0.4$ , patients with schizophrenia (SCZ):  $n = 9$ ,  $r = 0.9$ , 24 voxel extent or  $648 \mu\text{l}$ ,  $z$  for peak voxel = 3.38,  $p = 0.0007$ , uncorrected). (d) Correlation between LPFC connectivity and performance on the 2-back working memory task ( $r = 0.43$ ,  $p = 0.02$ ) for the whole group. Correlation coefficients for patients and controls did not differ from each other (SCZ = 0.38, NOR = 0.44, Fischer's transformation:  $z = -0.15$ ,  $p = 0.88$ ).

Given these results, we also investigated the relationship between percent total connectivity from the thalamus to two other cortical masks where significant BOLD activation occurs during the n-back task: parietal and medial prefrontal cortices (Supplementary Methods *d*, Supplementary Results, and Supplementary Figures S5 and S6).

## DISCUSSION

Based on suggestive but controversial findings from post-mortem studies and on data acquired with structural and functional neuroimaging, we had hypothesized that measures indexing thalamocortical connectivity to the LPFC would be reduced in patients with schizophrenia as compared with normal controls. Probabilistic tractography data obtained *in vivo* support the central hypothesis of this study. The measures derived with this method were highly reproducible in two repeated scans of a subset of the control subjects ( $\text{ICC} > 0.82$ ); the effect size of the differences between diagnostic groups appeared robust (Cohen's  $d \sim 0.8$ ), and unlikely to be due to several possible confounding factors (eg, age and chlorpromazine

equivalents). Our data offer a possible anatomical substrate for differences in functional connectivity between patients with schizophrenia and controls previously described with fMRI (Meda *et al*, 2010; Schlosser *et al*, 2003; Welsh *et al*, 2010; Zhou *et al*, 2007) and are consistent with a reduction in connectivity from multiple sources in the thalamus to the LPFC. Besides three studies showing that neurons specifically projecting to LPFC in the medio-dorsal nucleus of the thalamus may be reduced in schizophrenia (Byne *et al*, 2002; Popken *et al*, 2000; Young *et al*, 2000), reduced sizes of the pulvinar, of the centromedian nuclei (both projecting in part to the LPFC; Byne *et al*, 2007; Kemether *et al*, 2003) and reductions in oligodendrocyte number in the anterior principal nucleus (Byne *et al*, 2006, 2008) were found in schizophrenia. An unexpected increase in total connectivity from the thalamus to the sensorimotor cortices was found, but it is difficult to interpret this in the absence of a prior hypothesis. One possibility is that this is an artifact of the relative measures used here to assess thalamic connectivity: a decrease in connectivity to the LPFC necessarily has to correspond to a decrease somewhere else, however, it is unclear why this would be more prominent in the sensorimotor cortices rather than distributed in a more diffuse fashion.

It should be stressed that the reproducibility over repeated DTI sessions of the thalamo-LPFC connectivity measures reported here was satisfactory, with ICCs  $>0.69$ , a result consistent with another recent investigation where spatial reproducibility of this method was studied in detail (Traynor *et al*, 2010). The poor reproducibility in the OFC and MTC (Supplementary Table S2) were most likely due to EPI distortions for the orbitofrontal regions and the presence of complex fiber architecture on the pathway from the thalamus to the medial temporal cortex that is not fully accounted for by the current probabilistic connectivity models.

This is not the first study pointing to altered diffusion parameters in the thalamus or thalamocortical pathways. DTI findings supporting altered integrity of thalamocortical connectivity in schizophrenia include controversial alterations of fractional anisotropy in the anterior limb of the internal capsule (ALIC) (Buchsbaum *et al*, 2006; Kubicki *et al*, 2005; Mamah *et al*, 2010; Sprooten *et al*, 2009; Sussmann *et al*, 2009; Zhang *et al*, 2010; Zhou *et al*, 2008, but see Ashtari *et al*, 2007; Kito *et al*, 2009; Kyriakopoulos *et al*, 2008; Szeszko *et al*, 2005; White *et al*, 2007 for negative findings in younger individuals and Beasley *et al*, 2009 for lack of evidence of myelin abnormalities post-mortem), of the tracts connecting to the LPFC (Kim *et al*, 2008; Oh *et al*, 2009) and altered FA (Hashimoto *et al*, 2009) or mean diffusivity in the thalamus itself (Agarwal *et al*, 2008; Rose *et al*, 2006; Spoletini *et al*, 2011).

Kim *et al* (2007) have performed a similar DTI study, with an identical *a-priori* hypothesis, but found only differences in the thalamic CDR defined by connectivity to the orbitofrontal, parietal, and medial prefrontal cortices. No measure of reproducibility was reported in that paper and several methodological issues might have prevented those authors from finding similar results to ours: the more limited number of directions used, maximal  $b$  values of  $600 \text{ mm}^2/\text{s}$  (which will limit the accuracy of the determination of the direction of diffusion), the use of a larger definition for the LPFC ROI that included cortical structures not necessarily altered in schizophrenia, and the use of a processing software limited to modeling one fiber per voxel.

It is possible that these alterations in thalamocortical connectivity were due to alterations in diffusion properties in the tract connecting the thalamus to the LPFC, as detailed above. In this small sample, we could not detect a difference in the average FA or mean diffusivity for the tract connecting the thalamus to the LPFC (Supplementary Table S6), however, more subtle local differences in diffusion properties may exist along the tract that were not detected in the analysis of average values (Oh *et al*, 2009).

Although the weight of the evidence points towards a reduction in thalamic volume in schizophrenia (for meta-analyses see Adriano *et al*, 2011; Konick and Friedman, 2001, and for a recent large study see Rimol *et al*, 2010), it is possible that we did not detect significant differences in thalamic or cortical volumes because of limited power due to the sample size. Our findings, however, are consistent with those collected in a much larger cohort of patients and controls acquired and processed with identical methodology (Goldman *et al*, 2008). These negative findings are of interest because they make it more likely that the main results of this study are primary and not secondary to

volumetric changes or generic alterations in white matter integrity in the whole thalamus or in the ALIC and anterior thalamic radiations mentioned above. At the very least, though, in this small sample tractography-derived measures were more sensitive than volumetric measures in detecting anatomical differences in schizophrenia.

Using a multimodal approach, we also investigated whether the observed thalamic connectivity measures were biologically relevant for the activity of the LPFC during the performance of working memory. Indeed, percent total connectivity to the LPFC predicted both the degree of BOLD activation during working memory and n-back performance. This phenomenon was present especially in the ventral portions of the LPFC bilaterally and was significantly greater in patients as compared with controls in the right ventral LPFC. Further *post-hoc* analyses revealed that the latter finding was also true in the MPFC, whereas in the parietal cortex patients showed a significantly more negative slope for the correlation as compared with controls. We speculate that during development subtle alterations in the distribution of thalamo-cortical pathways to their cortical targets, not necessarily manifest in anisotropy alterations, contribute to changes in the compartmentalization of dorsal and ventrolateral PFC function and to excessive VLPFC activation in schizophrenia (Tan *et al*, 2006). These changes may be compensatory in nature given the positive relationship to performance in both patients and controls. Moreover, also parietal and medial prefrontal nodes of the working memory network may be affected, although less severely.

From our data, it is impossible to say whether the thalamic abnormality in patients is a cause of, a consequence of, or a simultaneous occurrence with the LPFC abnormality. However, the fact that thalamocortical tracts form early in development suggests that this abnormality could already be present at birth or in the first years of life and would be consistent with the neurodevelopmental nature of schizophrenia. Indeed, there is evidence for altered interstitial prefrontal neurons, considered remnants of the subplate (Kostovic *et al*, 2011), in schizophrenia (Akbarian *et al*, 1993; Anderson *et al*, 1996; Eastwood and Harrison, 2003, 2005; Kirkpatrick *et al*, 2003; Yang *et al*, 2011), supporting an early pathological process. Furthermore, as the PFC completes maturation well after the thalamocortical fibers have reached the subplate (Kostovic and Judas, 2010), it is conceivable that thalamic neuronal activity might be a potential effector of PFC maturation and developing function via its connectivity (Kanold, 2009). An early presence of the abnormalities reported here is also supported by the lack of a correlation between CDR size and total percent connectivity with illness duration and other possible confounding variables such as age and chlorpromazine equivalents, although only studies in first-episode patients will be able to confirm this hypothesis.

This structure–function relationship supports the biological importance of our DTI findings when comparing patients and controls. We have linked DTI-derived measures of probabilistic connectivity with cortical physiology measured with fMRI and working memory performance, which is critically affected in the developmental pathophysiology of schizophrenia. Others have shown a relationship of FA and working memory performance in patients with



schizophrenia (eg, Karlsgodt *et al*, 2008; Lim *et al*, 2006), and recent papers found correlations between working memory performance and anisotropy of the ALIC (Mamah *et al*, 2010) and of the left thalamus (Qiu *et al*, 2009) in schizophrenia, and mean diffusivity of the medial thalamus in healthy aging subjects (Charlton *et al*, 2010). Our findings also indicate that bulk thalamocortical connectivity is relevant to neurocognitive processes such as working memory.

Limitations of this study are the small number of subjects, inability to control for medication effects, and the fact that diagnostic groups were not well matched for years of education or premorbid IQ (although they did not differ in terms of parental socio-economic status, see Table 1), although this is commonly observed in naturalistic studies of schizophrenia. As the fMRI portion of the study was retrospective in nature, the demographics were not entirely representative of the full group, as in the case of sex distribution. Another limitation, especially in light of a recent report (Zhang *et al*, 2010) showing additive effects of smoking and schizophrenia on the FA of the ALIC, is the fact that 45% of our patients were current smokers compared with only one of our controls (5%); however, this discrepancy was less marked when any history of smoking was taken into account (41% of controls *vs* 60% of patients). It should be noted, though that no group effect of FA was found in the ALIC in the current investigation. Finally, distortions of the diffusion-weighted images were not fully corrected by our post-processing scheme and this might have affected accurate registration with the T1-weighted images. We are currently working on replicating these findings with a more rigorous post-processing scheme.

In conclusion, we have shown that putative measures of thalamocortical connectivity to LPFC were reduced in patients with schizophrenia and that there are functional implications of this reduction indicating the potential utility of DTI tractography measures in understanding white matter pathophysiology in schizophrenia.

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## DISCLOSURE

The authors declare no conflict of interest.

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